

A MULTI-PROCESSOR SYSTEM FOR THE

DETECTION OF

ELECTROCARDIOGRAM ARRHYTHMIAS

BRYAN THOMAS VICTOR WARTON

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The University of Aston in Birmingham.
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B.T.V. WARTON

S U M M A R Y

This thesis describes the research work performed to produce a real-time distributed microprocessor system, for the diagnosis of cardiac arrhythmias. The distributed microprocessor approach developed, allowed the allocation of a microprocessor to each patient for the purpose of electrocardiogram analysis. The functions performed by these patient-dedicated processors include digital filtering of the electrocardiogram, the detection and measurement of each heart beat complex, and the diagnosis of arrhythmias by decision tables.

These patient processors then communicate the required patient analysis results and diagnoses, to a centralised operator-dedicated processor. This operator-dedicated processor allows the functions of overall system control, display and storage to be centralised.

INDEXING TERMS : Multi-microprocessor, Electrocardiogram,
Arrhythmia, Real-Time.

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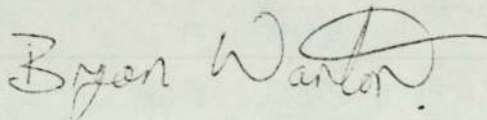
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Many thanks,

A handwritten signature in cursive script that reads "Bryan Warton". The signature is written in dark ink and is positioned above the printed name.

Bryan Warton.

CONTENTS

<u>CHAPTER</u>	<u>TITLE</u>	<u>PAGE</u>
1.	INTRODUCTION	1
1.1.	General	1
1.2.	Electrocardiography and Arrhythmia Criteria	2
1.3.	Monitoring Systems	3
1.4.	System Functions and Structure	3
1.5.	Patient-dedicated Processor System Design	3
1.6.	Operator-dedicated Processor System Design	4
1.7.	System Hardware	4
1.8.	System Performance and Results	4
2.	ELECTROCARDIOGRAPHY AND ARRHYTHMIA CRITERIA	6
2.1.	The Electrocardiogram	6
2.2.	Arrhythmia Criteria	8
2.2.1.	Initial Monitoring Criteria	8
2.2.2.	Alternative Monitoring Criteria	11
3.	MONITORING SYSTEMS	22
4.	SYSTEM FUNCTIONS AND STRUCTURE	26
4.1.	Introduction	26
4.2.	System Functions	26
4.2.1.	Signal Acquisition	26
4.2.2.	Signal Conditioning	26
4.2.3.	Signal Monitoring	27
4.2.4.	Diagnosis	28
4.2.5.	Display	28
4.2.6.	Storage	29
4.2.7.	Communication and Control	29
4.3.	The Ideal System Function Structure	30
4.4.	Performance of Functions in Real-Time	32
4.5.	Distributed Processor System Structure	35
4.6.	Conclusions	35

<u>CHAPTER</u>	<u>TITLE</u>	<u>PAGE</u>
5.	PATIENT-DEDICATED PROCESSOR SYSTEM DESIGN	37
5.1.	Introduction	37
5.2.	Signal Conditioning	37
5.3.	Signal Monitoring	52
5.3.1.	R-R Interval Measurement	58
5.3.2.	QRS Complex Width Measurement	59
5.3.3.	Wide QRS Percentage Calculation	62
5.3.4.	R-R Interval Classification	63
5.3.5.	Sequence Pattern Recognition	64
5.3.6.	Monitoring Function Output	67
5.3.7.	Alternative Monitoring Criteria	67
5.4.	Diagnosis Function	72
5.5.	Communications	80
5.5.1.	Input Task	81
5.5.2.	Microprocessor Communication Package	81
5.5.3.	Output Task	83
5.6.	Control	85
6.	OPERATOR-DEDICATED PROCESSOR SYSTEM DESIGN	91
6.1.	Introduction	91
6.2.	Inter-processor Communication Protocol	91
6.3.	Communications Function	99
6.3.1.	Input Task	99
6.3.2.	Output Task	103
6.3.3.	Microprocessor/Operator Communications Package	105
6.4.	Display	106
6.5.	Storage	114
6.6.	Control	115
6.6.1.	UART Interrupt Handler Program	115
6.6.2.	I/O Queue Handler Program	119
7.	SYSTEM HARDWARE	122
7.1.	General	122
7.2.	ADC Interface	124
7.3.	Inter-processor Communication Interface	125

<u>CHAPTER</u>	<u>TITLE</u>	<u>PAGE</u>
8.	SYSTEM PERFORMANCE	130
8.1.	Patient Processor Performance in Real-time	130
8.2.	Inter-processor Communication Performance	131
9.	CONCLUSIONS	145
9.1.	General	145
9.2.	Suggestions for Future Development	147
9.3.	Final Remarks	148
 <u>APPENDICES</u>		
A	The TMS 9900 Microprocessor	150
B	Patient Processor Program Listing	155
C	Alternative Patient Processor Program Listing	245
D	Operator/Nurse Processor Program Listing	267
E	PUBLISHED WORK.	338
 <u>REFERENCES</u>		348

CHAPTER 1

INTRODUCTION

1.1. General

In the early 1960s, Coronary Care Units (CCUs) were introduced into hospitals to provide centralised facilities for monitoring cardiac patients. The initial motivation for these units was the need for rapid detection and treatment of life-threatening events, such as cardiac arrest and ventricular fibrillation (disorganised heart activity).

The method used to monitor the cardiac condition of patients in CCUs, is via the amplification of the small potential differences associated with heart action, which occur on the surface of the chest. These electrical signals from the heart are referred to as electrocardiograms (ECGs).

Since the introduction of CCUs, continuous ECG monitoring in these units has shown that a high incidence of certain cardiac arrhythmias (abnormal changes in heart rate) precede life-threatening events. The treatment of these arrhythmias with antiarrhythmic agents, proved to be successful in reducing the number of mortalities in CCUs.

Conventional ECG monitoring in CCUs is based upon heart rate meter alarms, and nurse observation of oscilloscope displaying ECG signals. Despite the relatively good results achieved with this type of monitoring, it was quite clear that a great deal of information was lost.

A study made comparing the results obtained from conventional ECG monitoring, and subsequent detailed analysis of the recorded ECGs made at the same time, showed that less than 20% of the serious arrhythmias had been detected (Ref. 1.).

In an effort to relieve the nursing staff of continuous visual ECG monitoring and also to provide more detailed arrhythmia monitoring results, various computer monitoring systems have been developed. The high cost of these computer monitoring systems, however, has precluded their widespread use in CCUs.

The advent of the microprocessor has now provided the possibility of producing a cheaper and more flexible monitoring system, not only by a direct reduction in the cost of information processing, but also by the possibility of distributing this processing throughout the system.

This report describes the development of such a distributed microprocessor monitoring system, which uses a 16 bit microprocessor, the TMS 9900, for real-time detection and diagnosis of ECG arrhythmias (Appendix E Published Work).

1.2. Electrocardiography and Arrhythmia Criteria

The various deflections which occur in the ECG signal indicate the operation of the heart. The diagnosis of arrhythmias from such signals is concerned with changes in the shape and frequency of these deflections.

The interpretation of the deflections in the ECG signal, and the monitoring diagnosis criteria used by the

microprocessor system are described in Chapter 2. This Chapter also discusses the limitations and problems encountered with the initial monitoring criteria used, and suggests a possible set of alternative monitoring criteria.

1.3. Monitoring Systems

There are a large number of independent research and development groups producing different types of ECG monitoring systems. The different approaches used by these systems are briefly indicated in Chapter 3, and hence the reasons for the methods chosen for implementation in the microprocessor monitoring system are given.

1.4. System Functions and Structure

Having indicated the approach for implementation in the microprocessor system, Chapter 4 describes the individual functions performed by the monitoring system, and the ideal distribution of each function throughout the system. The performance of these functions in real-time, as obtained by actual implementations, are then examined in order to show that the ideal function distribution in the system can be implemented by the allocation of microprocessors on a one-per-patient basis. The overall system control is provided by a central operator-dedicated microprocessor.

1.5. Patient-dedicated Processor System Design

Those functions assigned to the patient-dedicated processor system are all implemented in the compact media

of software, as described in detail in Chapter 5. This Chapter also describes how these real-time functions are controlled by the patient processor operating system developed, which contains a real-time task scheduler.

1.6. Operator-dedicated Processor System Design

Those functions assigned to the operator-dedicated processor system, and produced in software, are described in detail in Chapter 6. This Chapter also describes the inter-processor communications protocol that was developed for the system, which allows communications between processors to operate without interfering with the real-time processing being performed by each patient-dedicated processor.

1.7. System Hardware

As the system functions produced for the developmental system are all in the compact media of software, the resulting system hardware is predominantly the basic microprocessor system circuit elements. The design of microprocessor hardware systems is described in detail in the TMS 9900 microprocessor support literature; therefore, only the basic structure of the hardware system is described in Chapter 7. This Chapter then proceeds to discuss in more detail, the analog to digital converter, and inter-processor communications interfaces used in the developmental system.

1.8. System Performance and Results

As a result of producing the developmental system,

it was possible to determine the real-time performance of the patient processor software, and hence the possibilities for expansion within the system, as discussed in Chapter 8.

Also examined in this chapter are the inter-processor communications performance results, obtained from studying a simulated three patient processor monitoring system. The results obtained indicate the effect of the current inter-processor communication performance, on the total number of patient processors which could be connected to the monitoring system.

CHAPTER 2

ELECTROCARDIOGRAPHY AND ARRHYTHMIA CRITERIA

2.1. The Electrocardiogram

The heart is the complex organ which pumps blood around the body. During the pumping action there is electrical activity within the heart, which can be detected by chest and limb lead electrodes (Ref. 2.). In all, there are 12 different lead arrangements used in clinical electrocardiogram diagnostic practice (Ref. 3.).

In order to observe the changing condition of patients in CCUs, one of the chest leads is continuously monitored. The type of signal obtained from a chest lead position, used in CCUs, is illustrated in Fig. 2.1. The P wave shown in Fig 2.1, corresponds to the contraction of the atrium (the two chambers which receive blood in the heart), and the QRS complex corresponds to the contraction of the ventricles (the two chambers which force the blood out of the heart).

The diagnosis of cardiac arrhythmias from such a signal is concerned with abnormal changes in the heart rhythm (Ref. 4.). When diagnosing the type of arrhythmia that has occurred, not only is the time interval between each beat (R-R interval) of importance, but also the shape of the QRS complex, and possibly its relationship to P and T waves, must be considered. This

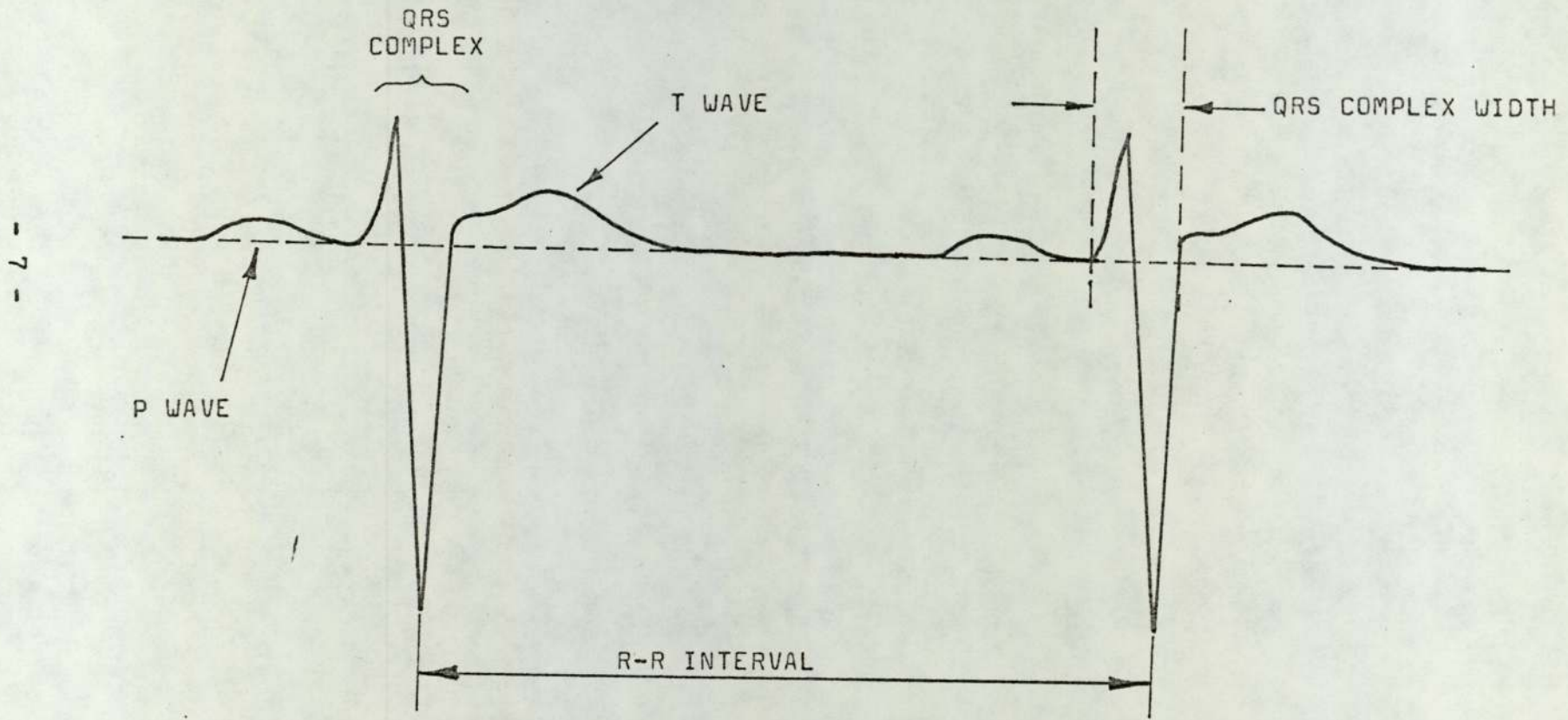


Fig 2.1. ECG CHARACTERISTICS

is because abnormal contractions of the heart can produce abnormal QRS complexes, and changes in heart rhythm.

2.2. Arrhythmia Criteria

The arrhythmia diagnosis approach adopted for the microprocessor monitoring system as discussed in Chapter 3, is that of pattern recognition. The diagnosis criteria used by real-time computer monitoring systems employing such an approach varies with each computer system as there is no agreed standard. As the criteria needed for the microprocessor system was initially required to enable the final structure of the system to be determined, it was decided that an existing set of criteria would be implemented. The requirements placed upon the criteria sought, ~~was~~^{were} that it should be as extensive as possible and representative of the type of criteria used in computer systems.

2.2.1. Initial Monitoring Criteria

The real-time computer monitoring system described by Rabin et. al. (Ref. 5.) provides a detailed list of arrhythmia diagnosis criteria, as reproduced in Table 2.1. From this list it can be seen that a total of 23 different arrhythmias or events are specified, the principal parameters involved being the R-R interval and QRS complex width.

As a result of discussions with cardiologists to determine their opinion of the diagnosis criteria shown in Table 2.1., the following points were noted :-

- (1) The diagnosis of Escape beat defines the tolerance on the R-R interval (IER), used to classify them as long, short or normal, as

$$IER = \frac{ISAMP}{12} \text{ if pulse rate } > 120 \text{ beats/min. (2.1)}$$

or

$$IER = ISAMP \left(\frac{1}{8} - \frac{RATE}{2880} \right) \text{ if pulse rate } \leq 120 \text{ beats/min. (2.2)}$$

No definition of ISAMP was given in the paper by Rabin et. al. After studying the above equations, it was concluded that the parameter ISAMP would be defined as, the average R-R interval measured in seconds. It was then possible to produce a graph showing the percentage tolerance allowed on the variation of the R-R interval, related to pulse rate, as shown in Fig. 2.2. From this graph it can be seen that the two equations above, give the same result at 120 beats/minute, and that as the pulse rate decreases from this point, the percentage tolerance increases.

It was then noted that in the opinion of cardiologists consulted, there was no need to relate the tolerance on the R-R interval to pulse rate. They considered that a constant percentage tolerance of 10 or 15 percent would be satisfactory.

- (2) In several diagnoses, notably Supraventricular tachycardia and Bundle Branch Block, it was noted that a criteria of, 82% or more of QRS complexes

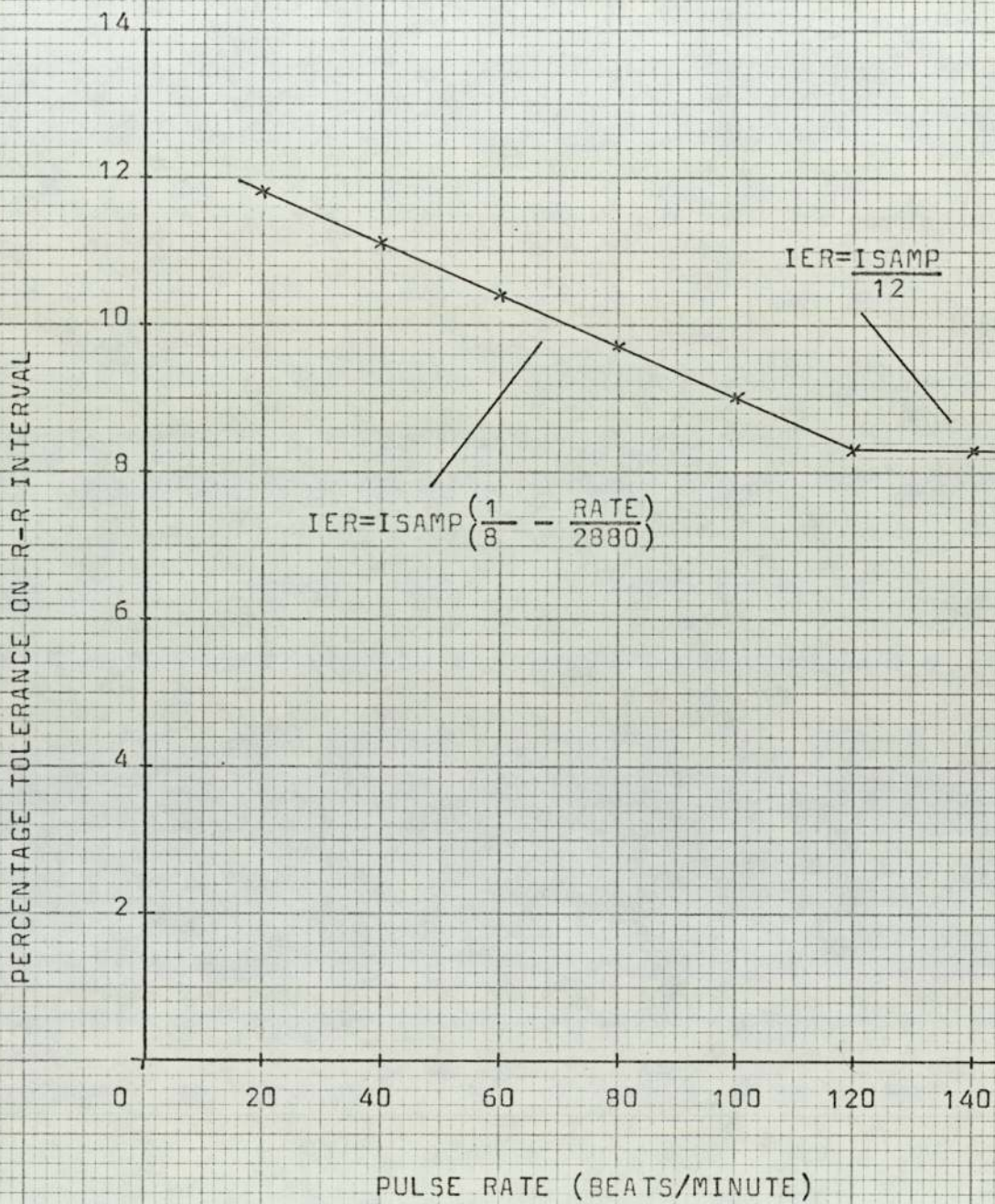


Fig 2.2. GRAPH SHOWING PERCENTAGE TOLERANCE ON R-R INTERVAL AGAINST PULSE RATE.

wide, had been specified. No indication was given as to how many beats this should be calculated from. Therefore, it was decided that this parameter would be calculated from between 200 and 400 of the most recent beats monitored. These values were chosen so that the parameter would not change too quickly nor too slowly.

The cardiologists also stated that there was no great medical significance to the value of 82%, and in fact this value could be made operator adjustable.

- (3) It was indicated that the parameter of 112mS, used to classify QRS complexes as wide, could be increased to as much as 120mS, for the detection of abnormally wide QRS complexes.
- (4) Doubt was also cast on the accuracy of diagnosing 23 different arrhythmias from only the QRS complex width, R-R interval duration and pulse rate. It was thought that for such a range of diagnoses, criteria relating to P waves should be included.

However, as this research project was not concerned with the development of new diagnostic criteria, it was decided that the criteria as given in Table 2.1., would be used as the initial system criteria, in order to enable the final distributed microprocessor system structure to be determined.

2.2.2. Alternative Monitoring Criteria

In an attempt to indicate an alternative set of

diagnosis criteria, discussions were held with a Doctor at St. Bartholomew's Hospital in London, during the final year of research.

The approach used to produce the alternative monitoring criteria, shown in Table 2.2., was the division of the arrhythmias into two main groups. These two groups were classified as non-paroxysmal arrhythmias (i.e. arrhythmias arrived at slowly, such as a fast pulse rate reached gradually), and paroxysmal arrhythmias (i.e. arrhythmias which occur suddenly, such as a premature beat).

Within each of these groups there was then the further classification of fast (tachycardia) or slow (bradycardia) pulse rates, or early (premature) or late (pause) beats. This approach meant that the diagnoses produced were of a general nature, and in no way attempted some of the precise diagnoses given in Table 2.1.

It is not claimed here that the criteria given in Table 2.2. is better than that in Table 2.1., but simply an alternative. The field of computer monitoring diagnosis criteria, requires further medical research and detailed specification.

TABLE 2.1. INITIAL ARRHYTHMIA DIAGNOSIS CRITERIA

1. VT; Ventricular tachycardia. This diagnosis was made if the pulse rate was greater than 140, 82% or more of the QRS complexes were wide (a wide QRS was 0.112 seconds or longer in duration), and the preceding rhythm (50 beats) contained multiple PVC's (greater than 10% of the QRS complexes were PVC's).
2. SVT; Supraventricular tachycardia. For this diagnosis there must be a pulse rate greater than 110 but less than 140; or if the rate was greater than 140, less than 82% of the QRS complexes were wide.
3. BBB; Bundle Branch Block. More than 82% of QRS complexes were wide with a rate less than 140.
4. BRAD; Bradycardia. Simply any case when pulse rate was less than 60 but greater than 40.
5. IDIOVT; Idioventricular rhythm. An exceptionally slow pulse rate, less than 40 but greater than 20 was the only criteria.
6. C. ARST; Cardiac Arrest. A diagnosis of cardiac arrest was made when the heart rate was less than 80 and an R-R interval was not followed by a QRS complex for a period greater than or equal to 6 sec.
7. ASYT; Asystole. A diagnosis of asystole was made when the heart rate was less than 80 and an R-R interval was greater than or equal to 2 times the

Table 2.1. Cont...

average R-R interval but less than 6 sec. in duration.

8. ESCBT; Escape beat. A diagnosis of escape beat was made if the rate was less than 60 and a long R-R interval was followed immediately by a wide QRS.

Long (L), normal (N), and short (S) R-R intervals were defined according to whether a specific R-R interval varied from the average by more or less than an amount called IER. If it was within IER of the average, it was normal (N), more than IER greater than average it was long (L) and more than IER below average it was short (S). IER was also used in other diagnoses; it is critical in identifying a PVC or a PAC. It was set as follows : If rate > 120 ; $IER = ISAMP/12$. If rate ≤ 120 ; $IER = ISAMP(1/8 - Rate/2880)$.

9. PVC; Premature ventricular contraction. A short (S) R-R interval, as defined in 8, followed by a wide QRS caused this diagnosis provided that less than 82% of QRS complexes were wide.
10. PVCRUN; A run of premature ventricular contractions. Two or more PVC's in succession caused this diagnosis.
11. VIBGY; A bigeminy rhythm produced by premature ventricular contractions.

The sequence of a short R-R interval (S) a wide QRS (WQRS), and then a not short R-R interval (\bar{S}) occurred 4 times in succession ($4(S-\bar{S})$). Note that an \bar{S} R-R interval could be either normal or long. In this rhythm, it would usually be long because of

Table 2.1. Cont...

compensatory pause after a PVC.

12. VITRIGY; A trigeminy rhythm caused by premature ventricular contractions. The sequence of a short R-R interval (S) a wide QRS (WQRS) a not short R-R interval (\bar{S}) and a normal R-R interval (N) occurred 4 times in succession (4(S- \bar{S} -N)).

The next 6 diagnoses, 13 through 18, all had 3 criteria in common. These 3 criteria will be listed first :

- A. Less than 82% of QRS complexes were wide.
- B. No diagnosis of atrial fibrillation (AF).
- C. The QRS complex following the R-R interval analysed was not wide.

13. PAC; Premature Atrial Contraction. In addition to the above 3 criteria a diagnosis of PAC was made on fulfilment of one of the following :

- A. A short R-R interval (S) when the rate was greater than 90. If the rate was less than 90 the diagnosis could be made on encountering any one of the following sequences of R-R intervals.
- B. S- \bar{S} -S; short, not short, short.
- C. S- \bar{S} -N- \bar{L} ; short, not short, normal, not long.

For example, a short R-R interval followed by normal R-R intervals would lead to the diagnosis.

14. PACRUN; A run of premature atrial contractions. Two or more PAC's (defined in 13) in succession

Table 2.1. Cont...

resulted in this diagnosis.

15. ABIGY; Bigeminy rhythm caused by premature atrial contractions. With the 3 criteria described prior to 13 there must be in addition a sequence of short R-R intervals followed by a not-short R-R interval ($S-\bar{S}$), which occurred 4 times in a row.
16. ATRIG; Atrial trigeminy. A trigeminy rhythm caused by contractions originating in the atrium. The sequence of a short R-R interval, a not short R-R interval, and a normal R-R interval ($S-\bar{S}-N$) must occur 4 times in succession.
17. ABCOND; Abnormal conduction. If the rate was greater than 110, a diagnosis of PACRUN had been made and the sequence of 3 short R-R intervals was followed by a wide QRS, this diagnosis was made.
18. SA; Sinus Arrhythmia. In addition to the 3 criteria described prior to 13 and a rate ≤ 90 , a diagnosis of SA was made on fulfilment of one of the following sequences of R-R intervals.
 - A. $S-\bar{S}-L$, short, not short, long.
 - B. $S-\bar{S}-N-L$, short, not short, normal, long.This ends the diagnoses which required the 3 criteria A-C described just before 13.
19. PC; Premature Contraction. Diagnosis of PVC or PAC with greater than 82% of QRS complexes wide would cause this diagnosis to be used rather than PVC or PAC.
20. AF; atrial fibrillation. No diagnosis of bigeminy or trigeminy rhythm. Less than 15% of QRS complexes

Table 2.1. Cont...

were PVC's. An irregularity indicator known as NODE(11) must be greater than a factor known as NODE(12). NODE(11) was the percentage of R-R intervals that differed by more than 4% from those immediately succeeding R-R intervals. The R-R intervals associated with PVC's were eliminated before making this calculation. NODE(12) was an arbitrary level described as $96 - \text{Rate}/5$. Thus, it was a linear function of rate which decreased as rate increased to recognise the fact that atrial fibrillation was more regular at fast rates than it was at slow rates.

Usually in atrial fibrillation 85 to 95% of R-R intervals differed by 4% or more from the next following R-R interval.

21. ACVTRT; Accelerated ventricular rate. If a diagnosis of BBB had been made and the rate was greater than 100, this diagnosis was designated instead of BBB. It was meant to indicate a more grave diagnosis than BBB. In some cases this could actually represent a ventricular tachycardia which was not diagnosed as ventricular tachycardia by the criteria, which required a pulse rate greater than 140.
22. SVTAC; Supraventricular tachycardia with abberant conduction. This diagnosis was made if the pulse rate was greater than 140, 82% or more of the QRS complexes were wide, and the preceding rhythm (50 beats) was SVT.

Table 2.1. Cont...

23. LS; Lost Signal. This diagnosis was made when the heart rate was greater than or equal to 80 and an R-R interval was not followed by a QRS complex for a period greater than or equal to 6 seconds.

TABLE 2.2. ALTERNATIVE ARRHYTHMIA DIAGNOSIS CRITERIA

NON-PAROXYSMAL ARRHYTHMIAS

(1) Non-Paroxysmal Tachycardia

This diagnosis is made when the average R-R interval (see Note 1) is less than 600ms, i.e. when the pulse rate is greater than 100 beats/minute. This diagnosis is not alarmed until the average R-R interval is less than 400ms (150 beats/minute), which should then produce a level 2 alarm (see Note 5).

(2) Non-Paroxysmal Bradycardia

This diagnosis is made when the average R-R interval exceeds 1 second, i.e. when the pulse rate falls below 60 beats/minute. This diagnosis is not alarmed until the average R-R interval exceeds 2 seconds (30 beats/minute), whereupon a level 2 alarm should be given.

PAROXYSMAL TACHYCARDIA

(3) Paroxysmal Tachycardia

This diagnosis is made when two or more short R-R intervals (see Note 2) occur in succession, and can be further characterised as having a "broad QRS" (see Note 3). This diagnosis should produce a level 2 alarm, unless the R-R interval becomes equal to or less than 300ms, (200 beats/minute) which should produce a level 1 alarm (see note 5).

(4) Premature Beat

This diagnosis is made if a short R-R interval

Table 2.2. Cont...

is followed by an interval which is not short. This diagnosis can be further specified as having a "broad QRS".

(5) Pause

This diagnosis is made if a very long R-R interval (see Note 4) occurs, and should result in a level 2 alarm being given.

(6) Asystole

This diagnosis is made if any R-R interval exceeds 5 seconds, and should result in a level 1 alarm being given.

NOTES

- (1) During the monitoring start-up process, the first 16 R-R intervals detected are stored and used to calculate the initial value of the average R-R interval. Thereafter this store is continuously updated with the subsequent R-R intervals, provided that they have not been labelled as long or short (see Note 2).
- (2) If an R-R interval measured, is found to be less than 85% of the average R-R interval time, it is labelled as short.

If an R-R interval measured, is found to be greater than 115% of the average R-R interval time, it is labelled as long.

Between these two limits the R-R interval is

Table 2.2. Cont...

considered to be normal, and can be used to update the average R-R interval.

- (3) A QRS complex is classified as a "broad QRS" if greater than 120mS, and is measured from the points shown in Fig. 2.1.
- (4) If an R-R interval is found to be greater than twice the average R-R interval time, it is labelled as very long.
- (5) Alarm level 1 is the highest priority alarm and indicates an imperative diagnosed condition.
Alarm level 2 indicates diagnosed condition requiring immediate warning.

CHAPTER 3

MONITORING SYSTEMS

Since the introduction of coronary care units (CCUs) in the early 1960s, many independent groups have been developing arrhythmia monitoring systems. Initially, the only monitoring equipment used in CCUs, employed analog techniques to monitor pulse rate, which allowed very slow or fast heart rates to be alarmed.

Although equipment, such as the hybrid device described by Neilson (Ref. 6, 7, 8, 9.) which enable certain arrhythmias to be detected, and high speed mass ECG monitoring to be performed, have been developed. The need for ever increasing detailed and efficient analysis of ECG signals, has resulted in increasing efforts being made to produce computer systems capable of real-time arrhythmia monitoring.

Several different approaches, such as cross-correlation (Ref. 10-15.) and Fourier transform (Ref. 16) techniques have been employed in computer monitoring systems, but the most common approach used is that of feature or pattern recognition (Ref. 17-38.). This last approach is currently preferred as it consumes less processing time compared to other techniques, and therefore is more amenable to real-time implementation. The systems using this approach vary considerably in complexity, for example, the sample rate used by such systems ranges between 60 and

500 samples per second. The work performed by Wartak et. al. (Ref.39.) recommends that a sample rate of 250 samples per second, with a quantisation accuracy greater than 7 bits, should be used by monitoring systems.

Similarly, the approach predominantly used to detect QRS complexes; which is a delayed-difference threshold method, varies in its implementation between each system. The main variations of this approach are concerned with the time interval (number of sample periods) between the samples used to produce the difference signal, and the value of the detection threshold. The work described by Van Eyll et. al. (Ref.40.) provides the optimal values for this detection approach, which were obtained using a sample rate of 250Hz.

This detection approach is also sometimes extended to classify QRS complexes as abnormal, by monitoring the number of difference values that occur after the difference signal has passed through the detection threshold (Ref.17.). Other systems, prefer to perform direct measurements on the QRS complex to classify it as wide or abnormal. Thus the criteria used in each system to diagnose the type of arrhythmias which occur, differ with each system produced. These differences arise not only because of the different monitoring approaches adopted, but also because of the individual medical interpretations made of the parameters monitored by the particular system. There is currently no standard arrhythmia monitoring^{ing} criteria, hence, each system produced employs and interprets the parameters

monitored, in the manner preferred by those developing each system.

These developmental systems usually consist of one or possibly two computers such as the PDP-8 (Ref.19.), PDP-9 (Ref.22.), PDP-12 (Ref.27.), CDC 1700 (Ref.20.), NOVA 1210 (Ref.31.) and the HP 2100 (Ref.34.). Some of these developmental systems only monitor one patient (Ref.41.), but normally they are multi-patient monitoring systems, the number of patients monitored depending on the sample rate, monitoring complexity and speed of the computer used by each system.

In the past few years one of the main computer monitoring systems to appear on the market in the Hewlett-Packard HP 78220 arrhythmia monitoring system (Ref.42.). This system uses the HP 2108 processor, and costs over £40,000 for an 8 bed unit.

Since the introduction of the first microprocessor (Intel 4004) in 1971, the performance of such devices has continually improved. As their speed and sophistication increases, their use in ECG monitoring systems increases (Ref. 43-47.). These initial implementations use 8 bit microprocessors such as the Intel 8008, the Motorola^a M6800 and the Zilog Z-80.

The introduction of a 16 bit microprocessor the TMS 9900 (Appendix A), provided the possibility of producing a microprocessor monitoring system, which could perform real-time ECG monitoring, previously only possible with computer systems. Although the execution time of

this microprocessor is still slower than those of computers used in monitoring systems, the cost of such devices would allow their distribution in a microprocessor monitoring system. In this way it was considered that any speed restriction problems would be overcome by this distributed microprocessor approach, and would also enable a more flexible and cheaper multi-patient monitoring system to be produced.

As the work by Wartak et. al. (Ref.39.) and Van Eyll et. al. (Ref.40.), mentioned above, were both concerned with a sample rate of 250Hz, their recommendations were chosen for use in the monitoring system to be developed. Similarly, the feature recognition approach was chosen for use in this system, because it is suited to real-time applications, hence the detailed criteria listed by Rabin et. al. (Ref. 5.) ^{WERE}~~WERE~~ chosen, for initial use in the system, as discussed in Chapter 2.

CHAPTER 4

SYSTEM FUNCTIONS AND STRUCTURE

4.1. INTRODUCTION

The overall function of the multi-patient microprocessor system required, was that of arrhythmia detection and diagnosis. However, the system may be sub-divided into a number of distinctly different types of functions. These functions are broadly classified as follows.

4.2. System Functions

4.2.1. Signal Acquisition

The signal acquisition function is concerned with the amplification of the chest electrode potentials, to provide the ECG signals required by the system. It was decided that this function could be satisfactorily performed by the analog equipment in common "bedside" use in CCUs, which usually provide a 1 volt ECG signal, that could be used by the monitoring system.

This decision also has the advantages that the final system would be cheaper, by the exclusion of this function, and more likely to be acceptable for CCU use, as it would make greater use of existing CCU equipment.

4.2.2. Signal Conditioning

The signal conditioning function is concerned with the processing of the ECG signals applied to the system,

to obtain a conditioned signal from which measurements may be taken with an appropriate degree of confidence. This is achieved by the detection of abnormal signal levels in the higher frequency components of the ECG signals, which would indicate the presence of artefact (unwanted muscle noise). Having detected the presence of noise, filtering of the ECG signal could then be performed. Also this function was to be responsible for the removal of very low frequency components, to remove d.c. and base-line drift from the signal.

As it is desirable to incorporate as many of the system functions as possible, in the more compact and flexible media of software, this function was implemented using digital filtering techniques (ref.48-53.), as described in section 5.2. The sampling rate of the ECG signal was set to 250Hz, as recommended by Wartak et. al. (ref.39.). Therefore, the signal conditioning function would have to be performed on each of these samples.

4.2.3. Signal Monitoring

The ECG signal monitoring function is concerned with the detection of each QRS complex, and the subsequent measurement and classification of features in the ECG signal which are of interest. The monitoring criteria to be initially used by the system, as described in Chapter 2, focuses attention principally on the length of the R-R interval, and the width of

the QRS complex. The detection of each QRS complex is to be achieved using a delayed difference signal approach, using the optimal parameters suggested by Van Eyll et. al. (ref.40.), as described in Section 5.3. Using this approach it is necessary that the monitoring function QRS detection algorithm, be performed for each of the ECG samples.

Having detected a QRS complex, this function then performs the measurements required, and therefore this aspect of the monitoring function would have a frequency of operation dependent on the pulse rate of the monitored patients.

4.2.4. Diagnosis

Having performed the required measurements and observations by the monitoring function, it was the task of the diagnosis function to interpret the results, and provide a diagnosis. The approach used to implement this function was by the use of decision table techniques (ref.54.), as described in Section 5.4.

This function is only called upon, when the monitoring function has detected and measured the required parameters. Therefore, this function has a frequency of execution which is dependent upon the pulse rate of the patients being monitored at the time.

4.2.5. Display

The display function is concerned with the presentation of information, such as ECG data, parameter values, diagnoses and trends to the system

operator. Therefore, there is the need for software to provide the data in its required form, to the appropriate system/operator interfaces, such as a VDU. This type of data would be of an intermittent nature, depending on such things as frequency of arrhythmia events.

4.2.6. Storage

The storage function is concerned with the retention of information such as trend data and stored arrhythmia events etc., which may be required for subsequent display to the system operator. This data would also be of an intermittent nature.

4.2.7. Communication and Control

In order for the system to perform as required by the operator, there is the need for a communication function to be present in the system. This function is concerned with the interpretation of input commands to the system, via a medi^{um} such as a VDU, and thus the activation of the system to perform the required task.

Also in order that the individual functions listed above should combine to produce the resulting system function of arrhythmia detection and diagnosis, there is the need for overall system control. The control function is thus the operating system (ref.56,61.) which allows the individual functions to interact to provide the system function required.

4.3. The Ideal System Function Structure

In order to determine a suitable structure for the system, it is necessary to examine the volume of information flowing between each individual function, as shown in Fig. 4.1.

As stated in section 4.2.1., only the signal acquisition function is by necessity distributed in the system, this being allocated on a one-per-patient basis. The remaining functions may therefore be distributed as required.

Since the highest rate of data transfer occurs permanently between the signal acquisition, conditioning and monitoring functions, the greatest benefits of a distributed processing network would be obtained if each of these functions were allocated on a one-per-patient basis.

If the diagnosis function was made a centralised function, the result would be a permanent flow of information, of low data rate converging on the centralised diagnosis function, from all the patient function nodes. If however, the diagnosis function was also allocated on a one-per-patient basis; it would result in the intermittent flow of information, of low data rate in the form of diagnoses, being the data sent to the centralised functions. This last configuration is the system structure which would result in the lowest volume of data flowing from the patient dedicated functions, to the centralised functions. Therefore,

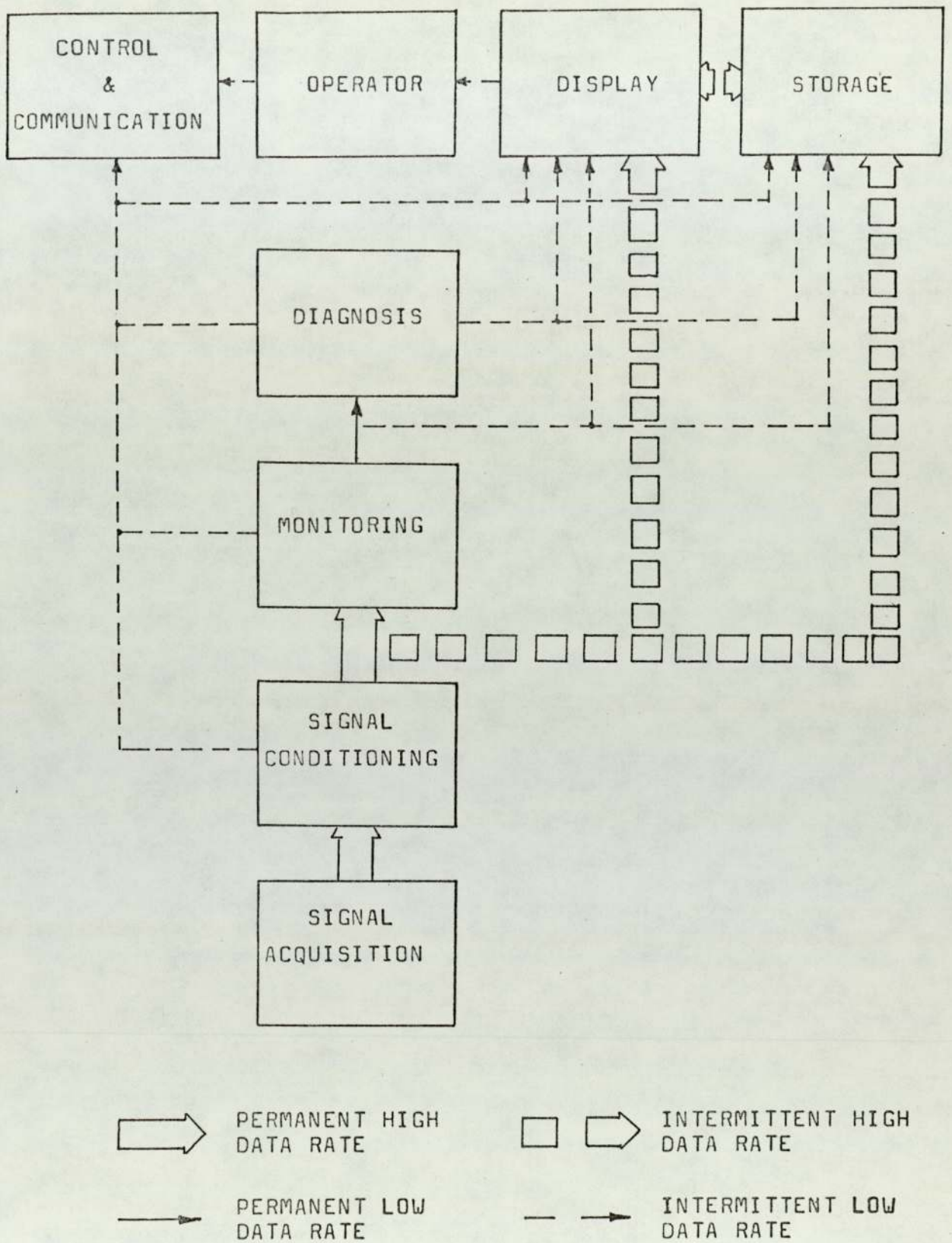


FIG. 4.1. SYSTEM FUNCTION AND INFORMATION FLOWS

this structure, as illustrated in Fig. 4.2., was considered as being the ideal system function structure.

4.4. Performance of Functions in Real-Time

Having determined the most suitable function structure for the distributed system, the allocation of processors to functions, or vice-versa was considered. However, this procedure was not capable of simple or precise quantifications. It was therefore necessary to implement each function in turn, to determine the extent of processor utilisation in performing each function, and hence the final distribution of processors within the system.

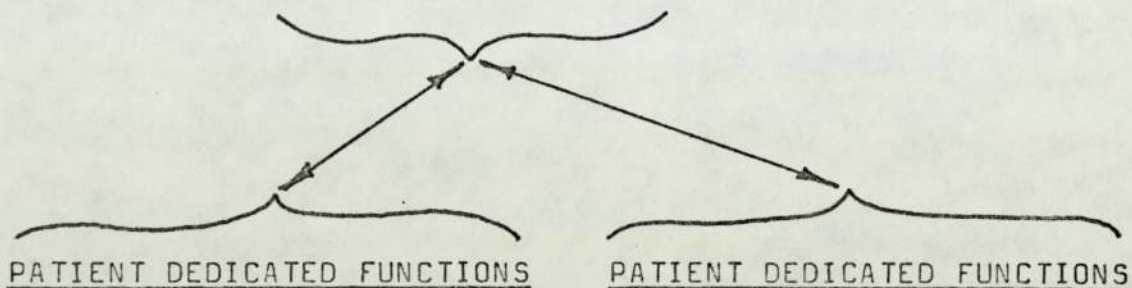
As a result of producing the functions, which are described in detail in Chapters 5 and 6, the results as shown in Table 4.1. were obtained. From these results it was found that, for a single patient, approximately 42% of the processing time of a single TMS 9900 microprocessor is used in performing all the functions given in Table 4.1. Leaving the remaining 58% of unused processing time available for use by the storage, display and operator communication functions.

Therefore, this assessment showed that for a single patient, performance of all functions shown in Fig. 4.1. is well within the capability of a single TMS 9900 microprocessor. However, the aim was to produce a multi-patient monitoring system, with centralised facilities of system control, storage and display. These functions being centralised for ease of system management, and cost of peripheral devices.

CENTRALISED FUNCTIONS

OF

DISPLAY, STORAGE
SYSTEM CONTROL AND
COMMUNICATION



OF

DIAGNOSIS

MONITORING

SIGNAL CONDITIONING

SIGNAL ACQUISITION

OF

DIAGNOSIS

MONITORING

SIGNAL CONDITIONING

SIGNAL ACQUISITION

4.2. IDEAL STRUCTURE OF DISTRIBUTED SYSTEM FUNCTIONS

FUNCTION	EXECUTION TIME	FREQUENCY OF EXECUTION	PERCENTAGE OF PROCESSING TIME CONSUMED BY FUNCTION PER SECOND
SIGNAL CONDITIONING	1 mS	250/Sec	25%
MONITORING	MIN 0.21mS	250/Sec	5.25%
	MAX 3.2mS	IF PULSE RATE=60 BPM THEN 1/Sec	0.32%
		IF PULSE RATE=180 BPM THEN 3/Sec	0.96%
DIAGNOSIS	0.2mS	IF PULSE RATE=60 BPM THEN 1/Sec	0.02%
		IF PULSE RATE=180 BPM THEN 3/Sec	0.06%
CONTROL	\approx 0.14mS	DEPENDENT ON FUNCTION ACTIVITY \approx 750/Sec	10.5%

TABLE 4.1. FUNCTION EXECUTION TIME AND PERCENTAGE OF PROCESSING TIME CONSUMED PER SECOND

4.5. Distributed Processor System Structure

The final structure therefore, of the multi-patient distributed processing system, is the allocation of a single microprocessor to each patient. Each of these patient dedicated processors performs the functions of signal conditioning, monitoring and diagnosis, plus the functions of patient processor function control and inter-processor communication, as described in Chapters 5 and 6.

These patient dedicated processors then communicate the required information, such as arrhythmia diagnoses, to the centralised functions controlled by an operator-dedicated processor as illustrated in Fig. 4.3. Thus the ideal system function structure is in fact the final solution.

4.6. Conclusions

Having distributed the system as shown in Fig. 4.3., the additional advantage that has been gained, apart from those previously mentioned, is that of surplus processing time available at each of the patient dedicated processor nodes. This is because, the only demand made on the available surplus processing time of 58% at each patient processing node, is that made by inter-processor communication. Therefore, there is the availability of improving and expanding any of the patient dedicated functions.

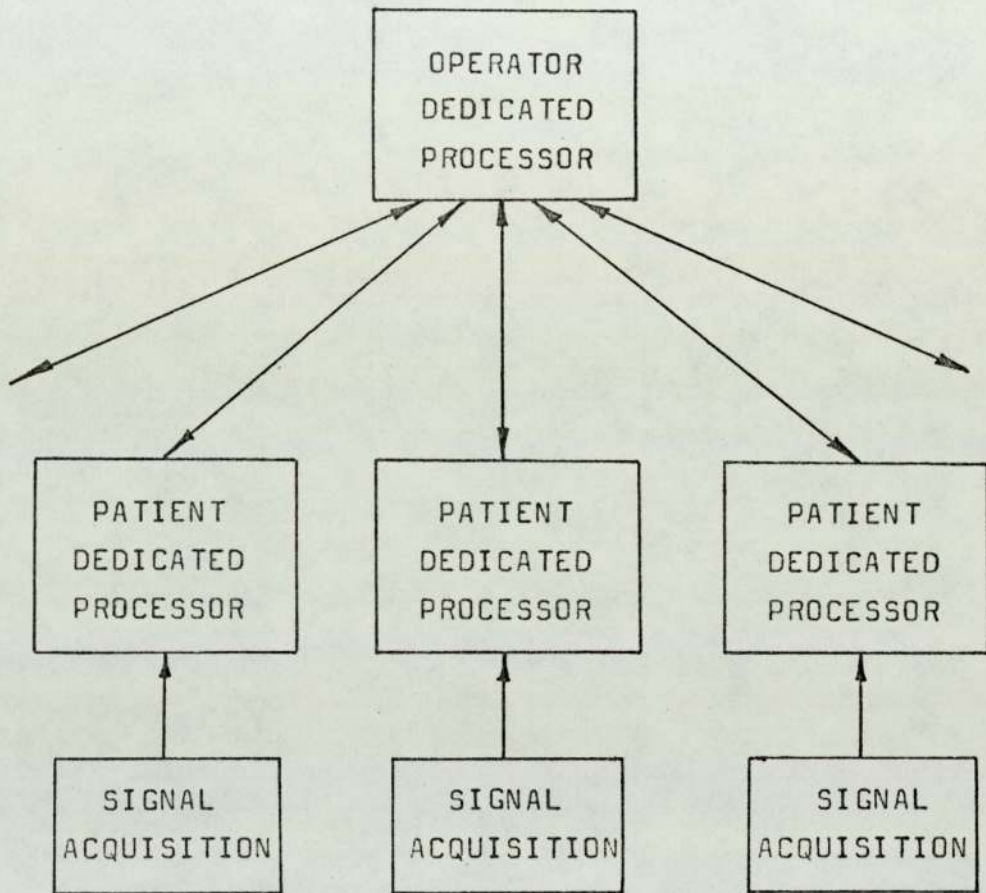


FIG. 4.3. STRUCTURE OF DISTRIBUTED PROCESSOR SYSTEM

CHAPTER 5

PATIENT-DEDICATED PROCESSOR SYSTEM DESIGN

5.1. INTRODUCTION

Each patient-dedicated processor system performs the functions of signal conditioning, monitoring, diagnosis and inter-processor communication, under the control of an operating system as shown in Fig 5.1. As can be seen from this diagram, the communication function consists of the three tasks of input, output and interpreter (microprocessor communication package), and the operating system is divided into the four modules of system initialisation, real-time task scheduler, ADC interrupt handler and UART interrupt handler.

In order to understand this system structure, let us consider each of the system tasks in turn, and hence the resulting control provided by the patient-dedicated operating system.

5.2. Signal Conditioning

The purpose of the signal conditioning function developed, is to improve the consistency of subsequent signal monitoring, by the removal of very low frequency components (d.c, and base-line drift), and the reduction, when present, of intermittent high frequency components (artefact), from the ECG signal.

A sketch of the normal ECG spectrum, as obtained by Golden et. al. (Ref.57.), is shown in Fig. 5.2. From

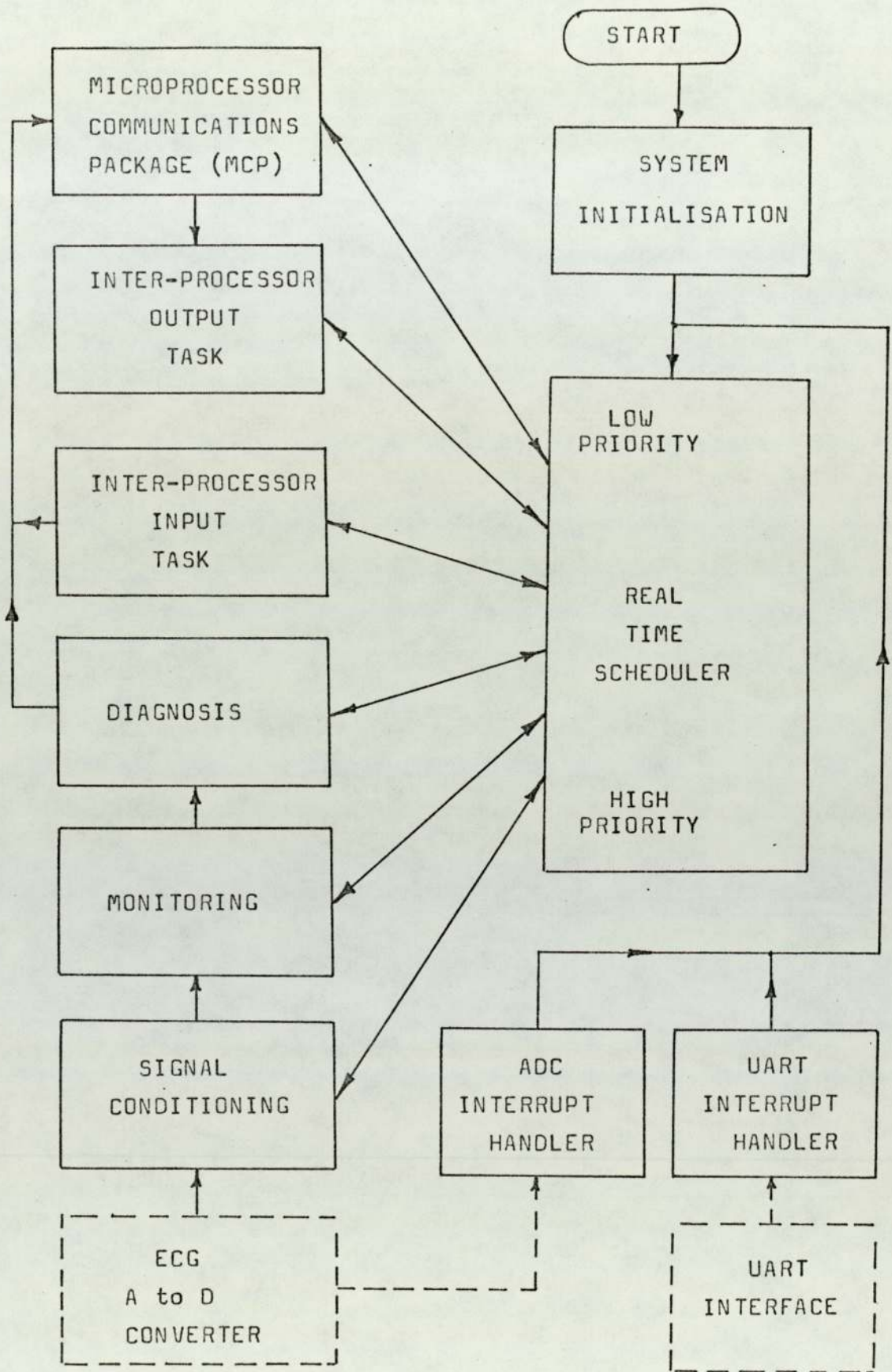


Fig. 5.1. SOFTWARE STRUCTURE OF PATIENT-DEDICATED PROCESSOR

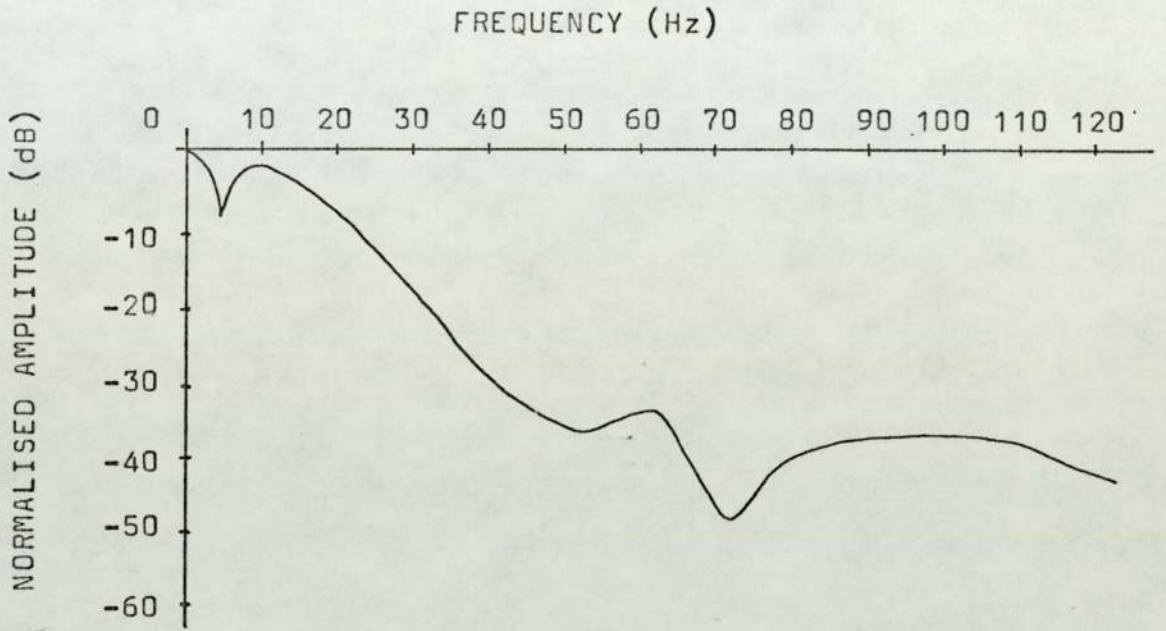


Fig. 5.2. SKETCH OF ECG SPECTRUM

this sketch it can be seen that the predominant portion of the ECG spectrum is below 60Hz.

The required signal conditioning is accomplished by an adaptive digital filtering algorithm, applied to the sampled ECG signal. The filtering algorithm developed contains three digital filters, the first of which is a high-pass filter with a very low cut-off frequency, used to remove the d.c. and base-line drift frequency components from the ECG signal. The remaining two digital filters perform the adaptive aspect of the filtering algorithm, concerned with the detection and reduction of artefact frequency components. The first of these two filters is a high pass filter used to monitor the frequency spectrum above the predominant portion of the ECG spectrum (Fig. 5.2.). It is this filter which enables artefact to be detected. The remaining filter is a low-pass filter, used to reduce the level of artefact in the ECG signal, when it has been detected. All of the filter cut-off frequencies were determined experimentally as described shortly.

As speed of operation is an important factor in the design of each function, it was decided that recursive digital filter techniques would be used, as this would reduce the number of time consuming multiplications to be performed by the algorithm.

The design of the digital filters used, was accomplished by transforming continuous Butterworth filters, into their discrete form using the Bilinear Transformation approach

(Ref. 48, 49, 50, 51, 52.). This approach states that continuous filter transfer functions in the form $H(s)$, can be transformed into their discrete form of $H(z)$ via the relationship

$$s \longrightarrow \frac{2(1 - z^{-1})}{T(1 + z^{-1})} \quad (5.1.)$$

However this transformation produces the effect known as "frequency warping" (Ref.49.) which results in the relationship between the analog filter cut-off frequency (ω_A) and the resulting digital filter cut-off frequency (ω_D) of

$$\omega_A = \frac{2}{T} \tan \frac{\omega_D T}{2} \quad (5.2.)$$

As stated previously, the analog filter that was to be transformed by this approach was the Butterworth filter, which was chosen because it has a relatively simple transfer function that produces a maximally flat frequency response. A second order low-pass Butterworth filter has a transfer function given by

$$H_{LP}(s) = \frac{s_1 s_2}{s^2 + \sqrt{2}s + 1} \quad (5.3.)$$

and a high-pass transfer function of the general form

$$H_{HP}(s) = \frac{s^2}{s^2 + \sqrt{2}s + 1} \quad (5.4.)$$

Using the Bilinear Transformation equation 5.1., and the above equations provides the discrete forms

of the filter transfer functions of

$$H_{LP}(z) = \frac{C_{LP}(1 + 2z^{-1} + z^{-2})}{1 + K_1z^{-1} + K_2z^{-2}} \quad (5.5.)$$

and

$$H_{HP}(z) = \frac{C_{HP}(1 - 2z^{-1} + z^{-2})}{1 + K_1z^{-1} + K_2z^{-2}} \quad (5.6.)$$

where

$$C_{LP} = \frac{w_A^2}{1 + \sqrt{2}w_A + w_A^2} \quad (5.7.)$$

$$C_{HP} = \frac{1}{1 + \sqrt{2}w_A + w_A^2} \quad (5.8.)$$

$$K_1 = \frac{2w_A^2 - 2}{1 + \sqrt{2}w_A + w_A^2} \quad (5.9.)$$

$$K_2 = \frac{1 - \sqrt{2}w_A + w_A^2}{1 + \sqrt{2}w_A + w_A^2} \quad (5.10.)$$

Using the Direct Form of block diagram construction (Ref.53.) on equations 5.5. and 5.6., it was possible to produce block diagrams of the digital filters (Fig. 5.3.) from which the software for the filters was produced.

The above theory was then used to produce filter

coefficients for a range of filter cut-off frequencies, using the recommendations of Wartak et. al. (Ref.39.), that the ECG signal should be sampled at a rate of 250Hz ($T=4\text{ms}$) with 8 bits quantization resolution.

From the experimental work with these filters, it was found that the d.c. eliminating filter produced computational values which were so large that they could not be handled speedily by the processor. Hence, another form of the discrete transfer function was obtained as follows.

A high-pass continuous Butterworth filter, with a cut-off frequency of ω_A , is given by

$$H_{HP}(s) = \frac{s^2}{s^2 + \sqrt{2}s\omega_A + \omega_A^2} \quad (5.11.)$$

Now let the sampling frequency be $r\omega_A$ i.e.,

$$T = \frac{1}{r\omega_A} \quad (5.12.)$$

Substituting equation 5.12. into 5.1. gives,

$$s \longrightarrow 2r\omega_A \left(\frac{z-1}{z+1} \right) \quad (5.13.)$$

Substituting equation 5.13. into 5.11. gives,

$$H_{HP}(z) = \frac{4r^2\omega_A^2 \left(\frac{z-1}{z+1} \right)^2}{4r^2\omega_A^2 \left(\frac{z-1}{z+1} \right)^2 + \sqrt{2}r\omega_A^2 \left(\frac{z-1}{z+1} \right) + \omega_A^2} \quad (5.14.)$$

which reduces to

$$H_{HP}(z) = \frac{\frac{4r^2}{4r^2 + 2\sqrt{2}r + 1}}{1 + \left\{ \frac{4r^2}{4r^2 + 2\sqrt{2}r + 1} \right\} \left\{ \frac{\sqrt{2}}{r(z-1)} + \frac{z}{(z-1)^2 r^2} \right\}} \quad (5.15)$$

Equation 5.15. is of the form

$$H(z) = \frac{K(z)}{1 + K(z)G(z)} \quad (5.16.)$$

which is of a standard feedback configuration, as shown in Fig. 5.4.

Using this alternative digital filter block diagram, the problem of large computational values was overcome, because the accumulations in the feedback path of the filter contain values of similar magnitude to that of the input to the filter.

The resulting filter produced using the alternative filtering approach was finally set to a cut-off frequency of 0.5Hz, with the resulting filter coefficients converted to 12 bits fractional accuracy as shown in Table 5.1.

In order to determine a suitable cut-off frequency for the filter to be used in the artefact detection section of the filtering algorithm, experiments were performed using a number of different cut-off frequencies and artefact detection threshold levels. From these experiments, it was observed that a filter cut-off

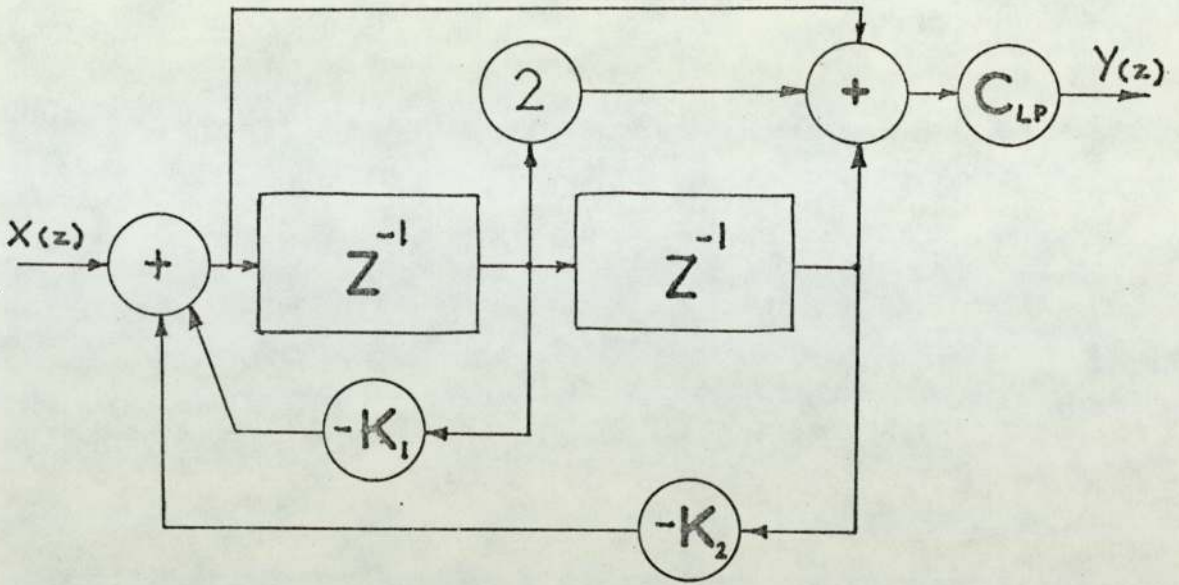


Fig. 5.3. LOW PASS DIGITAL FILTER BLOCK DIAGRAM

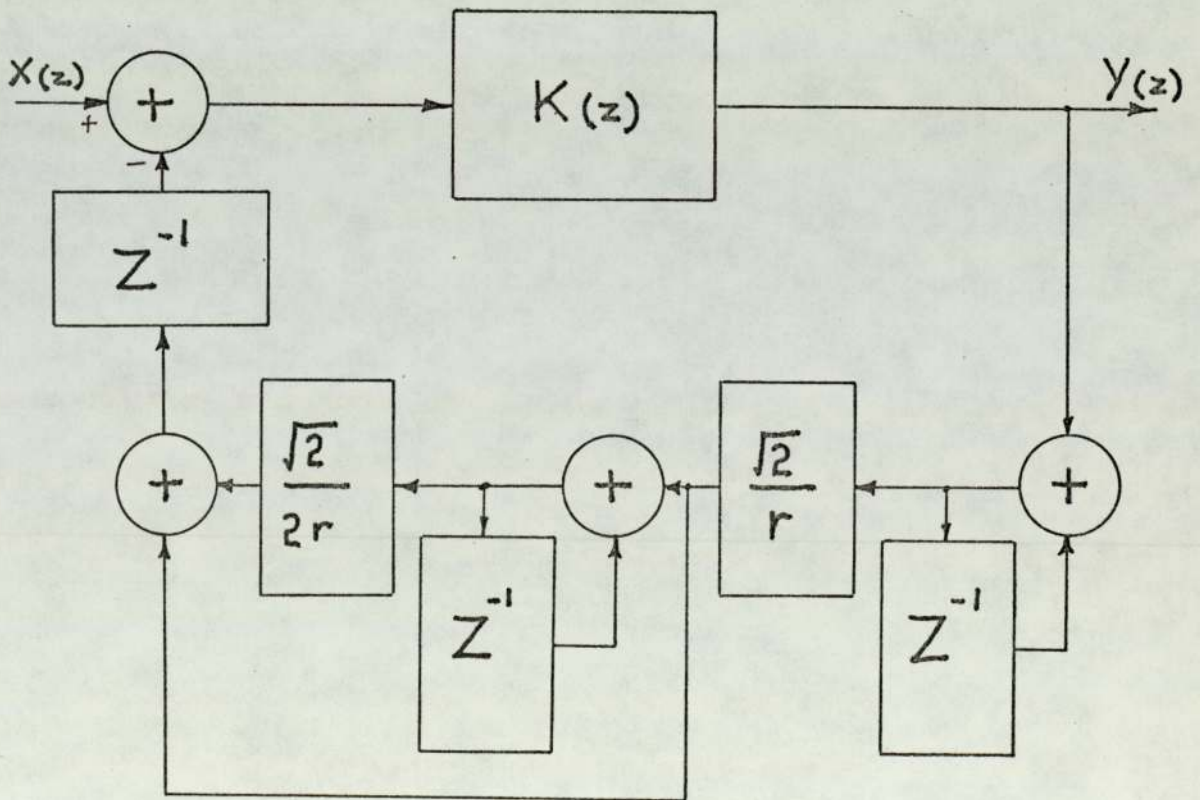


Fig. 5.4. STANDARD FEEDBACK CONFIGURATION OF DIGITAL FILTER

frequency of 60Hz combined with a noise threshold level of 26 quantization units, produced an arrangement whereby artefact was detected, but the high frequency ECG components due to QRS complexes were not. As shown in Fig. 5.5. The resulting artefact detection filter was produced using the standard feedback configuration (Fig. 5.4.) approach as this allowed the filter coefficients to be converted to 12 bits fractional accuracy as shown in Table 5.1.

Two approaches were then adopted to determine a suitable cut-off frequency for the artefact reduction filter. The first of these approaches was a theoretical attempt to determine to what extent the QRS complex widths would be affected by low pass filtering. This was achieved by producing a program which performed subsequently lower cut-off frequency filtering on a stored example of a QRS complex. Each resulting filtered QRS complex was then measured by the program, and the percentage change in QRS width calculated. Also, in an attempt to vary the stored example of a QRS complex, this data was perturbed about the reference axis, in order to vary the stored QRS complex width. The resulting limits of QRS complex width variation, as produced by the program, are shown in Fig. 5.6., and as can be seen, below a 20Hz cut-off frequency, the percentage change in QRS complex width increases rapidly. Also, it is noted that not only can

D.C. FILTER COEFFICIENTS (CUT OFF FREQUENCY 0.5Hz)

$$\begin{aligned}K(z) &= 0.99115 = 0FDB_{16} \\ \sqrt{2}/r &= 0.01777 = 0048_{16} \\ \sqrt{2}/2r &= 0.00888 = 0024_{16}\end{aligned}$$

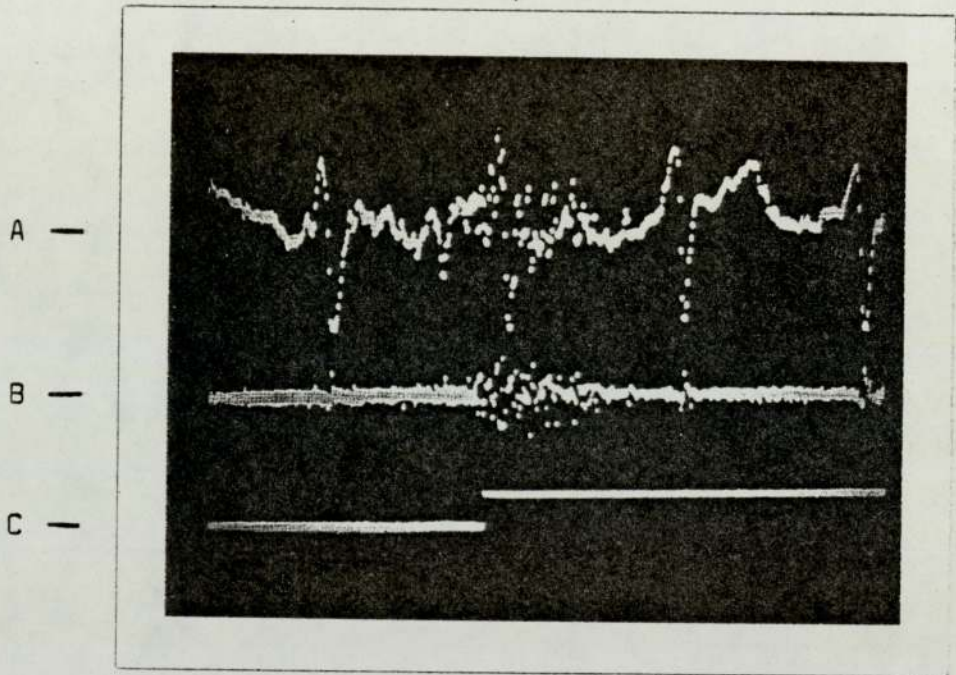
ARTEFACT DETECTION FILTER COEFFICIENTS (60Hz)

$$\begin{aligned}K(z) &= 0.311538 = 04FC_{16} \\ \sqrt{2}/r &= 2.656069 = 2A7F_{16} \\ \sqrt{2}/2r &= 1.328034 = 153F_{16}\end{aligned}$$

ARTEFACT REDUCTION FILTER COEFFICIENTS (25Hz)

$$\begin{aligned}C_{LP} &= 0.067455 = 0011_{16} \\ K_1 &= 1.142983 = 0124_{16} \\ K_2 &= -0.41280 = FF97_{16}\end{aligned}$$

TABLE 5.1. FILTER COEFFICIENTS



- A SAMPLED ECG SIGNAL
- B OUTPUT OF 60Hz HIGH-PASS FILTER
- C NOISE DETECTION INDICATOR

Fig. 5.5. OUTPUT FROM HIGH PASS FILTER

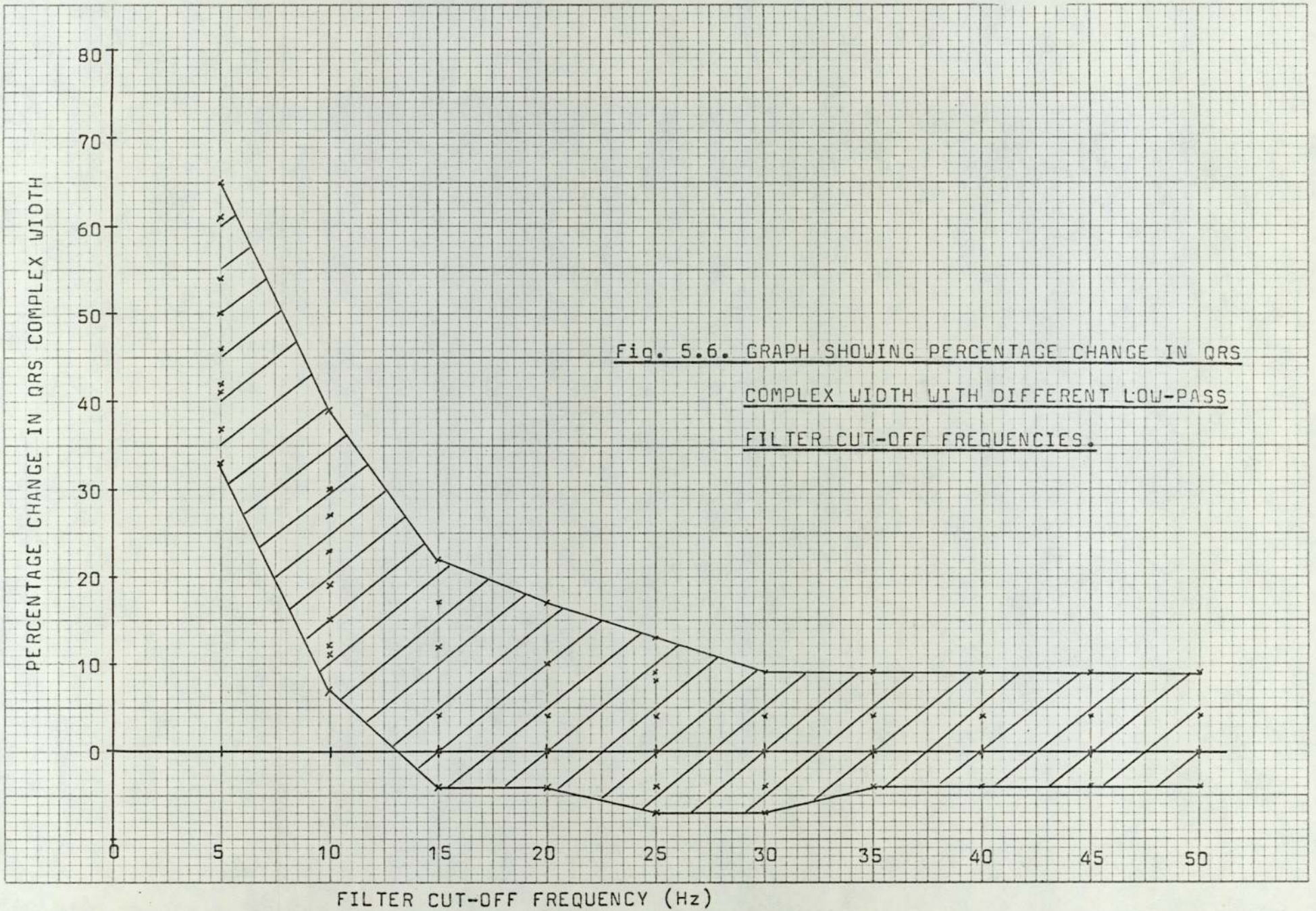


Fig. 5.6. GRAPH SHOWING PERCENTAGE CHANGE IN QRS
COMPLEX WIDTH WITH DIFFERENT LOW-PASS
FILTER CUT-OFF FREQUENCIES.

filtering increase the measured widths of QRS complexes, but as indicated by the occurrence of negative percentages, QRS complex widths measured can be reduced. This effect is due to the size of the samples at the extremes of the QRS complex. At these points the small sample values can easily change in sign as well as in amplitude, resulting in occasions where fewer sample periods are counted between the QRS width measurement points.

The second approach used to determine a suitable cut-off frequency for the artefact reduction filter, was the direct observation of the effect of reducing the filter cut-off frequency on actual ECG data. While performing this experiment observations were made of the effect of filtering on the QRS width, and the extent to which artefact was visibly reduced by each cut-off frequency.

As a result of this work, a cut-off frequency of 25Hz was chosen for the artefact reduction filter, because it provided good artefact level reduction, while not excessively increasing the QRS complex width. This particular filter was produced using the Direct Form of block diagram construction (Fig. 5.3.) and as a result of the larger computational values produced by such a filter, its coefficients were converted to 8 bits fractional accuracy, as shown in Table 5.1.

The resulting frequency characteristics of the three filters used in the filtering algorithm are shown in Fig. 5.7. Combining these filters in the

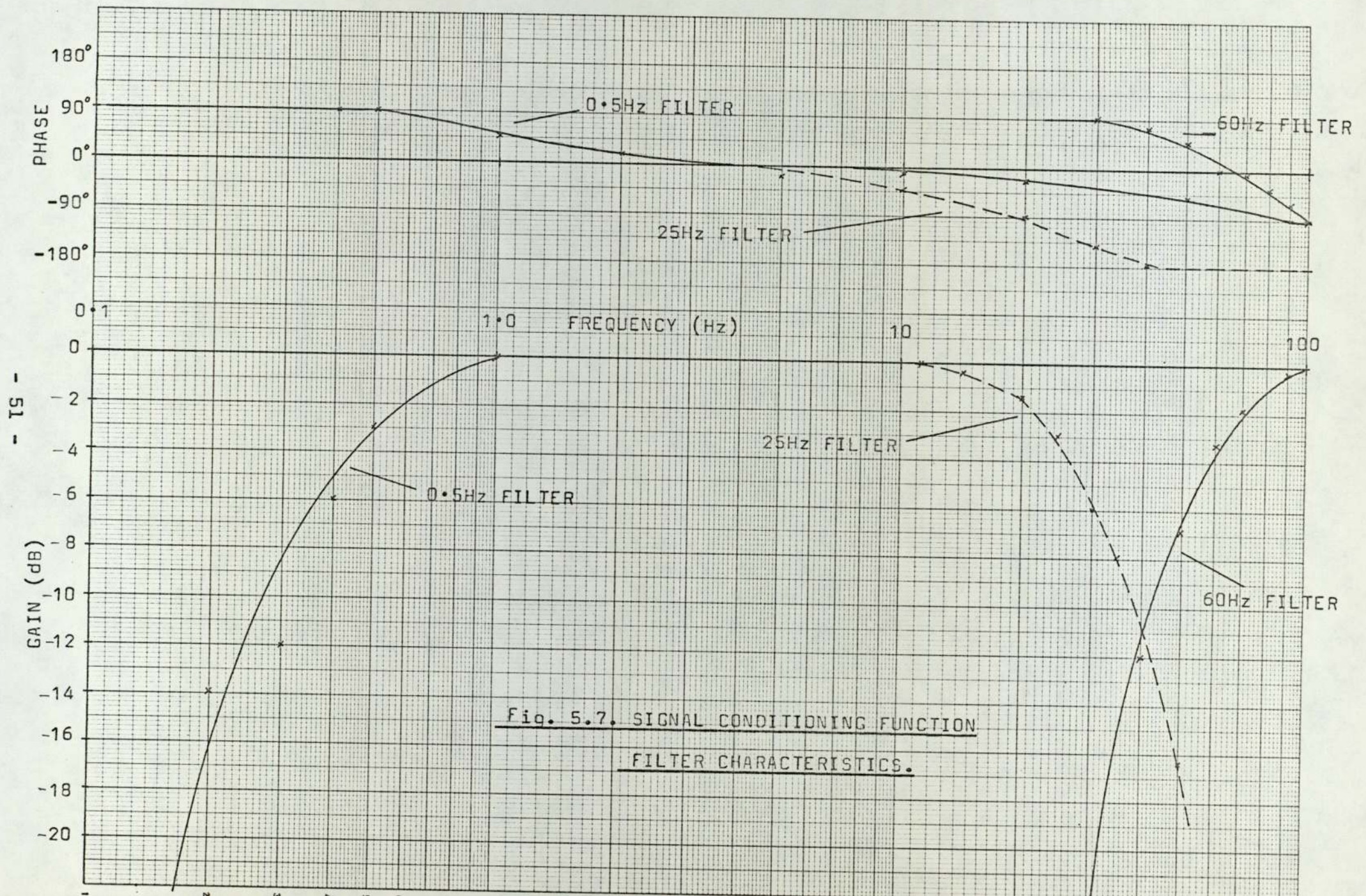


Fig. 5.7. SIGNAL CONDITIONING FUNCTION
FILTER CHARACTERISTICS.

manner shown in Fig. 5.8. produces the required signal conditioning function. The delays of N and n sample periods, shown in Fig. 5.8., are chosen to equalise the total delays through the 25Hz low-pass filter and the direct path, and also to ensure that the filtered signal is introduced just prior to the occurrence of the artefact to be reduced. The delayed hold is introduced into the system, to ensure that the low-pass filter remains in continuous operation when rapid bursts of artefact are present in the ECG signal. Some examples of conditioned ECG signals are given in Fig. 5.9.

The execution time of this signal conditioning function software is 1mS, which is well within the 4mS sampling period. The assembly program listing of this program can be found in the software appendix, under the program identifier IPDHTP.

5.3. Signal Monitoring

The first task of the monitoring function developed is the detection of each QRS complex. This is achieved using the optimal parameters suggested by Van Eyll et. al. (Ref.40.) for an on-line algorithm monitoring the QRS complex. This algorithm accomplishes the detection of the QRS complex by a delayed-difference threshold method. A signal is obtained by calculating the difference between samples of the ECG signal, which are separated by 6 sample periods (24mS). This signal is

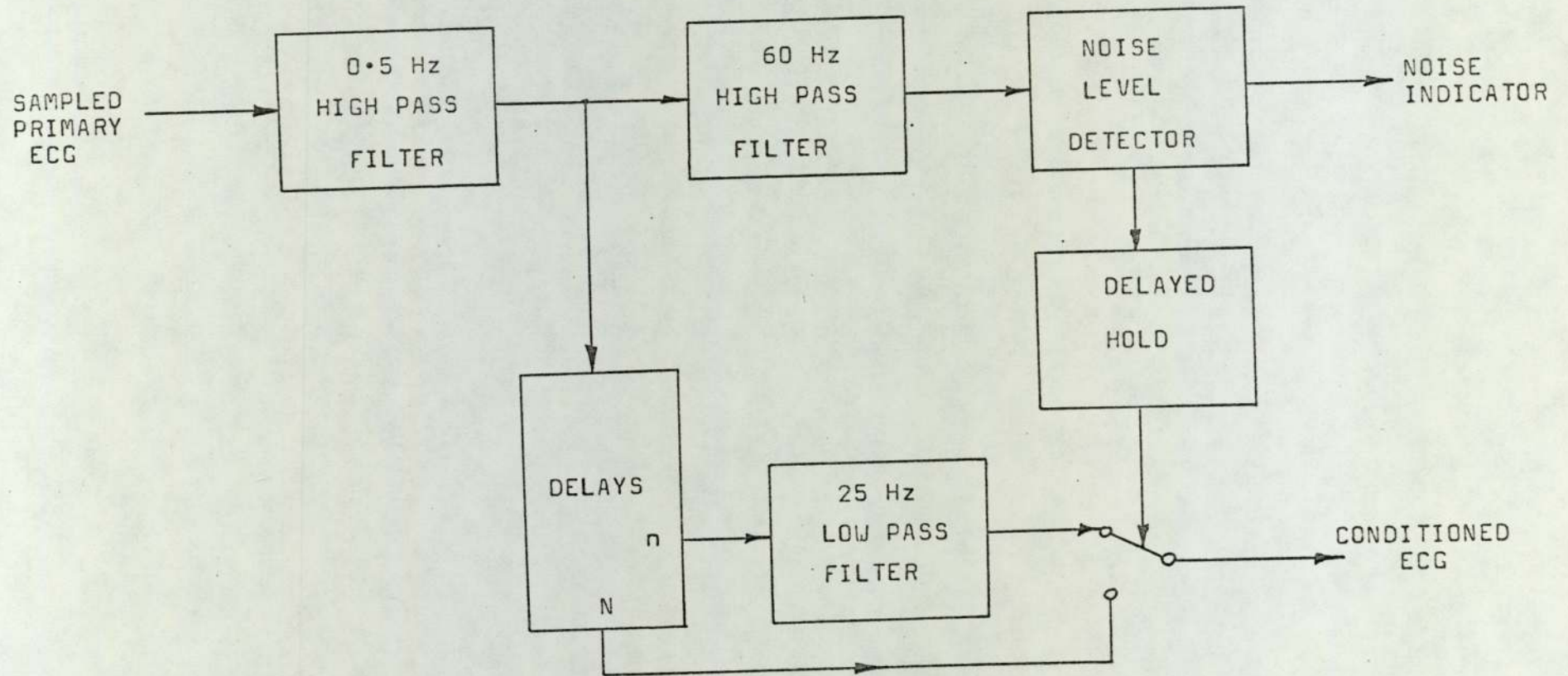
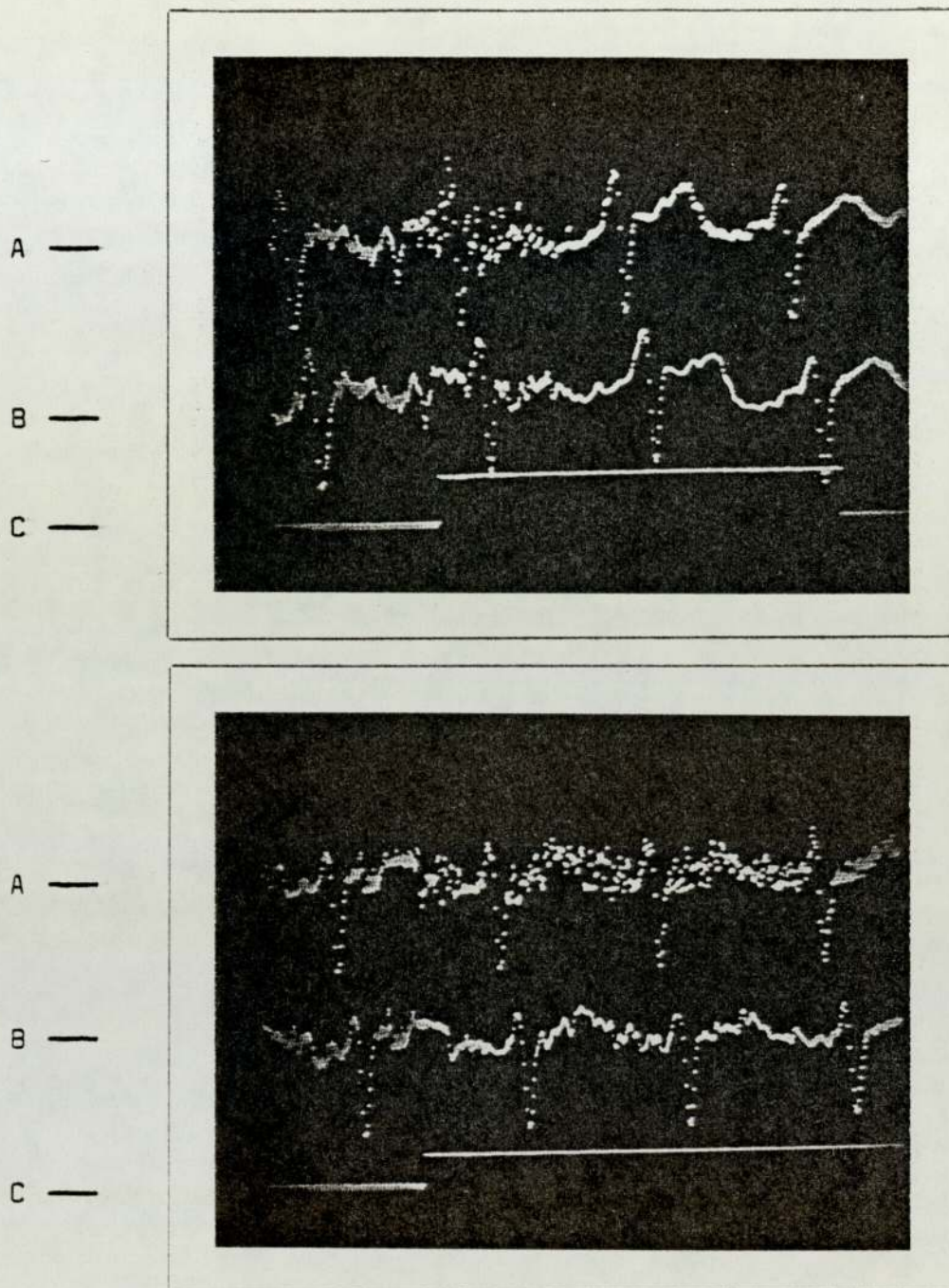


Fig. 5.8. BLOCK DIAGRAM OF ADAPTIVE FILTER



A SAMPLED ECG SIGNAL
 B CONDITIONED ECG SIGNAL
 C NOISE DETECTION INDICATOR

Fig. 5.9. EXAMPLES OF CONDITIONED ECG SIGNALS

then compared with a threshold (TD) which is 60% of the average minimal negative value (DMIN) of the delayed difference signal (Fig. 5.10.). When the delayed difference signal passes through this threshold the QRS complex is detected.

This detection method is adaptive, because the detection threshold (TD) is calculated from the average minimal negative value. The parameters used to calculate the average minimal negative value have also been optimised by Van Eyll et. al. (Ref.40.) as follows.

Every time a QRS is classified as normal the average minimal negative value is recalculated as :-

$$\text{DMIN(NEW)} = \text{DMIN(OLD)} \times 0.8 + 0.2 \times \text{DMIN(CURRENT)} \quad (5.17.)$$

and therefore the threshold (TD) is recalculated as

$$\text{TD} = 0.6 \times \text{DMIN(NEW)} \quad (5.18.)$$

The approach by Van Eyll uses the number of samples below the detection threshold (TD) to classify the QRS complex as normal or abnormal, and hence whether or not to update the average minimal negative value. However, the approach adopted for the microprocessor system was that of updating the average minimal negative value only when the QRS width measurement algorithm (to be described), classified the QRS width as normal.

This detection method was adopted, because it is a method in common use in computer monitoring systems,

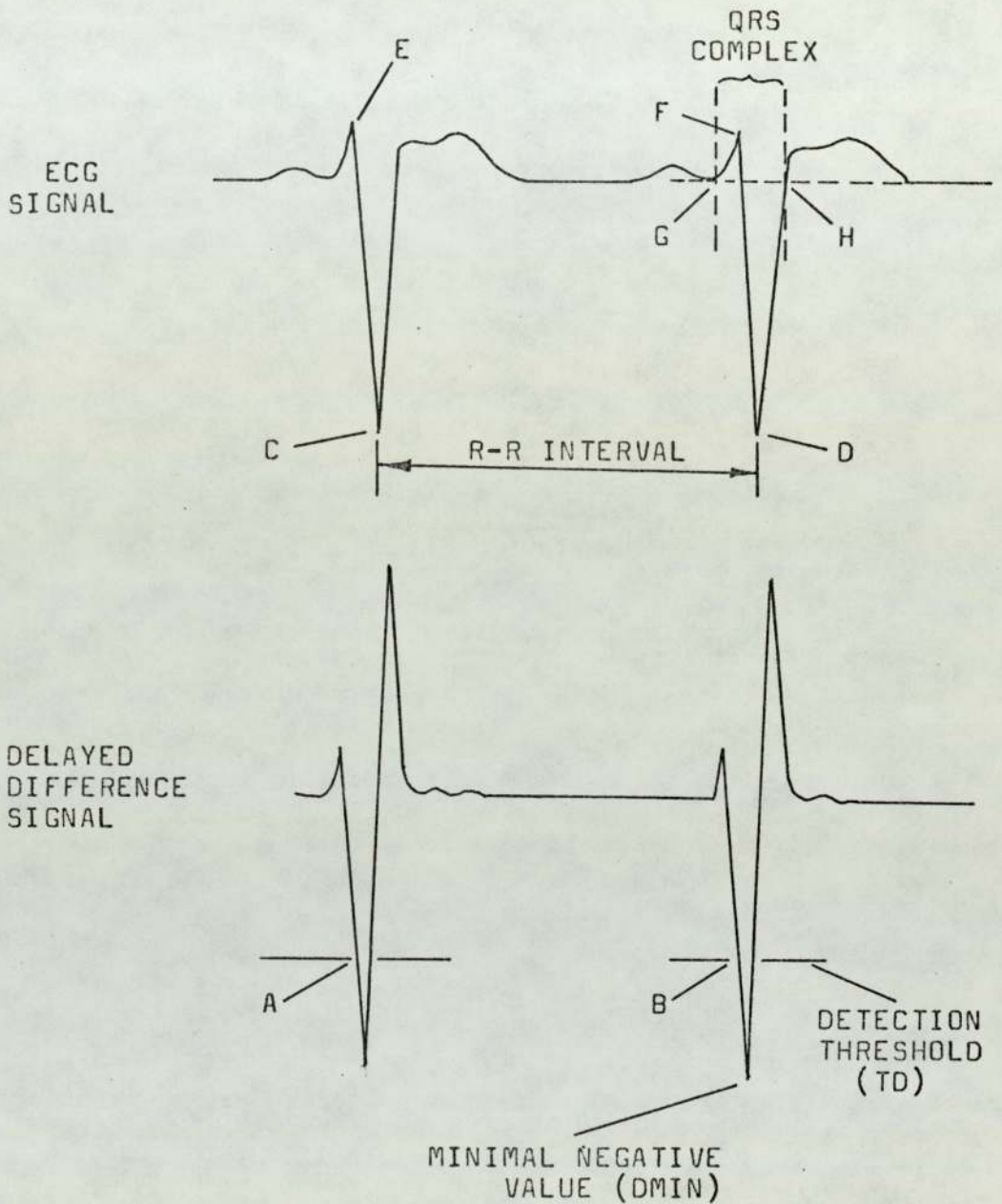


Fig. 5.10. DELAYED-DIFFERENCE DETECTION OF QRS COMPLEX

as it is relatively simple and therefore consumes as little processing time as possible. Also, the optimal values suggested by Van Eyll were developed for a sampling rate of 250Hz, which is that used by the signal conditioning function.

When the patient processor system is instructed to start the monitoring function, the first 2 seconds of ECG signal are used purely to determine a minimal negative value, which will be used initially by the detection software. This value, when found, is compared with a reference value to determine if it is large enough to be used as a minimal negative value. If the minimal negative value found, is too small, the monitoring function is stopped and a message, indicating that there has been a monitoring function start-up failure, is sent to the operator dedicated processor. If, however, the minimal negative value found is an allowable value, the detection threshold (TD) is calculated as 60% of this value, and a message is sent to the operator processor, indicating that the monitoring start-up procedure was successful.

Two consecutive QRS complexes are then detected and the R-R interval between them measured. This value is then used as the initial value for the average R-R interval (AVRR). Thereafter, any R-R interval which is classified as normal is used to up-date the average R-R interval.

After this initial starting-up process, the

monitoring function will then perform the monitoring measurements and observations required. As indicated in section 2.5., two slightly different sets of monitoring criteria were eventually to be implemented. The first set of criteria used was that suggested by Rabin et. al. (Ref. 5.) , as given in Table 2.1.

5.3.1. R-R Interval Measurement

The measurement of the R-R interval as illustrated in Fig. 5.10., is defined as the time between the two negative peaks of successive QRS complexes. The monitoring function measures this interval by first counting the number of sample periods received (RRC), between the points where the delayed difference signal first passes through the detection threshold (points labelled A and B in Fig. 5.10.). This first measurement is only an estimate of the R-R interval, as points A and B in Fig. 5.10. do not correspond to the true measurement points C and D.

As will be described shortly, during the measurement of the QRS complex width, the position and amplitude of the minimum and maximum values in the QRS complex (C,D,E and F) are easily located. Therefore, the differences that exist between the positions A and C, and B and D can be calculated as each beat occurs. These parameters are defined as follows :-

$$\text{OFFSET OLD} = \text{OFSETO} = A - C \quad (5.19.)$$

$$\text{OFFSET NEW} = \text{OFSETN} = B - D \quad (5.20.)$$

Therefore, to calculate the true R-R interval, the following calculation is performed.

$$\text{TRUE R-R} = \text{RRC} + \text{OFSETO} - \text{OFSETN} \quad (5.21.)$$

As each new beat occurs, the previous OFSETN value becomes the OFSETO value.

This approach was adopted because the parameter RRC was available as it was required to perform the monitoring requirements that,

(1) If $\text{RRC} < 32$ sample periods, no QRS complexes may be detected.

(2) If $\text{RRC} > \text{Maximum R-R limit}$ (such as 6 seconds = 1500 sample periods) is an alarm condition, and also that the parameter OFSETN is easily obtained once the QRS width measurement is performed. Performing the calculation given by equation 5.21. is then quicker than a completely separate measurement of the R-R interval by additional software using the stored ECG signal, plus the fact that the ECG storage buffer would have to be long enough (6 seconds = 1500 bytes) to accommodate the longest allowable R-R interval.

5.3.2. QRS Complex Width Measurement

The measurement of the QRS complex width, as illustrated in Fig. 5.10., was initially defined as the interval between the zero cross over points indicated by G and H. However, it was found that in some of the recorded ECGs, the signal would approach these points but remain just above or below the

cross-over point for a few extra sample periods. This resulted in a number of normal QRS complexes being labelled as wide. In an attempt to stop this situation, small thresholds were set at points G and H as shown in Fig. 5.11., to replace the zero crossover reference points. These thresholds were set to +5 quantization units for the positive threshold, and -5 units for the negative threshold, which in each case corresponds to approximately a 4% shift from the zero reference measurement points. The result of this new threshold approach was that QRS complexes previously incorrectly classified as wide were classified as normal. At the present time these threshold values are fixed, but if it was desirable they could easily be made operator adjustable parameters.

When a QRS complex has been detected, the monitoring function waits until the ECG signal passes through zero again, or until a counter estimating the QRS complex width exceeds the value for a wide complex. The algorithm which then measures the QRS complex width, functions as follows. First the position and amplitude of the minimum (MINP and MINV) and maximum (MAXP and MAXV) values within the QRS complex are found (Fig. 5.11.). A count is then made of the number of sample periods between MINP and the negative threshold, and similarly from MINP until the sample values pass down through the positive threshold. As this count is generated it is compared with the maximum count

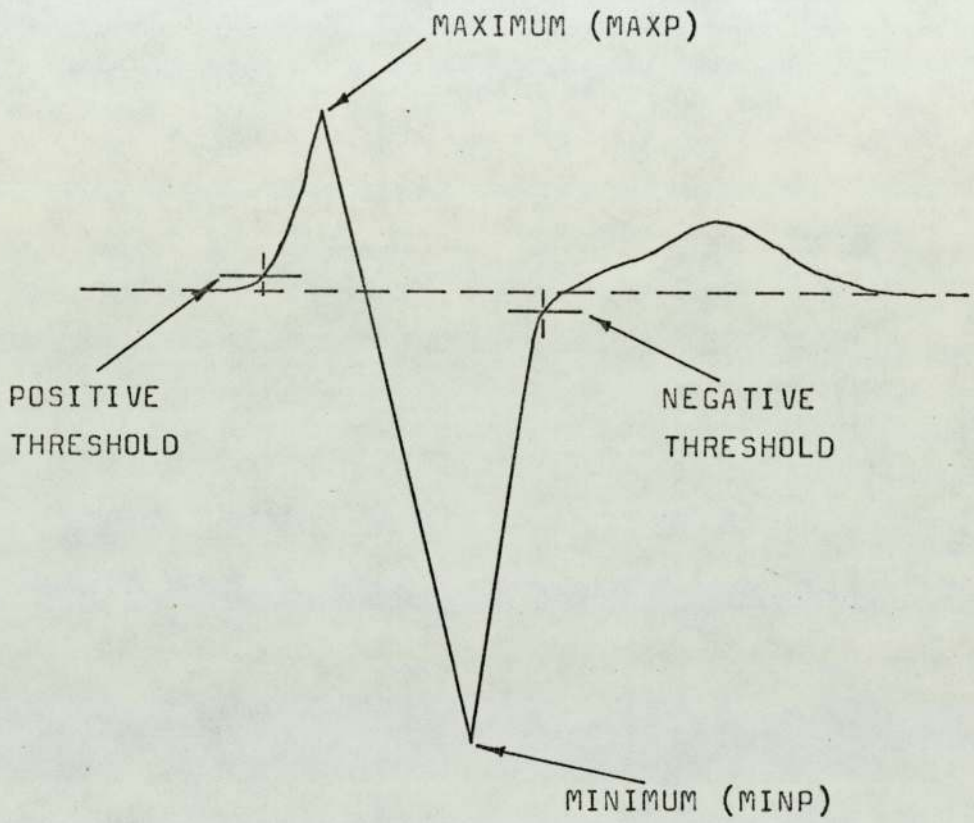


Fig. 5.11. THRESHOLD MEASUREMENT OF QRS
COMPLEX WIDTH

required to classify the complex as wide ($112\text{ms}=28$). If this value is exceeded the width measurement algorithm finishes and labels the complex as wide.

5.3.3. Wide QRS Percentage Calculation

Having classified the current QRS complex as normal or wide, the next operation performed by the monitoring function is to determine the percentage of wide QRS complexes. No definition of how this should be calculated was given in the criteria given by Rabin et. al., therefore the approach adopted for the microprocessor system is as follows. In order that this percentage should be a reasonably sensitive parameter it was decided that it should be calculated from 200 to 400 of the most recent beats. This was accomplished by using two pairs of accumulators, T1 and W1, and T2 and W2; where the T accumulators count the beats as they occur, up to a maximum of 200 each, and the W accumulators count the number of wide beats contained in the corresponding T accumulator. Therefore, the procedure was to increment T1 as each beat occurred, at the same time W1 would be incremented if the beat was classified as wide. Then when T1 became greater than 200, T2 and W2 would be set to zero and subsequently incremented as were T1 and W1. When T2 then exceeded 200, T1 and W1 would be set to zero and subsequently incremented, and so the process continues. Then as each beat occurred, the percentage

of wide complexes would be calculated as

$$\frac{W1 + W2}{T1 + T2} \times 100 = \text{Percentage of wide complexes} \quad (5.22.)$$

5.3.4. R-R Interval Classification

The R-R interval classification algorithm is concerned with labelling each R-R interval as either very long, long, short or normal.

An R-R interval is classified as very long, if the current R-R interval is greater than twice the average value.

The classification of intervals as long or short is via the equations illustrated in Fig. 2.2. In the simple case when the pulse rate is greater than 120 beats per minute, the tolerance (IER) on the current R-R interval is calculated as

$$IER = \frac{ISAMP}{12} \quad (5.23.)$$

where ISAMP is the average R-R interval.

When the pulse rate is less than 120 beats per minute, the tolerance (IER) is calculated as

$$IER = ISAMP \left(\frac{1}{8} - \frac{RATE}{2880} \right) \quad (5.24.)$$

The RATE parameter in the above expression can be expressed in terms of the average R-R interval by

$$RATE = \frac{250 \times 60}{AVRR} = \frac{15000}{AVRR} \quad (5.25.)$$

where AVRR is the average number of sample periods in

the R-R intervals.

Similarly ISAMP may be expressed as :-

$$ISAMP = \frac{AVRR}{250} \quad (5.26.)$$

Combining these equations gives,

$$IER = \frac{AVRR}{250 \times 8} - \frac{15000}{2880 \times 250} \quad (5.27.)$$

If IER is expressed in terms of the number of sample periods then,

$$IER = \frac{AVRR}{8} - 5.2 \quad (5.28.)$$

Approximating the coefficient in equation 5.28., to produce an expression easily and quickly performed by the microprocessor gives,

$$IER = \frac{AVRR}{8} - 5 \quad (5.29.)$$

An R-R interval is then classified as long if,

$$RRC > AVRR + IER \quad (5.30.)$$

or short if,

$$RRC < AVRR - IER \quad (5.31.)$$

where RRC is the number of sample periods in the current R-R interval.

Between these two limits the R-R interval is classified as normal.

5.3.5. Sequence Pattern Recognition

At this stage in the monitoring program, three workspace registers contain sequence information as

follows :-

RO = LONG R-R interval sequence bit flags
R1 = SHORT R-R interval sequence bit flags
R2 = WIDE QRS sequence bit flags

The information stored in each of these registers is obtained as follows. As each QRS complex is detected, all three registers are shifted left by one bit. Then, for example, if the QRS width algorithm finds the complex is wide, the least significant bit in register R2 is set to a one. The information stored in registers R0 and R1 is generated in a similar manner by the R-R interval classification algorithm. There is no need for a register to indicate normal R-R intervals, as this is indicated by zeros occurring in corresponding bit positions of registers R0 and R1.

The sequence pattern recognition algorithm, therefore uses these three registers to detect the sequences of long (L), short (S) or normal (N) R-R intervals, and wide QRS complexes (WQRS) that are specified in the diagnosis criteria of Table 2.1. A list of these sequences is given in Table 5.2. using a shorthand notation where, for example, a sequence consisting of a short R-R interval (S), followed by a wide QRS complex (WQRS), followed by an R-R interval which is not short (\bar{S}), all repeated 4 times, is written as, $4(S \rightarrow WQRS \rightarrow \bar{S})$.

The approach used to produce the sequence

SEQUENCES

- (1) $4(S \rightarrow \bar{S})$
- (2) $4(S \rightarrow WQRS \rightarrow \bar{S})$
- (3) $4(S \rightarrow \bar{S} \rightarrow N)$
- (4) $4(S \rightarrow WQRS \rightarrow \bar{S} \rightarrow N)$
- (5) $S \rightarrow \bar{S} \rightarrow S$
- (6) $S \rightarrow \bar{S} \rightarrow N \rightarrow \bar{L}$
- (7) $3(S) \rightarrow WQRS$
- (8) $S \rightarrow \bar{S} \rightarrow L$
- (9) $S \rightarrow \bar{S} \rightarrow N \rightarrow L$

TABLE 5.2. Sequence of R-R Intervals and QRS Complex Width to be Detected.

recognition algorithm, was the use of assembly language instructions capable of detecting bit patterns in words (compare ones corresponding (COC) and Compare zeros corresponding (CZC)). (Ref.58.).

The algorithm is structured such that certain simple comparisons eliminate groups of sequences if not present, as illustrated by the basic flow diagram given in Fig. 5.12. The "X" shown in some of the decision boxes in Fig. 5.12., indicate that these intervals are not tested at that point in the algorithm.

5.3.6. Monitoring Function Output

The output from the monitoring function is in the form of two 16 bit words (MF1 and MF2). The individual bits of each word indicates the true (1) or false (0) results from the various monitoring algorithms. The condition indicated by each of these bits, is given in Table 5.3.; and it is these two words which are supplied to the diagnosis function.

The program modules which combine to give the monitoring results for the initial monitoring criteria (section 2.5.1.), have program module identifiers MONTDP, MONS1P and MONS2P, as supplied in the program appendix.

5.3.7. Alternative Monitoring Criteria

The monitoring function produced for the alternative monitoring criteria (section 2.5.2.) is an



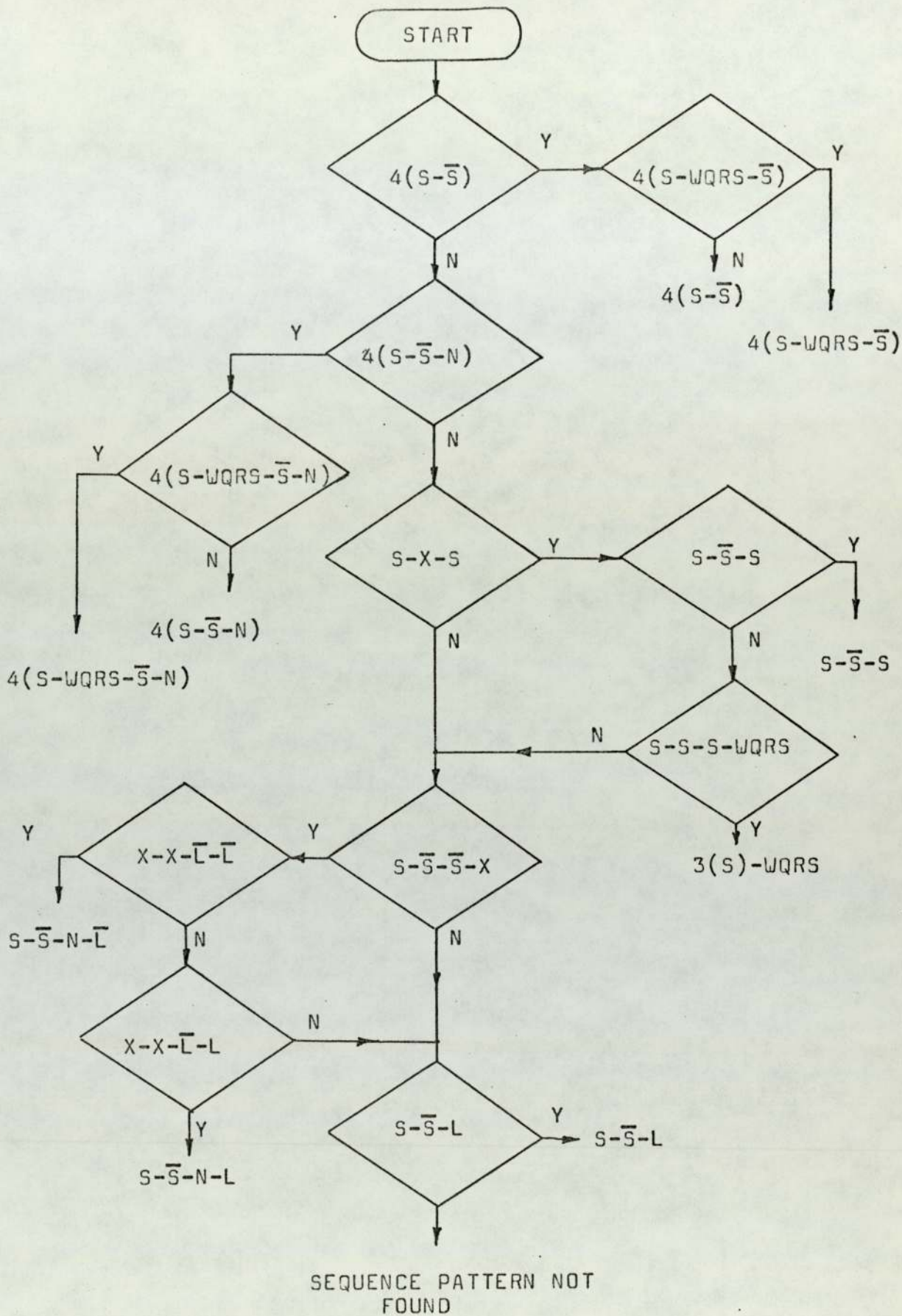


Fig. 5.12 BASIC FLOW DIAGRAM OF SEQUENCE
DETECTION ALGORITHM

EVENT WORD MF1	WORD 1 SET BIT
PULSE RATE IS GREATER THAN 140 BEATS PER MINUTE	0 *
PULSE RATE IS GREATER THAN 110 BEATS PER MINUTE	1
PULSE RATE IS GREATER THAN 100 BEATS PER MINUTE	2
PULSE RATE IS GREATER THAN 90 BEATS PER MINUTE	3
PULSE RATE IS GREATER THAN 80 BEATS PER MINUTE	4
PULSE RATE IS GREATER THAN 60 BEATS PER MINUTE	5
PULSE RATE IS GREATER THAN 40 BEATS PER MINUTE	6
PULSE RATE IS GREATER THAN 20 BEATS PER MINUTE	7 *
	8 *
NO QRS COMPLEX DURING THE LAST 6 SECONDS	9
CURRENT R-R INTERVAL IS \geq TWICE THE AVERAGE	10
CURRENT R-R INTERVAL IS LONG	11
CURRENT R-R INTERVAL IS SHORT	12
CURRENT QRS COMPLEX IS WIDE	13
MORE THAN 82% OF PREVIOUS QRS COMPLEXES ARE WIDE	14 *
	(MSB) 15 *
EVENT WORD MF2	WORD 2 SET BIT
A SEQUENCE 4(S \rightarrow \bar{S}) HAS OCCURRED	0
A SEQUENCE 4(S \rightarrow \bar{WQRS} \rightarrow \bar{S}) HAS OCCURRED	1
A SEQUENCE 4(S \rightarrow \bar{S} \rightarrow N) HAS OCCURRED	2
A SEQUENCE 4(S \rightarrow \bar{WQRS} \rightarrow \bar{S} \rightarrow N) HAS OCCURRED	3
A SEQUENCE S \rightarrow \bar{S} \rightarrow S HAS OCCURRED	4
A SEQUENCE S \rightarrow \bar{S} \rightarrow N \rightarrow \bar{L} HAS OCCURRED	5
A SEQUENCE 3(S \rightarrow \bar{WQRS}) HAS OCCURRED	6
A SEQUENCE S \rightarrow \bar{S} \rightarrow L HAS OCCURRED	7
A SEQUENCE S \rightarrow \bar{S} \rightarrow N \rightarrow L HAS OCCURRED	8
	9 *
	10 *
	11
	12
	13
	14
	(MSB) 15

* These bits have a different meaning when the alternative monitoring criteria are used.

TABLE 5.3. TESTS PERFORMED IN ECG MONITORING FOR INITIAL DIAGNOSIS CRITERIA.

adaptation of the initial monitoring function.

Consider the numbered process boxes shown in the basic flow diagram of the monitoring function Fig. 5.13. The modifications that were made to these processes, to produce the alternative monitoring function were as follows.

Process 1. Initial Value For the Average R-R Interval

The initial value for the average R-R interval (AVRR), is calculated from the first 16 R-R intervals received, when the monitoring function is started. This replaces the original approach which was to use the first R-R interval measured, as the initial average value.

Process 2. Setting of Pulse Rate Flags in MF1

Certain new pulse rate flags were introduced into the monitoring result word MF1, as specified in Table 5.4.

Process 3. QRS Widths Measurement

The QRS complex width limit, used to classify complexes as wide or normal, was increased from 112mS (28 sample periods) to 120mS (30 sample periods).

Process 4. Percentage of QRS Complexes Wide

This process was not required for the alternative monitoring function, so it was removed.

Process 5. Calculation of True R-R Interval

This process remained unchanged.

Process 6. Classification of R-R Intervals

The classification of R-R intervals as long or

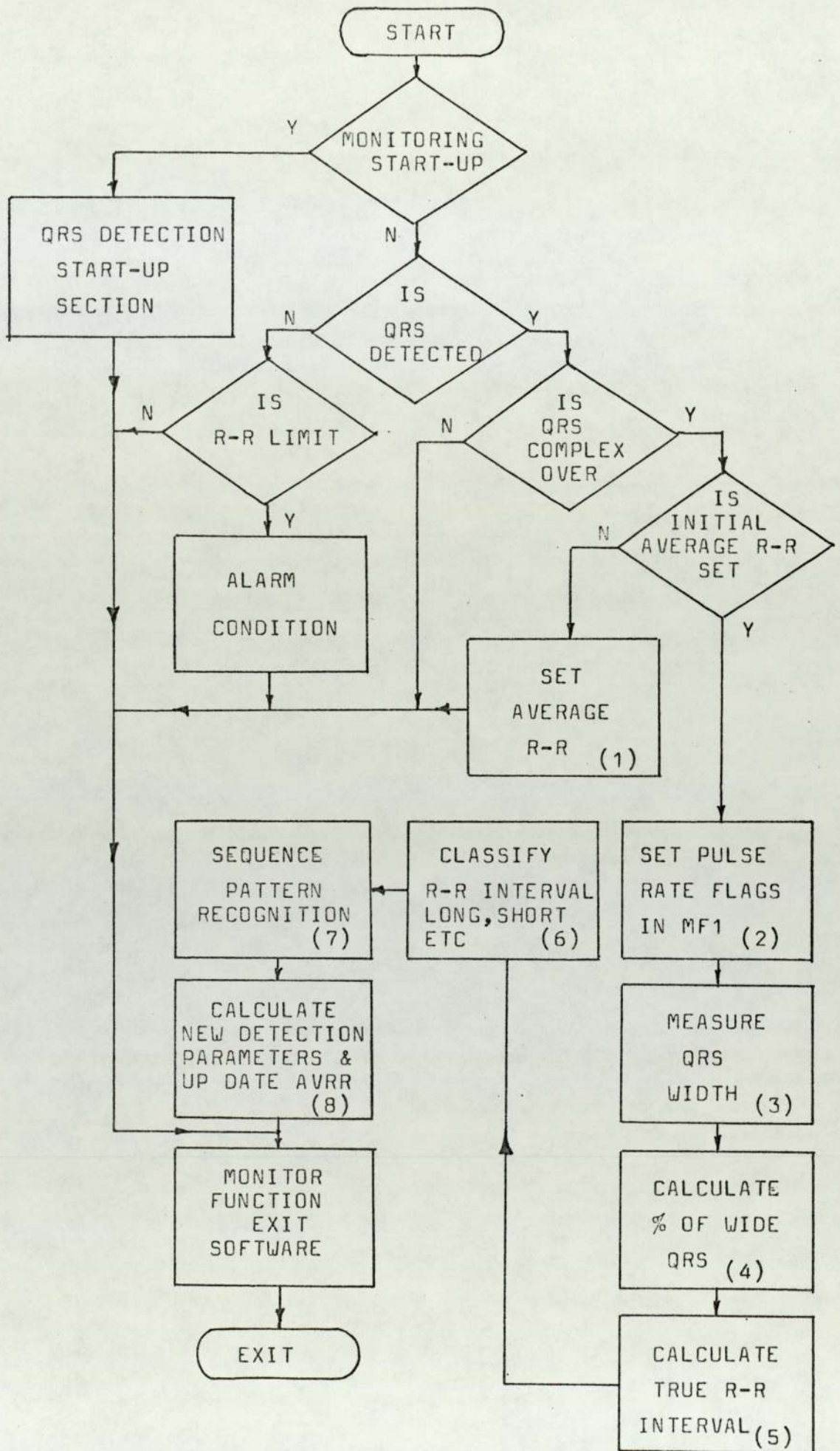


Fig. 5.13. BASIC FLOW DIAGRAM OF MONITORING FUNCTION.

short was changed, and in place of equations 5.23. and 5.29. previously used, a constant $\pm 15\%$ tolerance on the average R-R interval was adopted.

Process 7. Sequence Pattern Recognition

The sequence pattern recognition section was expanded to include the new sequences of (S - \bar{S}) and (S - S).

Process 8. Parameter Up-dating

The average R-R interval (AVRR) is calculated from the 16 most recent normal R-R intervals.

All modifications to the monitoring result words MF1 and MF2 for the alternative monitoring function are given in Table 5.4.

The program modules which combine to produce the alternative monitoring function, have program module identifiers of MONTDP, MONS3P and MONS4P as supplied in the program appendix.

5.4. Diagnosis Function

The diagnosis function is concerned with the recognition of specific arrhythmias from the bit patterns contained in the monitoring result words (MF1 and MF2).

The technique used to implement this function was a decision table type of approach (Ref.54.55.) A decision table is structured as shown in Table 5.5., where in the diagnosis function implementation, the condition stub contains the monitored events, such as "R-R interval long", and the condition body contains

EVENT WORD MF1	WORD 1 SET BIT
PULSE RATE IS GREATER THAN 150 BEATS PER MINUTE	0
PULSE RATE IS GREATER THAN 30 BEATS PER MINUTE	7
CURRENT R-R INTERVAL IS LESS THAN 600ms	8
NOT USED	14
PULSE RATE IS GREATER THAN 200 BEATS PER MINUTE	15
EVENT WORD MF2	WORD 2 SET BIT
A SEQUENCE S - \bar{S} HAS OCCURRED	9
A SEQUENCE S - S HAS OCCURRED	10

TABLE 5.4. MODIFICATIONS TO MONITORING RESULT WORDS
(TABLE 5.3.) FOR ALTERNATIVE MONITORING
CRITERIA.

CONDITION STUB	CONDITION BODY			
CONDITION 1	Y	Y	N	N
CONDITION 2	Y	N	-	N
ACTION 1	X			
ACTION 2		X		
ACTION 3			X	
ACTION 4				X
ACTION STUB	ACTION BODY			

TABLE 5.5. EXAMPLE DECISION TABLE.

the condition requirements of yes (Y), no (N), or a dash which means either (Y or N). The action stub is then either a diagnosis or an instruction, which are matched to the conditions via the "X"s in the action body.

One of the most important rules, when using decision tables is that relating to "ambiguity" (Ref.54.). This rule simply states that no two sets of conditions, in the condition body, can be the same. For example, in Table 5.5., there is "ambiguity" between action 3 and 4, due to the dash in the condition body. This particular "ambiguity" could be resolved by either substituting a "Y" for the dash, or combining actions 3 and 4.

When trying to convert the initial arrhythmia criteria given in Table 2.1., into a decision table, it was found that the 23 different diagnoses given were not all mutually exclusive. Therefore, in terms of producing a single decision table, this would result in the type of "ambiguities" described previously. The approach adopted therefore was the production of a number of small decision tables that could be used, and which did not contain ambiguities. Also, as there was some doubt about the final diagnosis criteria that was to be used by the system, only 8 of the arrhythmia diagnoses were used to produce the first diagnosis program from decision tables. The remaining diagnoses would then have been incorporated into this diagnosis

program, if this particular set of criteria was that chosen for use in the final system.

The resulting decision tables produced to diagnose 8 different arrhythmias are shown in Table 5.6. Using these tables, the first diagnosis program was produced, and is supplied in the program appendix under the program module identifier DIAT1P.

Although this program was produced from decision tables, it was apparent that the initial arrhythmia criteria did not lend themselves easily to decision table implementation. This is due mainly to the fact that the diagnoses were not specified so that they were mutually exclusive.

However, the alternative arrhythmia criteria given in Table 2.2., required only two decision tables for complete classification, as shown in Table 5.7. Using these decision tables, the alternative diagnosis program was produced much more easily, and is supplied in the program appendix under the program module identifier DIAT2P.

The output from the first diagnosis program is two 16 bit words (DF1 and DF2), the individual bits of which indicate, if set to a one, which arrhythmias have been diagnosed, as shown in Table 5.8. The output from the alternative diagnosis program is a single 16 bit word, the individual bits of which indicate the arrhythmias diagnosed and the corresponding alarm status etc. as shown in Table 5.9.

TABLE 1

IS PR 80 BPM	N	Y	-
NO QRS FOR 6 SEC	Y	Y	N
CARDIAC ARREST	X		
LOST SIGNAL		X	
GO TO TABLE 2			X
EXIT FUNCTION	X	X	

TABLE 2

IS PR 60 BPM	N	N	Y	-
IS PR 40 BPM	Y	N	Y	-
IS PR 20 BPM	Y	Y	Y	-
BRADYCARDIA	X			
IDIOVENTRICULAR		X		
GO TO TABLE 3			X	
GO TO TABLE 5	X	X		X

TABLE 3

IS PR 140 BPM	N	Y	-
IS PR 110 BPM	Y	Y	-
ARE 82% QRS WIDE	-	N	-
SUPERVENTRICULAR	X	X	
GO TO TABLE 4	X	X	X

TABLE 4

IS PR 140 BPM	N	-
ARE 82% QRS WIDE	Y	-
BUNDLE BRANCH BLOCK	X	
EXIT FUNCTION	X	X

TABLE 5

IS PR 80 BPM	N	-
IS RR 2.AVRR	Y	-
ASYSTOLE	X	
GO TO TABLE 6	X	X

TABLE 6

IS PR 60 BPM	N	-
WAS R-R LONG	Y	-
WAS QRS WIDE	Y	-
ESCAPE BEAT	X	
GO TO TABLE 4	X	X

TABLE. 5.6. DECISION TABLES USED TO PRODUCE
INITIAL DIAGNOSIS FUNCTION.

TABLE 1

R-R SHORT	Y	Y	Y	Y	N	N	N	N	N	-	-
R-R LONG	N	N	N	N	N	N	Y	Y	Y	-	-
R-R VERY LONG	N	N	N	N	N	N	N	N	Y	-	-
SEQUENCE S-S	Y	Y	Y	Y	N	N	N	N	-	-	-
SEQUENCE S-S̄	N	N	N	N	Y	Y	Y	Y	-	-	-
R-R 5 Sec.	N	N	N	N	N	N	N	N	N	Y	-
R-R 300ms	N	N	Y	Y	N	N	N	N	N	-	-
BROAD QRS (120ms)	N	Y	N	Y	N	Y	N	Y	-	-	-
PAROXYSMAL TACHYCARDIA	X	X	X	X							
PREMATURE BEAT					X	X	X	X			
PAUSE									X		
ASYSTOLE										X	
BROAD QRS		X		X		X		X			
ALARM 1 (HIGH)			X	X						X	
ALARM 2 (LOW)	X	X									
GO TO TABLE 2	X	X	X	X	X	X	X	X	X	X	X

TABLE 2

IS AVRR 400ms	N	Y	N	N	-
IS AVRR 600ms	Y	Y	N	N	-
IS AVRR 1 Sec.	Y	Y	N	N	-
IS AVRR 2 Sec.	Y	Y	Y	N	-
NON-PAROXYSMAL TACHYCARDIA	X	X			
NON-PAROXYSMAL BRADYCARDIA			X	X	
ALARM 2 (LOW)		X			
EXIT PROGRAM					X

TABLE 5.7. ALTERNATIVE DIAGNOSES
DECISION TABLES.

BITSDIAGNOSIS WORD DF1DIAGNOSIS WORD DF2

0		VENTRICULAR TACHYCARDIA		PREMATURE ATRIAL CONTRACTION
1	*	SUPRAVENTRICULAR TACHYCARDIA		PAC RUN
2	*	BUNDLE BRANCH BLOCK		BIGEMINY DUE TO PAC
3	*	BRADYCARDIA		ATRIAL TRIGEMINY
4	*	IDIOVENTRICULAR RHYTHM		ABNORMAL CONDUCTION
5	*	CARDIAC ARREST		SINUS ARRHYTHMIA
6	*	ASYSTOLE		PREMATURE CONTRACTION
7	*	ESCAPE BEAT		ATRIAL FIBRILLATION
8		PREMATURE VENTRICULAR CONTRACTION		ACCELERATED VENTRICULAR RATE
9		RUN OF PVC		SVT WITH ABBERANT CONDUCTION
10		BIGEMINY RHYTHM	*	LOST SIGNAL
11		TRIGEMINY RHYTHM		-
12		-		-
13		-		-
14		-		-
15		-		-

(* Currently implemented)

TABLE 5.8. DIAGNOSIS PROGRAM RESULT WORDS FOR INITIAL ARRHYTHMIA CRITERIA

<u>BIT</u>	<u>DIAGNOSIS WORD DF1</u>
0	NON PAROXYSMAL TACHYCARDIA
1	NON PAROXYSMAL BRADYCARDIA
2	PAROXYSMAL TACHYCARDIA
3	PREMATURE BEAT
4	PAUSE
5	ASYSTOLE
6	-
7	-
8	-
9	-
10	-
11	-
12	-
13	BROAD QRS
14	ALARM 1
15	ALARM 2

TABLE 5.9. ALTERNATIVE DIAGNOSIS PROGRAM
RESULT WORD BIT ASSIGNMENT

5.5. Communications

The communications function is concerned with the transfer of information between the patient-dedicated processor, and the operator-dedicated processor.

In order to minimise the number of wires carrying information between processors, all of which would converge on the operator-dedicated processor, serial asynchronous data channels were adopted. The UARTs (Universal Asynchronous Receiver Transmitter) required for such a communications link, were implemented by dedicated TMS 9902 asynchronous communications controllers, specifically designed for use with the TMS 9900 microprocessor.

The inter-processor communications protocol developed for use in this distributed processor system is described in Chapter 6, and is designed to allow communications to operate without interfering with the real-time processing being performed by the patient-dedicated processors. The information which passes between processors comes in two forms. The first is a single instruction, and the second is an instruction followed by 50 bytes of data, as described in Chapter 6.

Within each patient-dedicated processor system, the use of the UART communications channel is controlled by an operating system program, which is described in Section 5.6.

The remainder of the communications function is

divided into the three tasks of input, output and interpreter (microprocessor communications package), as illustrated in Fig. 5.1.

5.5.1. Input Task

The Input task (program module identifier IPPTOP) is activated by the patient processor operating system, when normal communications protocol start-up procedures have been performed. Having been activated, the input task then proceeds to store the incoming instruction and data (when present) into an input file (IPFILE), transmitting protocol reply characters as required.

On completion of communications, the input task activates the microprocessor communications package task, and then deactivates itself. The basic flow diagram of the input task is shown in Fig. 5.14.

5.5.2. Microprocessor Communication Package

The microprocessor communications package (program module identifier MCPTOP) is concerned with the interpretation of the instructions placed in the communications input file, and the generation of output data for transmission from the patient processor system. For example, the instruction received by the input task and placed in the input file, may be interpreted by this task as being a request for pulse rate data, from the operator processor. Having decoded this instruction, the task then produces the correct reply instruction, and the requested pulse rate data, all of which are placed in an output file

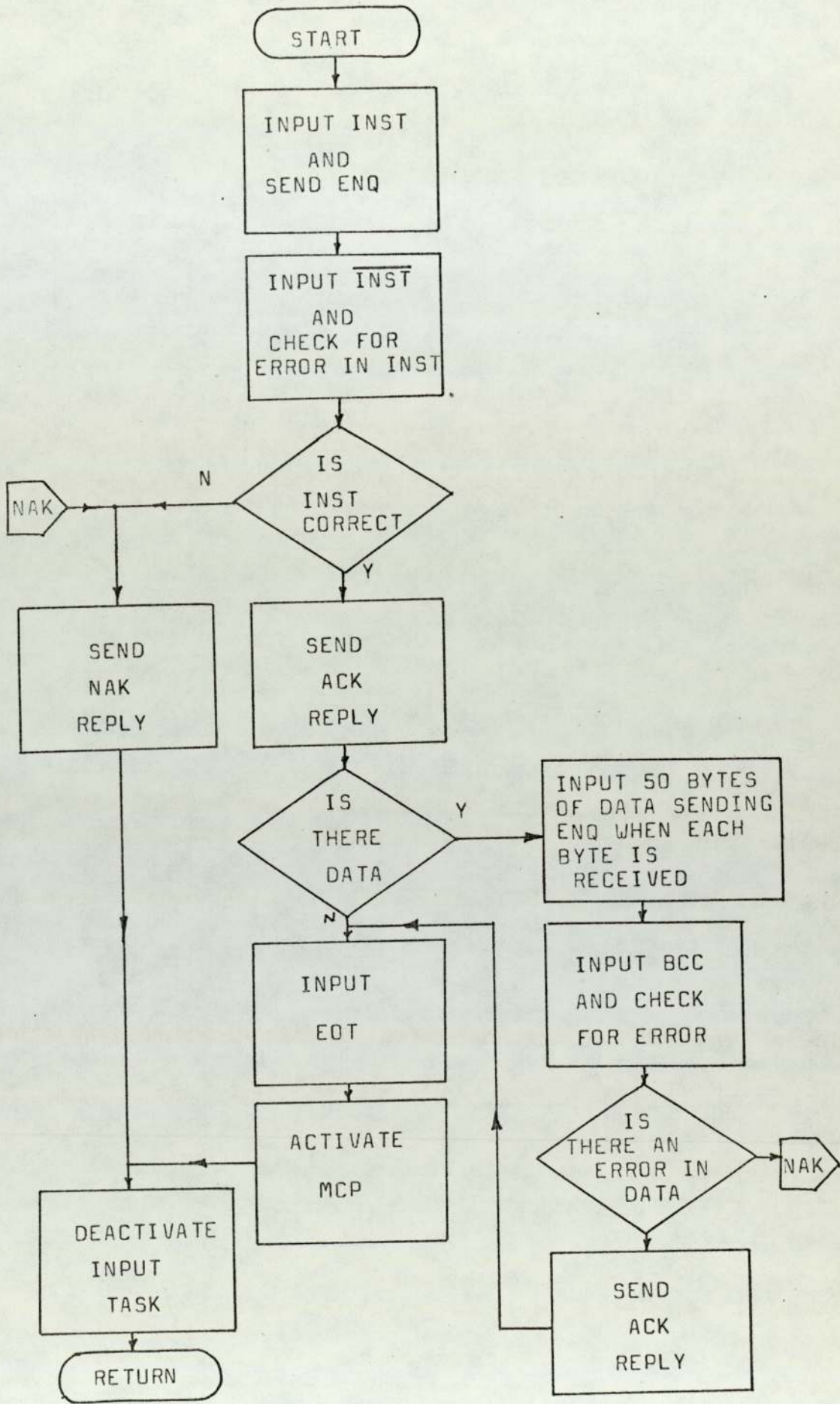


Fig. 5.14. BASIC FLOW DIAGRAM OF INPUT TASK.

(OPFILE). On completion of this operation, the task then goes to the operating system program which controls the use of the UART, so that communications can be established with the operator-dedicated processor, before activating the output task.

If the reply to the operator processor is a single instruction (i.e. no data), the address where the reply instruction is resident in PROM is supplied to the output task.

Before describing the operation of the output task, it should also be noted that the microprocessor communication package program, can also be activated by other system functions (monitoring and diagnosis). This allows messages and data associated with these functions to be sent to the operator processor. The basic flow diagram of the microprocessor communication package is shown in Fig. 5.15.

5.5.3. Output Task

When the output task (program module identifier OPPTOP) has been activated, it uses the address supplied to it, in order to locate the information to be transmitted. In the example given above, this address would be the location of the output file. As the transmission of information is performed by the output task, it waits for communication protocol replies from the operator processor, as described in Chapter 6.

The basic flow diagram of the output task is

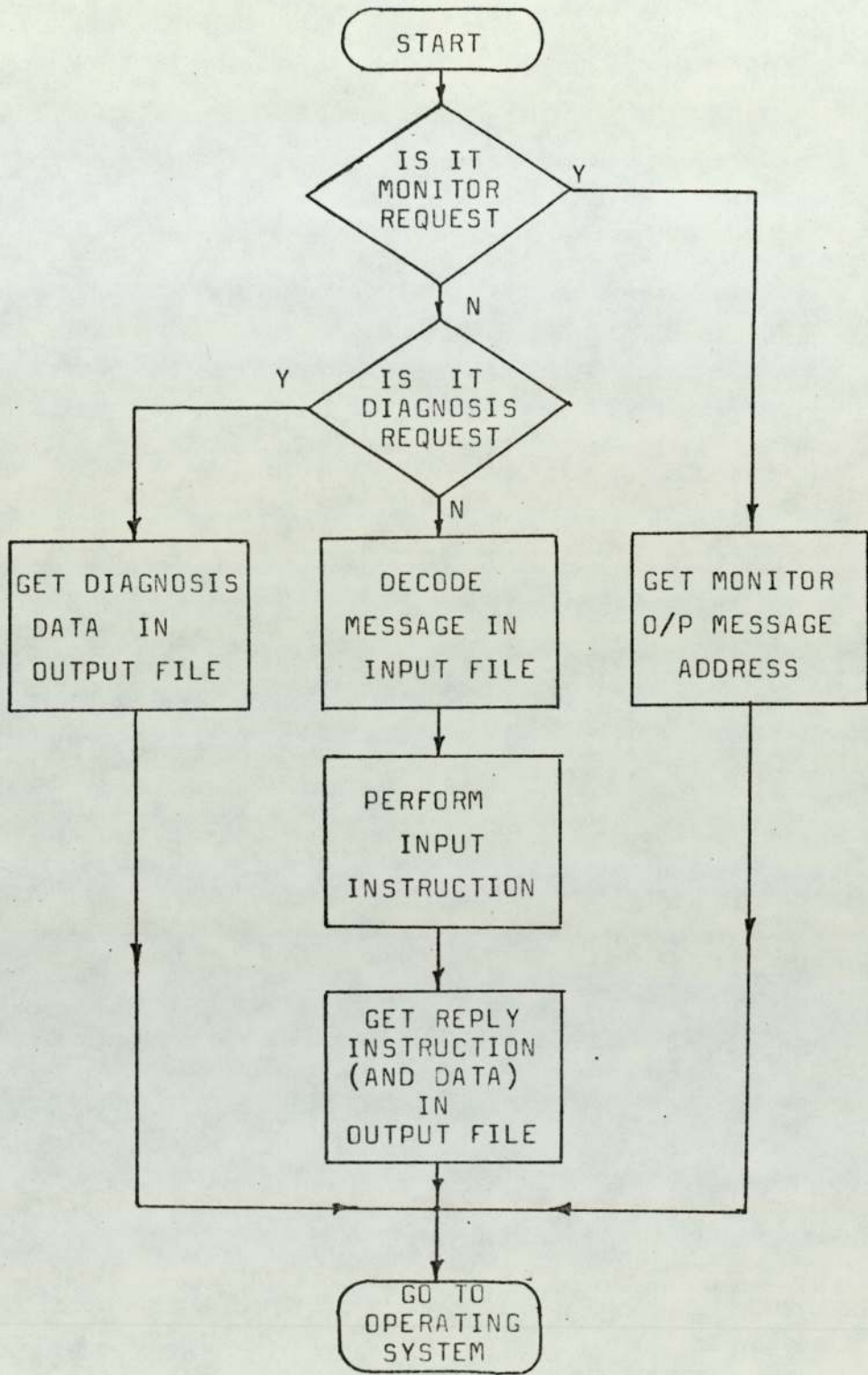


Fig. 5.15. BASIC FLOW DIAGRAM OF THE MICROPROCESSOR COMMUNICATION PACKAGE.

given in Fig. 5.16.

5.6. Control

As can be seen from Fig. 5.1., the operating system of the patient-dedicated processor consist of four programs.

The first of these programs is concerned with the patient processor system initialisation (program module identifier PPINIP), and is performed at system start-up time. The initialisation performed is that of memory (RAM) clearing and software environment setting, and the resetting and programming of hardware interfaces.

The second program module is concerned with handling the interrupt generated by the A to D converter (program module identifier PPCIHP). The function of this program is to determine which one of the 6 tasks, as shown in Fig. 5.1., was interrupted so that the software returns (WP, PC, and ST) (Ref.58.) can be saved, and the particular task concerned set suspended. Having done this the program then activates the signal conditioning task, and passes control to the real-time task scheduler program. Also during the operation of this program the time, since system start-up, is calculated using the 4mS interval of the ADC interrupt. The basic flow diagram of this program is shown in Fig. 5.17.

The real-time task scheduler program (program module identifier PPTHAP) is concerned with determining which of the 6 tasks should next be performed. The 6 tasks have different priorities, the highest being

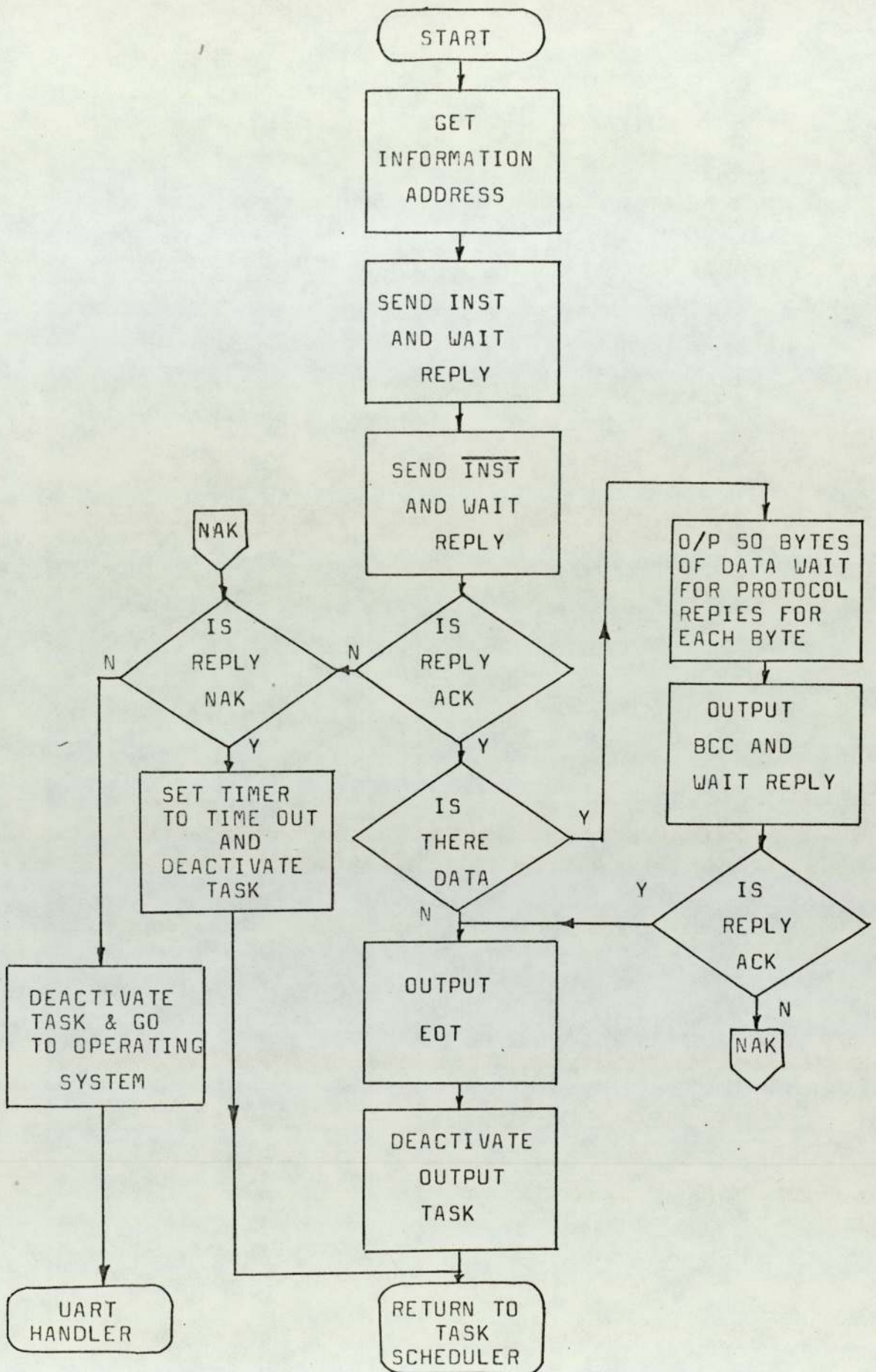


Fig. 5.16. BASIC FLOW DIAGRAM OF OUTPUT TASK

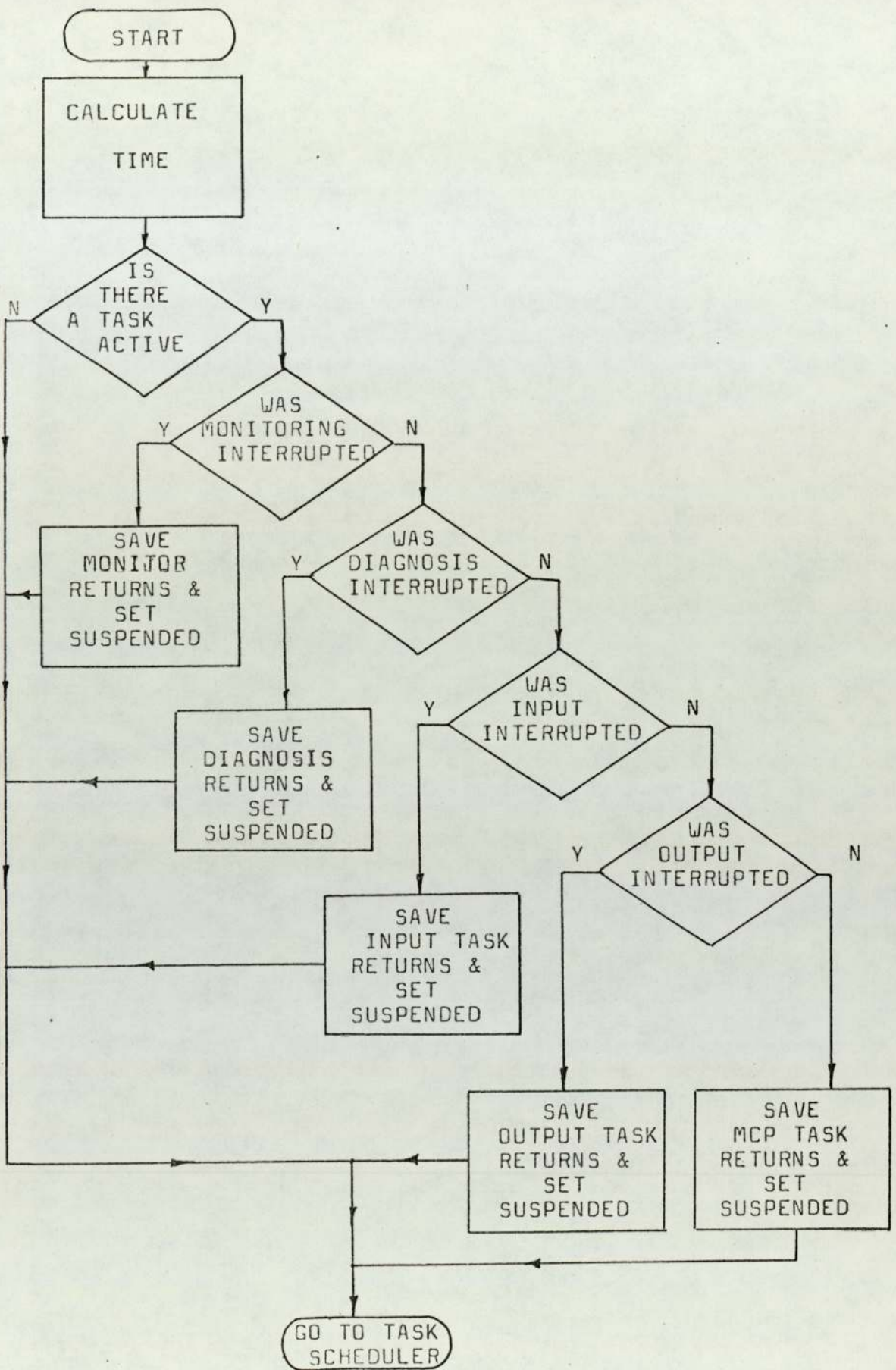


Fig. 5.17. BASIC FLOW DIAGRAM OF ADC INTERRUPT HANDLING PROGRAM.

signal conditioning as this consumes 25% of processing time (Table 4.1.). Having found an active task the scheduler program tests if the appropriate task is in a suspended state, having been previously interrupted, and passes control to the task accordingly. The basic flow diagram of the real-time task scheduler program is given in Fig. 5.18.

The fourth and final program which makes up the patient processor operating system, is the UART interrupt handling program (program module identifier PPUIHP).

This program performs the complex functions of :-

- (1) Establishing inter-processor communications.
- (2) Activating input or output tasks as and when required.
- (3) Deactivating input or output task, when an error occurs in the inter-processor communications.
- (4) Handling the TMS 9902 interval timer, to detect the error of excessive delays during inter-processor communication.
- (5) Handling output requests from the microprocessor communication package program.
- (6) Activating suspended output requests from the microprocessor communication package program, which would have been suspended due to input communications.

The basic flow diagram of this program is given in Fig. 5.19, and details of the inter-processor communication protocol developed for use in this distributed processor system is given in Chapter 6.

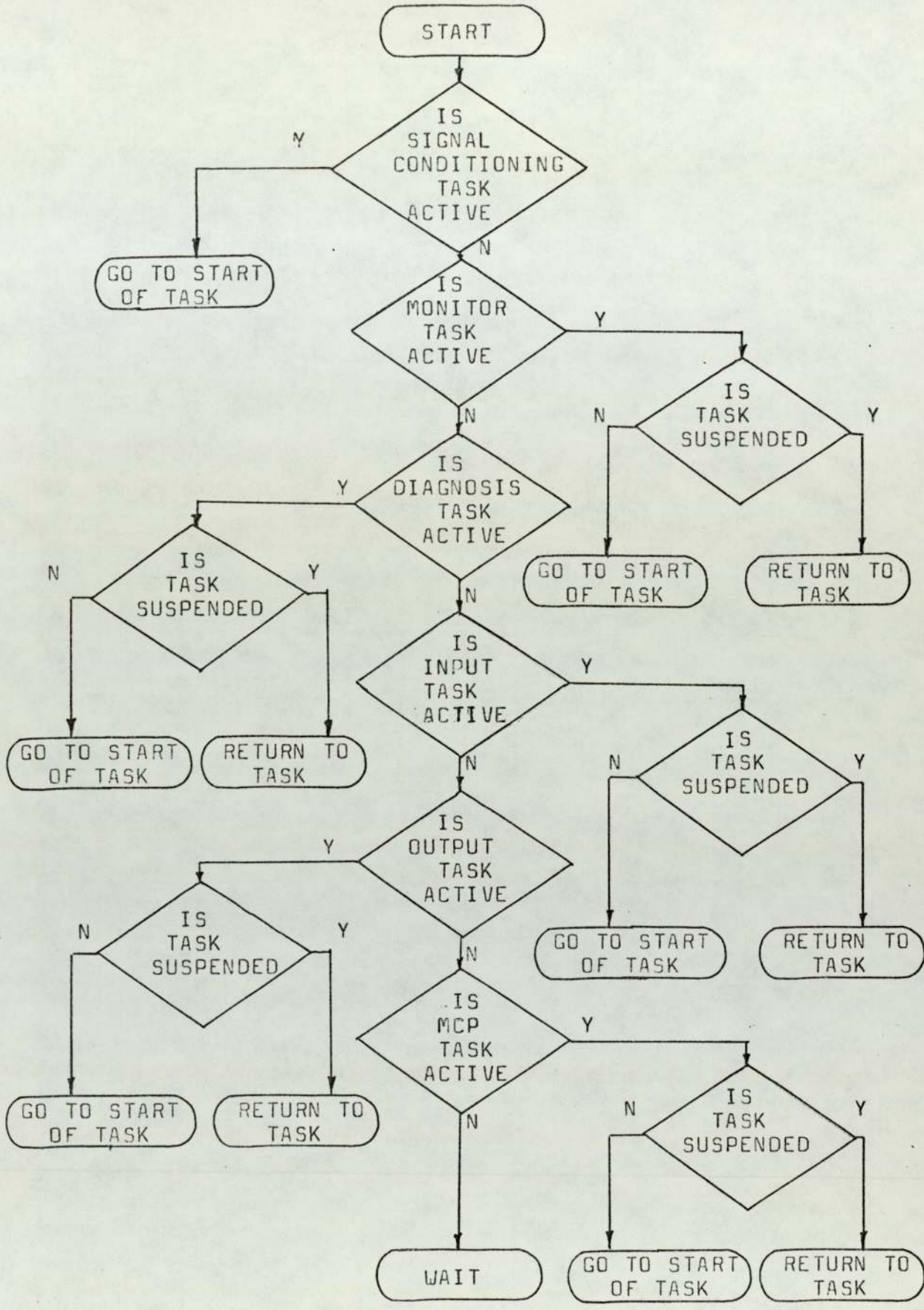


Fig. 5.18. BASIC FLOW DIAGRAM OF REAL-TIME TASK SCHEDULER PROGRAM.

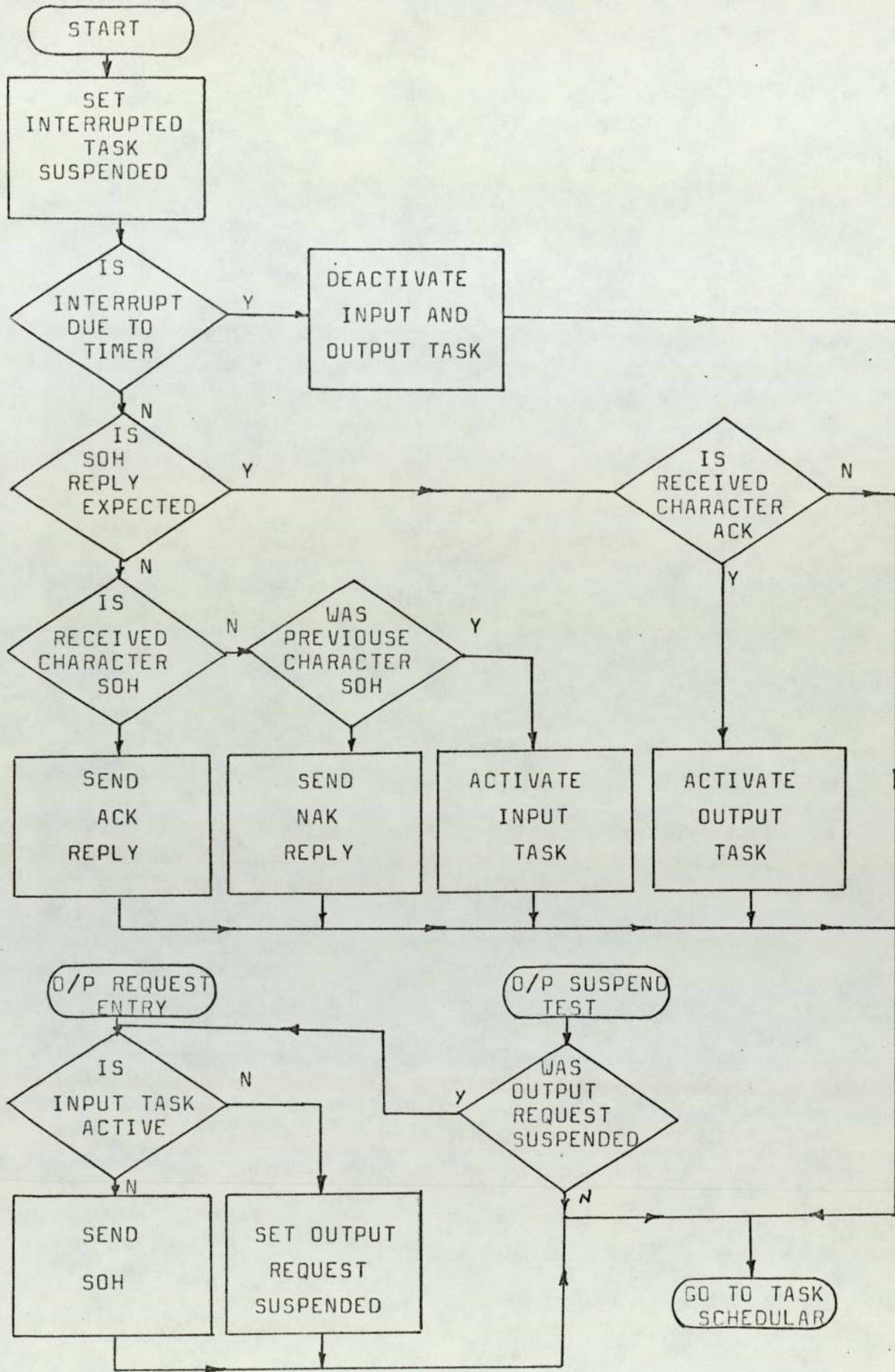


Fig. 5.19. BASIC FLOW DIAGRAM OF UART INTERRUPT HANDLING PROGRAM.

CHAPTER 6

Operator-dedicated Processor System Design

6.1. Introduction

The operator-dedicated processor (also referred to as the nurse station processor in the program appendix) is concerned with the centralised functions of display, storage, overall system control and system/operator communication. The software structure of the operator-dedicated processor system is given in Fig. 6.1., and as can be seen, it is similar to the patient-dedicated processor system. However, in this case the highest priority task is the inter-processor communications input task, and the lowest is the VDU peripheral controller task. The input task has the highest priority, because it is vital that information coming from patient-dedicated processors is handled quickly.

In order to understand the operation of this system, we must consider each of the system tasks in turn, and hence the resulting software control provided by the operator-dedicated processor operating system. However, an important feature which influences the operation of the system, is the inter-processor communication protocol, developed for use in this distributed processor system. Therefore, the inter-processor communications protocol developed will be described first.

6.2. Inter-processor Communications Protocol

The inter-processor communications are provided by

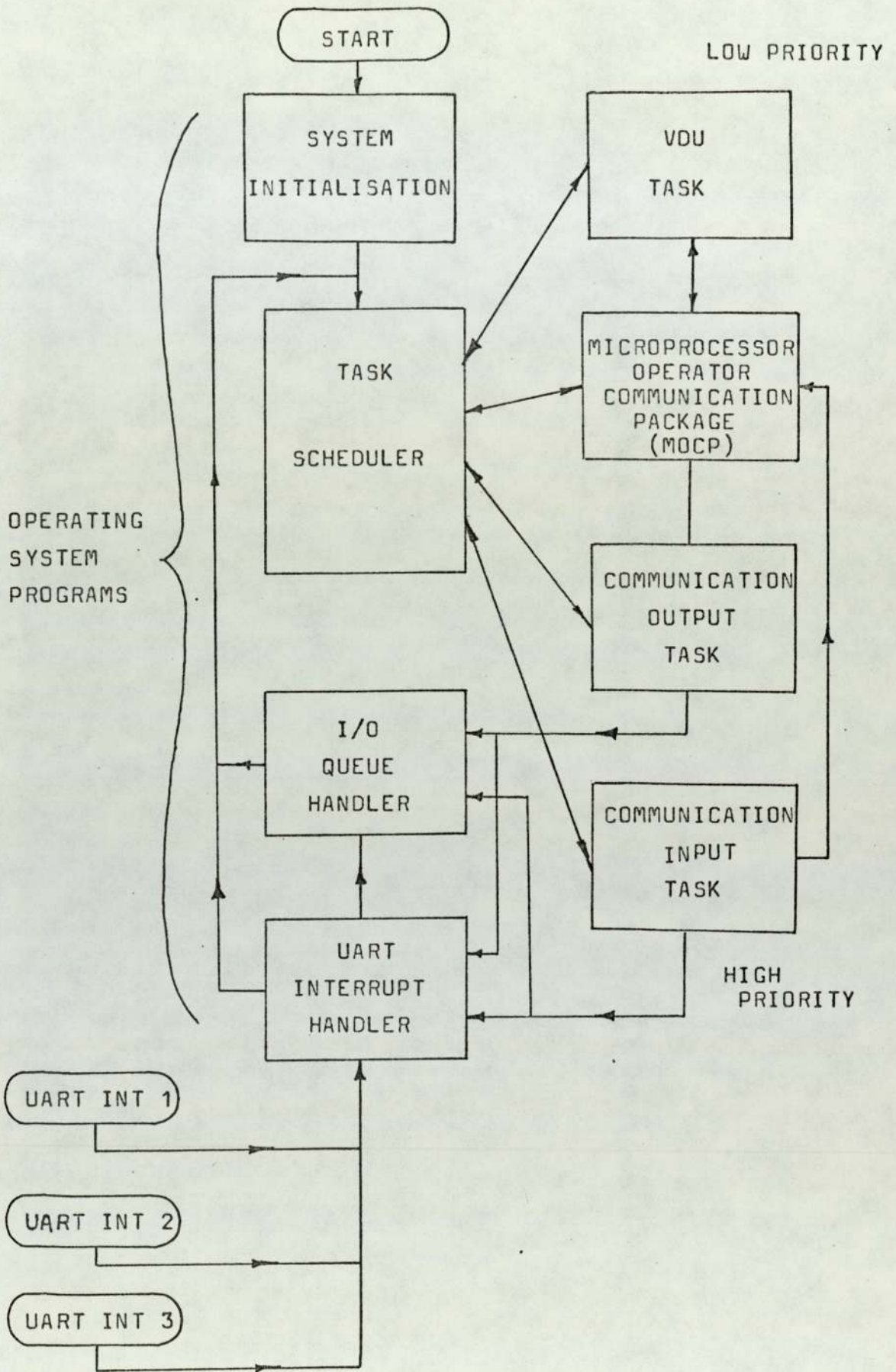


Fig. 6.1 SOFTWARE STRUCTURE OF OPERATOR-DEDICATED PROCESSOR SYSTEM.

serial data links in the form of UARTs (Universal Asynchronous Receiver Transmitters), which are used to transmit bytes of information between processors. This approach was chosen, to reduce the wiring converging on the operator system, and because of the availability of a device; the TMS 9902 asynchronous communication controller, which could provide the serial data links required, and which is specifically designed for use with the TMS 9900 microprocessor.

The aim therefore, was to provide a private serial communication link between each patient-dedicated processor and the operator-dedicated processor, as shown in Fig. 6.2. This structure and the inter-processor communication protocol developed, was influenced by the following important considerations.

- (1) Inter-processor communications should not interfere in the normal real-time processing being performed by each patient-dedicated processor.
- (2) The communications between processors should be as fast as possible. This is not only concerned with the bit rate used by the UARTs, but also with the speed with which the operator processor handles all of the communication channels at its disposal.

The first of these considerations was implemented by giving the patient processor communication function a lower priority than the real-time functions, as described in Chapter 5. However, by doing so one has produced the situation whereby the rate of data received or transmitted

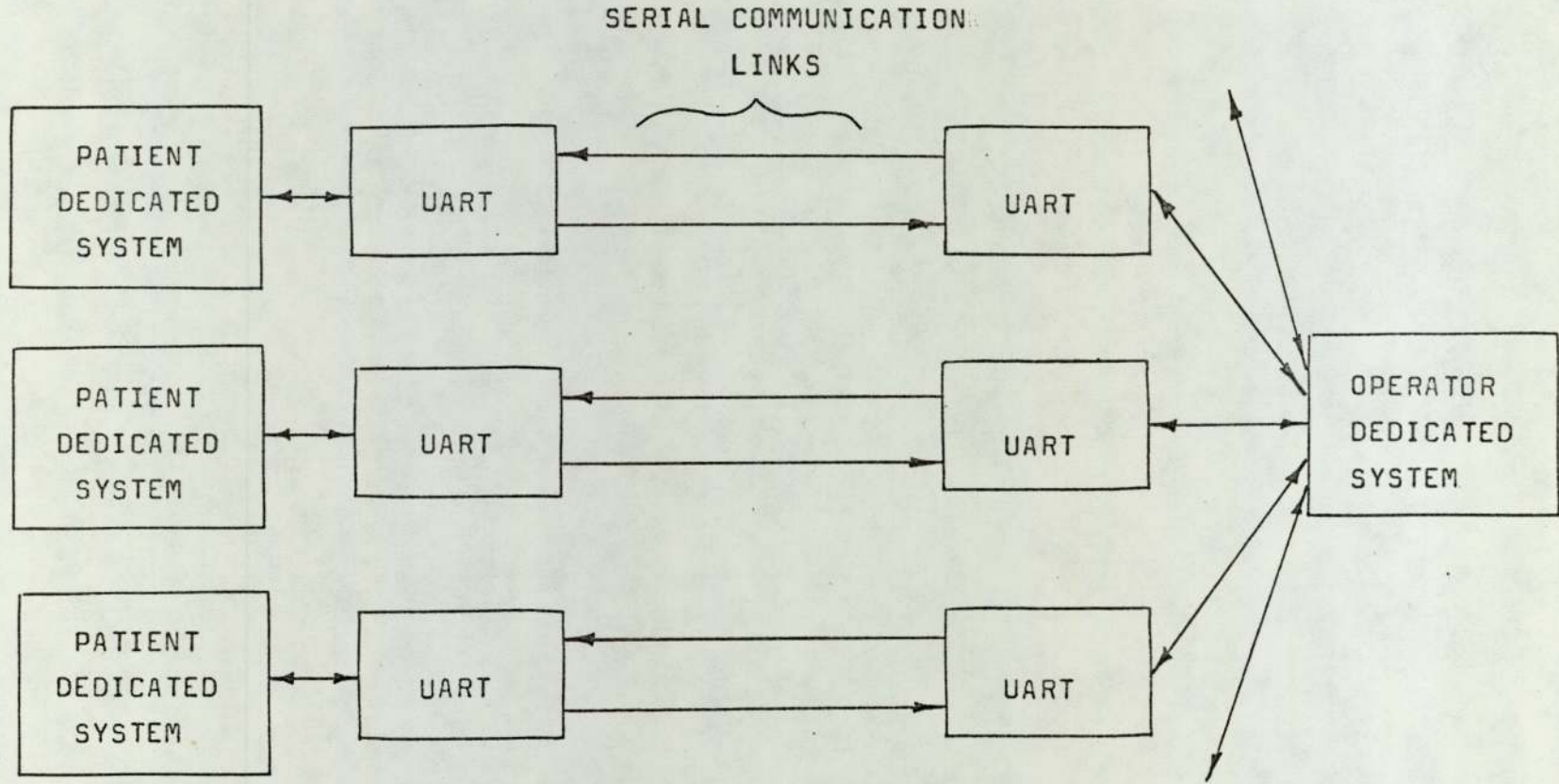


Fig. 6.2. DISTRIBUTED COMMUNICATION SYSTEM.

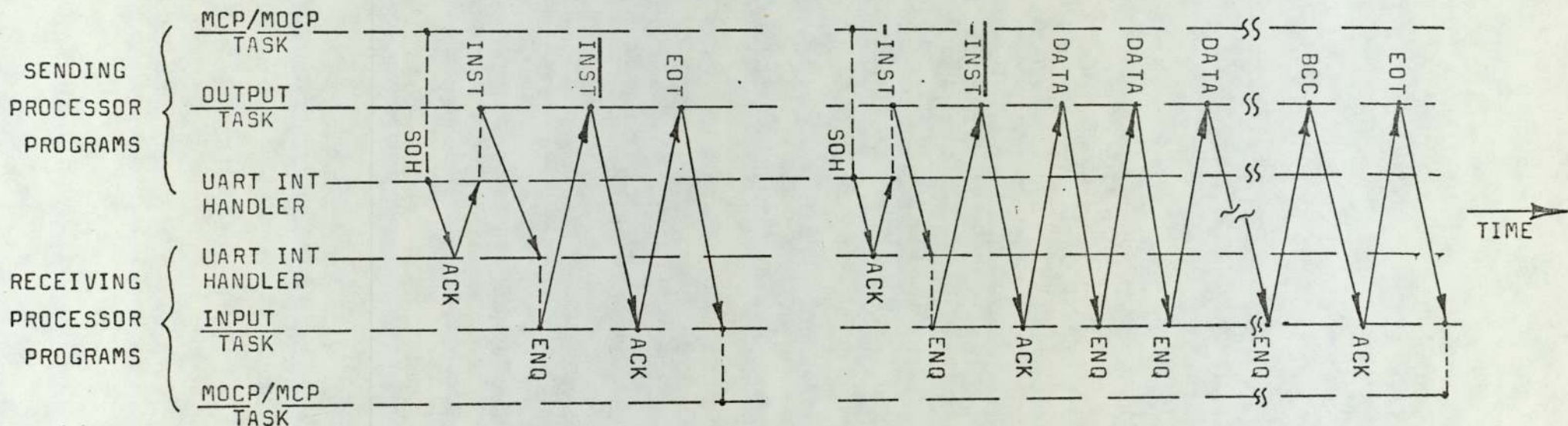
by the patient processor, is influenced by the real-time processing being performed by that processor. Therefore, for example, the operator processor could not transmit a continuous string of characters to the patient processor. This is because overrun errors would occur at the patient processor UART, while the patient processor was performing real-time functions.

The second consideration given above, is concerned with the manner in which the operator processor uses all the inter-processor communication channels. The approach chosen was to allow the operator processor to communicate simultaneously, if necessary, with all the patient-dedicated processors. The information passing between processors would then be handled as and when it occurred, and therefore this approach would make more efficient use of the processing time at the operator processor.

Therefore, the inter-processor communications protocol required, had to cater for all these considerations, and several approaches were considered (Ref. 59,60,61,62.). The final solution is shown diagrammatically in Fig. 6.3. and Fig. 6.4. which indicate the appropriate programs that are active during communications, and the sequence of ASCII control characters (SOH,ACK,NAK,ENQ and EOT) and information characters (INST,INST,DATA,BCC) sent, for correct inter-processor protocol. From Fig. 6.3. it will be seen that communications are established by the UART interrupt handler program of the sending processor, by the transmission of the "start of heading" (SOH) character,

(A) NORMAL TRANSFER OF SINGLE INSTRUCTION.

(B) NORMAL TRANSFER OF INSTRUCTION WITH DATA.



----- PROGRAM TRANSITION (x) → CHARACTER SENT (x)

SOH :-START OF HEADING

EOT :-END OF TRANSMISSION

ACK :-ACKNOWLEDGE

INST :-INSTRUCTION

ENQ :-ENQUIRY

INST ; :-INVERSE OF INST

NAK :-NEGATIVE ACK

BCC :-BLOCK CHECK CHAR

Fig. 6.3. PROTOCOL FOR NORMAL TRANSFER OF INFORMATION.

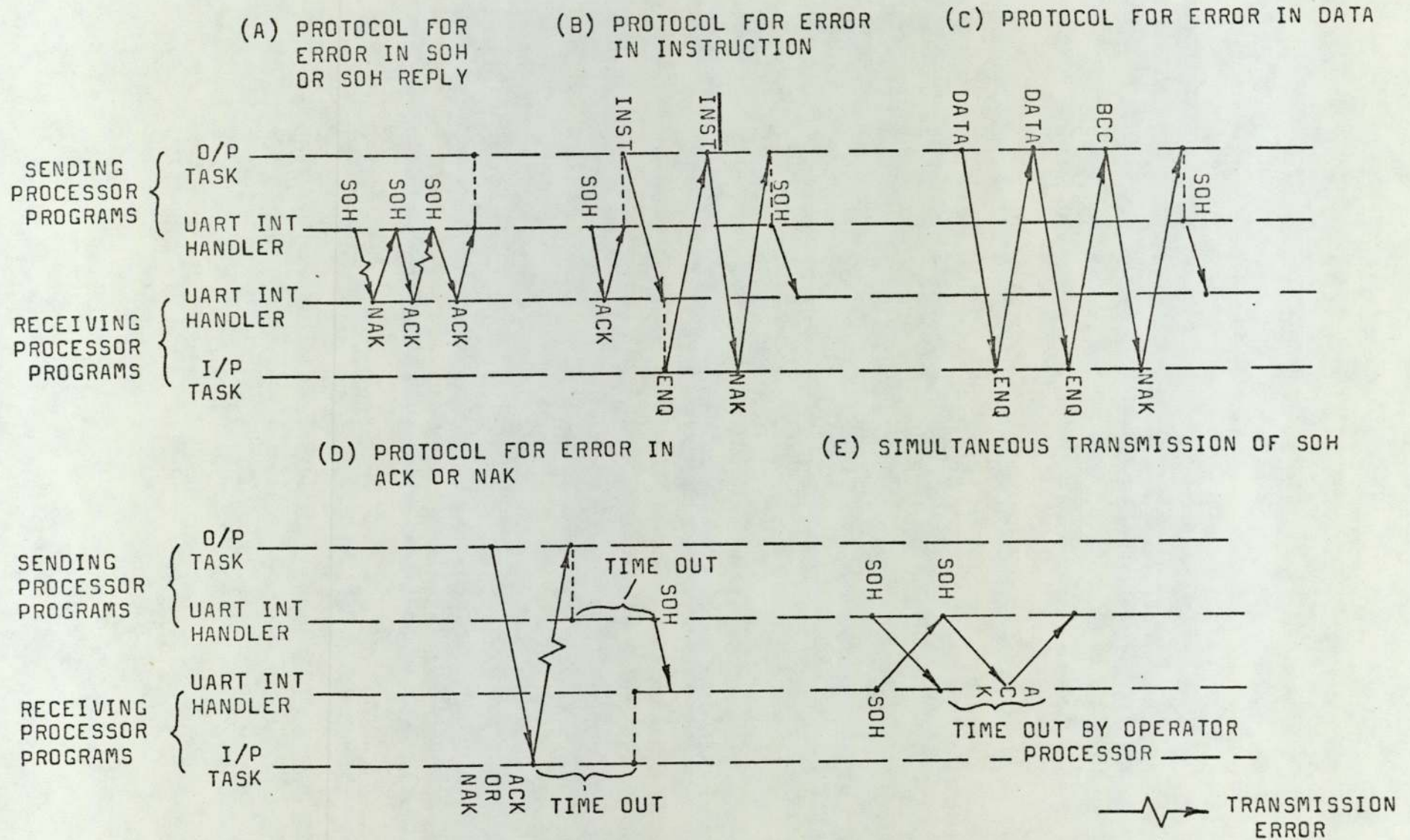


Fig. 6.4. COMMUNICATION PROTOCOL FOR ERROR CONDITIONS.

and the reception of the "acknowledge" (ACK) character. The instruction (INST) and its inverse ($\overline{\text{INST}}$) are then sent by the output task of the sending processor, and received and checked by the input task of the receiving processor. If the instruction is received correctly the input task replies with ACK (Fig. 6.3.), but if there is an error in the instruction the reply is "negative acknowledge" (NAK).

The instructions (INST) sent between processors are arranged such that a positive instruction character indicates that it is only this instruction being sent (Fig. 6.3.(A)). A negative instruction indicates that the instruction is followed by 50 bytes of data (Fig. 6.3.(B)).

On reception of the 50 bytes of data, a block check character (BCC) is sent, which is the sum of the 50 data bytes, without regard to overflow. If this character agrees with the total calculated at the receiving processor, the ACK reply is sent which results in the end of transmission (EOT) reply from the sending processor.

As can be seen from these diagrams, the inter-processor communications protocol requires that every character sent (except EOT) requires a reply character (ACK, NAK or ENQ). Using this approach ensures that characters are only sent, when the previous character has been read in by the receiving processor.

In the event of an error occurring during communications, there are protocol procedures to enable communications

to be re-established. Incorporated within this protocol is the use of the interval timer in each TMS 9902. These interval timers are used to detect excessive delays in replies which would indicate a communication failure, or to cause a "time out" operation in the other processor if a reply character was incorrect (Fig. 6.4.(D)).

The "time out" feature is also used by the inter-processor communications protocol, to resolve the simultaneous transmission of the SOH character between processors (Fig. 6.4.(E)).

6.3. Communications Function

In the structure of the operator software shown in Fig. 6.1., those programs which form the communications function are the input, output and microprocessor/operator communications package tasks, and the queue and interrupt handling operating system programs. The function of these operating system programs, is the controlled activation of the input and output tasks when there is information available in any of the inter-processor communication UARTs, as described in Section 6.6.

6.3.1. Input Task

The communications specification for the operator-system, was that it should be capable of simultaneous communication with all patient processors, to reduce patient processor waiting time and allow efficient use of operator-system processing time.

To provide this facility, the input task was produced as a multi-input re-entry program which receives

information from patient processors. The important features which influenced the structure of this program, and its control by the operating system, was that of the workspace area concept, and the interrupt handling features of the TMS 9900 microprocessor (Ref.58.).

Each inter-processor communication UART connected to the operator-system has associated with it workspace areas and memory files, as shown in Fig. 6.5. The first of these workspace areas is used by the operating system UART interrupt handling program, and the second by the input or output task. It is the address of this second workspace area that is supplied to the input task, by the operating system queue handler program, when a character is present in the associated UART. The contents of this workspace area supplies all the information required by the input task, such as the CRU base address of the UART associated with that workspace area, and the state of the communications protocol for that channel (given by the branch pointer in R1).

A simplified flow diagram of the input task is given in Fig. 6.6. From this diagram it can be seen that the program is divided into 5 sections, each one related to a different aspect of the communication protocol. The branch pointer (R1) in the workspace area supplied to the input task, indicates which section is to be performed when removing the character from the

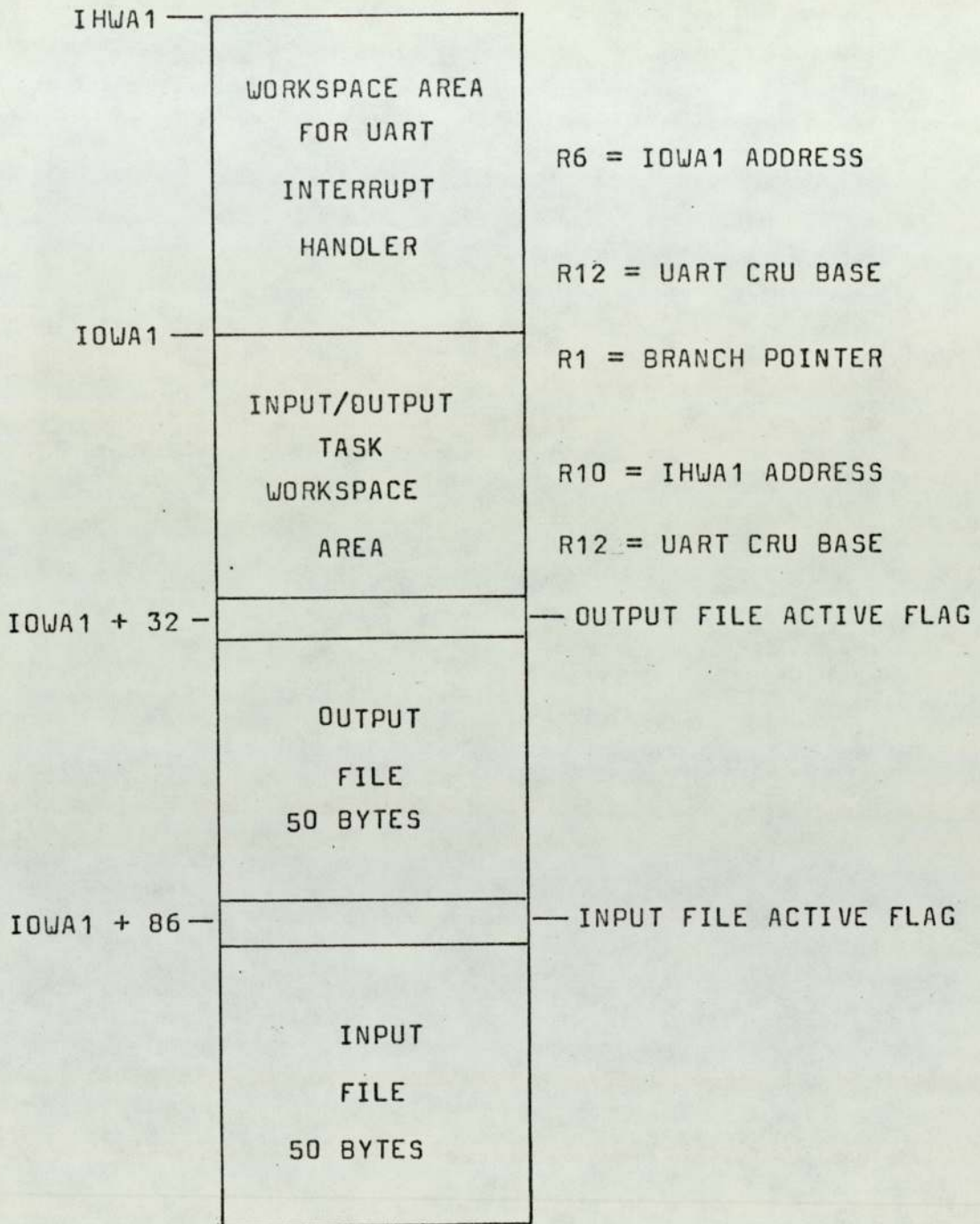


Fig. 6.5. WORKSPACE AREA & FILE STRUCTURE FOR EACH INTER-PROCESSOR COMMUNICATIONS CHANNEL.

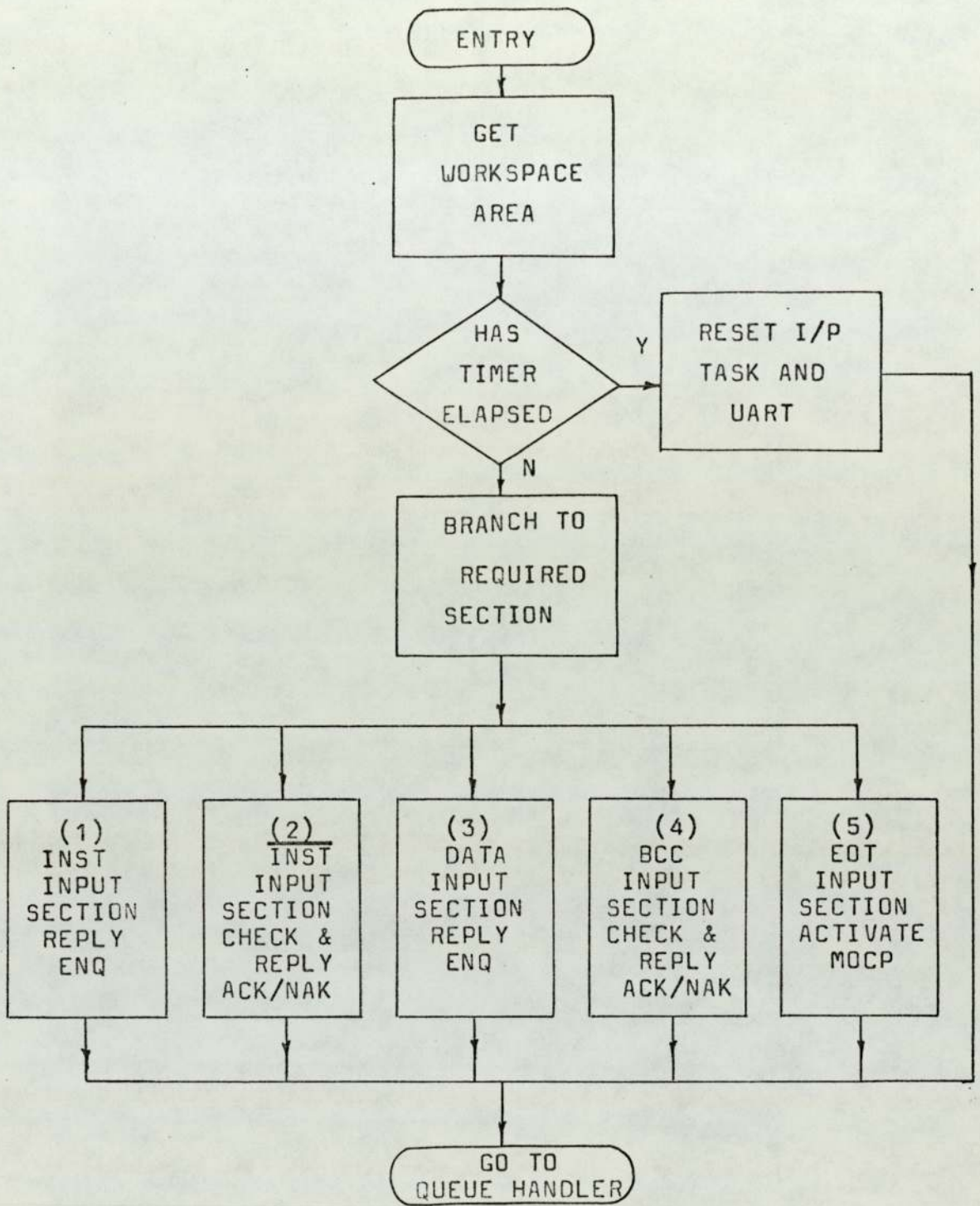


Fig. 6.6. BASIC FLOW DIAGRAM OF INPUT TASK.

appropriate UART, and placing it in the required input file. On completion of each section, the branch pointer is set to indicate which section is to be used, when the next character is received. In this way the input task can deal with each UART as the characters are received.

On successful completion of communications with a particular patient processor (Fig. 6.6. Section 5) the input task sets the corresponding input file active (Fig. 6.5.) and activates the microprocessor/operator communications package task (MOCP).

The execution time of this task, for one entry to it during the communications process, is approximately 0.2mS.

6.3.2. Output Task

The output task is concerned with the transmission of information from the operator processor to patient processors. As can be seen from Fig. 6.7., the structure of the output task is similar to that of the input task. In this case, however, there are six different sections associated with the transmission of information from output files (Fig. 6.5.).

Section 3 (Fig. 6.7.) is concerned with the reception of the ACK character (or NAK), and the transmission of the EOT character if no data is to be sent. If, however, data is to be transmitted, this is performed by sections 4 and 5, and the ACK character then received by Section 6 results in the EOT character

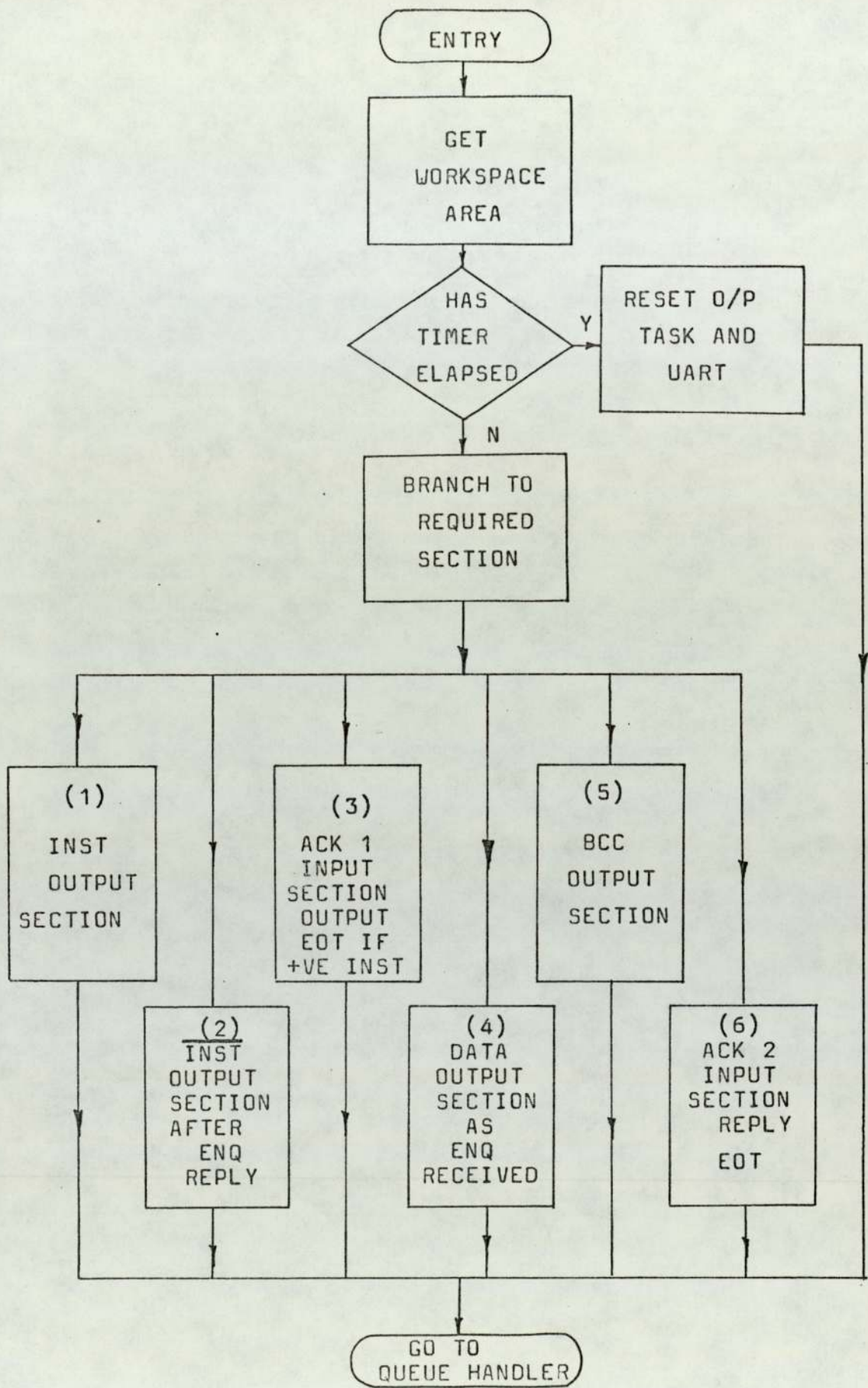


Fig. 6.7. BASIC FLOW DIAGRAM OF OUTPUT TASK.

being sent.

To indicate that the information contained in an output file has been sent, the output file active flag associated with it is reset; it having been set previously when data was placed in the file.

This approach results in the output task being active, only when a reply is present from a patient processor. This therefore, allows lower level tasks to be performed while the output task is awaiting replies.

As can be seen from Fig. 6.1., the output task has a lower priority than the input task. This is because the information coming from patient processors is real-time dependent, whereas output information from the operator-processor can be saved until an appropriate communication situation prevails.

The execution time of the output task, for a single character transmission is approximately 0.2mS.

6.3.3. Microprocessor/Operator Communications Package

The microprocessor/operator communications package (MDCP) task performs the following functions :-

- (1) The interpretation of commands from the operator, and the execution of the required action. This is concerned with the issuing of instructions to the patient processors concerned.
- (2) The interpretation of input information from patient processors. This information may be informing the operator-processor that a certain operation (such as

the successful initiation of the monitoring function) has been performed, or data which had been requested by the operator system.

The flow diagram in Fig. 6.8. shows the basic structure of the microprocessor/operator communications package task. As can be seen from this diagram, the task is divided into two sections concerned with the interpretation of operator or patient processor inputs. The mnemonic commands which the operator can give to the present system, via a VDU terminal, are given in Table 6.1. As can be seen, these instructions take the form of a two letter mnemonic command followed by the patient processor number concerned.

The inter-processor instruction codes (INST) which are currently in use, are given in Table 6.2. These codes were chosen from the chart shown in Table 6.3., which illustrates that the small region containing the ASCII codes used, has not been initially used to provide instruction codes. The remaining codes are divided into the two regions of positive (single instruction) codes, and negative (instructions with data) codes. It will also be seen that a pattern of codes have been eliminated for immediate use (those containing an X), leaving the remaining codes, which require a 2 bit change to give another allowed code, to be used first.

6.4. Display

The display function is concerned with the presentation

OPERATOR INPUT
INTERPRETER

PATIENT PROCESSOR
INPUT INTERPRETER

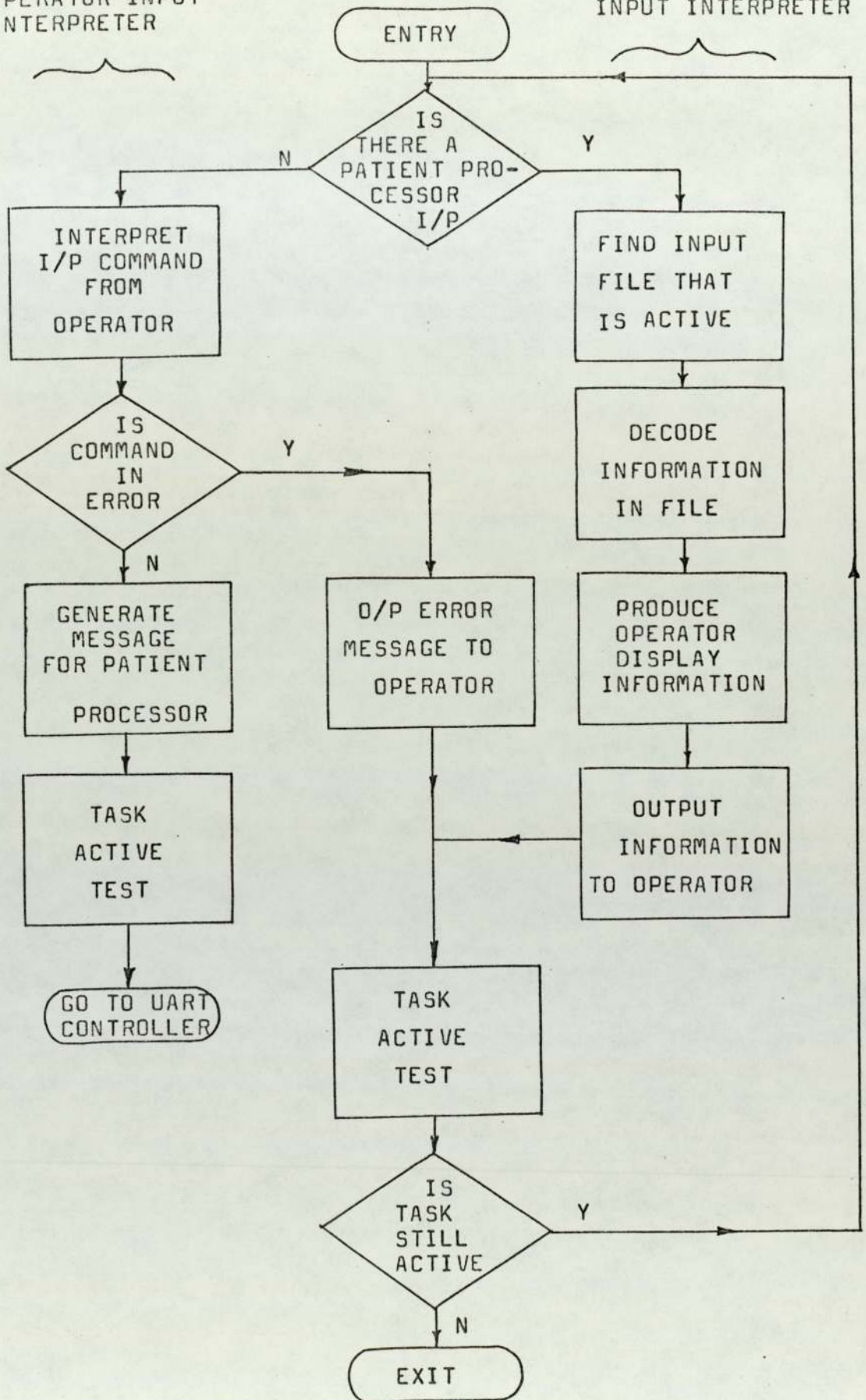


Fig. 6.8. BASIC FLOW DIAGRAM OF MICROPROCESSOR/
OPERATOR COMMUNICATIONS PACKAGE PROGRAM.

START MONITORING	SM1
END MONITORING	EM1
CONTINUE MONITORING	CM1
PATIENT STATUS	PS1
PULSE RATE	PR1

TABLE 6.1. OPERATOR INPUT COMMANDS

Instructions from Operator Processor to Patient Processor

		<u>HEXADECIMAL CODES</u>
OP1	START MONITORING	50
OP2	END MONITORING	53
OP3	CONTINUE MONITORING	55
OP4	SEND PATIENT STATUS DATA	56
OP5	SEND PULSE RATE	5C

Instructions from Patient Processors to Operator Processor

		<u>HEXADECIMAL CODES</u>	
		<u>SINGLE INSTRUCTION</u>	<u>INSTRUCTION WITH DATA</u>
P01	MONITORING	21	
P02	MONITORING START-UP OK	22	
P03	MONITORING START-UP FAIL	24	
P04	END OF MONITORING	27	
P05	MONITORING AGAIN	28	
P06	INSTRUCTION ERROR	2B	
P07	MONITORING ALREADY	2D	
P08	NOT MONITORING	2E	
P09	PATIENT STATUS DATA		81
P010	DIAGNOSIS		A3
P011	PULSE RATE DATA		C0

TABLE 6.2. INTER-PROCESSOR INSTRUCTION CODES

		SINGLE INST							INST WITH DATA								
		HEXADECIMAL															
MSB		0	1	2	3	4	5	6	7	8	9	A	B	C	D	E	F
LSB	0					OP1									P011		
	1	SOH	P01							P09							
	2		P02														
	3					OP2						P010					
	4	EOT	P03														
	5	ENQNAK				OP3											
	6	ACK				OP4											
	7		P04														
	8		P05														
	9																
	A																
	B		P06														
	C					OP5											
	D		P07														
	E		P08														
	F																
	ASCII																

Table. 6.3. INSTRUCTION CODE TABLE.

of information to the operator, which in the present system is performed by a visual display unit (VDU). The software which controls this peripheral, is the VDU task (Fig. 6.1.). This task performs both the functions of outputting information to the VDU, and receiving input commands from the operator, via the VDU keyboard. The output section of the task has priority over the input section, thereby allowing the system to interrupt the operator to indicate a patient's condition. The basic flow diagram of the input and output sections of the VDU task, are shown in Fig. 6.9. and Fig. 6.10.

When there are no active tasks, the operating system passes control over to the input section of the VDU task. The characters received by this task are placed in an input file, and on reception of a carriage return character, the VDU task activates the MOCP task, so that the contents of this buffer may be decoded.

The output section of the VDU task may be entered in two ways, the first is by scheduling the task, and the second is by direct access to the task. The second of these approaches is mainly used in the system, as it allows the MOCP task to output information as it is generated.

The information supplied to the VDU task, comes in two forms (Fig. 6.11.). The first is a list of addresses indicating the files to be used. In this case the last character in each file is either negative; indicating that the next file address should be used, or the

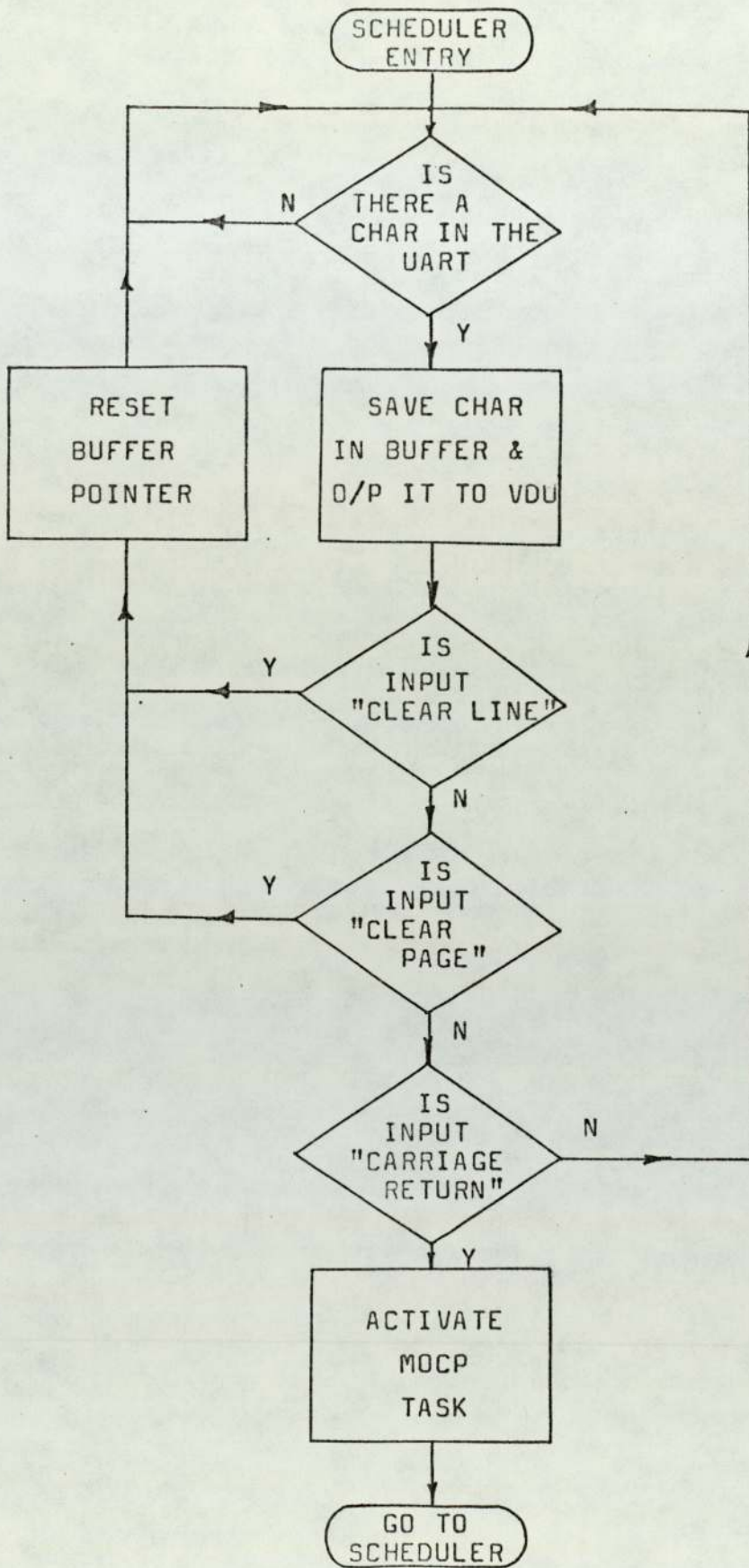


Fig. 6.9. BASIC FLOW DIAGRAM OF INPUT SECTION OF VDU TASK.

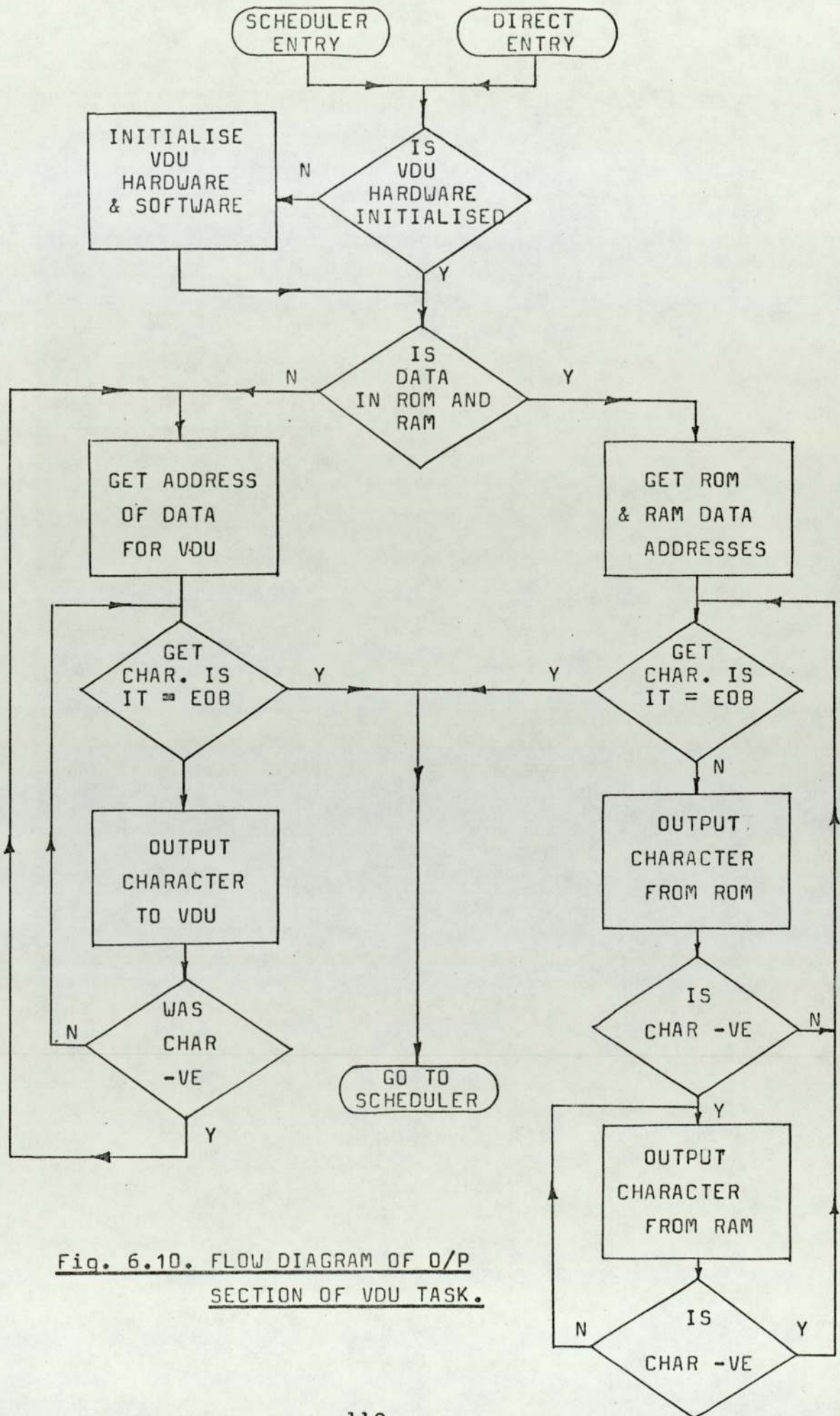
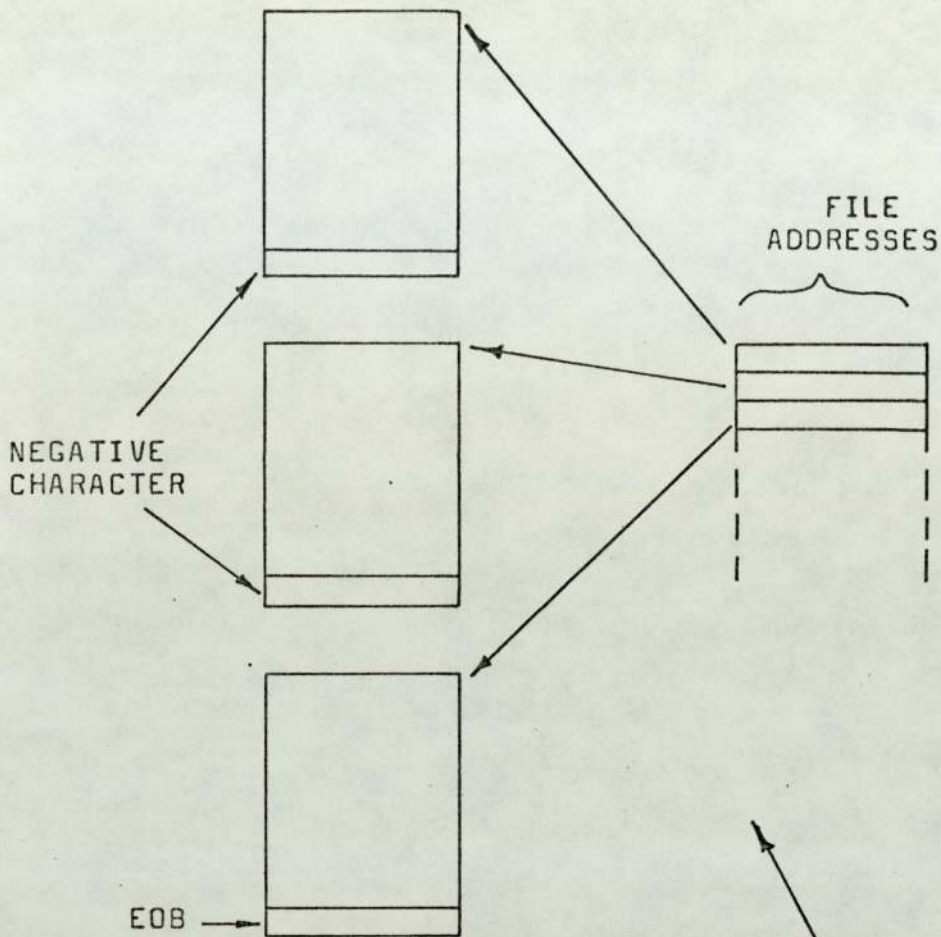


Fig. 6.10. FLOW DIAGRAM OF O/P SECTION OF VDU TASK.

FIRST FILE FORMAT



SET

ROMRAM

RESET

SECOND FILE FORMAT

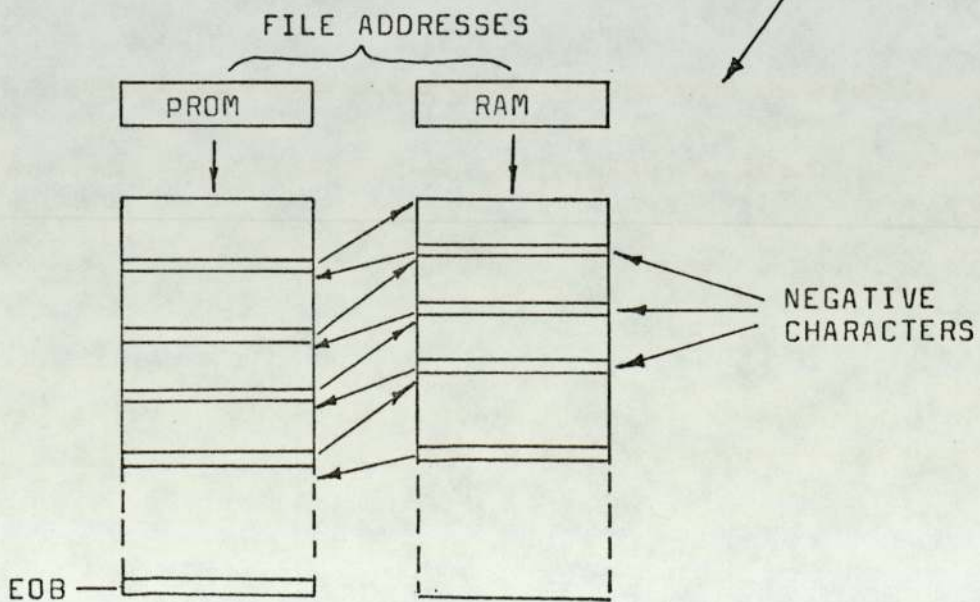


Fig. 6.11. OUTPUT FILE STRUCTURES FOR VDU TASK.

"end of buffer" (EOB) character, which indicates that there are no more file addresses.

However, it is often required that standard text and variable characters be mixed on the VDU display. In these situations, the standard text would be in "programmable read only memory" (PROM), and the variable characters would be present in read/write memory (RAM). In order to cater specifically for this situation, an alternative file format structure was developed. In this case only the address of PROM information and RAM information is given to the VDU task. The PROM resident characters are structured such that, at the points where variable characters should be present on the display, the character is made negative. Similarly, in the RAM generated information, at the point where the VDU task should return to PROM information, the character is made negative. The operation of the VDU task with this file structure, is simply to jump from one file to the other, when a negative character is detected, or to terminate this output operation on the detection of the "end of buffer" character in the PROM file (Fig. 6.11.). To indicate which file format is in operation, a software flag (ROMRAM) is set (first format) or reset (second format) accordingly.

6.5. Storage

The storage function was not implemented in the experimental system, as no definite decision was made as to what data should be saved, and also because of the

cost of peripheral equipment such as a disc store.

However, the type of data that could be stored by the system may take the form as follows.

- (1) The storage of the first arrhythmia of each type diagnosed.
- (2) The storage of one or more, of the most recent arrhythmias, of each type diagnosed.
- (3) The storage of trend data such as the number of each type of arrhythmia detected, in perhaps 1 or 5 minute intervals over a number of hours.
- (4) The storage of medication events.

6.6. Control

The operating system for the operator-dedicated processor software, as shown in Fig. 6.1., is similar to that of the patient processor system. The functions of the initialisation and task scheduler are the same in each system, the only differences being the task involved.

The major differences between the two operating systems is concerned with the UART interrupt handler and input/output queue handler programs.

6.6.1. UART Interrupt Handler Program

The UART interrupt handler program for the operator-dedicated processor system, is responsible for the control of all the inter-processor communication UARTs. It is therefore concerned with establishing or acknowledging, inter-processor communication start-up protocol procedures, and the subsequent supply of

information to the I/O queue handler program, which is responsible for activating the input or output tasks.

As illustrated in Fig. 6.5., each inter-processor UART, has associated with it a workspace area, which is used by the UART interrupt handler program. It is these workspace areas; supplied to the program via interrupt vectors, which contain information that informs the program of the state of communications with the associated patient processor (i.e. whether the UART is being currently used for inputting or outputting of information etc.).

When a character is received by a UART, the interrupt produced causes the UART interrupt handler program (Fig. 6.12.) to be performed. If this program finds that the particular UART concerned is in either the input or output mode, it supplies the address of the I/O workspace area associated with that UART (Fig. 6.5.), to the I/O queue handler program. This workspace area is then supplied by the I/O queue handler program, to either the input or output task as required.

Also included within the UART interrupt handler program are the sections concerned with :-

- (1) Acceptance of output requests from the MOCP task.
- (2) Testing for suspended output requests from MOCP.
- (3) The retransmission of the start-up protocol (SOH) due to an error detected by the output task.
- (4) The activation of the "timing out" process due to

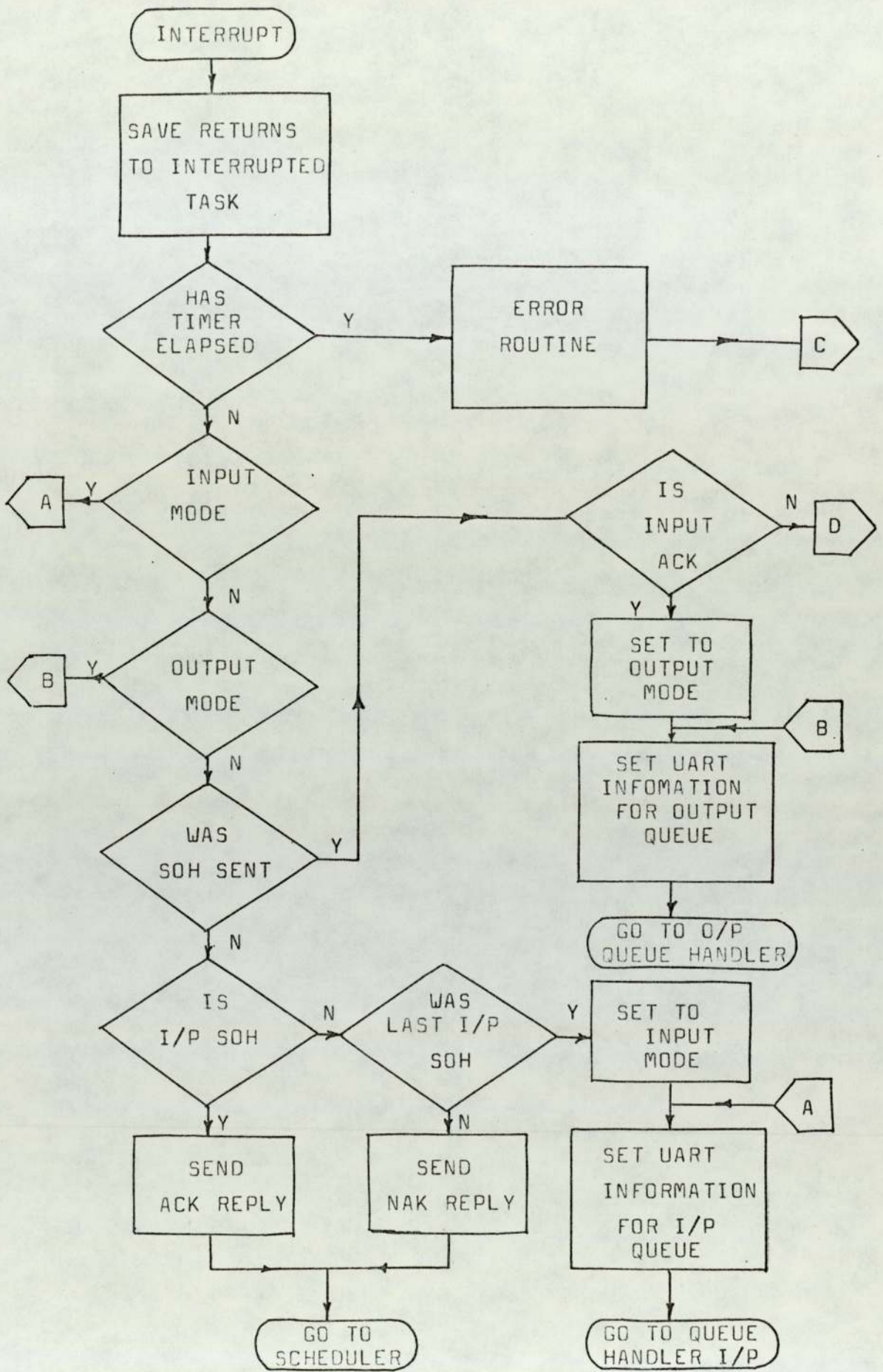


Fig. 6.12. BASIC FLOW DIAGRAM OF UART INTERRUPT HANDLER PROGRAM.

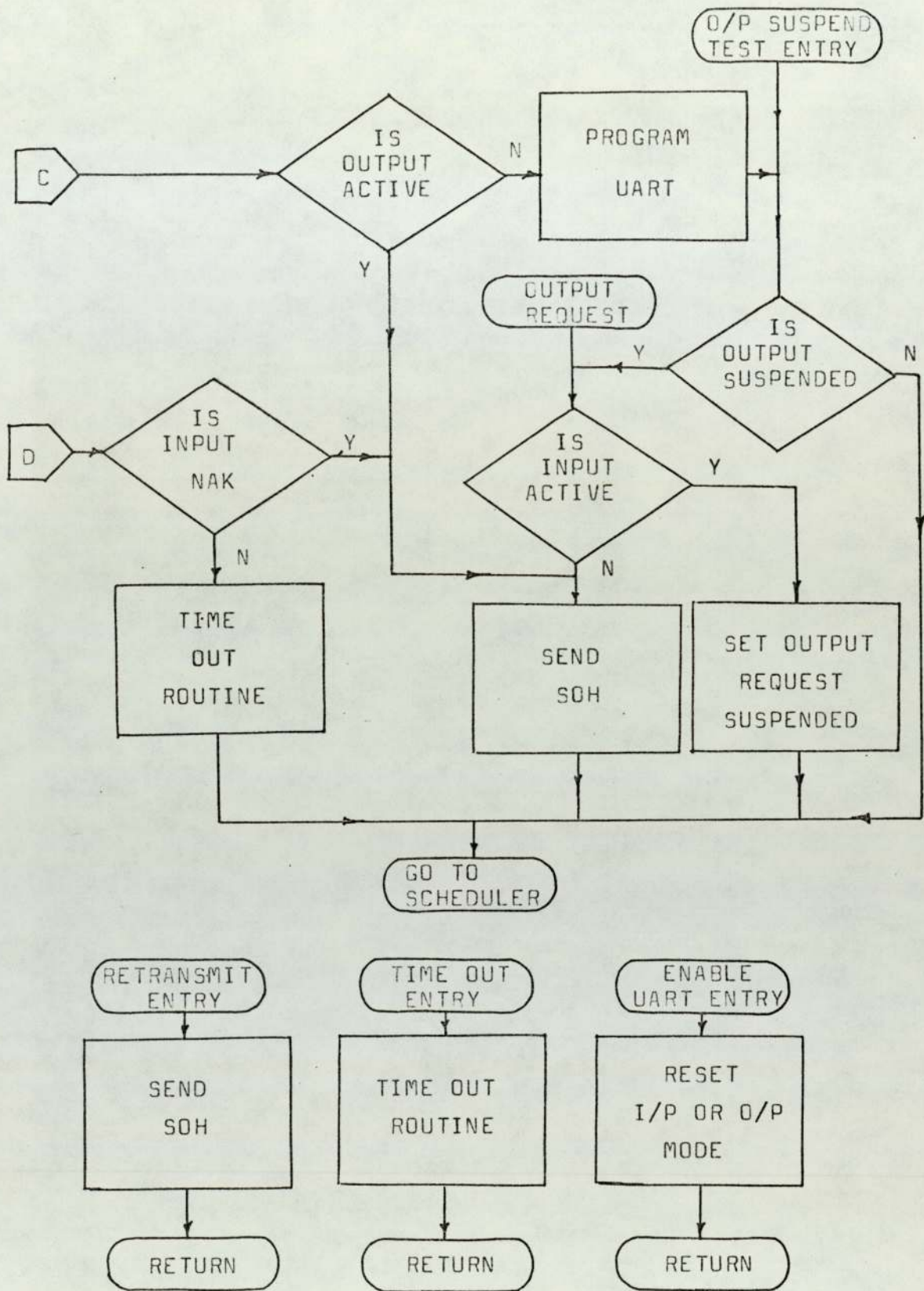


Fig. 6.12. continued.

BASIC FLOW DIAGRAM OF UART INTERRUPT HANDLER PROGRAM.

the reception of an illegal reply character detected by the output task.

- (5) The enabling of the UART interrupt handler program on successful completion of input or output communications.

6.6.2. I/O Queue Handler Program

The I/O queue handler program is concerned with the activation of the input and output tasks, as UARTS receive characters for those tasks. Therefore, for example, if a character is received by a UART which is in the input mode, the UART interrupt handler program will supply the I/O workspace area address associated with that UART to the input queue handler routine. The queue handler program places this I/O workspace area address in a, first in first out (FIFO) input queue, and then ensures that the input task is active. If other UARTs are in the input mode and have received characters, the addresses of the I/O workspace areas associated with those UARTs are placed in the input queue. Subsequently, the input task is scheduled by the task scheduler program whereupon it uses the first of the I/O workspace area addresses given to it by the I/O queue handler program. On completion of the input task for that particular I/O workspace area, the input task returns to the queue handler program so that the next address of an I/O workspace area in the input queue, may be given to

the task. If it is found by the queue handler program, that there are no more I/O workspace area addresses in the input queue, the input task is deactivated until such time as more characters have been received, for use by the input task.

When UARTs are in the output mode, the output queue and output task are handled in a similar manner by the output queue routines of the I/O queue handler program. The basic flow diagram of the I/O queue handler program is given in Fig. 6.13.

INPUT QUEUE HANDLER
ROUTINE, ENTRY FROM
UART INTERRUPT HANDLER

INPUT TASK ENTRY
TO GET NEXT
ADDRESS IN QUEUE

OUTPUT QUEUE HANDLER
ROUTINE, ENTRY FROM
UART INTERRUPT HANDLER

OUTPUT TASK ENTRY
TO GET NEXT
ADDRESS IN QUEUE

- 121 -

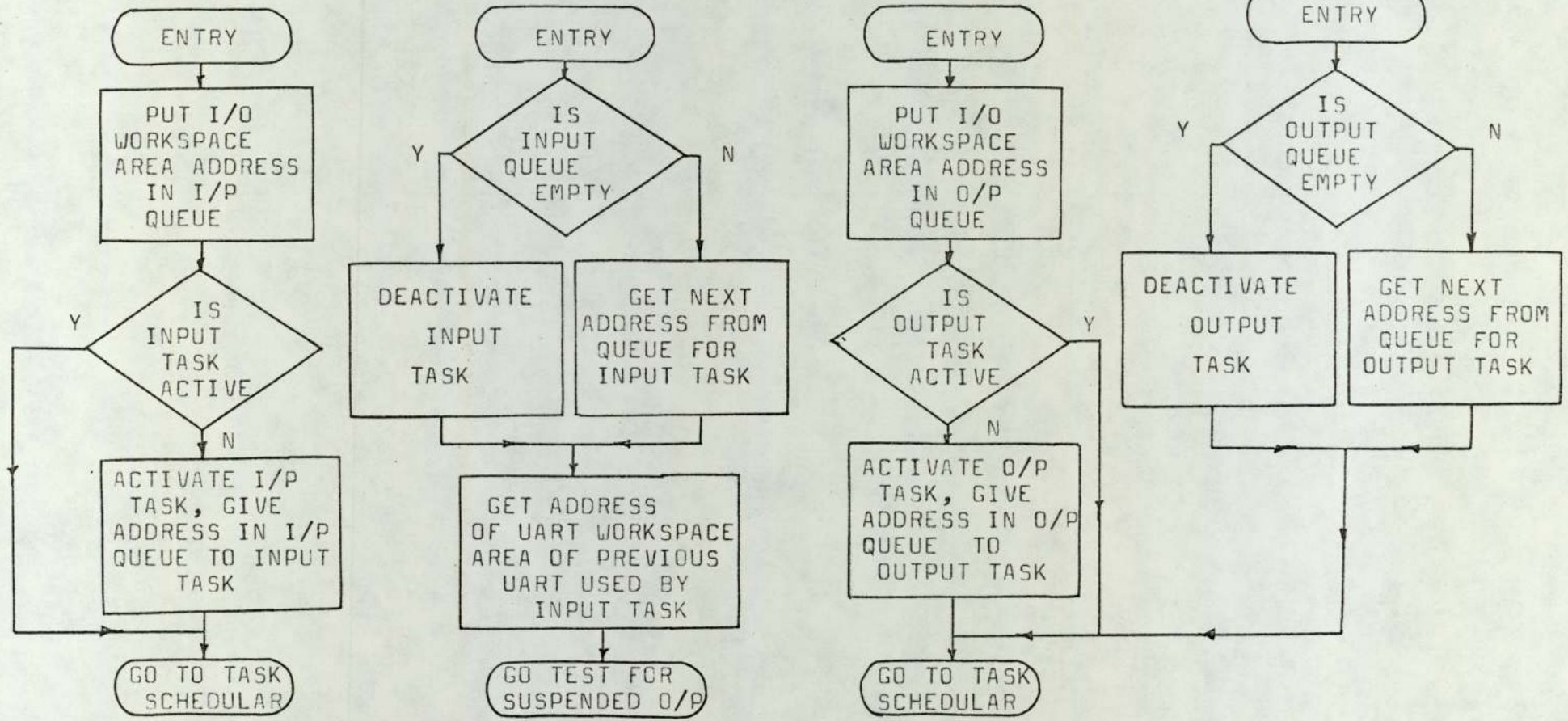


Fig. 6.13. BASIC FLOW DIAGRAM OF I/O QUEUE HANDLER PROGRAM.

CHAPTER 7

SYSTEM HARDWARE

7.1. General

When producing the various functions to be performed by the distributed system, the aim was to implement as much as possible in the compact form of software. As a result, it should therefore be possible to produce a single patient-dedicated processor system board, which would contain all the hardware requirements for a single patient. Such an approach would allow flexible system structure for different patient size CCUs, and would also aid mass production of the monitoring systems.

The basic block diagram of a microprocessor hardware system, is shown in Fig. 7.1., and a brief outline of the hardware and software features of the TMS 9900 microprocessor are given in the appendix. The only difference between the patient and operator dedicated processor hardware systems, is the size of memory (PROM and RAM) required, and the devices interfaced to each system.

In the present developmental system, the memory requirements for the patient system are met by 2K words of PROM and 2K words of RAM. The present operator system memory, does not exceed 2K words of PROM and 1K words of RAM, this being the memory required to implement the three patient (simulation) system. However, the memory requirements for the final operator system would be greatly increased, as more patient processors would be

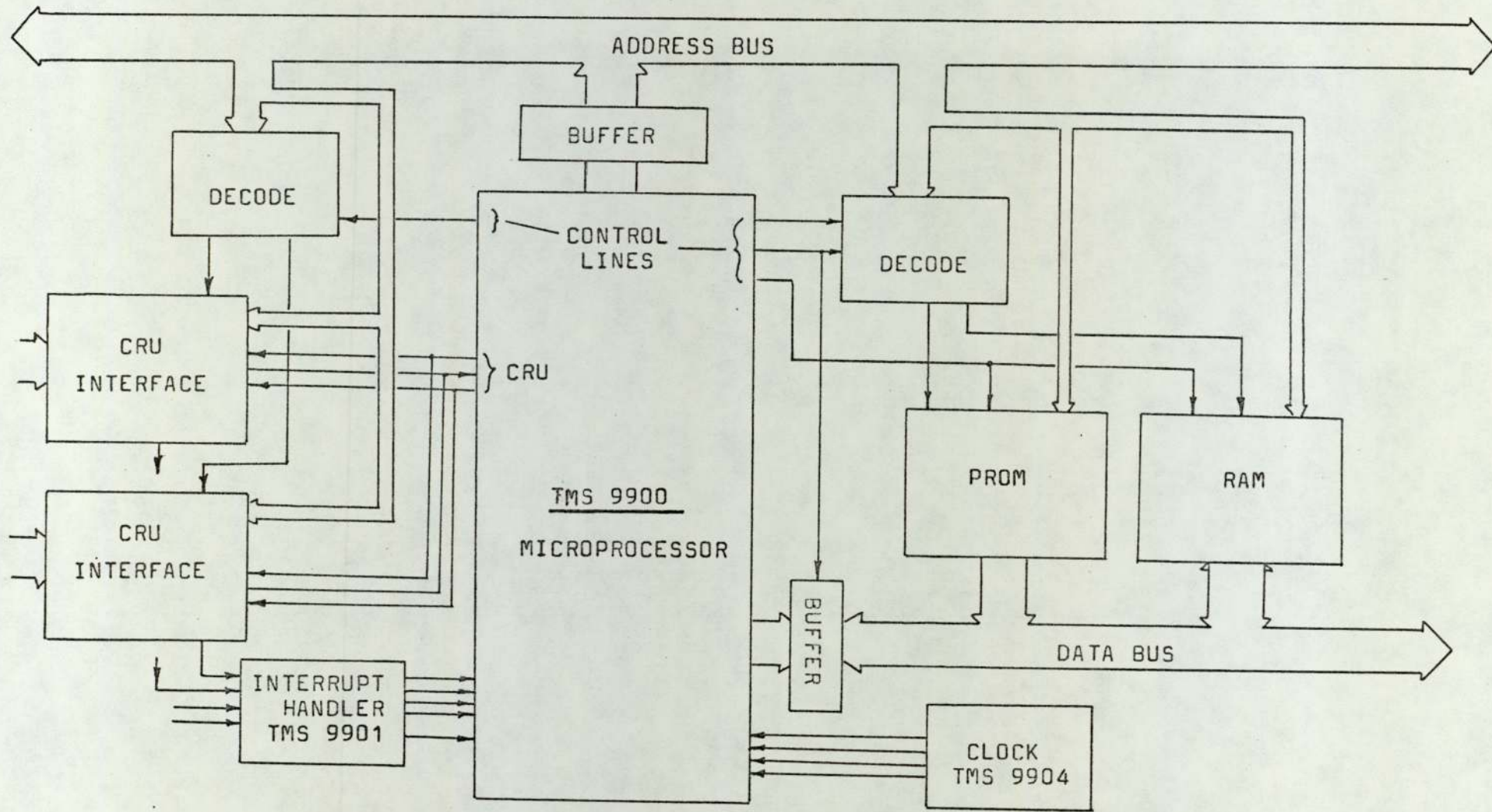


Fig. 7.1. BASIC HARDWARE BLOCK DIAGRAM OF A MICROPROCESSOR SYSTEM.

connected to the final system, and more software for the presentation of information would be incorporated into the system.

All the memory used in the system has an access time not in excess of 450nS, so that the microprocessors were never placed in a wait state, while waiting for data from memory.

As new components such as memory devices, and microprocessor support chips are continuously appearing on the market, no detailed circuit diagrams of such items will be given in this report. For information on such devices one should consult the latest microprocessor support components literature, and new devices specifications.

The following discussion will therefore be directed to the interface requirements for A to D conversion of the ECG signal, and inter-processor communication.

7.2. ADC Interface

The analog to digital converter (ADC), and the digital to analog converter (DAC), designed for use in the developmental system, are both interfaced to the patient processor system. In the final distributed system it is possible that the DAC would be dedicated to the operator system, allowing the display of stored arrhythmia events.

The requirements of the ADC interface are that it should convert the ECG signal to an 8 bit signed binary

value, every 4mS. A basic block diagram of the ADC interface designed is given in Fig. 7.2. It operates independently from the microprocessor such that every 4mS the ECG signal would be automatically sampled and converted, and then the value found would be presented to the microprocessor, by the generation of an interrupt. Conversion of the signal was achieved by the use of an inexpensive 8 bit DAC, which produced a ramped output which was compared to the sampled analog signal.

Having produced the software for the patient processor system, it was found that there is scope for expanding the various functions. One way in which this surplus processing time could be put to use, is in order to reduce the component count of the ADC. This could be achieved by replacing the control in the present interface (Fig. 7.2.), with control from the microprocessor, producing the structure for the interface shown in Fig. 7.3. The microprocessor could then instruct the interface to convert the signal, or possibly use a successive approximation algorithm itself to convert the signal. Timing of the 4mS sample period could then be performed by the interval timer present in the TMS 9901 interrupt handler device (Fig. 7.1.), which is now available and would be present in the system.

7.3. Inter-processor Communication Interface

As indicated in Section 6.2. (Fig. 6.2.), the approach used for inter-processor communication is via serial data

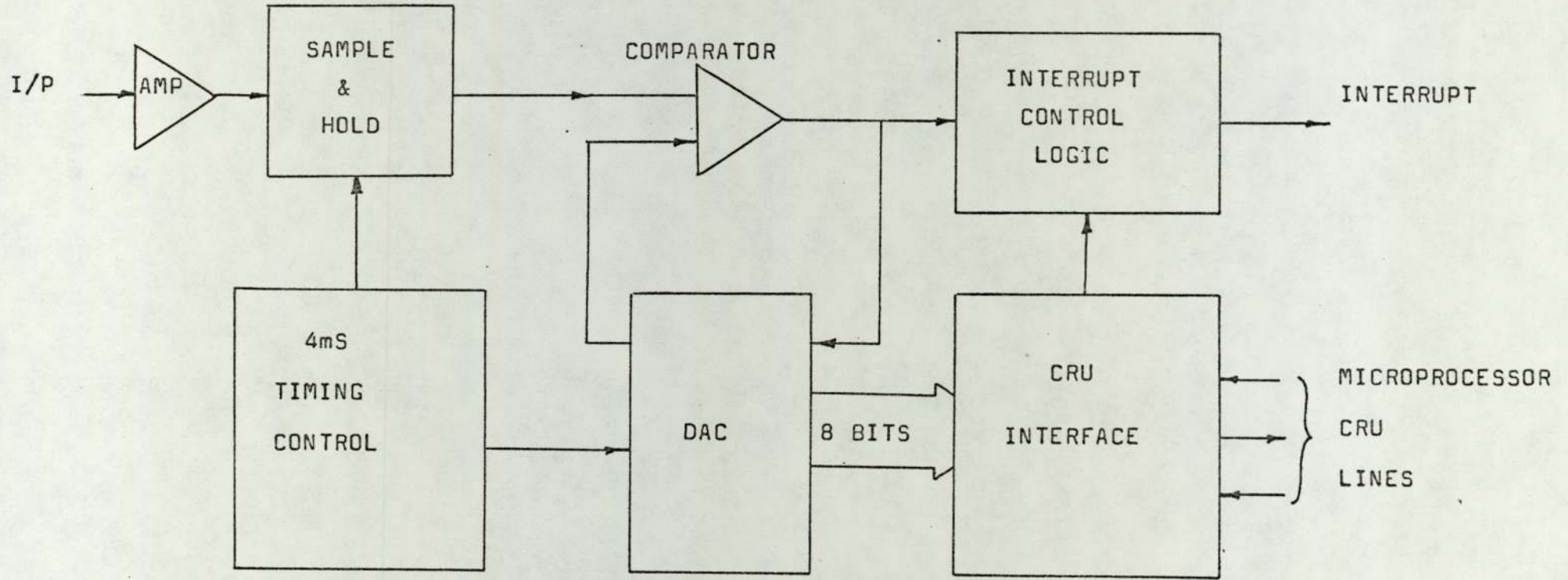


FIG. 7.2. BASIC STRUCTURE OF ADC USED IN DEVELOPMENTAL SYSTEM

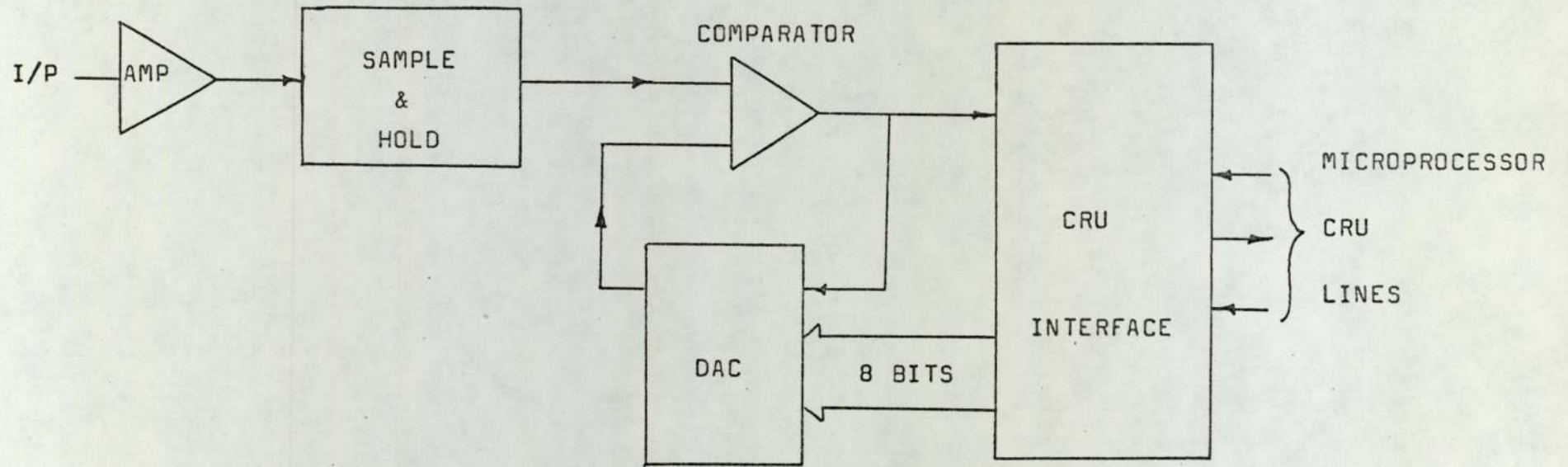


FIG. 7.3. ALTERNATIVE STRUCTURE OF ADC

links. The device used to provide the communication link is the TMS 9902 asynchronous communications controller, which is specifically designed for use with the TMS 9900 microprocessor.

The structure of the communications interface for the operator system is shown in Fig. 7.4. This diagram shows 3 communication channels but more TMS 9902's could easily be introduced into the interface, to provide communications with the final number of patient processors in the distributed system.

At the patient-dedicated processor systems, the communications interface is the same as in Fig. 7.4., but only one TMS 9902 is required.

The character transmission format, programmed into each TMS 9902 by the associated microprocessor at system start-up time, is one start bit, eight data bits, an even parity bit and two stop bits. The bit rate currently used in the system is 31250 bits/second, which corresponds to a character transmission time of 0.384mS.

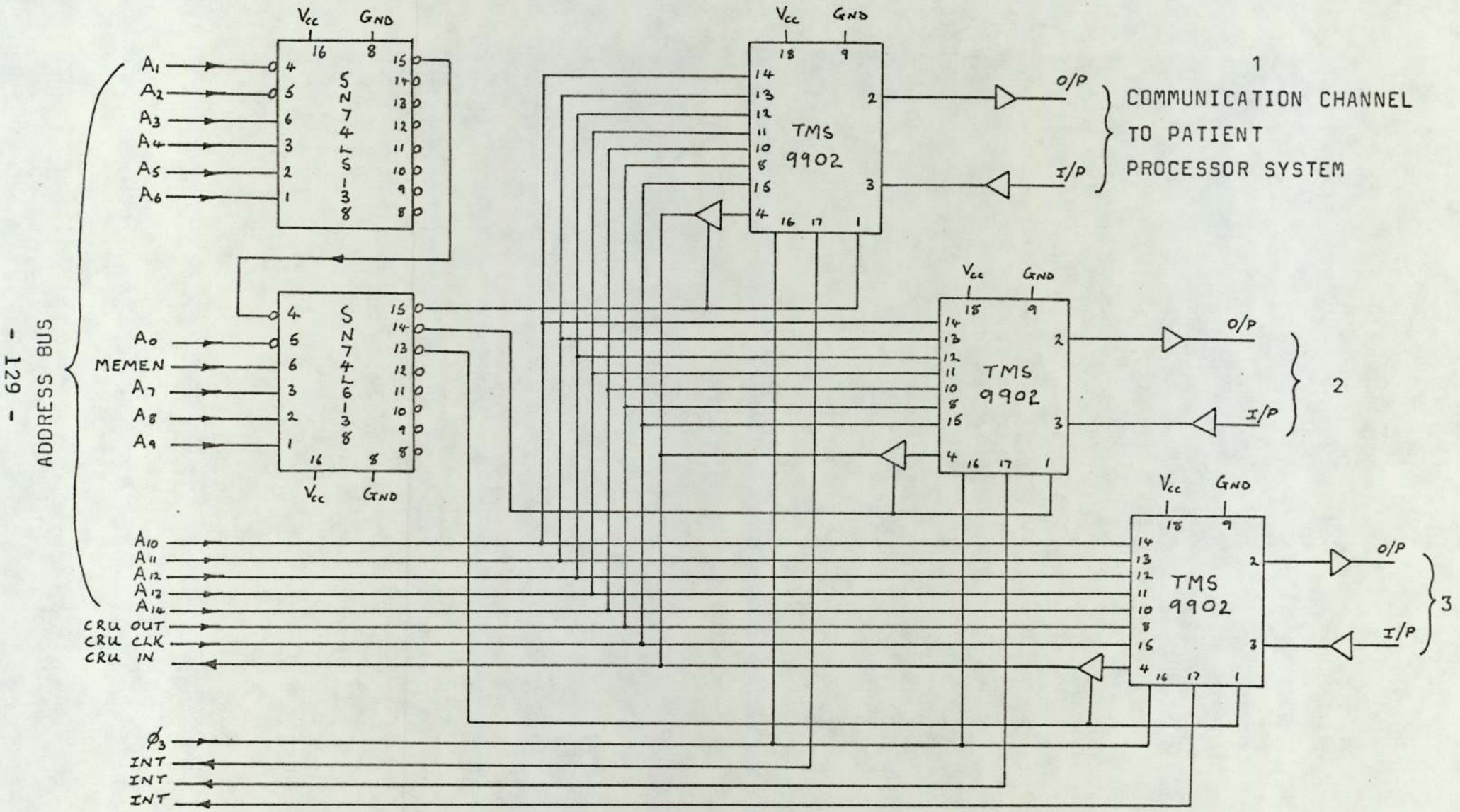


Fig. 7.4. CIRCUIT DIAGRAM OF OPERATOR SYSTEM COMMUNICATION INTERFACE.

CHAPTER 8

SYSTEM PERFORMANCE

8.1. Patient Processor Performance in Real-time

In the patient processor system, the real-time functions of signal conditioning, monitoring, diagnosis and control, consume approximately 42% of processing time (Table 4.1.). The remaining 58% of processing time is unused, except when communications between processors occurs. This surplus processing time therefore allows any of the patient processor functions to be expanded. However, the amount by which each function could be increased is dependent upon its frequency of execution.

If the execution time of the signal conditioning function (1mS) or the QRS detection algorithm (0.21mS) in the monitoring function were to be increased, the result would be a constant increase in the processing time consumed. This is because the frequency of execution of these algorithms is constant, at 250 per second. Therefore, for example, if both of these algorithms were increased by 50%, the processing time consumed would increase from 42% to approximately 56%.

If, however, the execution time of the monitoring function parameter measurement algorithms, or the diagnosis function were increased, the effect on processing time would be dependent on the pulse rate of the patient being monitored. For example, if these algorithms were increased by 10 or 20 times, the effect on the processing

time consumed, related to the patient's heart rate, would be as shown in Fig. 8.1. As can be seen from this graph, even a substantial increase in these algorithms, and a very high pulse rate, does not cause an excessive increase in the processing time consumed.

Therefore, it should be apparent that the frequency of execution of each algorithm, is the factor which limits the amount by which each may be expanded, but within this limit there is still room for considerable improvement. However, the penalty paid for increasing the processing time consumed by these functions, is a reduction in the speed of information flow between processors, as discussed in Section 8.2.

8.2. Inter-processor Communications Performance

As only a single patient processor system was available for use in the experimental system; simulation of a three patient processor system was performed, to determine the performance of inter-processor communications.

The simulation of a three patient system was achieved by connecting the single patient processor system that was available to three inter-processor communication UARTs, as illustrated in Fig. 8.2. The outputs to the imaginary patient processors were unused, and the interrupts from the UARTs were arranged such that the real patient processor had the lowest interrupt level. This arrangement produced the worst case conditions for communications to three patient processors, because

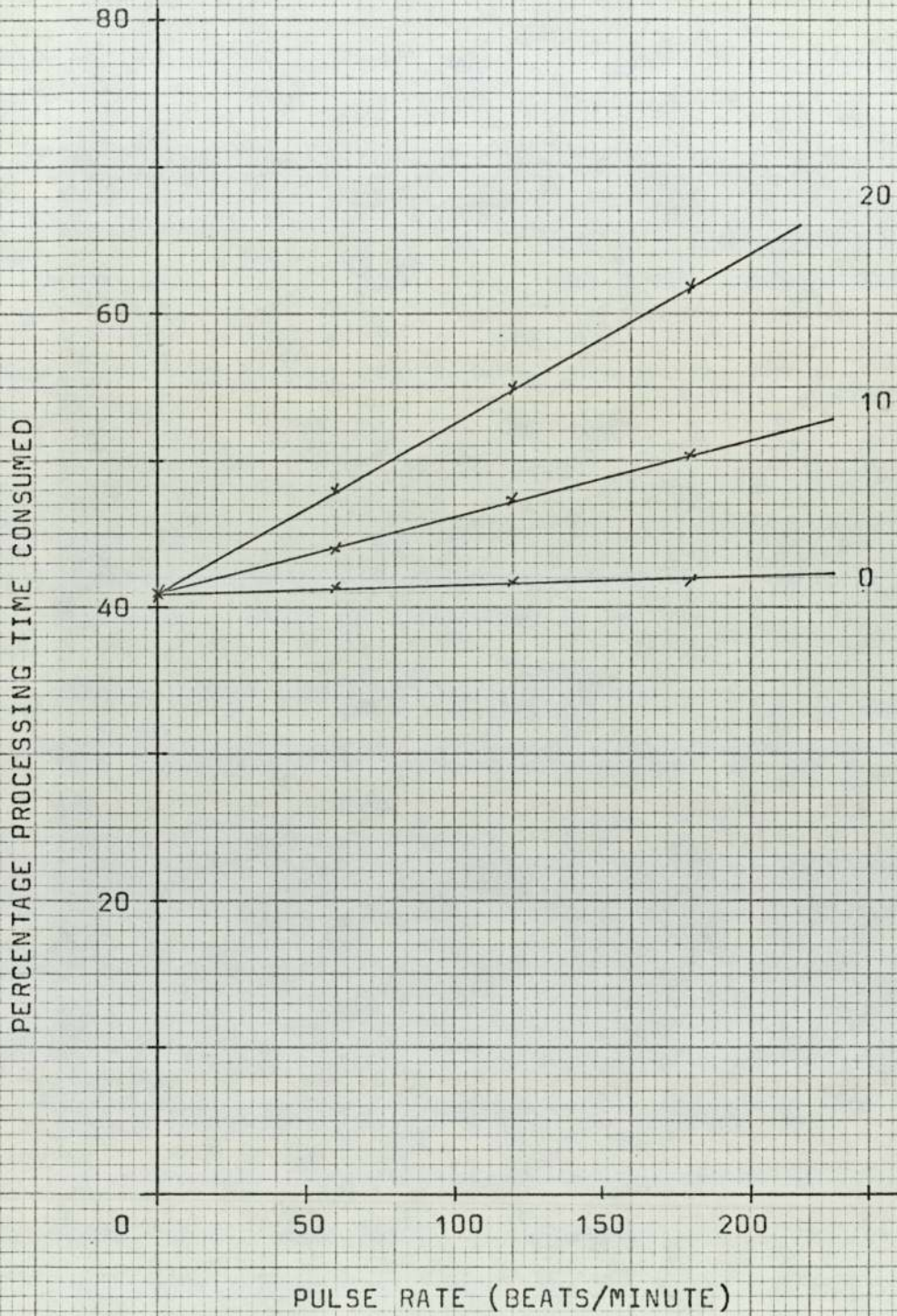


Fig. 8.1. GRAPH SHOWING EFFECT OF 10 & 20
TIMES INCREASE IN PULSE RATE
RELATED ALGORITHMS.

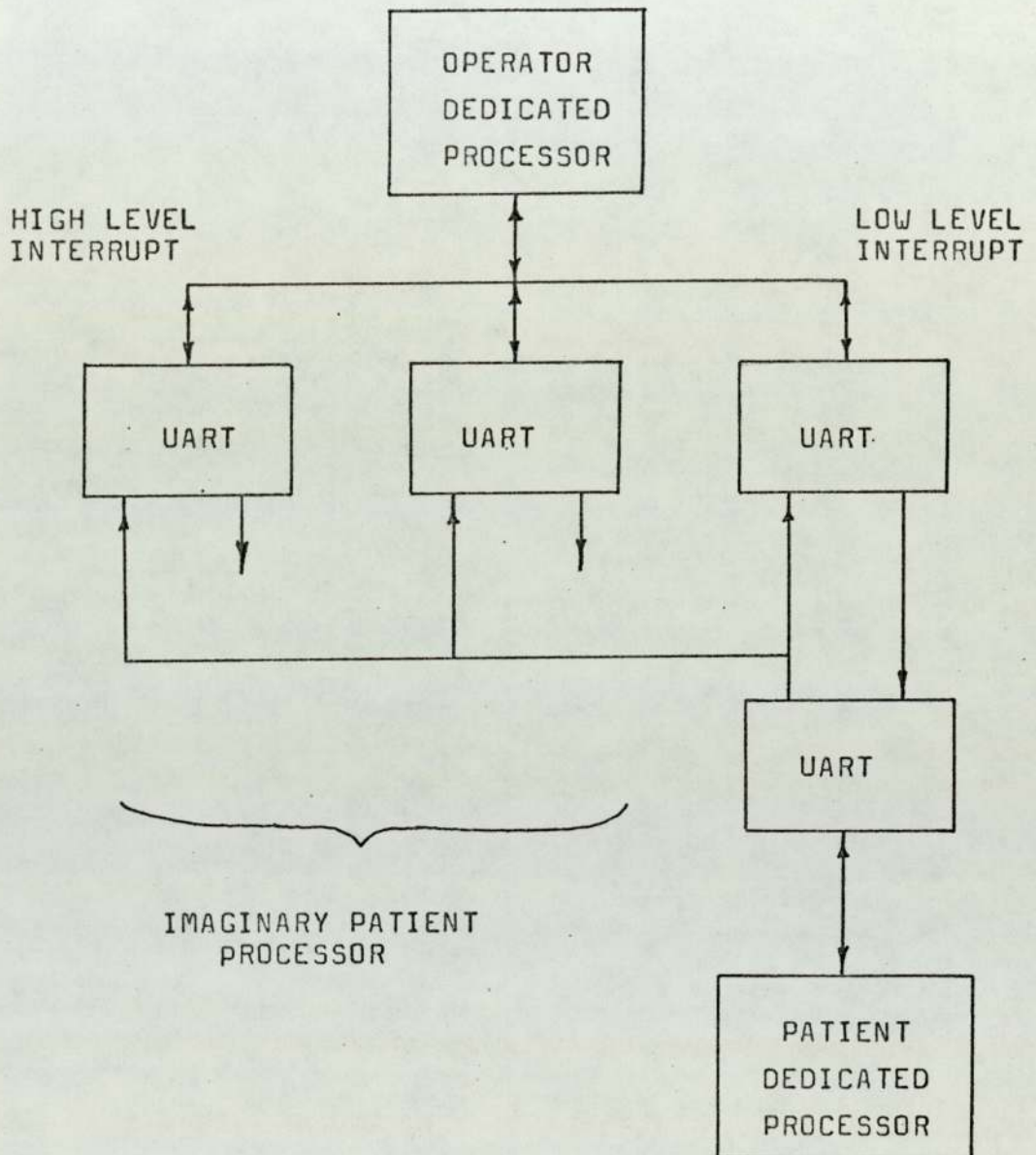


Fig. 8.2. BASIC STRUCTURE OF PATIENT PROCESSOR SIMULATION SYSTEM.

characters from the patient processor were received simultaneously in the UARTs at the operator system. This allowed the interrupt and queue handling facilities in the operator processor operating system to be tested, and measurements of communication rates for 1, 2 and 3 patient processors to be made.

The first experiments performed were to determine the effect of reducing the bit rate used by the UARTs, on the total transmission time of an instruction with 50 bytes of data (Fig. 6.3.(B)). This was performed with and without the monitoring function in operation in the patient processor system, and the results obtained are shown in Fig. 8.3. and Fig. 8.4. As can be seen from these graphs, some odd shaped curves were produced, which appeared to have discontinuities in them at regular intervals. These discontinuities were found to be due to the effect of the real-time processing performed by the patient processor, on the flow of information between processors. The introduction of the monitoring function (Fig. 8.4.) had the effect of increasing transmission times, but the points where the discontinuities occurred (70,110,220 mS) remain unchanged.

Consider the timing diagram given in Fig. 8.5., which shows the execution times of the signal conditioning and monitoring functions, and the transmission times of the characters transmitted and received by the patient processor. From this diagram it can be seen that the real-time processing performed by the patient processor,

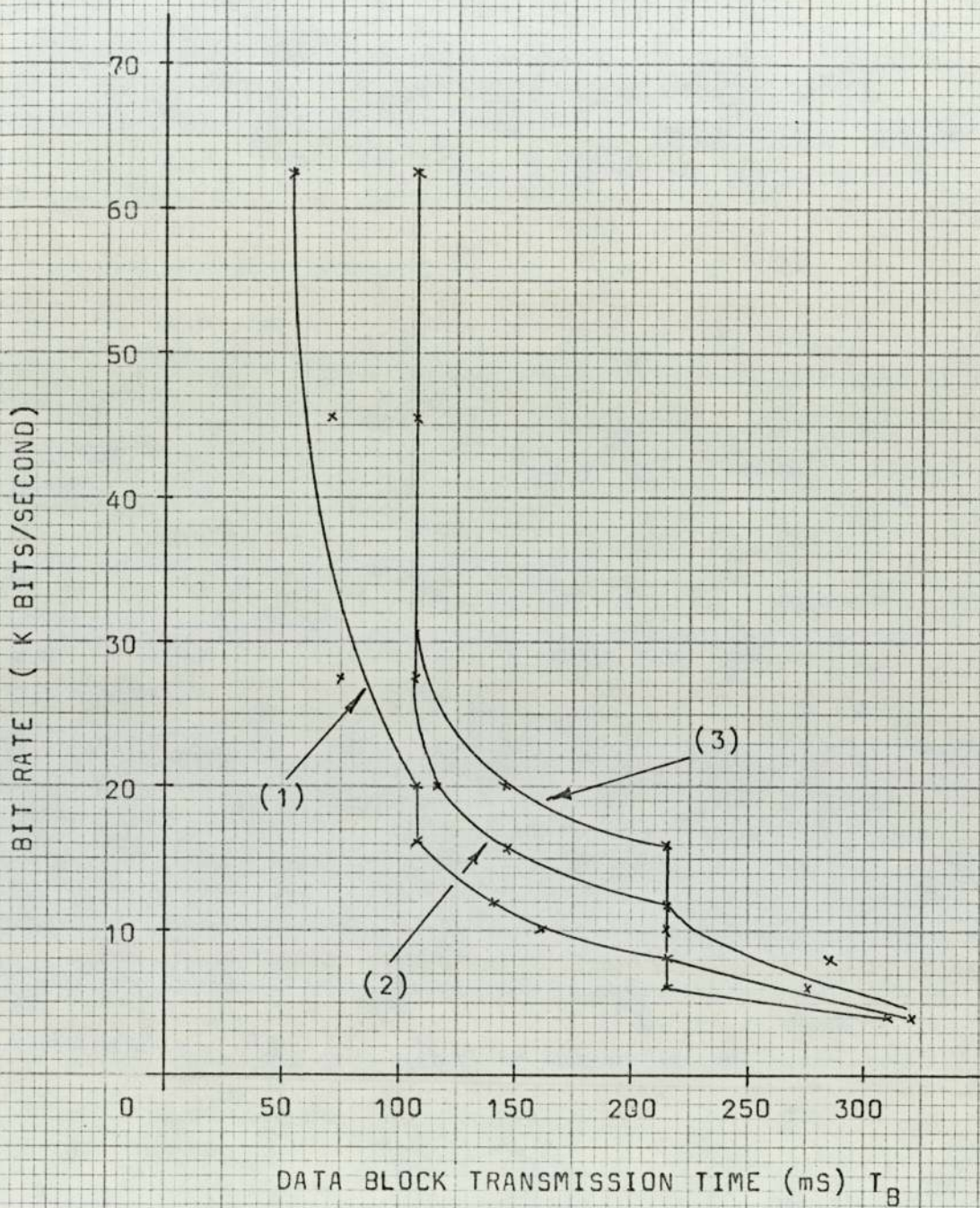


Fig. 8.3. GRAPH SHOWING EFFECT OF BIT RATE ON DATA BLOCK TRANSMISSION TIME FOR 1,2 & 3 PATIENT PROCESSORS (WITHOUT MONITORING FUNCTION OPERATING).

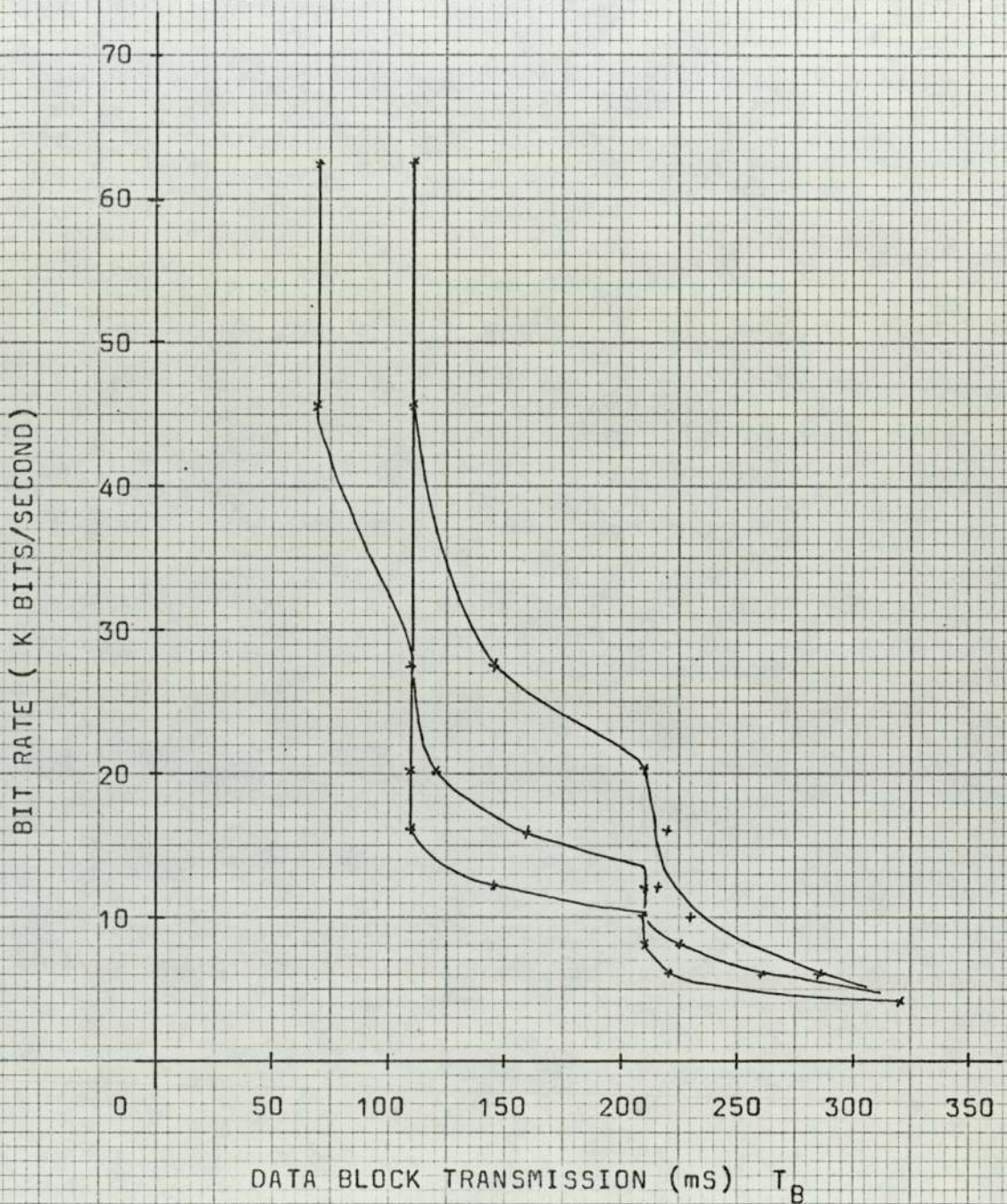


Fig. 8.4. GRAPH SHOWING EFFECT OF BIT RATE ON DATA BLOCK TRANSMISSION TIME FOR 1, 2 & 3 PATIENT PROCESSORS (WITH MONITORING FUNCTION OPERATING).

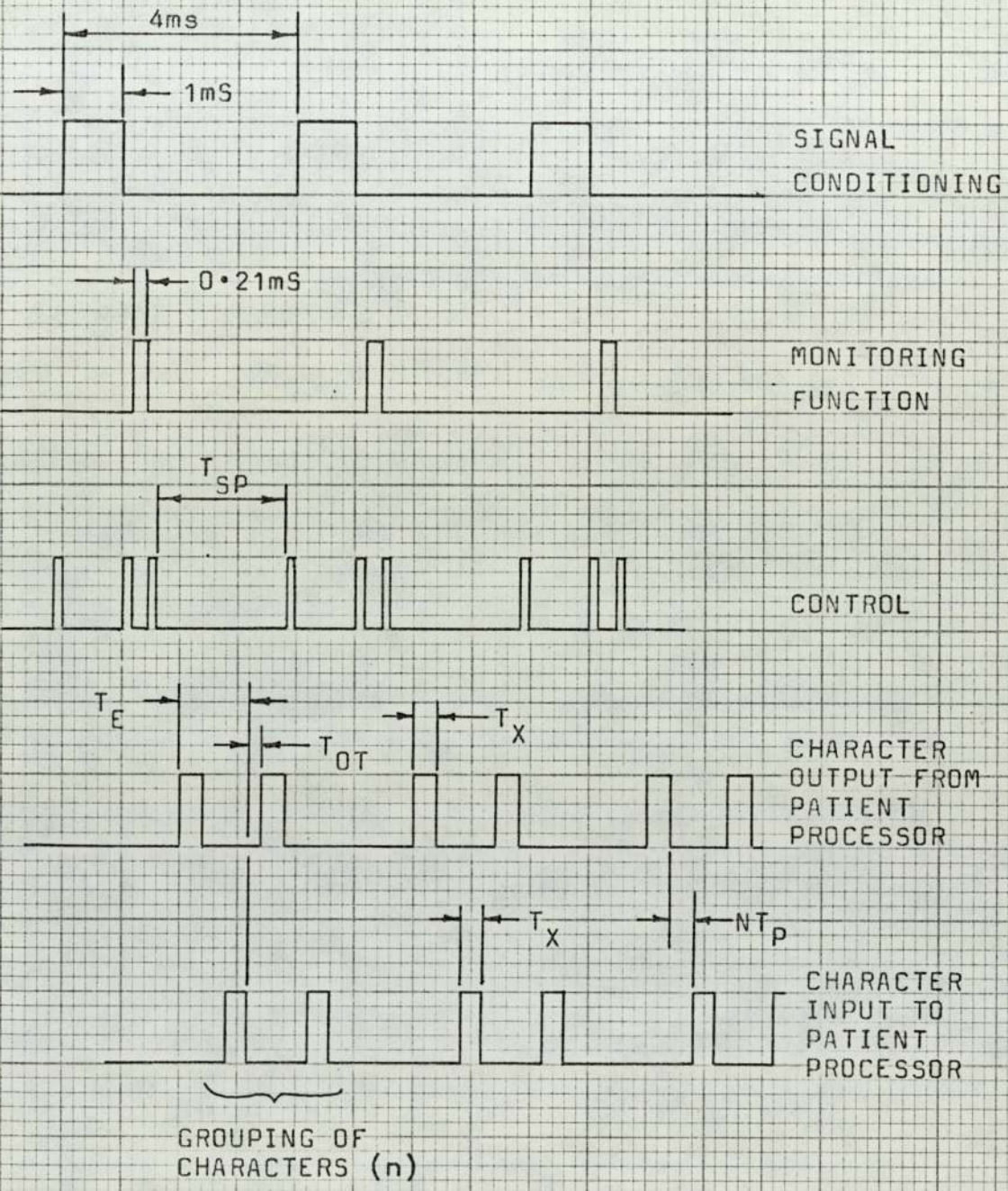


Fig. 8.5. INTER-PROCESSOR COMMUNICATION TIMING
DIAGRAM.

causes the flow of characters between the processors to be grouped together. The discontinuities seen in the graphs (Fig. 8.3. and Fig. 8.4.) are due to this grouping effect, because although the bit rate may be reduced considerably, the number of characters sent in each available time interval (T_{SP}), remains constant.

As these time intervals are regular, and the number of characters in each interval remains constant over a range of bit rates, the result is a constant block transmission time, and thus the discontinuity in the graph. The three discontinuities seen in the graphs, correspond to the transmission of 3, 2 and then 1 character in each time interval.

The intervals between the discontinuities are transition states where the number of characters in each interval varies.

In order to determine some analytical approach which would allow the transmission time for larger numbers of patient processors to be estimated; measurements were made of the time interval between the transmission of a character from the patient processor, and the reception of a reply character. This time interval was referred to as the transmission echo time (T_E) and the results obtained are shown in Fig. 8.6. As can be seen from these graphs, a linear relationship exists between the transmission echo time (T_E), the character transmission time (T_X) and the number of patient processors (N). This relationship

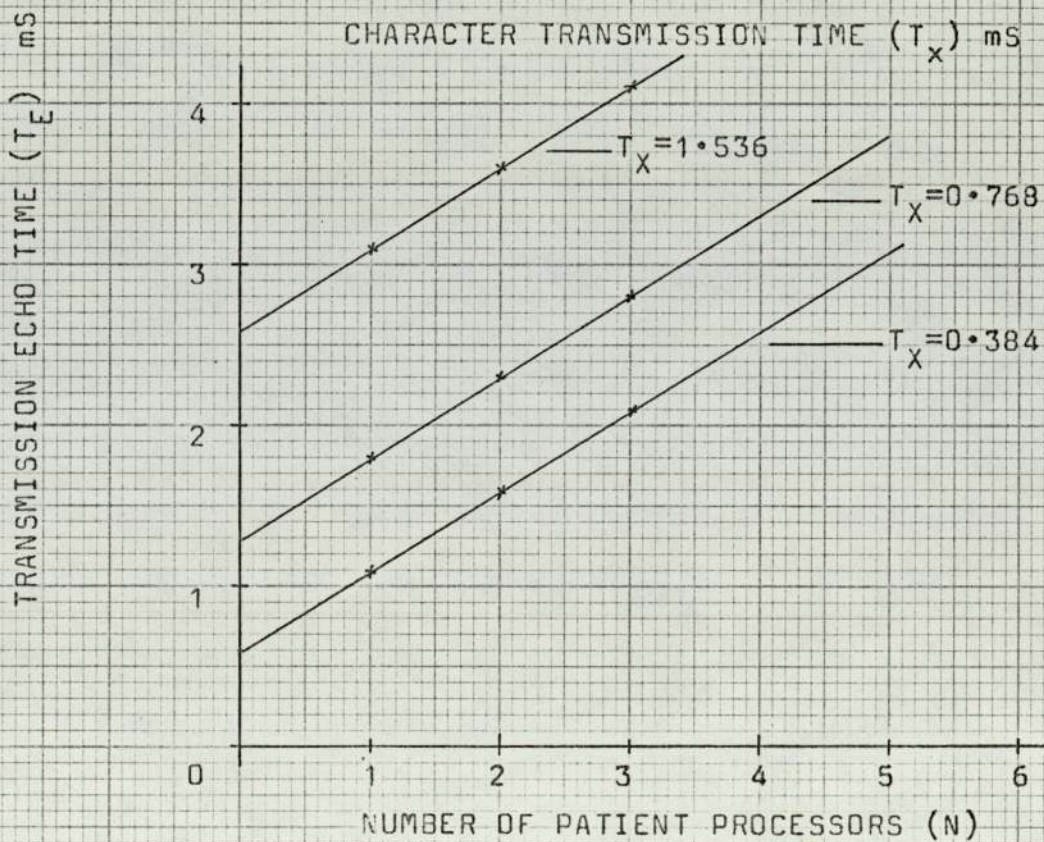
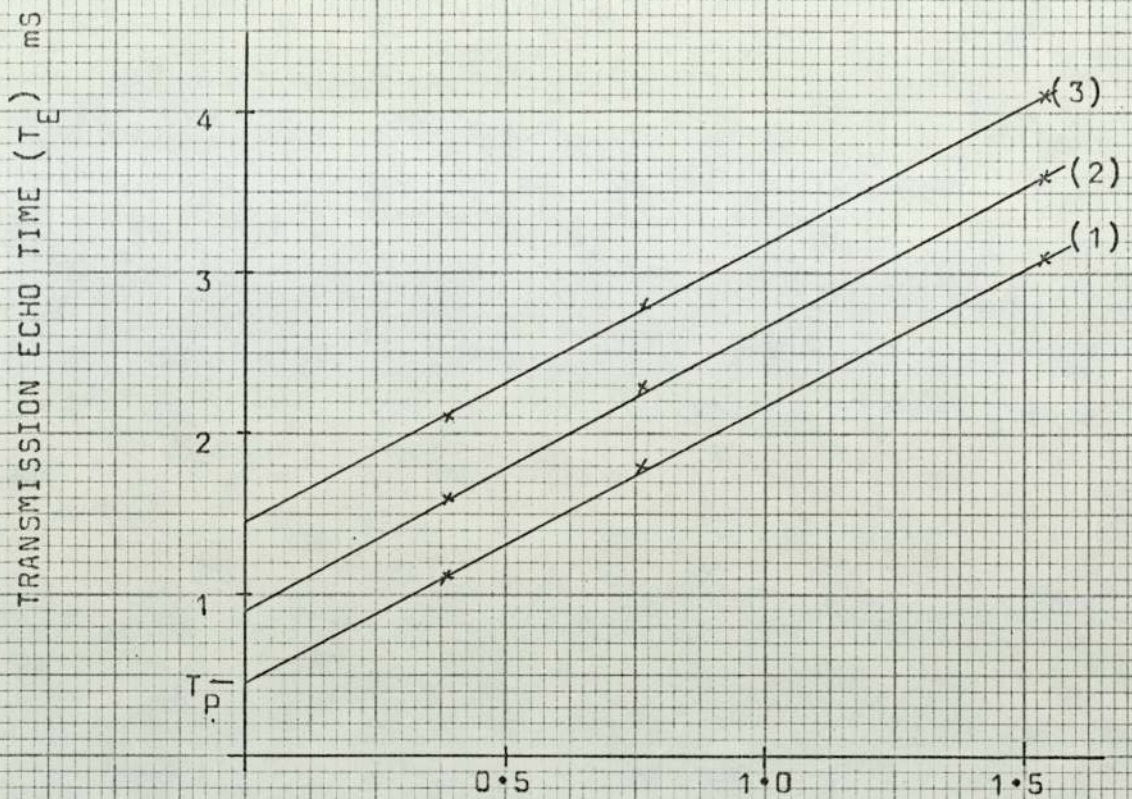


Fig. 8.6. EFFECT OF INCREASING T_X ON T_E (TOP GRAPH)
EFFECT OF INCREASING N ON T_E (BOTTOM GRAPH).

is therefore given by,

$$T_E = 2T_X + NT_P \quad (8.1.)$$

The time T_P (Fig. 8.5.) is the constant processing time at the operator processor system, and was found to be equal to 0.45mS as shown in Fig. 8.6.

In order to estimate the block transmission time, the number of characters (n) that are sent during the surplus processing time (T_{SP}), at the patient processor system, must be known. The number of characters (n) may be estimated by,

$$n \approx \frac{T_{SP}}{T_E + T_{OT}} \quad (8.2.)$$

where T_{OT} is the response time of the patient processor output task (Fig. 8.5.), which was measured as being approximately 0.08mS.

Having obtained values for n , which correspond to the number of characters sent in a 4mS interval, it is then possible to estimate the block transmission time (T_B) from,

$$T_B \approx \frac{4 \times 10^{-3} \times N_B}{n} \quad (8.3.)$$

where N_B is the number of bytes sent in a block.

Using this approach it was possible to produce the graph as shown in Fig. 8.7., which is an approximation to the graph shown in Fig. 8.4. From this graph (Fig. 8.7.)

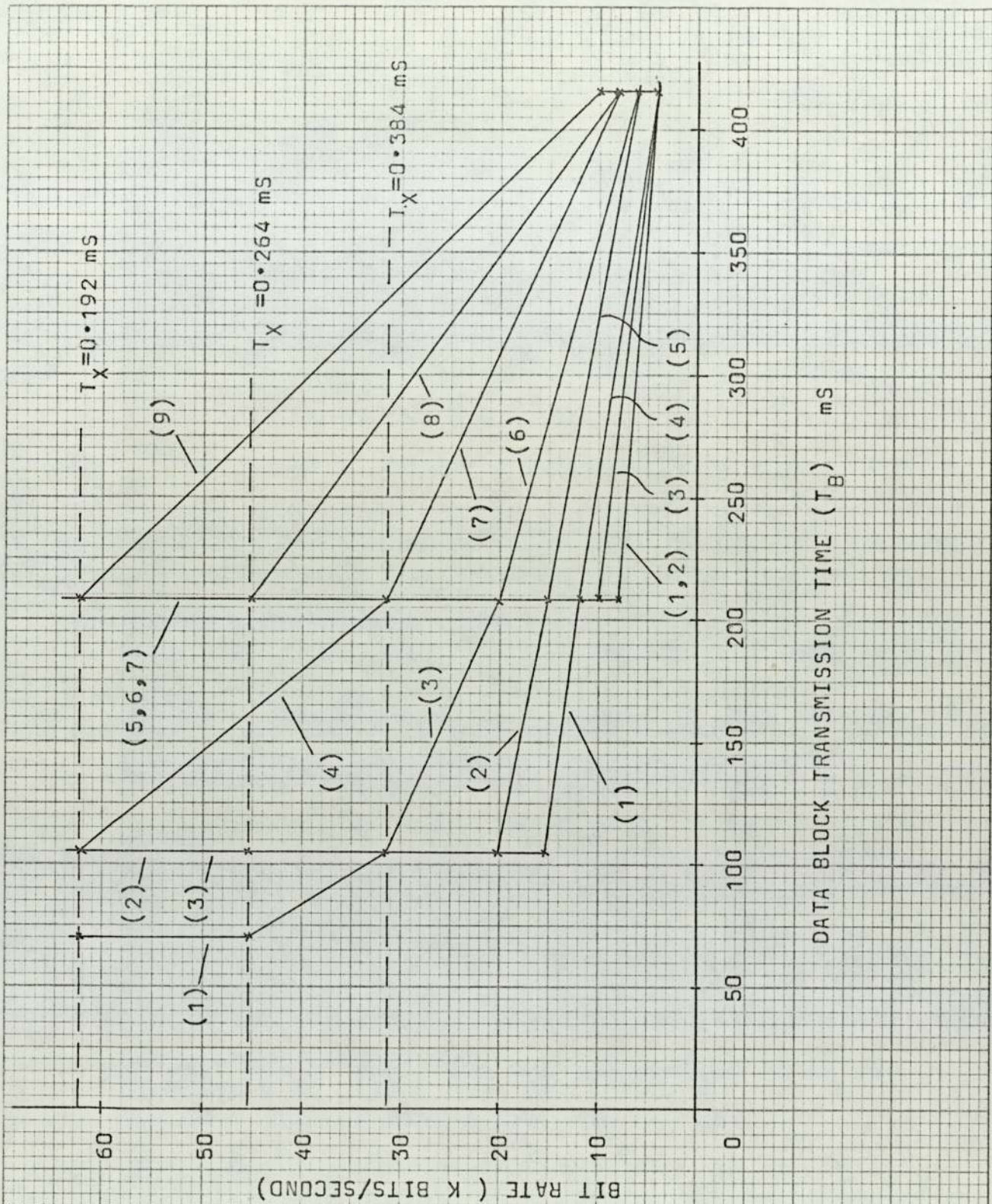


Fig. 8.7. GRAPH SHOWING CALCULATED EFFECT OF INCREASING THE NUMBER OF PATIENT PROCESSORS (N).

it was then possible to produce the curve shown in Fig. 8.8., which indicates the estimated maximum block transmission time for simultaneous communication with N patient processors. These results are for the worst case communication conditions, as they are calculated for simultaneous reception of all characters, as in the simulation system. In the normal system, however, if characters are received simultaneously, the operation of the operator processor operating system, causes the communications with each patient processor to become unsynchronised, and results in faster block transmission times.

It has been shown by the previous discussion that the real-time processing performed by each patient processor, is responsible for limiting the rate of information flow between processors. If the execution time of the signal conditioning function was increased, for example, the result would be a reduction in the surplus processing time (T_{SP}). This would result, as indicated by equations 8.2. and 8.3., in an increase in the block transmission times.

Within the present implementation of the inter-processor communications protocol, a time interval greater than 16mS between characters, indicates an error condition. With this arrangement, it allows the maximum block transmission time to be approximately 830mS, which would allow the operator system to communicate

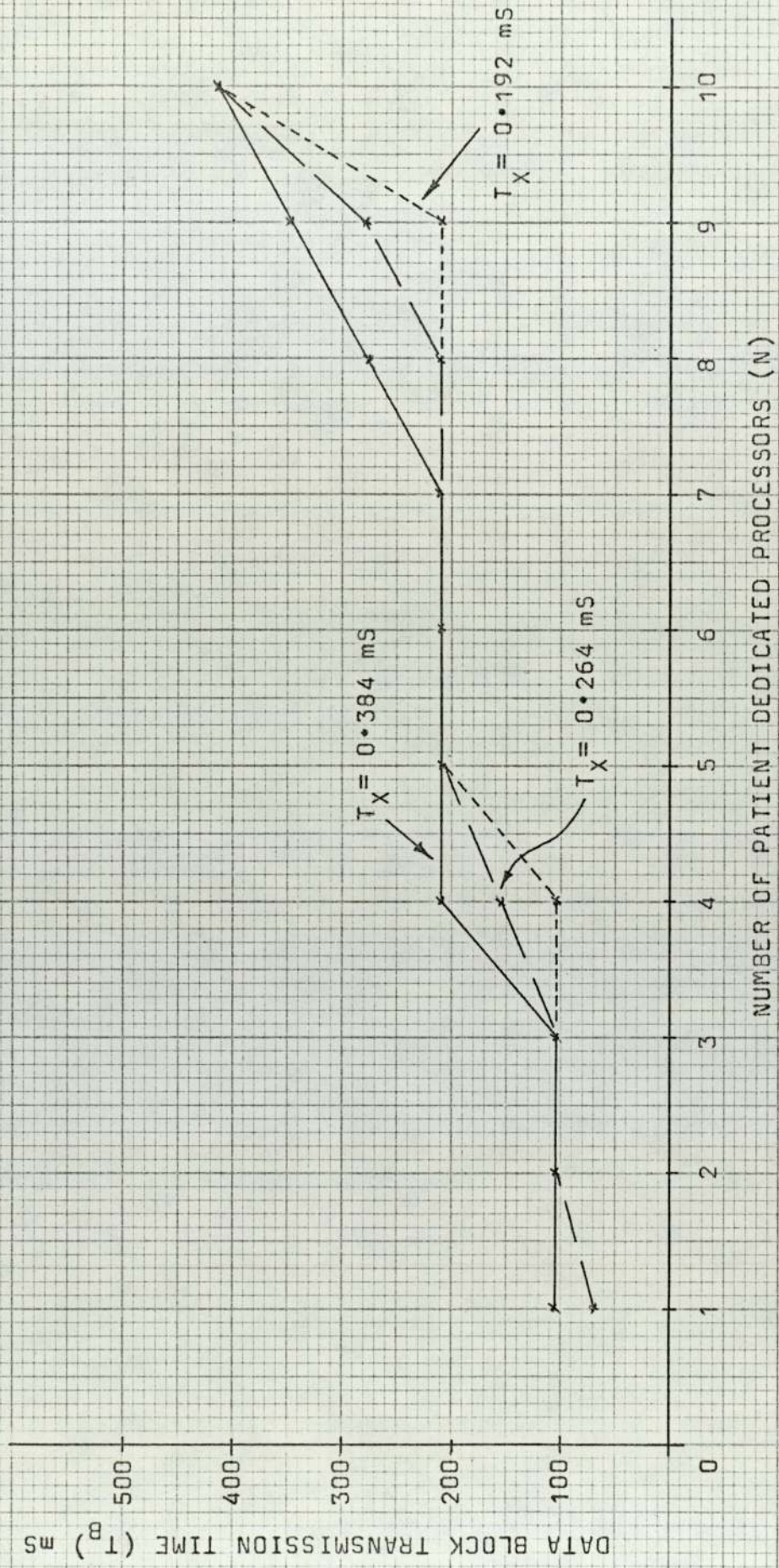


Fig. 8.8. MAXIMUM BLOCK TRANSMISSION TIME FOR SIMULTANEOUS COMMUNICATION WITH N PATIENT PROCESSORS.

simultaneously with approximately 30 patient processors without timing errors occurring. However, in a more practical system, it is likely that some other limit on the block transmission time would be specified. For example, it may be required that the block transmission time should not exceed the R-R time interval, when the pulse rate is 200 beats/minute (R-R interval = 300ms). With such a specification, it can be seen from Fig. 8.8., that the ideal number of patient processors in such a system would be eight.

Therefore, the number of patient processors in the final system will depend upon how much the existing real-time algorithms are expanded, and the maximum allowed block transmission time.

CHAPTER 9

CONCLUSIONS

9.1. General

The aim of this research project was to examine the possibility of using microprocessors, to produce an on-line real-time ECG arrhythmia monitoring system.

As a result of the research work performed, it has been demonstrated that although the execution times of current microprocessors are slower, compared to that of computers, their implementation in a distributed network enables a real-time ECG arrhythmia monitoring system to be produced. It has also been demonstrated that a suitable structure for a multi-patient distributed microprocessor system, is the allocation of a microprocessor to each patient, controlled by a centralised operator-dedicated microprocessor. The functions performed by these patient-dedicated processors are that of signal conditioning, monitoring and arrhythmia diagnosis.

This modular approach developed, results in a flexible system structure, which would allow mass produced systems to be tailored to each CCUs requirements.

The design of a system with this structure has been described, and the methods for realising each function have been examined in this report. The distributed structure of the monitoring system enabled the recommendations by Wartak et. al. regarding ECG sampling rate and Van Eyll et. al. regarding optimal parameters for QRS

detection, to be implemented in this system. Other multi-patient computer monitoring systems, have used sampling rates less than that recommended by Wartak et. al., to enable multi-patient monitoring to be performed. Also the distributed microprocessor approach eliminates the need for an operating system capable of allocating processing time to each patient, as is required in multi-patient computer systems.

As a result of the problems encountered regarding the monitoring criteria to be used by the system, as discussed in Chapter 2, and also due to the lack of detailed diagnosed ECG recordings, no detailed evaluation of the systems diagnosis performance was undertaken. It is considered that further medical research is required to specify precisely diagnosis criteria for use by monitoring systems, and also that medical experts should be deeply involved in any system diagnosis performance evaluation.

As the monitoring and diagnosis functions are implemented in software, any new or improved monitoring criteria obtained from further work could be introduced easily into the system, as demonstrated by the implementation of the suggested alternative monitoring criteria described in Section 2.2.2.

It has also been shown that within the present performance of the system there is ample scope for expansion, before the processing time consumed becomes excessive. This system performance is a direct result of

programming all software in assembly language. Although assembly language programming requires more programming effort, it enabled the execution times of the various algorithms to be made as short as possible. It is considered that had these programs been produced using a real-time high level language such as CORAL 66, the current opportunity for expansion would not have been so great.

It has been estimated that had these programs been produced in industry, the developmental cost of the software produced would have been £14,000. As this software is repeated and spread throughout the system, and if the patient-dedicated processor units were mass produced, the cost of software development per unit should not be excessive. The cost of a complete multi-microprocessor monitoring system, should therefore be far less than currently available computer monitoring systems.

Also, with the advent of microcomputers, such as the TMS 9940 (which is a single chip containing a CPU and currently limited ROM and RAM), there is the prospect of reducing the cost of the system still further.

9.2. Suggestions for Future Development

As it is apparent that there is the need for further medical research to be performed, to assess and develop new monitoring criteria, it is thought that a single microprocessor monitoring system could provide an inexpensive system for such studies.

Within the current patient processor system work could be performed to determine if QRS detection would be improved if the detection algorithm used only the low-pass filtered ECG signal, instead of the conditioned signal which may or may not have been filtered. Also the artefact indicator incorporated in the signal conditioning function, could be used to a greater extent, in order to inhibit certain monitoring operations, with a view to reducing the number of false positive diagnoses.

The introduction of a mass storage media into the system would enable trend data analysis to be performed, which could well be enhanced by some form of colour graphics display.

Other directions in which this project could be expanded, is by the introduction of another patient-dedicated processor, which could monitor the slower physiological signals, resulting in a total care monitoring system.

Alternatively, the system could be developed as a 12 lead monitoring system, enabling more sophisticated clinical diagnoses of individual patients to be obtained.

9.3. Final Remarks

There have been enquiries received from industry, relating to this research project, which have indicated that the system described in this report should have good commercial prospects. It is hoped that such interest will result in the benefits possible from a real-time arrhythmia monitoring system, being more widely available

than at the present moment.

At this time when many people see the advent of microprocessors as producing social problems, such as unemployment due to automation, it is hoped that work such as this research project, indicates that such devices can also improve the quality of life.

APPENDIX A

THE TMS 9900 MICROPROCESSOR

HARDWARE FEATURES

The microprocessor used throughout the development of the multi-microprocessor arrhythmia monitoring system, is the TMS 9900. This microprocessor is a single-chip 16 bit central processing unit (CPU), produced using N-channel silicon-gate MOS technology. The CPU comes in a 64 pin chip, and is driven by a 3MHz four phase clock.

The processor employs a memory-to-memory form of architecture, whereby blocks of memory designated as workspace registers, replace the more common internal hardware registers. The basic microprocessor memory structure is shown in Fig. A.1, and as can be seen the first 32 words of memory are used for the 16 interrupt trap vectors. The next block of 32 words are then used for extended operation (XOP) instruction trap vectors. The last two memory words, $FFFC_{16}$ and $FFFE_{16}$, are used for the trap vectors of the LOAD signal. The remaining memory is then available for programmes, data and workspace registers. A total of 32,768 words of memory can be addressed by the processors 15 bit address bus, which is separate from the 16 bit data bus, thus simplifying the system design.

Within the processor there are three registers which

are accessible by the user. These are the program counter (PC) which contains the address of the instruction following the current instruction being executed. The status register (ST) which contains the interrupt mask level and status information, relating to the instruction operation. The third and final register is the workspace pointer (WP) which contains the address of the first word in the current active workspace area. A workspace area consists of 16 consecutive memory words in the general memory area.

The workspace concept is particularly valuable during operations that require a context switch (i.e. a change from one program to another, or to a subroutine, for example when an interrupt occurs).

The processor can handle a total of 16 interrupt levels, which are serviced rapidly due to the memory-to-memory architecture.

Input and output data transfers to and from the processor are performed by a direct command-driven I/O Interface designated as the communications-register unit (CRU). The CRU provides up to 4096 directly addressable input and output bits. Both input and output bits can be addressed individually or in fields of 1 to 16 bits.

Software Features

The TMS 9900 microprocessor instruction set provides the same capabilities as those offered by full

minicomputers. The instruction set provides 69 different instructions, which includes unsigned multiply and divide instructions.

The multiply instruction allows two unsigned 16 bit numbers to be multiplied together to produce a 32 bit answer. The divide instruction allows an unsigned 32 bit number to be divided by a 16 bit number, the answer being given as a 16 bit quotient and a 16 bit remainder.

Other instructions which were to be of particular use during the development of the arrhythmia monitoring system were the "compare ones corresponding" (COC) and "compare zeros corresponding" (CZC) instruction, which can be used to implement decision table programs.

The complete list of instruction mnemonics is given in Table A.1., along with the explanation of how to calculate individual instruction execution times. With a clock frequency of 3MHz, the average instruction execution time is approximately 10 μ S.

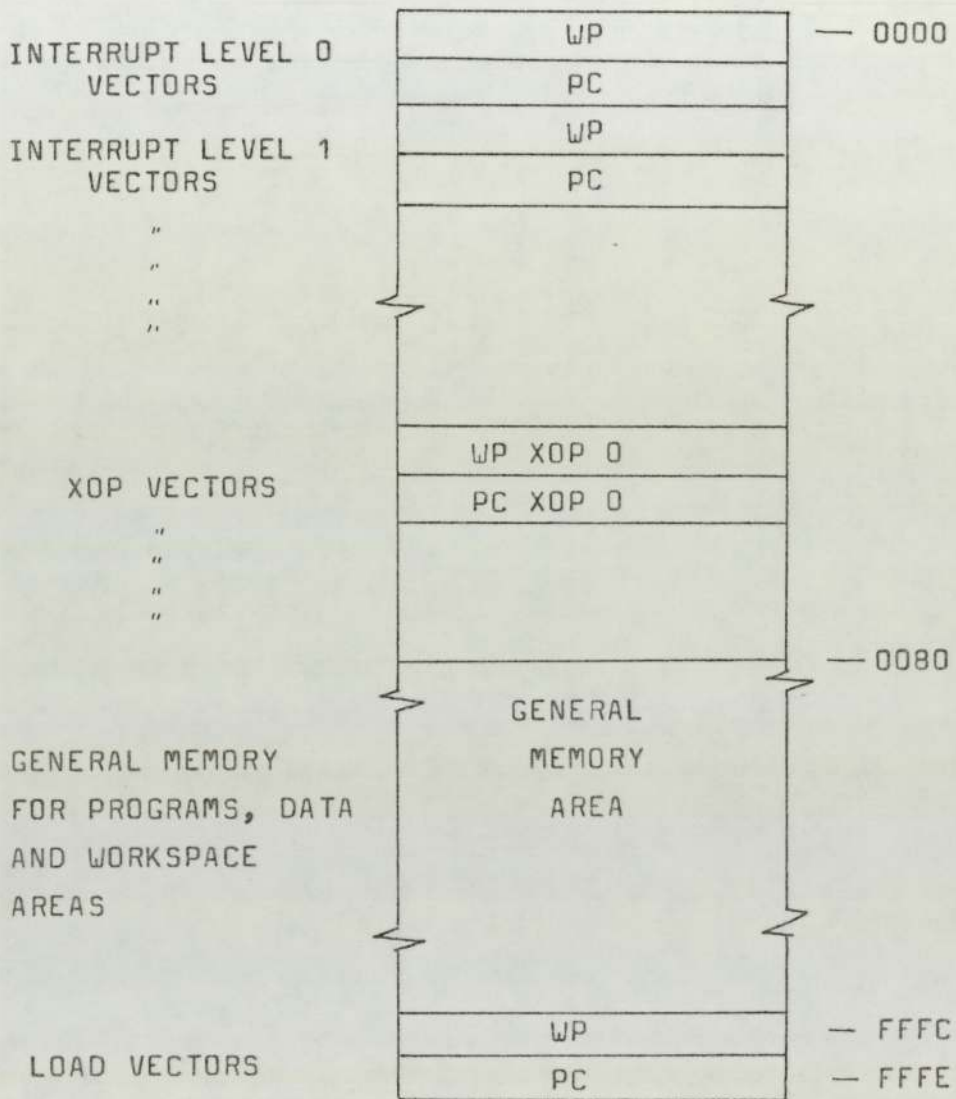


Fig. A.1. BASIC MEMORY STRUCTURE.

Instruction execution times for the TMS 9900 are a function of:

- 1) Clock cycle time, $t_{c(\phi)}$
- 2) Addressing mode used where operands have multiple addressing mode capability
- 3) Number of wait states required per memory access.

Table 3 lists the number of clock cycles and memory accesses required to execute each TMS 9900 instruction. For instructions with multiple addressing modes for either or both operands, the table lists the number of clock cycles and memory accesses with all operands addressed in the workspace-register mode. To determine the additional number of clock cycles and memory accesses required for modified addressing, add the appropriate values from the referenced tables. The total instruction-execution time for an instruction is:

$$T = t_{c(\phi)} (C + W \cdot M)$$

where:

- T = total instruction execution time;
- $t_{c(\phi)}$ = clock cycle time;
- C = number of clock cycles for instruction execution plus address modification;
- W = number of required wait states per memory access for instruction execution plus address modification;
- M = number of memory accesses.

TABLE 3
INSTRUCTION EXECUTION TIMES

INSTRUCTION	CLOCK CYCLES C	MEMORY ACCESS M	ADDRESS MODIFICATION ¹		INSTRUCTION	CLOCK CYCLES C	MEMORY ACCESS M	ADDRESS MODIFICATION ¹	
			SOURCE	DEST				SOURCE	DEST
A	14	1	A	A	LWPI	10	2	A	A
AB	14	4	B	B	MOV	14	4	A	A
ABS (MSB = 0)	17	2	A	-	MOVB	14	4	B	B
(MSB = 1)	14	3	A	-	MPY	52	5	A	-
AI	14	4	-	-	NEG	12	3	A	-
ANDI	14	4	-	-	ORI	14	4	-	-
B	8	2	A	-	RSET	12	1	-	-
BL	12	3	A	-	RTWP	14	4	-	-
BLWP	26	6	A	-	S	14	4	A	A
C	14	3	A	A	SB	14	4	B	B
CB	14	3	B	B	SIBD	32	2	-	-
CS	14	3	-	-	SIRZ	12	2	-	-
CAOI	12	1	-	-	SLTD	10	3	A	-
CAON	12	1	-	-	SHR (C=0)	12+2N	3	-	-
CLR	10	3	A	-	IC-0, Bn 12-15 of WRO-0)	52	4	-	-
COC	14	3	A	-	IC-0, Bn 12-15 of WRP-N=0)	20+2N	4	-	-
CZC	14	3	A	-	SOC	14	4	A	A
DEC	10	3	A	-	SOGB	14	4	B	B
DECT	10	3	A	-	STCR IC-0)	60	4	A	-
DIV (ST4 is set)	16	3	A	-	(1=Cx7)	42	4	B	-
DIV (ST4 is reset)	92-124	6	-	-	IC-8)	44	4	B	-
DIU	12	3	-	-	(9=Cx15)	58	4	A	-
INC	10	3	A	-	STST	8	2	-	-
INCT	10	3	A	-	STWP	8	2	-	-
INV	10	3	A	-	SWRB	10	3	A	-
Jump (PC is changed)	10	1	-	-	SZC	14	4	A	A
IPC is not changed)	8	1	-	-	SZCB	14	4	B	B
LDCH (C = 0)	52	3	A	-	TB	12	2	-	-
(1=Cx8)	20+2C	3	B	-	X**	8	2	A	-
(9=Cx15)	20+2C	3	A	-	XCP	44	8	A	-
LI	12	3	-	-	XDR	14	4	A	-
LISH	16	3	-	-					
STLR	12	1	-	-					
TEST function	28	6	-	-					
TESTAD function	24	6	-	-					
Interrupt context switch	24	6	-	-					
					Unlimited op codes				
					0000 011 F, 0320	6	1	-	-
					033F 0C00 0FFF				
					0780 07FF	8	2	A	-

*Execution time is dependent upon the partial quotient after each clock cycle during execution.
¹Execution time is added to the execution time of the instruction located at the source address.
²The letters A and B refer to the respective tables that follow.

ADDRESS MODIFICATION - TABLE A

ADDRESSING MODE	CLOCK CYCLES		MEMORY ACCESSES	
	C	M	C	M
WR (T _S or T _D = 00)	0	0		
WR indirect (T _S or T _D = 01)	4	1		
WR indirect auto-increment (T _S or T _D = 11)	8	2		
Symbolic (T _S or T _D = 10, S or D = 0)	8	1		
Indexed (T _S or T _D = 10, S or D ≠ 0)	8	2		

ADDRESS MODIFICATION - TABLE B

ADDRESSING MODE	CLOCK CYCLES		MEMORY ACCESSES	
	C	M	C	M
WR (T _S or T _D = 00)	0	0		
WR indirect (T _S or T _D = 01)	4	1		
WR indirect auto-increment (T _S or T _D = 11)	6	2		
Symbolic (T _S or T _D = 10, S or D = 0)	8	1		
Indexed (T _S or T _D = 10, S or D ≠ 0)	8	2		

As an example, the instruction MOVB is used in a system with $t_{c(\phi)} = 0.333 \mu s$ and no wait states are required to access memory. Both operands are addressed in the workspace register mode.

$$T = t_{c(\phi)} (C + W \cdot M) = 0.333 (14 + 0 \times 4) \mu s = 4.662 \mu s$$

If two wait states per memory access were required, the execution time is:

$$T = 0.333 (14 + 2 \times 4) \mu s = 7.326 \mu s$$

If the source operand was addressed in the symbolic mode and two wait states were required:

$$T = t_{c(\phi)} (C + W \cdot M)$$

$$C = 14 + 8 = 22$$

$$M = 4 + 1 = 5$$

$$T = 0.333 (22 + 2 \cdot 5) \mu s = 10.656 \mu s$$

4. TMS 9900 ELECTRICAL AND MECHANICAL SPECIFICATIONS

4.1 ABSOLUTE MAXIMUM RATINGS OVER OPERATING FREE-AIR TEMPERATURE RANGE (UNLESS OTHERWISE NOTED)*

Supply voltage, V _{CC} (see Note 1)	-0.3 to 20 V
Supply voltage, V _{DD} (see Note 1)	-0.3 to 20 V
Supply voltage, V _{SS} (see Note 1)	-0.3 to 20 V
All input voltages (see Note 1)	-0.3 to 20 V
Output voltage (with respect to V _{SS})	-2 V to 7 V
Continuous power dissipation	1.2 W
Operating free-air temperature range	0°C to 70°C
Storage temperature range	-55°C to 150°C

*Stresses beyond those listed under "Absolute Maximum Ratings" may cause permanent damage to the device. This is a stress rating only and functional operation of the device at these or any other conditions beyond those indicated in the "Recommended Operating Conditions" section of this specification is not implied. Exposure to absolute maximum rated conditions for extended periods may affect device reliability.
 NOTE 1. Under absolute maximum ratings voltage values are with respect to the most negative supply, V_{BB} (substrate), unless otherwise noted. Throughout the remainder of this section, voltage values are with respect to V_{SS}.

TABLE A.1. INSTRUCTIONS

APPENDIX B

PATIENT PROCESSOR PROGRAM LISTING

All the programs and data modules required to produce the patient processor software system, are supplied in this appendix, in the order in which they appear in the link editor listing shown below.

PHASE 0, PATIENT ORIGIN = 0000 LENGTH = 1830

MODULE	NO	ORIGIN	LENGTH
PMPTVP	1	0000	00A4
PPINIP	2	00A4	00A0
PPTHAP	3	0144	00D6
PPCIHP	4	021A	00BA
PPUIHP	5	02D4	014C
IPDHTP	6	0420	01B6
MONTDP	7	05D6	018A
MONS1P	8	0760	0284
MONS2P	9	09E4	0142
DIAT1P	10	0B26	00DC
IPPTOP	11	0C02	00B0
DPPTOP	12	0CB2	0082
MCPTOP	13	0D34	0130
P0001D	14	0E64	0014
P0002D	15	0E78	000C
P0003D	16	0E84	002E
P0004D	17	0EB2	0032
P0005D	18	0EE4	0034
P0009D	19	0F18	0018
IPDHTD	20	0F30	00C1
MONTDD	21	0FF2	0020
G0016D	22	1012	007A
G0017D	23	103C	0024
G0003D	24	10B0	02EE
G0004D	25	139E	0362
G0005D	26	1700	003E
G0006D	27	173E	0024
G0018D)	28	1762	00CE

PATIENT PROCESSOR PROGRAM LABELS

D E F I N I T I O N S

NAME	VALUE	NO	NAME	VALUE	NO	NAME	VALUE	NO	NAME	VALUE	NO
A1	0E68	14	A1DC	0E74	14	A2	0E6A	14	A2DC	0E76	14
ACTND	101C	22	ARST6	0EEC	18	ARTIF	109E	23	ASVT7	0EEE	18
AVRR	16FC	25	AVRRB	0E96	16	BBB3	0EE6	18	BEATS	0EA4	16
BPM100	0E8A	16	BPM110	0E88	16	BPM120	0E86	16	BPM140	0E84	16
BPM20	0E94	16	BPM40	0E92	16	BPM60	0E90	16	BPM80	0E8E	16
BPM90	0E8C	16	BRAD4	0EE8	18	BUFEND	0FEE	20	BUFFER	0FB4	20
BUFLEN	0E78	15	C	0E70	14	CLRWT	10AE	23	CM	0F23	19
CMS	10A0	23	CDC1	0EB2	17	CDC2	0EB6	17	CDC3	0EBC	17
CDC4	0EC0	17	CDC5	0EC8	17	CDC6	0ECA	17	CDUNT	0E9E	16
CPCRET	104C	22	CSTIMC	1060	22	CSTRET	104E	22	CWPRET	104A	22
CZC1	0EB4	17	CZC2	0EB8	17	CZC3	0EBA	17	CZC4	0EBE	17
CZC5	0EC2	17	CZC6	0EC4	17	CZC7	0EC6	17	DARST0	0F0A	18
DARST1	0F08	18	DASYT0	0F0E	18	DASYT1	0F0C	18	DEBB0	0EFE	18
DEBB1	0EFC	18	DBP1	168E	25	DBRAD0	0F02	18	DBRAD1	0F00	18
DBUFL	0E7A	15	DESCB0	0F12	18	DESCB1	0F10	18	DF1	175E	27
DF2	1760	27	DF6D	10A2	23	DIAG	1054	22	DIAGM	0F1A	19
DIARNT	108E	23	DIAT11	0B26	10	DIAT1W	173E	27	DIDID0	0F06	18
DIDID1	0F04	18	DISF	1098	23	DLS1	0F14	18	DMINC	1738	26
DMIND	1736	26	DPCRET	103A	22	DRTWP	101E	22	DSTIMC	105E	22
DSTRET	103C	22	DSVTA0	0EF6	18	DSVTA1	0EF4	18	DSVTB0	0EFA	18
DSVTB1	0EF8	18	DMPRET	1038	22	EIGHT	0EE2	17	EM	0F22	19
ESCBT8	0EF0	18	FINISH	0732	7	FIVE	0EAA	16	HOURS	106A	22
HPOP	0FB0	20	HUND	0EA6	16	IBP1	139E	25	IBUF	10B0	24
IDH	1050	22	IDIDV5	0EEA	18	IPCRET	1040	22	IPDHT1	0420	6
IPDHTW	0F30	20	IPFILE	1782	28	IPINT	1090	23	IPPT01	0C02	11
IPPT02	0C8A	11	IPPT03	0CA0	11	IPPT0W	1762	28	IPRTWP	1024	22
IPTASK	1056	22	ISTRET	1042	22	IMPRET	103E	22	K1LP	0E6C	14
K2LP	0E6E	14	KDC	0E72	14	KHP	0E66	14	LEVEL	0E64	14
LPOP	0FB2	20	LS23	0EF2	18	MAXP	172A	26	MAXV	1726	26
MCP	105A	22	MCPINT	1094	23	MCPIP	109C	23	MCPT01	0D34	13
MCPT0W	180A	28	MORTWP	1030	22	MF1	1700	26	MF2	1702	26
MFAIL	0F1F	19	MINL	0E7C	15	MINP	1728	26	MINUTE	1068	22
MINV	1724	26	MM1	0F25	19	MM2	0F26	19	MN3	0F27	19
MM4	0F28	19	MM5	0F29	19	MM6	0F2A	19	MONI	1052	22
MONINT	108C	23	MONS11	0760	8	MONS1W	1704	26	MONS21	09E4	9
MONSF	109A	23	MONTD1	05D6	7	MONTDW	0FF2	21	MONWR3	0FF8	21
MOTEXT	182C	28	MPCRET	1034	22	MRTWP	1018	22	MSEC	1064	22
MSTIMC	105C	22	MSTRET	1036	22	MSUVE	0F1E	19	MWPRET	1032	22
NDORS	0E0E	9	NP	16F4	25	NORS6B	0EDE	17	DFSET0	173C	26
OPAC	1062	22	OPCRET	1046	22	OPDATA	182A	28	OPFILE	17D6	28
OPINT	1092	23	OPPT01	0CB2	12	OPPT0W	17B6	28	OPRTWP	102A	22
OPTASK	1058	22	OSTRET	1048	22	DMPRET	1044	22	P2POS	173A	26
PER82	0EAC	16	POINT	16FE	25	PPCIH1	021A	4	PPCIH2	025A	4
PPINI1	00A4	2	PPTHAI	0144	3	PPTHAW	1012	22	PPUIH1	02D4	5
PPUIH2	03B6	5	PPUIH3	03CC	5	PPUIH4	03E8	5	PPUIH5	0402	5
PPUIHW	106C	22	PR	0F20	19	PRGT60	0F16	18	PRM	0F18	19
PS	0F24	19	PSD	0F1C	19	PUART	040C	5	QRSNT	0EB1	16
QRSPT	0EB0	16	QRSMB	0EA2	16	QRSMID	0EA0	16	RAM	0F30	20
RAM2	0F32	20	RAMEND	1830	28	RRC	16F6	25	RRC32	0E7E	15
RRLB	0E98	16	RRMAXT	0EE0	17	RRSAVE	16F8	25	RRSB	0E9A	16
SDELAY	10A4	23	SEC	1066	22	SEQ1	0EEC	17	SEQ2	0ECE	17
SEQ3	0ED0	17	SEQ4	0ED2	17	SEQ5	0ED4	17	SEQ6	0ED6	17
SEQ7	0ED3	17	SEQ8	0EDA	17	SEQ9	0EDC	17	SEQ8	0E9C	16
SETEND	10B0	23	SETNEG	10A2	23	SETONE	109C	23	SFP1	10A6	23
SIX	0E82	15	SIXTY	0F2E	19	SH	0F21	19	SR250	0F2C	19
SU	10A8	23	SU2	10AA	23	SU3	10AC	23	SVT2	0EE4	18
T1	172C	26	T2	172E	26	T3	1730	26	TDP1	16F2	25
TEN	0E80	15	TG	1096	23	TWELVE	0EA8	16	VALUE	0FF0	20
W1	1732	26	W2	1734	26	WADC	0F90	20	WAHP	0F50	20
WALP	0F70	20	WID82S	182E	28	WID82	0EAE	16	WORS	16FA	25

PATIENT MONITORING PROCESSOR TRANSFER
VECTOR PROGRAM MODULE

1. DESCRIPTION

This program module defines the interrupt and XOP transfer vectors used by the Patient Monitoring Processor. Interrupt level 2 and XOP level 15 have been initiated to their appropriate values for the 990/4 Monitor software.

2. IDENTIFICATION

SUBROUTINE NAME	PMPTV
PROGRAM MODULE	PMPTVP
GENERAL DATA MODULE	G0016D

3. SIZE

PROGRAM MODULE	164	Bytes
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4. CALLS FROM SUBROUTINE

INTERRUPT LEVEL	0	PPINI1
INTERRUPT LEVEL	3	PPCIH1
INTERRUPT LEVEL	4	PPUIH1

5. AUTHOR

B.T.V. WARTON.

SCR2.PROG.S.PMPTVP 16:46:30 TUESDAY, OCT 17, 1978.

```
TITL 'PATIENT MONITORING PROCESSOR TRANSFER VECTOR PROGRAM'
♦ PROGRAM MODULE IDENTIFIER (PROG)
  IDT 'PMPTVP'
♦ CALLED PROGRAM MODULES
  REF PPINIP,PPCIHP,PPUIHP
  REF PPINI1,PPCIH1,PPUIH1
♦ LINKED DATA MODULES
  REF 60016D,PPTHAW,PPUIHW
  RORG
  PSEG
♦ PROGRAM
  DATA PPTHAW,PPINI1
  DATA 0,0
  DATA 0,>5D26
  DATA PPTHAW,PPCIH1
  DATA PPUIHW,PPUIH1
  DATA 0,0,0,0,0,0,0,0
  DATA 0,0,0,0,0,0,0,0,0,0
  DATA 0,0,0,0
  DATA 0,0,0,0,0,0,0,0,0,0
  DATA 0,0,0,0,0,0,0,0,0,0
  DATA 0,0,0,0,0,0,0,0,0,0
  DATA >77D2,>604E
  BSS 32
ENTRY1 BLWP 70
END ENTRY1

INTERRUPT 0 TRANSFER VECTORS
  1
  2 REQUIRED BY MONITOR
  3
  4
  5 TO 8
  9 TO 13
  14 & 15
XDP TRANSFER VECTORS
  XDP 15 REQUIRED BY MONITOR
  WORKSPACE REQUIRED BY MONITOR
  EMULATE INT 0
```

PATIENT PROCESSOR INITIALISATION PROGRAM

1. DESCRIPTION

This program runs at system start up time to initialise software and hardware as follows. First all RAM used is cleared then all software flags that should be set to +1 or -1 are initialised. All workspace registers requiring CRU base addresses and other parameters are then initialised, and finally the ADC/DAC and UART are reset and initialised.

On completion of this program control is passed to the Patient Processor Task Handler program.

2. IDENTIFICATION

PROGRAM MODULE	PPINIP
SPECIFIC DATA MODULE	IPDHTD
SPECIFIC DATA MODULE	MUNTDD
GENERAL DATA MODULE	G0001D
GENERAL DATA MODULE	G0002D
GENERAL DATA MODULE	G0003D
GENERAL DATA MODULE	G0008D

3. SIZE

PROGRAM MODULE	160	Bytes
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4. CALLS TO SUBROUTINE

BLWP @PPINI1

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	PPTHAP
BLWP @PPTHAI	
PROGRAM MODULE	PPUIHP
BL @PUART	

6. AUTHOR

B.T.V. WARTON.

```

        TITL 'PATIENT PROCESSOR INITIALISATION PROGRAMME'
♦ PROGRAMME MODULE IDENTIFIER (TASK)
        IDT 'PPINIP'
♦ TRANSFER VECTORS OR ENTRIES
        DEF PPINI1
♦ CALLED PROGRAM MODULES
        REF PPATHA,PPUIHP
        REF PPATH1,PUART
♦ LINKED DATA MODULES
        REF IPDHTD,50001D,50002D,50003D,50003D,MONTDD
        REF WAHP,WADC,INTHA1,BUFFER,WALP,IPDHTW,MONTDW
        REF PPATHW,PPUIHW,IPPTOW,OPPTOW
        REF DF50,IDA,MONI,DIAG,DCPF,IOTF
        REF MONINT,DIINT,DCPINT,IOTINT,IPINT
        REF RAM,RAM2,RAMEND,SETONE,SETNEG,SETEND
        RORG
        PSEG

```

```

♦♦♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦
PPINI1 LWPI RAM
        LI R0,RAM2
CLEAR CLR *R0+ CLEAR FROM RAM TO RAMEND
        CI R0,RAMEND
        JNE CLEAR
        LI R0,SETONE
SET INC *R0+ INITIALIS FLAGS TO +1
        CI R0,SETNEG
        JNE SET
SET1 SETO *R0+ INITIALIS FLAGS TO -1
        CI R0,SETEND
        JNE SET1
        CLR *RAM
        LWPI WAHP
        LI R0,BUFFER
        LI R12,>100 9901 CRU BASE
        LI R15,>0018 ENABLE INT 3&4
        LDCR R15,0
        LI R12,>1100 CRU BASE
        LI R15,BUFFER
        AI R15,20 INITIALIS TO BUFFER +20
        LWPI WALP
        LI R0,BUFFER
        AI R0,22 INITIALIS TO BUFFER +22
        LWPI WADC
        LI R0,BUFFER INITIALIS TO BUFFER
        LI R12,>1100 ADC CRU BASE
        LWPI IPDHTW
        LI R12,>1100 CRU BASE ADC
        SBZ 3 ADC RESET
        SBO 3
        CLR R1 BUF COUNT
        LWPI MONTDW
        CLR R3
        LWPI PPATHW
        LI R12,>1100 ADC CRU BASE
        LWPI PPUIHW
        LI R12,>1A30 UART CRU BASE
        BL *PUART GO PROGRAM UART
        LWPI IPPTOW
        LI R12,>1A30 UART CRU BASE
        LWPI OPPTOW
        LI R12,>1A30 UART CRU BASE
        UP BLWP *PPATH1 INTERRUPT MASK
        JMP UP GO TO TASK HANDLER
        END

```

PATIENT PROCESSOR TASK HANDLER

1. DESCRIPTION

This program is an operating system program concerned with scheduling system tasks in order of priority. Before this program passes control to the highest active task, it determines whether the task is in the suspended state. If the task is found to be suspended, control is passed to it at the point it was interrupted, otherwise control is passed to it at its starting point.

As an aid for observing the operation of the system, various CRU lines are set when a particular task is active, and reset on completion of that task.

This operating system program runs under the privileged interrupt mask of level zero, so that it cannot be interrupted.

2. IDENTIFICATION

SUBROUTINE NAME	PPTHA
PROGRAM MODULE	PPTHAP
GENERAL DATA MODULE	G0016D
GENERAL DATA MODULE	G0017D

3. SIZE

PROGRAM MODULE	214	Bytes
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4. CALLS TO SUBROUTINE

BLWP	@PPTHA1
------	---------

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	IPDHTP
BLWP	@IPDHT1

PROGRAM MODULE	MONTOP
BLWP	@MONTD1
PROGRAM MODULE	DIAT1P
BLWP	@DIAT11
PROGRAM MODULE	IPPTOP
BLWP	@IPPT01
PROGRAM MODULE	OPPTOP
BLWP	@OPPTOP
PROGRAM MODULE	MCPTOP
BLWP	@MCPT01

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data to this program is the task active and interrupt flags listed below :-

IDH, MONI, DIAG, IPTASK, OPTASK, MCP,
MONINT, DIAINT, IPINT, OPINT, MCPINT.

7. EXTERNAL DATA TRANSFERS

PERIPHERAL	CRU INTERFACE (UNUSED BITS IN ADC INTERFACE)
------------	---

7.1. OUTPUT (TEST FACILITY)

CRU BASE	>1000	
CRU LINE	>B	MONITOR TASK ACTIVE BIT
CRU LINE	>C	DIAGNOSIS TASK ACTIVE BIT
CRU LINE	>D	INPUT TASK ACTIVE BIT
CRU LINE	>E	OUTPUT TASK ACTIVE BIT

8. TIMING

The maximum execution time of this program will not exceed 0.2 μ S

9. AUTHOR B.T.V. WARTON.


```

TITL 'PATIENT PROCESSOR TASK HANDLER'
♦ PROGRAMME MODULE IDENT (TASK)
  IDT 'PPTHAP'
♦ TRANSFER VECTORS OR ENTRIES
  DEF PPTHAP1
♦ CALLED PROGRAM MODULES
  REF IPDHTP,MONTDP,DIAT1P,DCOPTOP,OPPTOP
  REF IPDHT1,MONTD1,DIAT11,IPPT01,MCPT01,OPPT01
♦ LINKED DATA MODULES
  REF G0016D,G0017D
  REF PPTHAW, IDH, MONI, IPTASK, MCP, MCPINT, MCRTWP, OPINT
  REF DIAG, MONINT, MRTWP, DIAINT, DRTWP, OPRTWP, OPTF
  REF IPINT, IPRTWP, OPTASK
  RORG
  PSEG

```

```

♦♦♦♦♦♦♦♦♦♦ PROGRAMME ♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦
PPTHAP1 DATA PPTHAW, STARTS
STARTS LIM1 2 PRIVILEGE INT LEVEL
      LWPI PPTHAW
      MOV %IDH,R0 TEST IDH FLAG
      JNE BIDH JUMP IF ACTIVE
      MOV %MONI,R0 TEST MONI FLAG
      JNE BMONI JUMP IF ACTIVE
      MOV %BDIAS,R0
      JNE %BBDIAS
      MOV %IPTASK,R0 TEST I/O FLAG
      JNE BIPT JUMP IF ACTIVE
      MOV %OPTASK,R0 TEST OCP FLAG
      JNE BOPT JUMP IF ACTIVE
      MOV %MCP,R0
      JNE BMCP
      CLR R5 CLEAR TASK ACTIVE FLAG
      LIM1 7 UNMASK ALL INTS
TOIDLE IDLE
      JMP TOIDLE
BIDH EQU $
      LI R5,1 SET TASK ACTIVE TO 1
      BLWP %IPDHT1 GO TO IDH TASK
      JMP STARTS
BMONI EQU $
      LI R5,2 SET TO TASK 2
      ABS %MONINT WAS MONI TASK SUSPENDED
      JGT BM
      LWPI MRTWP GET MONI TASK WP FOR RET
      RTWP
BM LIM1 7 UNMASK ALL INTS
      SBO >B SET BIT TO INDICATE TASK ACTIVE
      BLWP %MONTD1 GO TO MONITOR TASK
      SBZ >B RESET MONI TASK ACTIVE BIT
      JMP STARTS
BDIAS EQU $
      LI R5,3 SET TO TASK 3
      ABS %DIAINT WAS DIAG TASK SUSPENDED
      JGT BD
      LWPI DRTWP GET DIAG TASK WP FOR RET
      RTWP
BD LIM1 7 UNMASK ALL INTS
      SBO >C SET DIAG TASK ACTIVE INDICATOR BIT
      BLWP %DIAT11 GO TO DIAGNOSIS TASK
      SBZ >C RESET DIAG ACTIVE BIT

```

SCR2.TASK.S.PPTHAP 14:22:27 TUESDAY, OCT 17, 1978.

```

      JMP  STARTS
BIPT  EQU  $
      LI   R5,4           SET TO TASK 4
      ABS  @IPINT        WAS I/P TASK SUSPENDED
      JGT  B0
      LWPI IPRTWP        GET I/P TASK WP FOR RET
      RTWP
B0    LIM1 7             UNMASK ALL INTS
      SBO  >D            SET I/P TASK ACTIVE BIT
      BLWP @IPPT01       GO TO I/P TASK
      SBZ  >D            RESET I/P TASK ACTIVE BIT
      JMP  STARTS
BOPT  EQU  $
      LI   R5,5           SET TO TASK 5
      ABS  @OPINT        WAS O/P TASK SUSPENDED
      JGT  B1
      LWPI OPRTWP        GET O/P TASK WP FOR RET
      RTWP
B1    LIM1 7             UNMASK ALL INTS
      SBO  >E            SET O/P TASK ACTIVE BIT
      BLWP @OPPT01       GO TO O/P TASK
      SBZ  >E            RESET O/P TASK ACTIVE BIT
      JMP  STARTS
BMCP  EQU  $
      LI   R5,6           SET TO TASK 6
      ABS  @MCPINT       WAS MCP TASK SUSPENDED
      JGT  BMCP1
      LWPI MCRTPW        GET MCP TASK WP FOR RET
      RTWP
BMCP1 LIM1 7             UNMASK ALL INTS
      BLWP @MCPPT01      GO TO MCP TASK
      JMP  STARTS
      END
```

PATIENT PROCESSOR ADC INTERRUPT HANDLER

1. DESCRIPTION

This program is an operating system program concerned with servicing the ADC interrupt. When the interrupt occurs this program determines which task, if any, was interrupted and will save the returns to that task and set it suspended. The signal conditioning task (IPDHTP) is then set active before this program branches to the task handling program (PPTHAP). Also incorporated in this program is a section of code concerned with calculating the time since system start up, in hours, minutes and seconds, from the 4mS interval ADC interrupt.

2. IDENTIFICATION

SUBROUTINE NAME	PPCIH
PROGRAM MODULE	PPCIHP
GENERAL DATA MODULES	G0016D
GENERAL DATA MODULES	G0017D
PERMANENT DATA MODULES	P0009D

3. SIZE

PROGRAM MODULE	186 Bytes
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4. CALLS TO SUBROUTINE

INTERRUPT LEVEL	3	@PPCIH1
BL		@PPCIH2

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	PPTHAP
BLWP	@PPTHAP

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data to this program is the 3 return vectors

in registers R13, R14 and R15, of the workspace area used to service the interrupt (PPTHAW), and also the word containing the current task active number (ACTNO).

6.2. OUTPUT DATA

As a result of the execution of this program the word ACTNO is reset to zero and one of the group of 3 words

MWPRET	DWPRET	IWPRET	OWPRET	CWPRET
MPCRET	DPCRET	IPCRET	OPCRET	CPCRET
MSTRET	DSTRET	ISTRET	OSTRET	CSTRET

are loaded with the 3 returns in R13, R14 and R15, that are required when reactivating the currently interrupted task. To indicate that the task which has just been interrupted, is in the suspended state, its interrupt flag word is set to -1. The interrupt flags for the various tasks are :-

MONINT	DIAINT	IPINT	OPINT	MCPINT
--------	--------	-------	-------	--------

Also during the execution of this program, the words MSEC, SEC, MINUTE , HOURS will be changed to indicate the time since the system was started.

7. AUTHOR

B.T.V. WARTON.

```

TITL 'PATIENT PROCESSOR ADC INT HANDLER'
♦ PROGRAMME MODULE IDENT (TASK)
  IDT 'PPCIHP'
♦ TRANSFER VECTORS OR ENTRIES
  DEF PPCIH1,PPCIH2
♦ CALLED PROGRAM MODULES
  REF PPTHAP
  REF PPTHAI
♦ LINKED DATA MODULES
  REF G0016D,G0017D,P0009D
  REF MWPRET,MPCRET,MSTRET,DWPRET,DPCRET,DSTRET
  REF OWPRET,OPCRET,OSTRET,IWPRET,IPCRET,ISTRET
  REF MONINT,DIINT,IPINT,OPINT,MCPINT
  REF RWPRET,RPCRET,RSTRET,OWPRET,OPCRET,CSTRET
  REF MSEC,SR250,SIXTY,SEC,MINUTE,HOURS,ACTNO
  REF IDH
  RORG
  PSEG

```

```

*****
PPCIH1 EQU $          P R O G R A M M E          *****
*****
                        T I M E                      *****
INC 0MSEC              INC 4MS INTERVAL COUNTER
C 0SR250,0MSEC        IS MSEC=250=1 SEC
JNE OUTIME
CLR 0MSEC              RESET MSEC
INC 0SEC               INC SECONDS COUNTER
C 0SIXTY,0SEC         IS SEC=60=1 MINUTE
JNE OUTIME
CLR 0SEC               RESET SECONDS COUNTER
INC 0MINUTE           INC MINUTES COUNTER
C 0SIXTY,0MINUTE     IS MINUTE=60=1 HOUR
JNE OUTIME
CLR 0MINUTE           RESET MINUTE
INC 0HOURS            INC HOURS COUNT
OUTIME EQU $
BL 0PPCIH2            GO SAVE RET OF INTERRUPTED TASK
SETD 0IDH              SET IDH TASK ACTIVE
BLWP 0PPTHAI          GO TO TASK HANDLER
PPCIH2 EQU $
MOV 0ACTNO,R5         GET ACTIVE TASK NUMBER
JEQ EXIT              IF=0 EXIT
DECT R5               IF MONI TASK GOTO MSAVE
JEQ MSAVE
DEC R5                IF DIAG TASK GOTO DSAVE
JEQ DSAVE
DEC R5                IF I/P TASK GOTO ISAVE
JEQ ISAVE
DEC R5                IF O/P TASK GOTO OSAVE
JEQ OSAVE
DEC R5                IF MCP TASK GOTO MCSAVE
JEQ MCSAVE
EXIT CLR 0ACTNO       RESET TASK ACTIVE NUMBER
RT
MSAVE MOV R13,0MWPRET  SAVE MONITOR WP RET
      MOV R14,0MPCRET  SAVE MONITOR PC RET
      MOV R15,0MSTRET  SAVE MONITOR ST RET
      SETD 0MONINT     SET MONI INT FLAG
      JMP EXIT
DSAVE MOV R13,0DWPRET  SAVE DIAGNOSIS WP RET
      MOV R14,0DPCRET  SAVE DIAGNOSIS PC RET

```

SCR2.TASK.S.PPCIHP 15:08:06 TUESDAY, OCT 17, 1978.

```
      MOV R15, @DSTRET      SAVE DIAGNOSIS ST RET
      SETD @DIAINT          SET DIAG INT FLAG
      JMP EXIT
ISAVE MOV R13, @IWPRET      SAVE I/P TASK WP RET
      MOV R14, @IPCRET      SAVE I/P TASK PC RET
      MOV R15, @ISTRET      SAVE I/P TASK ST RET
      SETD @IPINT           SET IP INT FLAG
      JMP EXIT
OSAVE MOV R13, @OWPRET      SAVE O/P TASK WP RET
      MOV R14, @OPCRET      SAVE O/P TASK PC RET
      MOV R15, @OSTRET      SAVE O/P TASK ST RET
      SETD @OPINT           SET O/P TASK INT FLAG
      JMP EXIT
MCSAVE MOV R13, @MCPRET     SAVE MCP TASK WP RET
      MOV R14, @MPCRET      SAVE MCP TASK PC RET
      MOV R15, @MSTRET      SAVE MCP TASK ST RET
      SETD @MCPINT          SET MCP TASK INT FLAG
      JMP EXIT
      END
```

PATIENT PROCESSOR UART INTERRUPT HANDLER

1. DESCRIPTION

This program is an operating system program and is concerned with the interrupt generated by the UART (Universal Asynchronous Receiver Transmitter) which is the means by which the patient dedicated processor communicates to the operator dedicated processor.

The functions performed by this program are :-

- (1) The testing of the UART interrupt to determine if it is due to a character being received, or the interval timer.
- (2) The transmission or reception of the Start of Heading (SOH) character "Acknowledge" (ACK) or "Negative Acknowledge" (NAK) characters for the correct start up of communication between processors.
- (3) The activation of either the Input Task or Output Task as required.
- (4) The de-activation of successful or unsuccessful communication by the Input or Output tasks.
- (5) The de-activation of either the Input or the Output task if the UART interval timer interrupt should occur, and the indication of the error to the operator if necessary.
- (6) The programming of the UART for its correct operation at the required bit rate and transmission/reception format.

This operating system program is allowed the privilege of

running under an interrupt mask of level 2.

2. IDENTIFICATION

SUBROUTINE	NAME	PPUIH
PROGRAM	MODULE	PPUIHP
GENERAL DATA	MODULE	G0016D

3. SIZE

PROGRAM MODULE	332	BYTES
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4. CALLS TO SUBROUTINE

INTERRUPT LEVEL	4	@PPUIH1
	B	@PPUIH2
	B	@PPUIH3
	B	@PPUIH4
	B	@PPUIH5
	BL	@PUART

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	PPTHAP
BLWP	@PPTHAI
PROGRAM MODULE	PPCIHP
BL	@PPCIH2

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The three return vectors stored in R13, R14 and R15 of PPUIHW workspace area are saved by a BL @PPCIH2.

6.2. OUTPUT DATA

During the operation of this program, the software flags for activating or suspending the Input or Output task may be set or reset according to the communication situation at the time.

7. EXTERNAL DATA TRANSFER

PERIPHERAL TMS 9902 UART

7.1. INPUT

INTERRUPT LEVEL 4
CRU BASE >1A80
CRU BIT FUNCTIONS AS SPECIFIED
IN THE TMS 9902 DATA SHEETS.

7.2. OUTPUT

CRU BASE >1A80
CRU BIT FUNCTIONS AS SPECIFIED
IN THE TMS 9902 DATA SHEETS.

8. TIMING

Execution time for this program is of the order of 0.2ms in normal communication situations.

9. NOTES

The PPUIH1 entry point to this program is due to the UART interrupt which can be generated either by a character being received, or the UART interval timer elapsing.

The PPUIH2 entry point to the program is due to the Microprocessor Communication Package Task (MCP) requesting that a message be transmitted from the patient processor.

The PPUIH3 entry point to the program is due to the completion of the Input task, which allows the program to reset the UART software flags etc., and to test if output communication has been requested.

The PPUIH4 entry point to this program is due to the successful completion of the Output Task, and allows this program to reset UART software flags.

The PPUIH5 entry point to this program is due to the unsuccessful attempt by the Output task to communicate with the Operator dedicated processor. This section of program re-starts the inter-processor communication protocol by transmitting the "Start of Heading" (SOH) character.

10. AUTHOR

B.T.V. WARTON.


```

        BL   @SETIME          GO SET TIME
        SBZ  18              INHIBIT INT
BOUT    BLWP @PPTHA1        GO TO TASK HANDLER
♦
♦ OUTPUT NAK SECTION
OPNAK  CI   R4,>1500        WAS IT NAK
        JEQ  NAKER
        BL   @PUART          GO PROGRAM UART
        LI   R4,>1500        NAK
        CLR  R2              RESET I/P FLAG
        BL   @OP             O/P NAK
NAKER   BL   @ERROR        GO TO ERROR SECTION
        JMP  BOUT
♦
♦ ERROR SECTION
ERROR  INC  R10             INC ERROR COUNTER
        CI   R10,100        IS THERE 100 ERRORS
        JLT  RTOUT
♦ INDICATE ERROR
        LI   R12,>1BE0      SET ERROR CRU BASE
        SBO  0              SET ERROR INDICATOR BIT
        LI   R12,>1A80      RET TO UART CRU BASE
RTOUT  RT
♦
♦ SET UART TIMER SECTION
SETIME SBO  13             LDIR
        LI   R5,>FA00        16 MS
        LDCR R5,8           LOAD TIMER
        SBO  20             ENABLE INTERVAL INT
        RT
♦
♦ TIMER INTERRUPT HANDLER SECTION
TIMELP CLR  @IPTASK        DEACTIVATE IPTASK
        CLR  @OPTASK        DEACTIVATE OPTASK
        ABS  @IPINT         RESET I/P INT FLAG
        ABS  @OPINT         RESET O/P INT FLAG
        CLR  R0             RESET RESP EXP FLAG
        CLR  R1             RESET SOH FLAG
        CLR  R2             RESET I/P FLAG
        BL   @ERROR        GO TO EROR SECTION
        MOV  @OPAC,@OPAC    TEST O/P ACTIVE FLAG
        JNE  OPSOH
        BL   @PUART          GO PROGRAM UART
        JMP  BOUT
♦ INDICATE ERROR
OPSOH  LI   R4,>0100        SOH
        BL   @OP            O/P SOH
        SETD R0             O/P RES EXPECTED
        BL   @SETIME        GO SET TIME
        BLWP @PPTHA1        GO TO TASK HANDLER
♦
♦ O/P REQUEST ENTRY FROM MCP
PPUIH2 LIM1 2             LOAD PRIVILEGE MASK
        SETD @OPAC          SET O/P REQUEST ACTIVE
        LWPI PPUIHW
        CLR  R1
        MOV  R2,R2
        JEQ  OPSOH
        BLWP @PPTHA1
        GO TO TASK HANDLER
♦

```

SCR2.PROG.S.PPUIHP 16:23:41 WEDNESDAY, OCT 18, 1978.

◆ ENTRY FROM IPPTOP

PPUIH3	LIMI 2	LOAD PRIVILEGE MASK
	CLR @IPTASK	DEACTIVATE IPTASK
	LWPI PPUIHW	
	CLR R2	RESET I/P FLAG
	MOV @OPAC,@OPAC	IS OP ACTIVE
	JNE OPSOH	SEND SOH
	SBO 18	REC INT ON
	BLWP @PPTHAI	GO TO TASK HANDLER

◆ ENTRY FROM SUCCESSFUL OPPTOP

PPUIH4	LIMI 2	LOAD PRIVILEGE MASK
	CLR @OPTASK	DEACTIVATE OPTASK
	LWPI PPUIHW	
	CLR R0	RESET RESP FLAG
	CLR R1	RESET SOH FLAG
	CLR @OPAC	RESET O/P ACTIVE TASK
	SBO 18	ENABLE INT
	BLWP @PPTHAI	GO TO TASK HANDLER

◆ ENTRY FROM UNSUCCESSFUL OPPTOP

PPUIH5	LIMI 2	LOAD PRIVILEGE MASK
	CLR @OPTASK	DEACTIVATE OPTASK
	JMP OPSOH	GO TO O/P SOH

◆ PROGRAMME UART SECTION

PUART	SBO 31	RESET
	LI R7,>6300	8BITS EVEN PARIT 2STOP
	LDCR R7,8	LOAD UART
	SBZ 13	TIMER NOT PROG
	LI R7,>0010	LOAD UART
	LDCR R7,12	LOAD UART
	SBO 18	ENABLE INT
	RT	
	END	

INPUT DATA HANDLER TASK

1. DESCRIPTION

This program is the highest priority task in the patient dedicated processor system, and performs the required signal conditioning on the sampled E C G. signal. It contains the three digital filters and noise detecting software as described in Chapter 5.

This program runs under the interrupt mask of level 2, and thus cannot be interrupted by the UART interrupt at level 4.

2. IDENTIFICATION

SUBROUTINE NAME	IPDHT
PROGRAM MODULE	IPDHTP
SPECIFIC DATA MODULE	IPDHTD
GENERAL DATA MODULE	G0002D
GENERAL DATA MODULE	G0003D
PERMANENT DATA MODULE	P0001D

3. SIZE

PROGRAM MODULE	438	BYTES
----------------	-----	-------

4. CALLS TO SUBROUTINE

BLWP	@IPDHT1
------	---------

5. INTERNAL DATA TRANSFER

5.1. INPUT DATA

The DFG0 software flag is tested but not changed by this program, to determine if it must activate the Monitoring Task.

5.2. OUTPUT DATA

The input samples obtained by this program from the AtoD Converter are conditioned by the digital filters, and the output data from this program is placed in the IBP1 Buffer.

5.3. ADDITIONAL DATA CHANGES

Software flags that may be changed by the program are :-

ARTIF which equals -1 if artefact is present in the input signal.

MONI which is set to -1 if Monitoring Task is activated, and

IDH which is set to 0 to de-activate this program.

6. EXTERNAL DATA TRANSFERS

6.1. INPUT

CRU BASE		> 1100
CRU BITS	0 TO 7	ADC INPUT

6.2. OUTPUTS

CRU BASE		> 1100
CRU BITS	0 TO 7	DAC OUTPUT
CRU BIT	8	INTERRUPT MASK OR RESET
CRU BIT	9	DAC OUTPUT HOLD

7. TIMING

Execution time 1 mS

8. NOTE

The digital filters implemented in this task are designed for a sample rate of 4mS (i.e. 250 sps).

9. AUTHOR

B.T.V. WARTON.

```

TITL <INPUT DATA HANDLER TASK (WITH DIGITAL FILTERS)>
* PROGRAMME MODULE IDENT (PROG)
  IDT <IPDHTP>
* TRANSFER VECTORS OR ENTRIES
  DEF IPDHT1
* LINKED DATA MODULES
  REF IPDHTD,G0002D,G0003D,P0001D
  REF BUFFER,BUFEND,WAHP,WALP,WADC,HPOP
  REF LPOP,LEVEL,KHP,A1,A2,K1LP
  REF K2LP,KDC,A1DC,A2DC,C
  REF IPDHTW,IBUF,IBP1,BUFLEN
  REF DFGD,MONTDW,MSTIMC,MONI,IDH,VALUE
  REF ARTIF
RDRG
PSEG

```

***** P R O G R A M M E *****

```

IPDHT1 DATA IPDHTW,STARTI
STARTI STCR R0,8          GET INPUT IN MSB
      MOVB R0,@IBUF(R1)   SAVE UNFILTERED DATA
*
* D C FILTER (WADC) *****
STARTF LWPI WADC          GET DC WA
      MOV @IPDHTW,R1      GET I/P
      SRA R1,8            I/P<1>-1
      MOV R1,R5           I/P TO ACC1
      S R4,R5             ACC1-Z3
D11    MOV R5,R9          GET ACC1
      MOV @KDC,R10        GET CONSTANT
      BL @MULT12          12 BIT MULT
      MOV R9,*R0+         PUT IN BUFFER
      CI R0,BUFEND        IS R0>BUFFER END
      JLE D12
D12    LI R0,BUFFER        RESET R0 TO BUFFER START
      MOV R9,R6           D/P TO ACC2
      A R2,R6             ACC2+Z1
D2     MOV R6,R9          GET ACC2
      MOV @A1DC,R10       GET A1
      BL @MULT12          GO MULTIPLY
      MOV R9,R7           ANS TO ACC3
      MOV R9,R8           ANS TO ACC4
      A R3,R7             ACC3+Z2
D3     MOV R7,R9          GET ACC3
      MOV @A2DC,R10       GET A2
      BL @MULT12          GO MULTIPLY
      A R9,R8             ADD TO ACC4
D4     MOV R8,R4          ACC4 TO Z3
      MOV R7,R3          ACC3 TO Z2
      MOV R6,R2          ACC2 TO Z1
*
* LOW PASS (2ND ORDER) FILTER
D1     LWPI WALP          GET LOW PASS FILTER WA
      MOV *R0+,R4         GET VALUE FROM BUFFER
      CI R0,BUFEND        IS R0>BUFFER END
      JLE D5
D5     LI R0,BUFFER        RESET TO START OF BUFFER
      MOV R2,R9           GET Z1
      MOV @K1LP,R7        GET LP FILT K1 CONSTANT
      BL @MULT8           8 BIT MULT
      A R9,R4             ADD TO ACC1
      MOV R3,R9           GET Z2

```


MOV	0K2LP,R7	GET LP FILTER K2 CONSTANT
BL	0MULT8	GO MULTIPLY
A	R9,R4	ADD TO ACC1
MOV	R4,R5	ACC1 TO ACC2
MOV	R2,R6	GET Z1
SLA	R6,1	X 2
A	R6,R5	ADD TO ACC2
A	R3,R5	ADD Z2 TO ACC2
MOV	R5,R9	
MOV	0C,R7	GET LP FILTER C CONSTANT
BL	0MULT8	O/P IN R9
MOV	R2,R3	SAVE NEW Z2
MOV	R4,R2	SAVE NEW Z1
MOV	R9,0LPOP	SAVE O/P

◆ HIGH PASS (ARTIFACT DETECTION) FILTER

	LWPI	0AHP	
	MOV	0R0+,R1	GET VALUE FROM BUFFER
	CI	R0,0UFEND	IS R0> BUFFER END
	JLE	D6	
D6	LI	R0,0BUFFER	RESET TO START OF BUFFER
	MOV	R1,R5	I/P TO ACC1
	S	R4,R5	ACC1-Z3
	MOV	R5,R9	GET ACC1
	MOV	0KHP,R10	GET CONSTANT
	BL	0MULT12	12 BIT MULT
	MOV	R9,0HPOP	SAVE HP O/P
	MOV	R9,R6	O/P TO ACC2
	A	R2,R6	ACC2+Z1
	MOV	R6,R9	GET ACC2
	MOV	0A1,R10	GET A1
	BL	0MULT12	GO MULTIPLY
	MOV	R9,R7	ANS TO ACC3
	MOV	R9,R8	ANS TO ACC4
	A	R3,R7	ACC3+Z2
	MOV	R7,R9	GET ACC3
	MOV	0A2,R10	GET A2
	BL	0MULT12	GO MULTIPLY
	A	R9,R8	ADD TO ACC4
	MOV	R8,R4	ACC4 TO Z3
	MOV	R7,R3	ACC3 TO Z2
	MOV	R6,R2	ACC2 TO Z1

◆ LEVEL DETECTION SECTION

	MOV	0HPOP,R9	GET HP O/P
	ABS	R9	MAKE VALUE +VE
	SRA	R13,1	Z/2
	A	R13,R9	R9+Z/2
	SRA	R13,1	R13/2
	A	R13,R9	R9+Z/4
	MOV	R9,R13	REPLACE Z
	MOV	0R15+,R10	GET UNFILTERED O/P
	CI	R15,0UFEND	IS R15>BUFFER END
	JLE	D7	
D7	LI	R15,0BUFFER	RESET R15 TO START OF BUFFER
	C	R9,0LEVEL	TEST LEVEL OF SIGNAL
	JLT	0NART	
	LI	R14,250	1 SEC DELAY
	SET0	0ARTIF	SET ARTEFACT FLAG
	SBO	>A	SET ARTIFACT CRU BIT

```

U2      DEC   R14                1 SEC DELAY COUNT
        JEQ   OVER
        MOV   @LPOP,R9           GET LP FILT O/P
        MOV   R9,R10            SAVE R9 IN R10
U1      SLA   R9,8               IS VALUE > 8 BITS ACCURACE
        JND   DOK
        MOV   R10,R10           IS VALUE +VE
        JGT   P
        LI    R9,>8000           SET TO MIN 8 BIT -VE VALUE
        JMP   DOK
P       LI    R9,>7F00           SET TO MAX 8 BIT +VE VALUE
DOK     MOVB  R9,@VALUE         SAVE R9 AT VALUE
        SBO   9                 DAC HOLD
        LDCR R9,8               O/P
        SBZ   9                 DAC SAMPLE
        SBZ   8                 RESET
        SBO   8                 RESET
        LWPI IPDHTW            RETURN TO IPDHTW
        MOVB  @VALUE,@IBP1(R1) SAVE VALUE IN BUF
        MOV   @DFGO,R2         TEST DFGO
        JGT   GO
        CLR   R1                BUF COUNT
        LWPI MONTDW            GET MONITOR WA
        CLR   R3                RESET. COUNT
        LWPI IPDHTW
        JMP   RETNS            RET NO STIM.
GO      INC   R1                INC BUF COUNT
        C     R1,@BUFLN        IS R1>BUFFER LENGTH
        JLE  STIM
        CLR   R1                RESET COUNT
♦
♦ ACTIVATION OF MONITOR TASK SECTION
STIM    INC   @MSTIM           INC MONI STIM COUNT
        SETO @MONI            SET MONITOR TASK ACTIVE
♦
♦ DEACTIVATION OF IPDHTP
RETNS   CLR   @IDH            RESET IPDHTP TASK ACTIVE FLAG
        RTWP                  RETURN TO TASK HANDLER
♦
♦ DELAYED HOLD TIME OVER SECTION
OVER    MOV   R10,R9           GET UNFILTERED O/P IN R9
        ABS   @ARTIF           RESET ARTEFACT FLAG
        SBZ   >A              RESET ARTEFACT CRU BIT
        JMP   U1
♦
♦ NO ARTIFACT DURING DELAY TEST SECTION
NOART   MOV   R14,R14         TEST 1 SEC DELAY
        JEQ   OVER
        JMP   U2
♦
♦ 12 BIT MULT *****
MULT12  ABS   R9                MAKE R9 +VE
        JGT   R9P              JUMP IF R9 +VE
        MPY  R10,R9            R10 X R9 ANSWER IN R9&R10
        SLA  R9,4              GET CORRECT BINARY POINT POSITION
        SRL  R10,12            GET CORRECT BINARY POINT POSITION
        A    R10,R9            MAKE ANSWER INTO SINGLE 16 BIT NUMBER
        NEG  R9                MAKE ANSWER -VE
        RT
R9P     MPY  R10,R9            R10 X R9 ANSWER IN R9&R10

```


MONITOR PROGRAM

1. DESCRIPTION

This first module of the monitoring task is concerned with the monitoring start up procedure and the subsequent detection of QRS Complexes. This module also has the exit section from the monitoring program.

2. IDENTIFICATION

SUBROUTINE NAME	MONTD
PROGRAM MODULE	MONTD1
SPECIFIC DATA MODULE	MONTD0
GENERAL DATA MODULE	G0002D
GENERAL DATA MODULE	G0003D
GENERAL DATA MODULE	G0004D
PERMANENT DATA MODULE	P0002D

3. SIZE

PROGRAM MODULE	394	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

BLWP	@MONTD1
B	@FINISH

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	MONS1P
B	@MONS11
PROGRAM MODULE	MONS2P
B	@NOQRS

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data for this program is found in IBP1 Buffer as supplied by the Signal Conditioning task (IPDHTP).

6.2. OUTPUT DATA

The output data from this program, which consists of the delayed difference signal, is placed in the buffer DBP1. Also supplied is a word labeled POINT which indicates the position of the QRS complex in the IBP1 buffer, and a word labeled RRC which is the estimate of the current R-R interval.

6.3. ADDITIONAL DATA CHANGES

Software flags which may change during the program operation are the start up flags SU, SU2 and SU3, and also the monitor MCP request flag. Also an address is placed in MOTEXT and the MCP task flags set when the Monitoring function wishes information to be transmitted to the operator dedicated processor.

7. TIMING

The normal execution time for this program is 0.21mS and occurs while a QRS complex has not been detected.

When a QRS complex is detected the maximum execution time of this program module combined with the other two (MONS1P and MONS2P) which make up the complete monitoring software package is 3.2mS.

For more information on software timing see Chapters 5 and 7.

8. AUTHOR

B.T.V. WARTON.

```

TITL 'MONITOR PROGRAM'
♦ PROGRAMME MODULE IDENT (PROG)
  IDT 'MONTDP'
♦ TRANSFER VECTORS OR ENTRIES
  DEF MONTD1,FINISH
♦ CALLED PROGRAM MODULES
  REF MONS1P,MONS2P
  REF MONS11,NOORS
♦ LINKED DATA MODULES
  REF MONTD0,60002D,60003D,60004D,P0002D
  REF MONTDW,SDELAY,SFP1,SU,DBP1
  REF TDP1,BUFLEN,DMINC
  REF MINL,IBP1,SU2,RR0,RR032,RRMAXT
  REF TEN,SIX,MSTIMC,MONI,DBUFL,SU3,POINT
  REF MSUDVE,MFAIL,MONSF,MOTEXT,CSTIMC,MCP
  REF WAHP,MCP
  REF DFG0,AVRR,CMS,MONS1W,NP,P2POS,QRSWID
  RORG
  PSEG

```

```

♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦
MONTD1 DATA MONTDW,SMONIT      BLWP VECTORS
SMONIT MOV  @SU,R0              IS START UP ACTIVE
      JGT  MON                  JUMP & CONTINUE MONITORING
♦

```

```

♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦ START UP SECTION ♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦
      MOV  @SDELAY,R0           IS START UP DELAY REQUIRED
      JGT  D1                   JUMP IF DELAY NOT REQUIRED
      INC  R3                   INC P2
      CI   R3,6                 IS P2=6 I/P DELAYS
      JLT  RET1                 JUMP<6
      ABS  @SDELAY              SET DELAY TO NOT REQUIRED
      CLR  R2                   CLR POSITION POINTER P1
      CLR  R4                   DIFF REG
      CLR  R5                   COUNTER 2
      CLR  R12                  RESET DBP1 COUNTER
RET1   B    @EXIT              THIS RET DOES NOT INC P1&P2
D1     MOVB @IBP1(R3),R4       GET VALUE AT P2
      SRA  R4,8                 MSB TO LSB
      MOVB @IBP1(R2),R7       GET P1
      SRA  R7,8                 MSB TO LSB
      S    R7,R4               P2-P1=R4
      MOV  R4,@DBP1(R12)      SAVE D IN DBP1
      MOV  R2,R2              TEST R2 (P1)
      JNE  D2                 JUMP IF R2NOT=0 (P1)
      MOV  @DBP1,R5          PLACE INMIN REG 5
      CLR  R6                 MIN POSITION
      B    @FINISH           GO TO FINISH SECTION
D2     C    R5,@DBP1(R12)     IS NEW DIFF<MIN(R5)
      JLT  D3                 JUMP IF NO
      MOV  @DBP1(R12),R5     SAVE NEW MIN
      MOV  R12,R6            SAVE POS OF NEW MIN
D3     CI   R2,500           HAVE 500 DIFF VALUES BEEN FOUND
      JGT  D4                 JUMP IF YES
      B    @FINISH           GO TO FINISH SECTION
D4     CI   R6,450           IS POS OF MIN>450
      JLT  D5                 JUMP IF NO
      CI   R2,550           HAVE 550 DIFFS BEEN FOUND
      JGT  D5                 JUMP IF YES
      B    @FINISH           GO TO FINISH SECTION
D5     C    @MINL,R5         IS MIN LIMIT <MIN

```

```

        JLT  BFAIL          MIN>MINL  SU FAIL #####
♦
♦♦♦♦♦♦♦♦♦♦ THE NEXT SECTION FINDS TD FOR PAT 1
MOV  R5,R9          GET MIN VALUE
ABS  R9             MAKE +VE
MPY  @SIX,R9        MIN X 6 ANS IN R10
DIV  @TEN,R9        R9=ANS IE MIN X PARATD
NEG  R9             MAKE R9 -VE
MOV  R9,@TDP1      SAVE TDP1
ABS  @SU           START UP OVER
SETD @SU2          SET START UP 2 FLAG YES
SETD @SU3          SET START UP 3  "  "
SETD @MONSF        SET MON DCP FLAG
LI   R0,MSUDVE     GET D/P ADDRESS
MOV  R0,@MOTEXT    LOAD MOTEXT WITH D/P TEXT ADDRESS
INC  @CSTIMC       SU D/P TEXT STIM
SETD @MCP          ACTIVATE MCP TAK
B    @FINISH       GO TO FINISH SECTION
BFAIL B  @FAIL     GO TO START UP FAIL SECTION
♦♦♦♦♦♦♦
♦
♦♦♦♦♦♦♦ CONTINUOUS MONITORING SECTION ♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦
MON  MOVVB @IBP1(R3),R4  GET VALUE AT P2
SRA  R4,8           MSB TO LSB
MOVVB @IBP1(R2),R7     GET P1
SRA  R7,8           MSB TO LSB
S    R7,R4          P2-P1=R4
MOV  R4,@DBP1(R12)   SAVE DIFF VALUE IN DBP1
MOV  @CMS,R0        IS CONTINUE MON FLAG SET -VE
JLT  TESTTD        INC RR INTERVAL COUNT
INC  @RRC           IS RR INTERVAL>=6 SECONDS
C    @RRC,@RRMAXT   JUMP IF YES
JGT  BNDQRS        IS RR INT =>32SAMPLES
C    @RRC,@RRC32    JUMP IF YES
JGT  TESTTD        GO TO FINISH SECTION
B    @FINISH       GO TO NO QRS SECTION
BNDQRS B  @NDQRS    IS DIFF>TD
TESTTD C  R4,@TDP1  JUMP IF >LIMIT
JGT  D10           SEARCH FLAG PAT 1
ABS  @SFP1         NP+1
INC  R1            IS NP=1
CI   R1,1          JUMP IF NO
JNE  D11           SAVE MIN VAL
MOV  R4,R5         SAVE POS OF MIN
MOV  R3,R6         GO TO FINISH SECTION
B    @FINISH       IS THIS MIN<MIN SO FAR
D11  C  R5,R4      SAVE NEW MIN
JLT  BFIN         SAVE POSITION OF NEW MIN
MOV  R4,R5         GO TO FINISH SECTION
MOV  R3,R6         TEST SEARCH FLAG
D10  B    @FINISH  CLR NP COUNTER
JGT  BSEARC       CLR SIGN CHANGE COUNT
CLR  R1           GO TO FINISH SECTION
CLR  R10          SAVE DMIN CURRENT
BFIN B  @FINISH   TEST & RESET CONTINUE MON FLAG
BSEARC MOV  R5,@DMINC
ABS  @CMS         MOVE AVERAGE RR INTO RR CURRENT
JST  CMOK
MOV  @AVRR,@RRC

```

SCR2.PROG.S.MONTDP 16:56:30 WEDNESDAY, OCT 18, 1978.

CMOK	MOV	R6,@PDINT	SAVE POS OF MIN
	MOV	R1,@NP	SAVE NP
	INC	R10	SHORT TERM QRS WIDTH COUNTER
	C	R10,@QRSWID	IS COUNT=QRSWID
	JEQ	MONSGO	GO MONI SEARCH IF QRS FOUND WIDE
	MOV	B,@IBP1(R3),R0	TEST FOR SIGN CHANGE
	JLT	FINISH	
MONSGO	MOV	R3,@P2POS	SAVE P2 POSITION
	B	@MONS11	
FAIL	SETD	@MONSF	SET MONI MCP FLAG
	LI	R0,MFAIL	GET D/P ADDRESS
	MOV	R0,@MOTEXT	LOAD MOTEXT WITH ADDRESS OF D/P
	INC	@CSTIMC	STIM MCP
	SETD	@DF60	SET DF60 SO IPDHTP NOT STIM MONTDP
	SETD	@MCP	ACTIVATE MCP

♦
♦♦♦♦♦♦♦ THE NEXT SECTION IS THE EXIT FROM MONITOR

FINISH	LWPI	MONTDW	
	INC	R2	P1+1
	C	R2,@BUFLEN	IS P1>BUFFER LENGTH
	JLE	D8	
	CLR	R2	RESET P1
D8	INC	R3	P2+1
	C	R3,@BUFLEN	ISP2>BUFFER LENGTH
	JLE	DE	
	CLR	R3	RESET P2
DE	INCT	R12	DBP1 COUNT
	C	R12,@DBUFL	IS DBP1>BUFFER LENGTH
	JLE	EXIT	
	CLR	R12	RESET R12
♦	THE NEXT LINES CONTROL	MONI STIM COUNTER	
EXIT	DEC	@MSTIMC	DEC MONI STIM COUNT
	JNE	EXIT1	
	CLR	@MONI	DEACTIVATE MONI TASK
EXIT1	RTWP		
	END		

MONITOR SEARCH SECTION

1. DESCRIPTION

This program is the second module in the monitoring program, and is concerned with the monitoring start-up procedure for setting the initial value of the average R-R interval (AVRR). From then on this program is concerned with setting the test bits in the monitoring word MF1 as follows :-

- (1) The setting of pulse rate flags in MF1.
- (2) QRS complex width measurement.
- (3) Calculating the percentage of wide QRS complexes.
- (4) Calculating the true R-R interval.
- (5) Classification of R-R intervals as long, short or normal.

2. IDENTIFICATION

SUBROUTINE NAME	MONS1
PROGRAM MODULE	MONS1P
GENERAL DATA MODULE	G0003D
GENERAL DATA MODULE	G0004D
GENERAL DATA MODULE	G0005D
PERMANENT DATA MODULE	P0003D

3. SIZE

PROGRAM MODULE	644	Bytes.
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4. CALLS TO SUBROUTINE

B @MONS11

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	MONTOP
B	@FINISH
PROGRAM MODULE	MONS2P
B	@MONS21

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data for this program is the output data from the program module MONTDP, this data being the current estimate of the R-R interval (RRC), and the position of the QRS complex (POINT) in the input buffer (IBP1).

6.2. OUTPUT DATA

The output from this program is the monitoring result word MF1, the individual bits of which are the TRUE/FALSE answers to the tests performed by the program. Also supplied by this program is the true R-R interval measurement which is placed in RRSAVE.

6.3. ADDITIONAL DATA CHANGES

The software flags that are effected by this program are SFP1, SU2 and SU3.

7. TIMING

This program is executed only when the MONTDP program has detected a QRS complex. The combined execution time of all the monitoring modules (MONTDP, MONS1P and MONS2P) is 3.2ms.

For more information on software timing see Chapters 5 and 7.

8. AUTHOR

B.T.V. WARTON.

```

TITL 'MONITOR SEARCH SECTION'
♦ PROGRAMME MODULE IDENT (TASK)
  IDT 'MONS1P'
♦ TRANSFER VECTORS OR ENTRIES
  DEF MONS11
♦ CALLED PROGRAM MODULES
  REF MONTDP,MONS2P
  REF FINISH,MONS21
♦ LINKED DATA MODULES
  REF G0003D,G0004D,G0005D,P0003D
  REF SFP1,SU,DEP1
  REF TDP1,BUFLN,QRSPT,QRSNT
  REF MINL,IEP1,POSIT,SU2,RRC
  REF AVRR,MF1,MF2,BPM140,BPM110,BPM100,BPM90,BPM80
  REF BPM60,BPM40,BPM20,BPM10,RRSAVE
  REF AVRRB,RRSB,SEQB,RRLB,COUNT,MINV,MINP,QRSWID
  REF QRSWB,TDS,CLRWT,BEATS,HUND,T1,W1,T2,W2,T3
  REF PER82,WID82,WID82S,MAXV,MAXP,MONWR3
  REF MONS1W,SU3,DMINC,DMIND,POINT
  REF BPM120,TWELVE,FIVE,WQRS
  REF P2POS,DFSETD
  RDRG
  PSEG

```

***** P R O G R A M M E *****

```

♦
♦ REG ASSIGNMENT
♦ R0=SEQL R1=SEQS R2=SWQRS R8=MF1&MF2
♦

```

```

♦♦♦♦♦ SEARCH SECTION ♦♦♦♦♦
MONS11 LWPI MONS1W
SETD @SFP1 RESET SEARCH FLAG
MOV @RRC,@RRSAVE SAVE RR COUNT
CLR @RRC RESET RRC
MOV @SU2,R9 TEST SU2 FLAG
JGT SU2NO JUMP IF SU2=NO
MOV @SU3,R9 TEST SU3
JGT SU3NO JUMP IF SU3 NO
ABS @SU3 RESET SU3
B @FINISH
SU3NO MOV @RRSAVE,@AVRR MAKE RRSAVE=AVERAGE RR FOR START UP
MOV @DMINC,@DMIND MAKE DMIND=DMINC FOR START UP
ABS @SU2 RESET SU2

```

```

♦♦♦♦ SETTING PULSE RATE FLAGS
♦
SU2NO CLR R8 MF1=R8
C @AVRR,@BPM80 IS PULSE >80 BPM
JLE GT80 JUMP IF YES
C @AVRR,@BPM60 IS PULSE >60 BPM
JGT LE60 JUMP IF NO
AI R8,>00E0 SET FLAGS >60
JMP SD1
LE60 C @AVRR,@BPM40 IS PULSE >40
JGT LE40 JUMP IF NO
AI R8,>00C0 SET FLAGS >40
JMP SD1
LE40 C @AVRR,@BPM20 IS PULSE >20
JGT LE20 JUMP IF NO
AI R8,>0080 SET FLAGS >20
JMP SD1
LE20 AI R8,>0000 SET FLAG <20

```



```

COMP2  CDC  @QRSWB,R8          IS QRSWB=1
        JNE  INCT2
        INC  @W2              INC WIDE COUNT
INCT2  INC  @T2              ^^ TOTAL ^^
        C    @T2,@BEATS      IS T2=BEATS
        JNE  SUM
        ABS  @T05            RESET FLAG
        SET0 @CLRWT         SET FLAG
SUM     MOV  @W1,R9          GET W1
        A    @W2,R9          W1+W2=R9
        MPY  @HUND,R9       R9*100=R9/R10
        MOV  @T1,@T3        GET T1
        A    @T2,@T3        T1+T2=T3
        DIV  @T3,R9         R9/T3=R9 REMAINDER R10
        MOV  R9,@WID82S     T
        C    R9,@PER82      IS R9>=82 PERCENT
        JLT  CALRR
        SDC  @WID82,R8      SET 82 WIDE BIT FLAG YES (=1)

```

◆
◆◆◆◆◆◆◆◆◆◆ TRUE R-R SECTION ◆

```

CALRR  MOV  @P2POS,R13      GET P2 CROSS OVER POINT
        S    @MINP,R13
        JGT  DIFOK
        JEQ  DIFOK
        A    @BUFLN,R13     ANS SHOULD BE +
DIFOK  MOV  @RRSAVE,R14
        A    @OFSET0,R14
        S    R13,R14        R14=RRC+OFSET0-OFSETN=TRR
        JLT  RRERRD
        MOV  R14,@RRSAVE
        MOV  R13,@OFSET0
RRERRD EQU  $

```

◆
◆◆◆◆ START OF 2 X AVRR SECTION ◆◆◆◆◆◆◆◆◆◆

```

LT82   MOV  @AVRR,R9       GET AVRR
        SLA  R9,1          AVRR X 2
        C    @RRSAVE,R9    IS RRSAVE>=2 X AVRR
        JLT  RRLT         JUMP IF RRSAVE <
        SDC  @AVRRB,R8     SET AVRR BIT=1

```

◆
◆◆◆◆ START OF RR = LONG, SHORT OR NORMAL SECTION ◆◆◆◆◆

```

RRLT   SLA  R0,1           SHIFT SEQ LONG REG
        SLA  R1,1           ^^ ^^ SHORT REG
        CLR  R9
        MOV  @AVRR,R10      GET AVRR
        C    R10,@BPM120
        JLE  GT120
        SRA  R10,3          1/8
        S    @FIVE,R10     R10 - 5
TESTLS MOV  @AVRR,R9       GET AVRR
        A    R10,R9        AVRR + IER
        C    @RRSAVE,R9
        JGT  RRLONG        JUMP IF RR IS LONG
        S    R10,R9        R9=AVRR
        S    R10,R9        AVRR- IER
        C    @RRSAVE,R9
        JHE  SAVEMF        JUMP IF NOT (IE NORMAL RR)

```

SCR2.TASK.S.MONS1P 15:55:04 TUESDAY, OCT 17, 1978.

```

        SDC  @RRSB,R8          SET SHORT BIT=1
        SDC  @SEQB,R1         SET SEQ SHORT BIT=1
        JMP  SAVEMF
GT120   DIV  @TWELVE,R9
        MOV  R9,R10
        JMP  TESTLS
RRLONG  SDC  @RRLB,R8         SET LONG BIT=1
        SDC  @SEQB,R0         SET SEQ LONG BIT=1
♦
♦♦♦♦♦♦♦♦ SAVE MF1 ♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦
♦
SAVEMF  EQU  $
        MOV  R8,@MF1         SAVE MF1
        B    @MONS21         GO TO MONS21 PROGRAMME
        END
```

MONITOR SEQUENCE SEARCH SECTION

1. DESCRIPTION

This program is concerned with testing for 9 different sequences of R-R intervals and QRS complex widths, and placing the result in monitoring word MF2.

At the end of this program is the updating procedures for the parameters DMIN, TDPI and AVRR, and also the procedure for alarming the condition of "no QRS for 6 seconds".

2. IDENTIFICATION

SUBROUTINE NAME	MONS2
PROGRAM MODULE	MONS2P
GENERAL DATA MODULES	G0003D
GENERAL DATA MODULES	G0004D
GENERAL DATA MODULES	G0005D
PERMANENT DATA MODULES	P0004D

3. SIZE

PROGRAM MODULE 322 Bytes.

4. CALLS TO SUBROUTINE

B	@MONS21
B	@NOQRS

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	MONTDP
B	@FINISH

6. INTERNAL DATA TRANSFER

6.1. INPUT DATA

The input data for this program is supplied in register R0, R1 and R2 of workspace area MONS1W.

The contents of the registers are :-

- (i) R0 = Long R-R interval sequence bits.
- (ii) R1 = Short R-R interval sequence bits.
- (iii) R2 = Wide QRS complex sequence bits.

Data also used by this program, are words MF1, DMINC, DMIND, TDPI, RRSAVE and AVRR.

6.2. OUTPUT DATA

The output from this program is the Monitoring result word MF2, the individual bits of which indicate which sequence of R-R intervals and QRS widths have been detected.

7. TIMING

This program is executed only when the MONTDP program has detected a QRS complex. The combined execution time of all the monitoring modules (MONTDP, MONDIP, MONS2P) is 3.2ms.

For more information on software timing see Chapters 5 and 7.

8. AUTHOR

B.T.V. WARTON.


```

CZC @CZC4,R1 TEST NOT SHORT -NS-
JNE FAIL6
MOV @SEQ5,R8 SET S-NS-S FLAG BIT =1
JMP RETMF2
FAIL6 CDC @CDC5,R2 TEST WORS --W
JNE SFAIL3
CZC @CZC5,R2 TEST NOT WORS MWNW-
JNE SFAIL3
MOV @SEQ7,R8 SET S-S-S(W) FLAG BIT=1
JMP RETMF2

```

```

♦
♦♦♦♦♦♦ SEQUENCES S-NS-N-NL & S-NS-N-L
SFAIL3 CDC @CDC4,R1 TEST SHORT S---
JNE SFAIL4
CZC @CZC5,R1 TEST NOT SHORT -NSNS-
JNE SFAIL4
CZC @CZC6,R0 TEST NOT LONG --NLNL
JNE SFAIL5
MOV @SEQ6,R8 SET S-NS-N-NL FLAG=1
JMP RETMF2
SFAIL5 CZC @CZC7,R0 TEST NOT LONG --NL-
JNE SFAIL4
CDC @CDC5,R0 TEST LONG ---L
JNE SFAIL4
MOV @SEQ9,R8 SET S-NS-N-L FLAG BIT=1
JMP RETMF2

```

```

♦
♦♦♦♦♦♦ SEQUENCE S-NS-L
SFAIL4 CDC @CDC6,R1 TEST SHORT S--
JNE RETMF2
CZC @CZC7,R1 TEST NOT SHORT -NS-
JNE RETMF2
CDC @CDC5,R0 TEST LONG --L
JNE RETMF2
MOV @SEQ8,R8 SET S-NS-L FLAG BIT=1
RETMF2 MOV R8,@MF2 SAVE MF2

```

```

♦
♦♦♦♦♦♦ FINDING NEW DMIN & TD IF NEEDED
MOV @MF1,R9 GET MF1
CDC @QRSWB,R9 TEST WORSIN MF1
JEQ AVRUD NO UP DATE
MOV @DMINO,R9 GET DMIN OLD
ABS R9 IS R9 +VE
JLT PD1
JEQ PD1
BL @DMINER DMIN +VE GO TO ERROR SECTION
PD1 MPY @EIGHT,R9 DMINO X 8=R9&R10
DIV @TEN,R9 R9&R10 / 10=DMINX0.8=R9
MOV R9,R8 R8=DMINO X 0.8
MOV @DMINC,R10 GET DMIN CURRENT
ABS R10 IS DMINC +VE
JLT PD2
JEQ PD2
BL @DMINER DMINC +VE GO TO ERROR SECTION
PD2 SLA R10,1 DMIN CURRENT X 2
CLR R9
DIV @TEN,R9 R9=DMIN CURRENT X0.2
A R9,R8 R8=NEW DMINO
MOV R8,R9
MPY @SIX,R9

```

SCR2.PROG.S.MONS2P 17:18:21 WEDNESDAY, OCT 18, 1978.

```

      DIV  @TEN,R9          R9= +TD
      NEG  R9              R9= -TD
      MOV  R9,@TDP1        LOAD NEW TD
      NEG  R8
      MOV  R8,@DMINO        LOAD NEW DMINO
♦      AVRUD UPDATE SECTION
      MOV  @MF1,R9
      CDC  @RRSB,R9        WAS RR SHORT
      JEQ  NUD
      CDC  @RRLB,R9        WAS IT LONG
      JEQ  NUD
      MOV  @AVRR,R9        GET AVERAGE RR
      A    @RRSAVE,R9
      SRA  R9,1            DIV BY 2 TO FIND NEW AVERAGE
      MOV  R9,@AVRR        SAVE NEW AVERAGE
      NUD  JMP  STIM
      DMINER RT
♦      INSERT HERE ERROR SECTION FOR +DMIN'S IF REQUIRED
♦
♦♦♦♦♦♦♦♦ NO QRS FOR SIX SECONDS SECTION
      NOQRS MOV  @MF1,R9          GET MF1
      CDC  @NQRS6B,R9          SET NQRS6 BIT=1
      MOV  R9,@MF1            RET MF1
      STIM  INC  @DSTIMC        INC DIAG STIM COUNT
      SETD @DIAG              SET DIAG F L A G
      B    @FINISH            GO TO FINISH SECTION
      END
```

DIAGNOSIS PROGRAM

1. DESCRIPTION

This program's function is to use the results from the Monitoring Task (MF1 and MF2), to determine if a diagnosis can be made. If a diagnosis is obtained, the diagnosis program activates the MCP task so that the diagnosis is communicated to the operator dedicated processor.

2. IDENTIFICATION

SUBROUTINE NAME	DIAT1
PROGRAM MODULE	DIAT1P
GENERAL DATA MODULE	G0002D
GENERAL DATA MODULE	G0005D
GENERAL DATA MODULE	G0006D
PERMANENT DATA MODULE	P0005D

3. SIZE

PROGRAM MODULE 220 Bytes.

4. CALLS TO SUBROUTINE

BLWP @DIAT11

5. INTERNAL DATA TRANSFERS

5.1. INPUT DATA

The input data to this program is the two words MF1 and MF2 which are generated by the monitoring task.

5.2. OUTPUT DATA

The output data from this program is the two words DF1 and DF2, the individual bits of which indicate (if equal to one) which diagnoses have been found.

5.3. ADDITIONAL DATA CHANGES

The software flags that may be effected by this program are those to activate the MCPTOP Task, i.e. flags DISF, CSTIMC and MCP, and also those flags to de-activate the diagnosis task, i.e. DSTIMC and DIAG.

6. TIMING

The execution time of this program is 0.2mS.

7. AUTHOR

B.T.V. WARTON.


```

        SOC  @BRAD4,R3          SET BRAD DIAG BIT IN DF1
        JMP  ASYT

♦
♦♦♦♦♦♦♦♦  IDIOVENTRICULAR TACH
IDIOVT  COC  @DIDID1,R1        TEST FOR TRUE COND
        JNE  ASYT
        CZC  @DIDID0,R1        TEST FOR FALSE COND
        JNE  ASYT
        SOC  @DIDID5,R3        SET IDIOV DIAG BIT IN DF1

♦
♦♦♦♦♦♦♦♦  ASYSTOLE
ASYT    COC  @DASYT1,R1        TEST FOR TRUE COND
        JNE  ESCBT
        CZC  @DASYT0,R1        TEST FOR FALSE COND
        JNE  ESCBT
        SOC  @DASYT7,R3        SET ASYT DIAG BIT IN DF1

♦
♦♦♦♦♦♦♦♦  ESCAPED BEAT
ESCBT   COC  @DESCB1,R1        TEST FOR TRUE COND
        JNE  BBB
        CZC  @DESCB0,R1        TEST FOR FALSE COND
        JNE  BBB
        SOC  @DESCBT8,R3       SET ESCBT DIAG BIT IN DF1

♦
♦♦♦♦♦♦♦♦  BUNDLE BRANCH BLOCK
BBB     COC  @DBBB1,R1         TEST FOR TRUE COND
        JNE  DIAGOP
        CZC  @DBBB0,R1         TEST FOR FALSE COND
        JNE  DIAGOP
        SOC  @DBBB3,R3         SET BBB DIAG BIT IN DF1

♦♦♦♦♦♦♦♦  DIAGNOSIS D/P
DIAGOP  MOV  @DISF,R0          HAS LAST REQUEST BEEN DONE
        JLT  EXITA             JUMP IF NO
        MOV  R3,@DF1           SAVE DF1
        MOV  R4,@DF2           SAVE DF2
        A    R3,R4             IS DIAG <> 0
        JEQ  EXITA             JUMP IIF NO DIAGNOSIS
        SETO @DISF             SET MCP DIAG FLAG
        INC  @CSTIMC           STIM MCP
        SETO @MCP             STIM MCP
EXITA   DEC  @DSTIMC           DEC DIAG STIM
        JNE  EXIT
        CLR  @DIAG             CLR DIAG STIM
EXIT    RTWP                   RET TO TASK HANDLER
        END

```


INPUT DATA PROCESSOR TASK (PATIENT)

1. DESCRIPTION

The function of this program is to receive the instructions and data that are transmitted by the Output task of the operator dedicated processor. During this communication the input program must transmit to the operator processor, replies such as Acknowledge (ACK), Negative Acknowledge (NAK) and Enquiry (ENQ) as and when required by the interprocessor communication protocol.

This task also uses the UART interval timer to detect abnormal delays in the normal communication protocol.

2. IDENTIFICATION

SUBROUTINE NAME	IPPT0
PROGRAM MODULE	IPPTOP
GENERAL DATA MODULE	G0016D
GENERAL DATA MODULE	G0018D

3. SIZE

PROGRAM MODULE	176	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

BLWP	@IPPT01
BL	@IPPT02
BL	@IPPT03

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	PPUIHP
B	@PPUIH3

6. INTERNAL DATA TRANSFER

6.1. OUTPUT

The data received by this program is placed in a

file called IPFILE.

6.2. ADDITIONAL DATA CHANGES

The software flags effected by this program are those to activate the MCP task i.e. CSTIMC, MCPIP and MCP flags.

7. EXTERNAL DATA TRANSFERS

PERIPHERAL TMS 9902 UART

7.1. INPUT

INTERRUPT LEVEL 4
CRU BASE >1A80
CRU BIT FUNCTIONS AS SPECIFIED IN THE
TMS 9902 DATA SHEETS.

7.2. OUTPUT

CRU BASE >1A80
CRU BIT FUNCTIONS AS SPECIFIED IN THE
TMS 9902 DATA SHEETS.

8. TIMING

The timing of this program is dependent on the data rate.

9. AUTHOR

B.T.V. WARTON.

TITL 'INPUT DATA PROCESSOR TASK (PATIENT)'

◆ PROGRAMME MODULE IDENT (PROG)

IDT 'IPPTOP'

◆ TRANSFER VECTORS OR ENTRIES

DEF IPPT01,IPPT02,IPPT03

◆ CALLED PROGRAMME MODULES

REF PPUIH3

◆ LINKED DATA MODULES

REF 60016D,60018D

REF IPPT0W,IPFILE,MCP,MCPIP,CSTIMC

REF PPTHAW

RORG

PSEG

◆◆◆◆◆◆◆◆◆◆ P R O G R A M M E ◆◆◆◆◆◆◆◆◆◆

IPPT01 DATA IPPT0W,START

START	LI R1,IPFILE	LOAD FILE ADDRESS
	TB 25	TIMELP
	JEQ EXIT	ABANDON I/P
	BL @INPUT	GO I/P CHAR
	MOVB R5,*R1	PUT IT IN I/P FILE
	LI R4,>0500	END
	BL @IPPT03	O/P END & WAIT
	SETO R5	MAKE R5=-1
	BL @INPUT	GO I/P CHAR
	AB *R1,R5	LAST INST +THIS INST
	INC R5	+1 SHOULD=0 IF INST OK
	JNE OPNAK	
	LI R4,>0600	ACK
	BL @IPPT03	GO O/P ACK & WAIT
	MOVB *R1+,R5	IS INST +VE
	JLT NEGINS	

◆

◆ END OF TRANSMISSION SECTION

EOTOK	INC @CSTIMC	STIM MCP TASK
	SETO @MCP	STIM MCP
	SETO @MCPIP	SET MCP FLAG
EXIT	EQU \$	
	LMPI PPTHAW	GET WP
	SBZ >D	RESET I/P TASK CRU INDICATOR BIT
	B @PPUIH3	GOTO PPUIHP ENTRY FROM IPPTOP

◆

OPNAK	LI R4,>1500	NAK
	BL @IPPT02	O/P NAK
	JMP EXIT	EXIT PROGRAM
NEGINS	LI R9,50	COUNT FOR 50 BYTES OF DATA
	CLR R8	BCC
NEXT1	STOR R5,8	GET CHAR
	SBZ 18	RESET UART
	AB R5,R8	BCC SUM
	MOVB R5,*R1+	STORE DATA
	DEC R9	DEC BYTE COUNT
	LI R4,>0500	END
	BL @IPPT03	O/P END & WAIT
	MOV R9,R9	HAS ALL DATA BEEN RECEIVED
	JNE NEXT1	
	STOR R5,8	GET CHAR
	SBZ 18	RESET UART
	CB R5,R8	IS BCC = BCC
	JNE OPNAK	
	LI R4,>0600	ACK

SCR2.PROG.S.IPPT0P 18:04:50 WEDNESDAY, OCT 18, 1978.

BL @IPPT03 D/P ACK& WAIT
JMP EDTOK

◆
◆◆◆◆◆◆◆ INPUT CHAR
INPUT SBZ 20 TIMER INT OFF
STCR R5,8 STORE CHAR
SBZ 18 RESET UART
RT

◆
◆◆◆◆◆◆◆ OUTPUT CHAR
IPPT02 SBZ 18 RESET RBRL
SBO 16 TRANSMITTER ON
LDCR R4,8 LOAD UART
SBZ 16 TRAN OFF
RT

◆
◆◆◆◆◆◆◆ SET TIMER
SETIME SBO 13 ENABLE TIMER COUNT IN UART
LI R5,>FA00 16 MS
LDCR R5,8 LOAD UART COUNT
SBO 20 ENABLE TIMER INT
RT

◆
◆◆◆◆◆◆◆ OUTPUT CHAR & WAIT FOR ECHO
IPPT03 MOV @R11,R10 SAVE RET
BL @IPPT02 GO D/P CHAR
BL @SETIME GO SET TIMER
RCVLP TB 21 RBRL
JNE RCVLP JUMP IF CHAR NOT RECEIVED
SBZ 20 TURN OFF TIMER INT,CHAR RECEIVED
B @R10 RETURN
END

OUTPUT DATA PROCESSOR TASK (PATIENT)

1. DESCRIPTION

The function of this program is to transmit instructions and data to the input task of the operator dedicated processor. The information to be transmitted is supplied to this program by the MCP task. During the communication this output task must receive the replies transmitted from the operator processor, informing this task of normal (ACK) or abnormal (NAK) communication, or requesting the next character (ENQ).

This task also uses the UART interval timer to detect abnormal delays in the normal communication protocol.

2. IDENTIFICATION

SUBROUTINE NAME	OPPT0
PROGRAM MODULE	OPPTOP
GENERAL DATA MODULES	G0016D
GENERAL DATA MODULES	G0018D

3. SIZE

PROGRAM MODULE	130	BYTES.
----------------	-----	--------

4. CALLS TO SUBROUTINE

BLWP	@OPPT01
------	---------

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	PPUIHP
B	@PPUIH4
B	@PPUIH5
SUBROUTINE NAME	IPPTOP
BL	@IPPT02
BL	@IPPT03

6. INTERNAL DATA TRANSFER

6.1. INPUT

The input data for this task is found at the address placed in word OPDATA. This allows PROM resident messages to be sent. If however data is to be transferred, the instruction and data are placed in the file called OPFILE.

6.2. ADDITIONAL DATA CHANGES

The only software flag effected by this task is the output task active flag (OPTASK), which is reset when the task is completed.

7. EXTERNAL DATA TRANSFERS

PERIPHERAL TMS 9902 UART

7.1. INPUT

INTERRUPT LEVEL 4
CRU BASE >1A80
CRU BIT ASSIGNMENT AS SPECIFIED IN
THE TMS 9902 DATA SHEETS.

7.2. OUTPUT

CRU BASE >1A80
CRU BIT ASSIGNMENT AS SPECIFIED IN
THE TMS 9902 DATA SHEETS.

8. TIMING

The timing of this program is dependent on the data rate.

9. AUTHOR

B.T.V. WARTON.

TITL 'OUTPUT DATA PROCESSOR TASK (PATIENT)'

- ◆ PROGRAMME MODULE IDENT (PROG)
 - IDT 'OPPTOP'
- ◆ TRANSFER VECTORS OR ENTRIES
 - DEF OPPT01
- ◆ CALLED PROGRAM MODULES
 - REF PPUIHP,IPPT0P
 - REF PPUIH4,PPUIH5,IPPT02,IPPT03
- ◆ LINKED DATA MODULES
 - REF OPPT0W,OPDATA,OPTASK
 - REF PPTHAW
 - RORG
 - PSEG

◆◆◆◆◆◆◆◆◆◆ P R O G R A M M E ◆◆◆◆◆◆◆◆◆◆

```

OPPT01 DATA OPPT0W,START
START TB 25 TIMELP
      JEQ BADGO
      MOV @OPDATA,R1 GET O/P TEXT ADDRESS
      MOVB *R1+,R4 GET INST
      BL @IPPT03 O/P INST & SET TIMER & WAIT
      INV R4 INV INST
      BL @IPPT03 O/P INV INS SET TIMER & WAIT
      STCR R5,8 GET I/P
      SBZ 13
      CI R5,>0600 IS IT ACK
      JNE TRYNAK
      INV R4 IS INST POS
      JLT NEGINS
OPEOT LI R4,>0400 EDT
      BL @IPPT02 GO O/P CHAR
      LWPI PPTHAW T
      SBZ >E T
      B @PPUIH4 GOTO PPUIHP ENTRY FROM OPPTOP
TRYNAK CI R5,>1500 NAK
      JNE TOUT
BADGO EQU $
      LWPI PPTHAW T
      SBZ >E T
      B @PPUIH5 GOTO PPUIHP FROM UNSUCCESSFUL OPPTOP
TOUT BL @SETIME
      CLR @OPTASK
      RTWP
SETIME SBD 13
      LI R5,>FA00 16 MS
      LDCR R5,8
      SBD 20
      RT
NEGINS LI R9,50 COUNT=50
      CLR R8 BCC
NEXT MOVB *R1+,R4 GET DATA
      AB R4,R8 BCC=BCC+DATA
      DEC R9 COUNT=COUNT-1
      BL @IPPT03
      MOV R9,R9 TEST COUNT
      JNE NEXT
      MOVB R8,R4 GET BCC
      BL @IPPT03
      STCR R5,8 GET I/P
      CI R5,>0600 ACK
      JEQ OPEOT
      JMP TRYNAK
      END

```

MICROPROCESSOR COMMUNICATION PACKAGE

1. DESCRIPTION

This program's function is to generate or interpret the communication instructions and data which are passed between the patient and operator dedicated processors. The generation of instructions and data by this program is due to either a request from the Monitoring or Diagnosis tasks, or by a request for data from the operator processor. The instructions sent by the operator processor are interpreted by this program and the requested action performed.

2. IDENTIFICATION

SUBROUTINE NAME	MCPT0
PROGRAM MODULE	MCPTOP
GENERAL DATA MODULES	G0004D
GENERAL DATA MODULES	G0005D
GENERAL DATA MODULES	G0017D
GENERAL DATA MODULES	G0018D
PERMANENT DATA MODULES	P0009D

3. SIZE

PROGRAM MODULE	304	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

BLWP	@MCPT01
------	---------

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	PPUIHP
B	@PPUIH2

6. INTERNAL DATA TRANSFER

6.1. INPUT

The input data to this program are the request

MONSF, DISF and MCPIP

and the data found at locations,

MOTEXT, IPFILE, DF1, DF2, MF1, MF2, and AVRR.

6.2. OUTPUT

The output from this program is used by the output task and is in the form of an address placed in location OPDATA, and instructions and data placed in the output file (OPFILE).

6.3. ADDITIONAL DATA CHANGES

As a result of instructions received by this program the following flags and data locations may be set or reset accordingly :-

MONSF, DISF, CSTIMC, MCP, SU, SU2, SU3,
T1, T2, T3, W1, W2, MONSLW, DFGO, SDELAY.

7. TIMING

The execution time of this program is dependent on the complexity of the operation it has been requested to perform, and also the number of times it is interrupted by higher priority tasks.

8. AUTHOR

B.T.V. WARTON.

```

TITL 'MICROPROCESSOR COMMUNICATION PACKAGE'
* PROGRAMME MODULE IDENT (PROG)
  IDT 'MCPTOP'
* TRANSFER VECTORS OR ENTRIES
  DEF MCPT01
* CALLED PROGRAMME MODULES
  REF PPUIH1
  REF PPUIH2
* LINKED DATA MODULES
  REF G0004G,G0005D,G0017D,G0018D,P0009D
  REF MCPT0W,MCP1P,MONSF,DISF,MOTEXT
  REF SM,EM,PR,CM,OPDATA,CSTINC,MCP
  REF SU,SU2,SU3,RRC,T1,T2,T3,W1,W2,MONS1W
  REF DFGD,MM3,MM1,OPFILE,PRM,AVRR,IPFILE,CMS,MM4
  REF OPAC,DF1,DF2,DIAGM,MM2,SDELAY,MM5,MM6
  REF PS,PSD,MF1,MF2
RORG
PSEG

```

***** P R O G R A M M E *****

```

MCPT01 DATA MCPT0W,START
START ABS @MCP1P          IS IT I/P FROM UP
      JLT MINPUT
      ABS @MONSF          IS IT MONI MCP REQUEST
      JLT MIM
      MOV @DISF,R7        IS IT DIAG MCP REQUEST
      JLT DIM
      B @OUT              JUMP OUT
*
***** MONITOR TASK MESSAGE O/P REQUEST
MIM MOV @MOTEXT,R2        GET MON O/P ADDRESS
    JMP STIMOP
*
***** DIAGNOSIS TASK MESSAGE O/P REQUEST
DIM LI R1,OPFILE          GET OPFILE ADDRESS
DOCLR CLR *R1+             CLEAR OPFILE
      CI R1,MCPT0W
      JNE DOCLR
      LI R1,OPFILE          GET OPFILE ADDRESS
      MOV @DIAGM,*R1+       SAVE DIAG MESSAGE IN OPFILE
      MOV @DF1,*R1+        SAVE DF1 IN OPFILE
      MOV @DF2,*R1+        SAVE DF2 IN OPFILE
      LI R2,OPFILE          GET OPFILE ADDRESS
      ABS @DISF             RESET DIAG MESSAGE REQUEST
      JMP STIMOP
*
***** INTER PROCESSOR MESSAGE REQUEST FROM I/P TASK
MINPUT LI R4,IPFILE        GET ADDRESS OF I/P FILE
       CB @SM,*R4           IS IT START MON INST
       JEQ DOSM
       CB @EM,*R4           IS IT END MON INST
       JEQ DOEM
       CB @PR,*R4           IS IT PULSE RATE INST
       JEQ DOPR
       CB @CM,*R4           IS IT CONTINUE MON INST
       JEQ DOCM
       CB @PS,*R4           IS IT PATIENT STATUSE REQUEST
       JEQ DOPS
*
* ERROR IN INST TELL OPERATOR
LI R2,MM2          GET ERROR MESSAGE ADDRESS

```

```

***** ACTIVATION OF O/P TASK IF NOT ACTIVE
STIMOP MOV  @OPAC,R0      IS O/P ACTIVE
        JNE  STIMOP      WAIT FOR NOT ACTIVE *****
        MOV  R2,@OPDATA   GIVE O/P TASK O/P DATA ADDRESS
OUT     DEC  @CSTIMC      DEC MCP STIM COUNT
        JNE  EXIT
        CLR  @MCP         RESET MCP TASK ACTIVE FLAG
EXIT    B    @PPUIH2     GO TO UART INT HANDLER TO O/P SOH

```

```

***** START MONITORING SOFTWARE SECTION
DOEM    MOV  @DFG0,R7     IS IT MONITORING
        JGT  SMON
        SETO @SU         SET MON START UP FLAGS
        SETO @SU2       SET MON START UP FLAGS
        SETO @SU3       SET MON START UP FLAGS
        SETO @SDELAY    SET MON START UP DELAY FLAG
        CLR  @RRC       CLEAR MON LOCATIONS
        CLR  @T1        CLEAR QRS TOTAL 1
        CLR  @T2        CLEAR QRS TOTAL 2
        CLR  @T3        CLEAR QRS TOTAL 3
        CLR  @W1        CLEAR QRS WIDE TOTAL 1
        CLR  @W2        CLEAR QRS WIDE TOTAL 2
        LI   R5,MONS1W
        CLR  @R5+       CLEAR MON SEQUENCE REGS
        CLR  @R5+       CLEAR MON SEQUENCE REGS
        CLR  @R5        CLEAR MON SEQUENCE REGS
        ABS  @DFG0      SET FLAG SO PPIDHP STIMS MON TASK
        LI   R2,MM3     MONITORING MESSAGE
        JMP  STIMOP
SMON    LI   R2,MM5     GET ALREADY MON MESSAGE
        JMP  STIMOP

```

```

***** END OF MONITORING SECTION
DOEM    MOV  @DFG0,R7     IS SYSTEM MONITORING
        JLT  EMNO       JUMP IF NO
        SETO @DFG0      SET DFG0 SO IPDHTP DOSE NOT STIM MONI
        LI   R2,MM1     END MONITORING MESSAGE
        JMP  STIMOP
EMNO    LI   R2,MM6     GET NOT MONITORING MESSAGE
        JMP  STIMOP

```

```

***** PULSE RATE DATA TRANSMISSION SECTION
DOPR    LI   R3,OPFILE   GET OPFILE ADDRESS
        MOV  @PRM,@R3+   LOAD PR INST IN FILE
        MOV  @AVRR,@R3+  LOAD AVERAGE RR DATA IN FILE
        LI   R2,OPFILE   GET OPFILE ADDRESS
        JMP  STIMOP

```

```

***** DO CONTINUE MONITORING INSTRUCTION
DOCM    MOV  @SU,R7      IS SYSTEM MONITORING
        JLT  CMNO       JUMP IF NO
        ABS  @DFG0      RESET DFG0 FLAG SO IPDHTP STIMS MONI
        SETO @CMS       SET CMS SO MONI KNOWES TO CONT MONI
        LI   R2,MM4     GET CONT MONI REPLY,MONITORING AGAIN
        JMP  STIMOP
CMNO    LI   R2,MM5     GET NOT MONITORING MESSAGE
        JMP  STIMOP

```

```

***** PATIENT STATUS DATA TRANSMISSION SECTION
DOPS    LI   R3,OPFILE   GET OPFILE ADDRESS

```

SCR2.PROG.S.MCPT0P 18:17:54 WEDNESDAY, OCT 18, 1978.

MOV	@PSD,*R3+	LOAD OPFILE WITH PATIENT STATUS INST
MOV	@AVRR,*R3+	LOAD OPFILE WITH AVERAGE RR
MOV	@DF1,*R3+	LOAD OPFILE WITH DF1
MOV	@DF2,*R3+	LOAD OPFILE WITH DF2
MOV	@MF1,*R3+	LOAD OPFILE WITH MF1
MOV	@MF2,*R3+	LOAD OPFILE WITH MF2
LI	R2,OPFILE	GET OPFILE ADDRESS
JMP	STIMOP	
END		

PERMANENT DATA MODULE P0001D

1. DESCRIPTION

This data module contains the digital filter coefficients used in the signal conditioning program (IPDHTP).

2. IDENTIFICATION

PERMANENT DATA MODULE P0001D

3. SIZE

20 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

      TITL 'PERMANENT DATA MODULE P0001D'
♦ PERMANENT DATA MODULE IDENTIFIER
      IDT 'P0001D'
      EVEN
      DEF LEVEL,KHP,A1,A2,K1LP,K2LP,C
      DEF KDC,A1DC,A2DC
      RORG
      PSEG
LEVEL  DATA >1A           NOISE THRESHOLD
KHP    DATA >04FC        60 HZ HP FILTER
A1     DATA >2A7F        //
A2     DATA >153F        //
K1LP   DATA >0124        25 HZ LP FILTER
K2LP   DATA >FF97        //
C      DATA >11         //
KDC    DATA >0FDB        DC FILTER
A1DC   DATA >0048        //
A2DC   DATA >0024        //
      END

```

PERMANENT DATA MODULE P00020

1. DESCRIPTION

This data module contains the data specifying the length of the input ECG and difference buffers etc., used by the Monitoring Task.

2. IDENTIFICATION

PERMANENT DATA MODULE P00020

3. SIZE

12 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'PERMANENT DATA MODULE P0002D'
♦ PERMANENT DATA MODULE IDENTIFIER
        IDT 'P0002D'
        EVEN
        DEF BUFLN, DBUFL, MINL, RRC32, TEN, SIX
        RDRG
        PSEG
BUFLN DATA 750          BUFFER LENGTH
DBUFL DATA >60        DIFF BUFF LENGTH
MINL DATA >FFF5       MIN LIMIT *****
RRC32 DATA 32         32 RR SAMPLES DELAY
TEN DATA 10           CONSTANT
SIX DATA 6            CONSTANT
        END

```


PERMANENT DATA MODULE P0003D

1. DESCRIPTION

This data module contains the information used by the Monitoring Task, such as pulse rate comparison words and normal QRS width limit etc.

2. IDENTIFICATION

PERMANENT DATA MODULE P0003D

3. SIZE

46 Bytes.

4. AUTHOR

B.T.V. WARTON.

```

TITL 'PERMANENT DATA MODULE P0003D'
♦ PERMANENT DATA MODULE IDENTIFIER
IDT 'P0003D'
EVEN
DEF BPM140,BPM120,BPM110,BPM100,BPM90
DEF BPM80,BPM60,BPM40,BPM20
DEF AVRRB,RRLB,RRSB,SEQB,COUNT,QRSWID
DEF QRSWID,QRSWB,BEATS,HUND,TWELVE,FIVE
DEF PER82,WIDE82,QRSPT,QRSNT
RORG
PSEG
BPM140 DATA 107 RR INT = 140 BPM
BPM120 DATA 125 RR INT = 120 BPM
BPM110 DATA 136 RR INT = 110 BPM
BPM100 DATA 150 RR INT = 100 BPM
BPM90 DATA 166 RR INT = 90 BPM
BPM80 DATA 187 RR INT = 80 BPM
BPM60 DATA 250 RR INT = 60 BPM
BPM40 DATA 375 RR INT = 40 BPM
BPM20 DATA 750 RR INT = 20 BPM
AVRRB DATA >0400 RR<2XAVRR BIT
RRLB DATA >0800 RR LONG BIT
RRSB DATA >1000 RR SHORT BIT
SEQB DATA >0001 SEQUENCE BIT
COUNT DATA 20
QRSWID DATA 28 NORMAL WIDTH
QRSWB DATA >2000 QRS WIDE BIT
BEATS DATA 200 BEATS COUNT
HUND DATA 100 CONST
TWELVE DATA 12 CONST
FIVE DATA 5 CONST
PER82 DATA 82 82 PERCENT
WIDE82 DATA >4000 // // BIT
QRSPT BYTE 5 QRS +VE THRESHOLD
QRSNT BYTE -5 QRS -VE THRESHOLD
END

```

PERMANENT DATA MODULE P0004D

1. DESCRIPTION

This data module contains the comparison words used by the Monitoring Task, to detect various sequences of R-R interval and QRS complex width.

2. IDENTIFICATION

PERMANENT DATA MODULE P0004D

3. SIZE

50 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'PERMANENT DATA MODULE P0004D'
♦ PERMANENT DATA MODULE IDENTIFIER
        IDT  'P0004D'
        EVEN
        DEF  CDC1,CDC2,CDC3,CDC4,CDC5,CDC6
        DEF  CZC1,CZC2,CZC3,CZC4,CZC5,CZC6,CZC7
        DEF  SEQ1,SEQ2,SEQ3,SEQ4,SEQ5,SEQ6,SEQ7
        DEF  SEQ8,SEQ9
        DEF  NQRS6B,EIGHT,RRMAXT
        RORG
        PSEG
CDC1    DATA >00AA          4(S-NS) & 4(S(W)-NS)
CDC1    DATA >0055          ''
CDC2    DATA >0924          4(S-NS-N) & 4(S(W)-NS-N)
CDC2    DATA >06DB          ''
CDC3    DATA >0249          ''
CDC3    DATA >0005          S-NS-S
CDC4    DATA >2             ''
CDC4    DATA >8             S-NS-N-NL
CDC5    DATA >6             ''
CDC5    DATA >3             ''
CDC6    DATA >3             S-NS-N-L
CDC6    DATA >1             ''
CDC6    DATA >4             S-NS-L
SEQ1    DATA >1             4(S-NS)
SEQ2    DATA >2             4(S(W)-NS)
SEQ3    DATA >4             4(S-NS-N)
SEQ4    DATA >8             4(S(W)-NS-N)
SEQ5    DATA >10            S-NS-S
SEQ6    DATA >20            S-NS-N-NL
SEQ7    DATA >40            3S-W
SEQ8    DATA >80            S-NS-L
SEQ9    DATA >100           S-NS-N-L
NQRS6B  DATA >0200          NO QRS 6SEC BIT
RRMAXT  DATA 1500           MAX TIME TO QRS 6SEC
EIGHT   DATA 8             CONSTANT
        END

```

PERMANENT DATA MODULE P0005D

1. DESCRIPTION

This data module contains the comparison words used by the diagnosis Task, to diagnose the different kinds of ECG arrhythmias. Also included in this module are the words used when setting the different diagnosis bits in DF1 and DF2.

2. IDENTIFICATION

PERMANENT DATA MODULE P0005D

3. SIZE

52 Bytes.

4. AUTHOR

B.T.V. WARTON.

```

TITL 'PERMANENT DATA MODULE P0005D'
* PERMANENT DATA MODULE IDENTIFIER
  IDT 'P0005D'
  EVEN
  DEF SVT2, BBB3, BRAD4, IDIOV5, ARST6
  DEF ASYT7, ESCBT9, LS23
  DEF DSVTA1, DSVTA0, DSVTB1, DSVTB0, DBBB1, DBBB0
  DEF DBRAD1, DBRADO, DIDIO1, DIDIO0, DARST1, DARST0
  DEF DASYT1, DASYT0, DESCB1, DESCB0, DLS1
  DEF PRGT60
  RDRG
  PSEG
SVT2  DATA >0002          SVT DIAG BIT SET
BBB3  DATA >0004          BBB DIAG BIT SET
BRAD4 DATA >0003          BRAD DIAG BIT SET
IDIOV5 DATA >0010        IDIOV DIAG BIT SET
ARST6 DATA >0020          ARST DIAG BIT SET
ASYT7 DATA >0040          ASYT DIAG BIT SET
ESCBT9 DATA >0080        ESCBT DIAG BIT SET
LS23  DATA >0040          LS DIAG BIT SET
DSVTA1 DATA >00FF        SVT DIAG TEST
DSVTA0 DATA >4000        SVT DIAG TEST
DSVTB1 DATA >00FE        SVT DIAG TEST
DSVTB0 DATA >0001        SVT DIAG TEST
DBBB1  DATA >0400        BBB DIAG TEST
DBBB0  DATA >0001        BBB DIAG TEST
DBRAD1 DATA >00C0        BRAD DIAG TEST
DBRADO DATA >003F        BRAD DIAG TEST
DIDIO1 DATA >0080        IDIO DIAG TEST
DIDIO0 DATA >007F        IDIO DIAG TEST
DARST1 DATA >0200        ARST DIAG TEST
DARST0 DATA >001F        ARST DIAG TEST
DASYT1 DATA >0400        ASYT DIAG TEST
DASYT0 DATA >0A1F        ASYT DIAG TEST
DESCB1 DATA >2800        ESCBT DIAG TEST
DESCB0 DATA >103F        ESCBT DIAG TEST
DLS1   DATA >02F0        LOST SIG DIAG TEST
PRGT60 DATA >00E0        PR > 60 TEST
  END

```

PERMANENT DATA MODULE P0009D

1. DESCRIPTION

This data module contains the list of allowed instructions which can be received by the patient monitoring processor; and also the list of allowed messages which can be sent to the operator dedicated processor (MM1 TO MM6).

2. IDENTIFICATION

PERMANENT DATA MODULE P0009D

3. SIZE

24 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

      TITL 'PERMANENT DATA MODULE P0009D'
* PERMANENT DATA MODULE IDENTIFIER
      IDT 'P0009D'
      EVEN
      DEF MSUOVE,MFAIL,PRM,PR,SM,EM,CM,DIAGM
      DEF MM1,MM2,MM3,MM4,MM5,MM6,SR250,SIXTY
      DEF PSD,PS
      RDRG
      PSEG
PRM      DATA >C000      PR DATA MESSAGE
DIAGM    DATA >A300      DIAG  ' '  ' '
PSD      DATA >8100      PATIENT STATUS DATA
MSUOVE   BYTE >22        START UP OVER
MFAIL    BYTE >24        MONITOR FAIL
PR        BYTE >5C        SEND PR
SM        BYTE >50        START MON
EM        BYTE >53        END MON
CM        BYTE >55        CONTINUE MON
PS        BYTE >56        SEND PATIENT STATUS
MM1       BYTE >27        END OF MONITORING
MM2       BYTE >2B        ERROR MESSAGE
MM3       BYTE >21        MONITORING
MM4       BYTE >28        CONT MON
MM5       BYTE >2D        ALREADY MON
MM6       BYTE >2E        NOT MON
      EVEN
SR250    DATA 250        250 SAMPLES IN 1 SECOND
SIXTY    DATA 60        60 SEC 1 MIN
      END

```


SPECIFIC DATA MODULE IPDHTD

1. DESCRIPTION

This data module contains the workspace areas used for the different digital filters in program module IPDHTP, plus the locations where the output from the high and low pass filters are saved, as well as the output from the filtering network.

Also included in this module is the delay buffer present in the filtering network. It should be noted that this module must be the first in RAM as it contains the label RAM used by the initialisation program.

2. IDENTIFICATION

SPECIFIC DATA MODULE IPDHTD

3. SIZE

CLASS TWO 132 BYTES.

CLASS THREE 61 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'INPUT DATA HANDLER SPECIFIC DATA MODULE'
♦ SPECIFIC DATA MODULE IDENTIFIER
        IDT 'IPDHTD'
        EVEN
♦ CLASS TWO
        DEF RAM, RAM2
        DEF IPDHTW, WAHP, WALP, WADC, HPOP, LPOP
        RORG
        PSEG
RAM      EQU    $           START OF RAM
RAM2    EQU    $+2        SECOND WORD IN RAM
IPDHTW  BSS    32         IPDHT WORKSPACE AREA
WAHP    BSS    32         HIGH PASS FILT WORKSPACE AREA
WALP    BSS    32         LOW PASS FILT WORKSPACE AREA
WADC    BSS    32         DC FILTER WORKSPACE AREA
HPOP    BSS    2         HIGH PASS FILTER O/P
LPOP    BSS    2         LOW PASS FILTER O/P
♦
♦ CLASS THREE
        DEF VALUE, BUFFER, BUFEND
BUFFER  BSS    58        DELAY BUFFER IN IPDHTP
BUFEND  BSS    2         END OF THIS BUFFER
VALUE   BSS    1         O/P FROM FILTER NETWORK
        END

```

SPECIFIC DATA MODULE MONTDD

1. DESCRIPTION

This data module contains the workspace area used by the monitoring task MONTDP.

2. IDENTIFICATION

SPECIFIC DATA MODULE MONTDD

3. SIZE

CLASS TWO 32 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'MONITOR SPECIFIC DATA MODULE'
♦ SPECIFIC DATA MODULE IDENTIFIER
        IDT 'MONTDD'
        EVEN
♦ CLASS TWO
        DEF MONTDW,MONWR3
        RORG
        PSEG
MONTDW BSS 32                MONITOR WORKSPACE AREA
MONWR3 EQU MONTDW+6
        END

```

GENERAL DATA MODULE GO016D

1. DESCRIPTION

This data module contains the task handler workspace area, in which R5 is the task active number store. Also present in this module are the storage locations for the return vectors of suspended tasks; task active flags and counters, storage of time counters and the workspace area used by the PPUIHP program module.

2. IDENTIFICATION

GENERAL DATA MODULE GO016D

3. SIZE

CLASS TWO 122 BYTES.

4. AUTHOR

B.T.V. WARTON.

TITL 'GENERAL DATA MODULE 60016D'
 * GENERAL DATA MODULE IDENTIFIER

IDT '60016D'

EVEN

* CLASS TWO

DEF PPTHAW, MRTWP, DRTWP, IPRTWP, OPRTWP, MCRTWP
 DEF MWPRET, MPCRET, MSTRET, DWPRET, DPCRET, DSTRET
 DEF DWPRET, DPCRET, DSTRET, IWPRET, IPCRET, ISTRET
 DEF CWPRET, CPCRET, CSTRET
 DEF IDH, MONI, DIAG, MSTIMC, DSTIMC, IPTASK, OPTASK
 DEF CSTIMC, MCP, DPAC, ACTNO, MSEC, SEC, MINUTE
 DEF HOURS, PPUIHW

RDRG
 PSEG

PPTHAW	BSS	6	TASK HANDLER WA START POINT
ACTNO	EQU	PPTHAW+10	R5 IN PPTHAW IS ACTIVE TASK STORE
MRTWP	BSS	6	ADDRESS FOR MONITOR RETURNS
DRTWP	BSS	6	ADDRESS FOR DIAGNOSIS RETURNS
IPRTWP	BSS	6	ADDRESS FOR I/P TASK RETURNS
OPRTWP	BSS	6	ADDRESS FOR O/P TASK RETURNS
MCRTWP	BSS	2	ADDRESS FOR MCP TASK RETURNS
MWPRET	BSS	2	MONITOR WP RET STORE
MPCRET	BSS	2	MONITOR PC RET STORE
MSTRET	BSS	2	MONITOR ST RET STORE
DWPRET	BSS	2	DIAGNOSIS WP RET STORE
DPCRET	BSS	2	DIAGNOSIS WP RET STORE
DSTRET	BSS	2	DIAGNOSIS WP RET STORE
IWPRET	BSS	2	I/P TASK WP RET STORE
IPCRET	BSS	2	I/P TASK PC RET STORE
ISTRET	BSS	2	I/P TASK ST RET STORE
DWPRET	BSS	2	O/P TASK WP RET STORE
DPCRET	BSS	2	O/P TASK PC RET STORE
DSTRET	BSS	2	O/P TASK ST RET STORE
CWPRET	BSS	2	MCP TASK WP RET STORE
CPCRET	BSS	2	MCP TASK PC RET STORE
CSTRET	BSS	2	MCP TASK ST RET STORE
IDH	BSS	2	IPDHTP ACTIVE FLAG (0=TASK NOT ACTIVE)
MONI	BSS	2	MONITOR TASK ACTIVE FLAG (-1=TASK ACTIVE)
DIAG	BSS	2	DIAGNOSIS TASK ACTIVE FLAG
IPTASK	BSS	2	I/P TASK ACTIVE FLAG
OPTASK	BSS	2	O/P TASK ACTIVE FLAG
MCP	BSS	2	MCP TASK ACTIVE FLAG
MSTIMC	BSS	2	MON STIM COUNT
DSTIMC	BSS	2	DIAG " " "
CSTIMC	BSS	2	MCCP " " "
DPAC	BSS	2	UART O/P ACTIVE FLAG
MSEC	BSS	2	4MS COUNTER
SEC	BSS	2	SECONDS COUNTER
MINUTE	BSS	2	MINUTES COUNTER
HOURS	BSS	2	HOURS COUNTER
PPUIHW	BSS	32	UART WORKSPACE AREA
	END		

GENERAL DATA MODULE G0017D

1. DESCRIPTION

This data module contains software flags which are to be initialised to +1 or -1 by the initialisation program (PPINIP) at system start up time.

2. IDENTIFICATION

GENERAL DATA MODULE G0017D

3. SIZE

CLASS TWO 36 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'GENERAL DATA MODULE G0017D'
♦ GENERAL DATA MODULE IDENTIFIER
        IDT 'G0017D'
        EVEN
♦ CLASS TWO
        DEF MONINT, DIAINT, IPINT
        DEF DFGD, SDELAY, SFP1, SU, SU2, SU3, CMS
        DEF TOG, CLRWT
        DEF DISF, MONSF
        DEF ARTIF, OPINT, MCPINT, MCPIP
        DEF SETONE, SETNEG, SETEND
        RORG
        PSEG
SETONE EQU $           THE FOLLOWING FLAGS ARE INITIALISED TO 1
MONINT BSS 2           MONITOR INTERRUPTED FLAG
DIAINT BSS 2           DIAGNOSIS INTERRUPTED FLAG
IPINT  BSS 2           I/P TASK INTERRUPTED FLAG
OPINT  BSS 2           O/P TASK INTERRUPTED FLAG
MCPINT BSS 2           MCP TASK INTERRUPTED FLAG
TOG    BSS 2           TOGGLE FLAG
DISF   BSS 2           MCP DIAGNOSIS REQUEST FLAG
MONSF  BSS 2           MCP MONITOR REQUEST FLAG
MCPIP  BSS 2           MCP IPTASK REQUEST FLAG
ARTIF  BSS 2           ARTIFACT FLAG
CMS    BSS 2           +1=CONTINUE MONITORING
♦
SETNEG EQU $           THE FOLLOWING FLAGS ARE INITIALISED TO -1
DFGD   BSS 2           -1=NO MONITORING
SDELAY BSS 2           -1=DELAY
SFP1   BSS 2           -1=SEARCH
SU     BSS 2           -1=START UP
SU2    BSS 2           //
SU3    BSS 2           //
CLRWT  BSS 2           CLEAR QRS WIDE & TOTAL FLAG
SETEND EQU $           THIS IS END OF INITIALISED FLAG SECTION
        END

```


GENERAL DATA MODULE G0003D

1. DESCRIPTION

This data module contains the input buffer,
which can store 3 seconds of unfiltered ECG signal.

2. IDENTIFICATION

GENERAL DATA MODULE G0003D

3. SIZE

CLASS THREE 750 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

      TITL 'GENERAL DATA MODULE 60003D'
♦ GENERAL DATA MODULE IDENTIFIER
      IDT '60003D'
      EVEN
♦ CLASS THREE
      DEF IBUF
      RORG
      PSEG
IBUF  BSS  750          INPUT BUFFER FOR 3 SECONDS
♦                                OF SAVED ECG SIGNAL
      END

```

GENERAL DATA MODULE G00040

1. DESCRIPTION

This data module contains, the conditioned signal input buffer (IBP1), the delayed difference signal buffer (DBP1), and the various locations where QRS complex detection and measurement parameters are saved.

2. IDENTIFICATION

GENERAL DATA MODULE G00040

3. SIZE

CLASS TWO 866 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'GENERAL DATA MODULE 60004D'
♦ GENERAL DATA MODULE IDENTIFIER
        IDT '60004D'
        EVEN
♦ CLASS TWO
        DEF IBP1, DBP1, TDP1, NP, RRC, RRSVE, WQRS, AVRR
        DEF POINT
        RORG
        PSEG
IBP1   BSS   752           I/P BUFF
DBP1   BSS   100          DIFF BUFF
TDP1   BSS    2           DIFFERENCE THRESHOLD
NP     BSS    2           NUMBER OF POINTS BELOW THRESHOLD
RRC    BSS    2           RR COUNT
RRSVE  BSS    2           RR SAVE LOCATION
WQRS   BSS    2           QRS WIDTH
AVRR   BSS    2           AVERAGE RR
POINT  BSS    2           ADDRESS POINTER TO QRS
        END

```

GENERAL DATA MODULE G00050

1. DESCRIPTION

This data module contains the monitoring result words MF1 and MF2, monitor workspace area (MONSLW), plus the storage locations of the various parameters calculated by the monitoring task.

2. IDENTIFICATION

GENERAL DATA MODULE G00050

3. SIZE

CLASS TWO 62 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

      TITL 'GENERAL DATA MODULE 60005D'
♦ GENERAL DATA MODULE IDENTIFIER
      IDT '60005D'
      EVEN
♦ CLASS TWO
      DEF MF1, MF2, MONS1W, MINV, MAXV
      DEF MINP, MAXP, T1, T2, T3, W1, W2, DMIND, DMINC
      DEF P2POS, DFSETD
      RDRG
      PSEG
MF1      BSS 2          MONITOR FLAG REG
MF2      BSS 2          ""
MONS1W   BSS 32        MONITOR WORKSPACE AREA
MINV     BSS 2          MIN VALUE
MAXV     BSS 2          MAX ""
MINP     BSS 2          MIN POSITION
MAXP     BSS 2          MAX ""
T1       BSS 2          TOTAL 1
T2       BSS 2          ""
T3       BSS 2          ""
W1       BSS 2          WIDE TOTAL 1
W2       BSS 2          "" "" 2
DMIND    BSS 2          DMIN OLD
DMINC    BSS 2          DMIN CURRENT
P2POS    BSS 2          P2 POSITION
DFSETD   BSS 2          OFF SET OLD
      END

```

GENERAL DATA MODULE G0006D

1. DESCRIPTION

This data module contains the diagnosis workspace area, and diagnosis result words DF1 and DF2.

2. IDENTIFICATION

GENERAL DATA MODULE G0006D

3. SIZE

CLASS TWO 36 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

          TITL 'GENERAL DATA MODULE G0006D'
♦ GENERAL DATA MODULE IDENTIFIER
          IDT 'G0006D'
          EVEN
♦ CLASS TWO
          DEF DIAT1W,DF1,DF2
          RDRG
          PSEG
DIAT1W BSS 32          DIAGNOSIS WORKSPACE AREA
DF1    BSS 2          DIAGNOSIS FLAG
DF2    BSS 2          ''
          END

```


GENERAL DATA MODULE GO018D

1. DESCRIPTION

This data module contains the workspace areas and files used by the Input, Output and MCP tasks.

It should be noted that this must be the last data module in RAM as it contains the end of RAM label RAMEND, used by the initialisation program.

2. IDENTIFICATION

GENERAL DATA MODULE GO018D

3. SIZE

CLASS TWO 206 Bytes.

4. AUTHOR

B.T.V. WARTON.

```

TITL 'GENERAL DATA MODULE G0018D)
♦ GENERAL DATA MODULE IDENTIFIER
  IDT 'G0018D)
  EVEN
♦ CLASS TWO
  DEF IPPTOW,IPFILE,OPPTOW,OPFILE,MCPTOW
  DEF OPDATA,MOTEXT,WID82S,RAMEND
  RORG
  PSEG
IPPTOW BSS 32      INPUT TASK WORKSPACE AREA
IPFILE BSS 52      INPUT FILE
OPPTOW BSS 32      OUTPUT TASK WORKSPACE AREA
OPFILE BSS 52      OUTPUT FILE
MCPTOW BSS 32      MCP WORKSPACE AREA
OPDATA BSS 2       O/P DATA ADDRESS
MOTEXT BSS 2       MONITOR O/P MESSAGE ADDRESS
WID82S BSS 2       % QRS WIDE
RAMEND EQU $       THIS SHOULD BE END OF RAM
END

```

APPENDIX C

ALTERNATIVE PATIENT PROCESSOR PROGRAM LISTING

The programs supplied in this appendix are those required to produce the alternative patient processor software system. They are indicated by the '*' in the following,

PHASE 0, PATIENT ORIGIN = 0000 LENGTH = 1824

	MODULE	NO	ORIGIN	LENGTH
	PMPTVP	1	0000	00A4
	PPINIP	2	00A4	00A0
	PPTHAP	3	0144	00D6
	PPCIHP	4	021A	00EA
	PPUIHP	5	02D4	014C
	IPDHTP	6	0420	01B6
	MONSDP	7	05D6	018A
*	MONS3P	8	0760	024E
*	MONS4P	9	09AE	015C
*	DIAT2P	10	0B0A	00C4
	IPPT0P	11	0BCE	00B0
	DPPT0P	12	0C7E	0082
	MCPT0P	13	0D00	0130
	P0001D	14	0E30	0014
	P0002D	15	0E44	000C
	P0003D	16	0E50	002E
	P0009D	17	0E7E	0018
*	P0010D	18	0E96	006A
	IPDHTD	19	0F00	00C1
	MONTDD	20	0FC2	0020
	G0016D	21	0FE2	007A
	G0017D	22	105C	0024
	G0003D	23	1080	02EE
	G0004D	24	136E	0362
	G0005D	25	16D0	003E
*	G0019D	26	170E	0048
	G0018D)	27	1756	00CE

ALTERNATIVE PATIENT PROCESSOR PROGRAM LABELS

DEFINITIONS

NAME	VALUE	NO	NAME	VALUE	NO	NAME	VALUE	NO	NAME	VALUE	NO
A1	0E34	14	A1DC	0E40	14	A2	0E36	14	A2DC	0E42	14
ACTND	0FEC	21	ALARM1	0EEB	18	ALARM2	0EF0	18	ARTIF	106E	22
ASYST	0EE2	18	AVRR	160C	24	AVRRB	0E62	16	*BEATS	0E70	16
BPM100	0E56	16	BPM110	0E54	16	*BPM120	0E52	16	*BPM140	0E50	16
BPM150	0EFA	18	*BPM20	0E60	16	BPM200	0EFC	18	BPM30	0EF8	18
BPM40	0E5E	16	BPM60	0E5C	16	BPM80	0E5A	16	BPM90	0E58	16
BROAD	0EF2	18	BUFEND	0FDE	19	BUFFER	0F84	19	BUFLEN	0E44	15
C	0E3C	14	*CLRWT	107E	22	CM	0E89	17	CMS	1070	22
CDC1	0E96	18	CDC2	0E9A	18	CDC3	0EA0	18	CDC4	0EA4	18
CDC5	0EAC	18	CDC6	0EAE	18	CDUNT	0E6A	16	CPCRET	101C	21
CSNS	0EF6	18	CSS	0EF4	18	CSTIMC	1030	21	CSTRET	101E	21
CMPRET	101A	21	CZC1	0E98	18	CZC2	0E9C	18	CZC3	0E9E	18
CZC4	0EA2	18	CZC5	0EA6	18	CZC6	0EA8	18	CZC7	0EAA	18
D0T1	0ECA	18	D0T2	0ECC	18	D1T1	0ECE	18	D1T2	0ED0	18
D2T1	0ED2	18	D2T2	0ED4	18	D2T3	0ED6	18	D2T4	0ED8	18
D3T1	0EDA	18	D3T2	0EDC	18	D4T1	0EDE	18	D5T1	0EE0	18
DBP1	165E	24	DBUFL	0E46	15	DF1	172E	26	DF2	1730	26
DFG0	1072	22	DIAG	1024	21	DIAGM	0E80	17	DIARNT	105E	22
DIAT11	0B0A	10	DIAT2W	170E	26	DISF	1068	22	DMINC	1703	25
DMIND	1706	25	DPCRET	100A	21	DRTWP	0FEE	21	DSTIMC	102E	21
DSTRET	100C	21	DMPRET	1008	21	EIGHT	0E08	18	EM	0E88	17
FINISH	0732	7	*FIVE	0E76	16	HOURS	103A	21	HPDP	0F80	19
HUND	0E72	16	IBP1	136E	24	IBUF	1080	23	IDH	1020	21
IPCRET	1010	21	IPDHT1	0420	6	IPDHTW	0F00	19	IPFILE	1776	27
IPINT	1060	22	IPPT01	0BCE	11	IPPT02	0C56	11	IPPT03	0C6C	11
IPPT0W	1756	27	IPRTWP	0FF4	21	IPTASK	1026	21	ISTRET	1012	21
IMPRET	100E	21	K1LP	0E38	14	K2LP	0E3A	14	KDC	0E3E	14
KHP	0E32	14	LEVEL	0E30	14	LPOP	0F82	19	MAXP	16FA	25
MAXV	16F6	25	MCP	102A	21	MCPINT	1064	22	MCP1P	106C	22
MCPT01	0D00	13	MCPT0W	17FE	27	MORTWP	1000	21	MF1	16D0	25
MF2	16D2	25	MFAIL	0E85	17	MINL	0E48	15	MINP	16F8	25
MINUTE	1039	21	MINV	16F4	25	MM1	0E8B	17	MM2	0E8C	17
MM3	0E8D	17	MM4	0E8E	17	MM5	0E8F	17	MM6	0E90	17
MONI	1022	21	MONINT	105C	22	MONS11	0760	8	MONS1W	16D4	25
MONS41	09AE	9	MONSF	106A	22	MONTD1	05D6	7	MONTDW	0FC2	20
MONWR3	0FC3	20	MOTEXT	1820	27	MPCRET	1004	21	MRTWP	0FEB	21
MSEC	1034	21	MSTIMC	102C	21	MSTRET	1006	21	MSUDVE	0E84	17
MMPRET	1002	21	NDRS	0AF2	9	NP	1604	24	*PERAD	0E8A	18
NPTACH	0EEC	18	NDRSB	0E06	18	DFSETD	170C	25	DPAC	1032	21
DPCRET	1016	21	OPDATA	181E	27	OPFILE	17CA	27	DPINT	1062	22
OPPT01	0C7E	12	OPPT0W	17AA	27	OPRTWP	0FFA	21	DPTASK	1028	21
DSTRET	1018	21	OMPRET	1014	21	P2POS	170A	25	PAUSE	0EE4	18
PBEAT	0EE6	18	*PER32	0E78	16	PERCEN	1752	26	PERFLA	1754	26
POINT	16CE	24	PPCIH1	021A	4	PPCIH2	025A	4	PPIN11	00A4	2
PPTHAR1	0144	3	PPTHAW	0FE2	21	PPUIH1	02D4	5	PPUIH2	03B6	5
PPUIH3	030C	5	PPUIH4	03E8	5	PPUIH5	0402	5	PPUIHW	103C	21
PR	0E86	17	PRM	0E7E	17	PS	0E8A	17	PSD	0E82	17
PTACH	0EE8	18	PUART	040C	5	QRSNT	0E7D	16	QRSPT	0E7C	16
QRSWB	0E6E	16	QRSWID	0E6C	16	RAM	0F00	19	RAM2	0F02	19
RAMEND	1824	27	RRBAVR	0788	8	RRBEND	1750	26	RRBUF	1732	26
RRC	1606	24	RR032	0E4A	15	RALB	0E64	16	RRMAXT	0EFE	18
RRSAVE	1608	24	RRSB	0E66	16	SDELAY	1074	22	SEC	1036	21
SEQ1	0EB0	18	SEQ10	0EC2	18	SEQ11	0EC4	18	SEQ2	0EB2	18
SEQ3	0EB4	18	SEQ4	0EB6	18	SEQ5	0EB8	18	SEQ6	0EBA	18
SEQ7	0EDC	18	SEQ8	0EBE	18	SEQ9	0EC0	18	SEQB	0E68	16
SETEND	1030	22	SETNEG	1072	22	SETONE	105C	22	SFP1	1076	22
SIX	0E4E	15	SIXTY	0E94	17	SM	0E87	17	SR250	0E92	17
SU	1078	22	SU2	107A	22	SU3	107C	22	T1	16FC	25
T2	16FE	25	T3	1700	25	TDP1	1602	24	TEN	0E4C	15
*TDG	1066	22	*TWELVE	0E74	16	VALUE	0FC0	19	W1	1702	25
W2	1704	25	WADC	0F60	19	WAHP	0FC0	19	WALP	0F40	19
*WID32S	1822	27	*WID82	0E7A	16	WURS	16CA	24			

MONITOR SEARCH SECTION SYSTEM 2

1. DESCRIPTION

This program module is an alternative program to program module MONS1P. The differences between these two programs are :-

- (1) The start-up procedure of this program calculates the average R-R interval from 16 stored R-R intervals.
- (2) This program does not calculate the percentage of wide QRS complexes.
- (3) Various parameters have been changed to meet the new monitoring requirements.

2. IDENTIFICATION

SUBROUTINE NAME	MONS3
PROGRAM MODULE	MONS3P
GENERAL DATA MODULES	G0003D
GENERAL DATA MODULES	G0004D
GENERAL DATA MODULES	G0005D
GENERAL DATA MODULES	G0018D
PERMANENT DATA MODULES	P0003D
PERMANENT DATA MODULES	P0009D

3. SIZE

PROGRAM MODULE 590 BYTES.

4. CALLS TO SUBROUTINE

B	@MONS11
BL	@RRBAVR

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	MONTPD
B	@FINISH
PROGRAM MODULE	MONS4P
B	@MONS41

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data for this program is the output data from the program module MONTPD; this data being the current estimate of the R-R interval (RRC), and the position of the QRS complex (POINT) in the input buffer (IBP1).

6.2. OUTPUT DATA

The output from this program is the monitoring result word MF1, the individual bits of which are the True/False answers to the tests performed by the program. Also supplied by this program is the true R-R interval measurement, which is placed in RRSAVE.

6.3. ADDITIONAL DATA CHANGES

The software flags that are effected by this program are SFPI, SU2 and SU3.

7. TIMING

The combined execution time of the monitoring modules (MONTPD, MONS3P and MONS4P) does not exceed 3.2mS.

8. AUTHOR

B.T.V. WARTON.

BL	QRRBAVR	GO CALCULAT AVERAGE RR
LI	R9,MSUOVE	GET ADDRESS OF SU OVE MESSAGE
MOV	R9,QMOTEXT	SET O/P ADDRESS
INC	QCSTIMC	STIM MCP
SETD	QMCP	REQUEST MCP
ABS	QSU2	RESET START UP FLAG

◆

◆◆◆◆ SETTING PULSE RATE FLAGS

SU2ND	CLR R8	MF1=R8
	C QAVRR,QBPM30	IS PULSE >30 BPM
	JLE GT80	JUMP IF YES
	C QAVRR,QBPM60	IS PULSE >60 BPM
	JGT LE60	JUMP IF NO
	AI R8,>00E0	SET FLAGS >60
	JMP SD1	
LE60	C QAVRR,QBPM40	IS PULSE >40
	JGT LE40	JUMP IF NO
	AI R8,>00C0	SET FLAGS >40
	JMP SD1	
LE40	EQU \$	
	C QAVRR,QBPM30	IS PULSE >30
	JGT LE20	JUMP IF NO
	AI R8,>00B0	SET FLAGS >20
	JMP SD1	
LE20	AI R8,>0000	SET FLAG <20
	JMP SD1	
GT80	C QAVRR,QBPM90	IS PULSE >90
	JLE GT90	JUMP IF YES
	AI R8,>00F0	SET FLAGS >80
	JMP SD1	
GT90	C QAVRR,QBPM100	IS PULSE >100
	JLE GT100	
	AI R8,>00F8	SET FLAGS >90
	JMP SD1	
GT100	EQU \$	
	C QAVRR,QBPM110	IS PULSE >110
	JLE GT110	
	AI R8,>00FC	SET FLAGS>100
	JMP SD1	
GT110	C QAVRR,QBPM150	IS PULSE >150
	JLE GT150	
	AI R8,>00FE	SET FLAGS >110
	JMP SD1	
GT150	C QAVRR,QBPM200	
	JLE GT200	
	AI R8,>00FF	SET FLAGS >140
	JMP SD1	
GT200	AI R8,>80FF	
SD1	EQU \$	

◆

◆◆◆◆◆ QRS WIDTH SECTION ◆◆◆◆◆

WIDTH	EQU \$	
	SLA R2,1	SHIFT SEQ WIDE REG
	MOV QPOINT,R4	GET POINTER TO QRS POS
	CLR R5	MIN REG
	CLR R9	MAX
	S QCOUNT,R4	POINT-COUNT
	JGT INBUF	
	JEQ INBUF	
	A QBUFLN,R4	ADD BUFFER LENGH TO R4

INBUF	MOVB @IBP1(R4),R5 MOV R4,R6	GET VALUE IN QRS SAVE POS
	CLR R9 MOVB R5,R9 MOV R6,R10 CLR R7	MAX PUT VALUE IN R9 MAX POS COUNTER
QU1	INC R4 C R4,@BUFLN JLE QD3	INC POS POINT IS IT STILL INSIDE BUFFER JUMP IF YES RESET
QD3	CLR R4 CB R5,@IBP1(R4) JLT QD1	IS MIN<THIS VALUE JUMP IF YES
	MOVB @IBP1(R4),R5 MOV R4,R6 JMP Q1	SAVE NEW MIN SAVE NEW POS
QD1	CB R9,@IBP1(R4) JGT Q1	IS VALUE IN R9 > IN BUFFER
	MOVB @IBP1(R4),R9 MOV R4,R10	PUT VALUE IN BUFFER IN R9 SAVE POSITION
Q1	C R4,@MONWR3 JNE QU1	COMPARE WITH CURRENT POS
◆◆◆◆	AT THIS POINT R5=MIN @ R6=POS% R9=MAX%R10=POS	
QD3A	SRA R5,8 MOV R5,@MINV MOV R6,@MINP SRA R9,8 MOV R9,@MAXV MOV R10,@MAXP	MAKE BYTE WORD SAVE MIN SAVE POS MAKE BYTE WORD SAVE MAKE VALUE SAVE MAKE POSITION
QU3	CLR R3 INC R3 C R3,@QRSWID JGT WIDE INC R6 C R6,@BUFLN JLE QD5 CLR R6 C R6,@P2POS	WIDTH REG WIDTH COUNT+1 IS R3 > QRS WIDE WIDTH INC POS IS R6 > BUFFER LENGTH
QD5	JEQ QD5A CB @IBP1(R6),@QRSNT	RESET POS IS R6=CURRENT P2 POSITION
QD5A	JLT QU3 MOV @MINP,R6	TEST IBP1 VALUE FOR SIGN CHANGE JUMP IF STILL -VE GET MIN POS
QU4	INC R3 C R3,@QRSWID JGT WIDE DEC R6 JGT QD6 JEQ QD6 MOV @BUFLN,R6	WIDTH+1 IS R3 > QRS WIDE WIDTH DEC POS. BACKWARD SEARCH
QD6	MOVB @IBP1(R6),R9 JLT QU4	SET R6 TO BUFFER LENGTH TEST IBP1 FOR SIGN CHANGE JUMP IF STILL -VE
QU5	INC R3 C R3,@QRSWID JGT WIDE DEC R6 JGT QD7 JEQ QD7 MOV @BUFLN,R6	WIDTH+1 IS R3 > QRS WIDE WIDTH BACKWARD SEARCH
QD7	CB @IBP1(R6),@QRSPT JGT QU5	SET POS TO BUFLN TEST IBP1 FOR CHANGE IN SIGN JUMP IF STILL +VE
◆	AT THIS POINT R3=WIDTH OF QRS	

```

QU6A  MOV  R3,@MORS
      C    R3,@RRSWID      IS WIDTH NORMAL
      JLE  QRSN            JUMP IF NORMAL
WIDE  SOC  @RRSWB,R3      SET BIT WIDTH=1
      SOC  @SEQB,R2       SET SEQ BIT WIDE
QRSN  EQU  $
♦
♦♦♦♦♦♦♦♦  TRUE R-R SECTION
CALRR  MOV  @P2POS,R13    SET P2 CROSS OVER POINT
      S    @MINP,R13      P2POS-MINP
      JGT  DIFOK
      JEQ  DIFOK
      A    @BUFLN,R13     ANS SHOULD BE +
DIFOK  MOV  @RRSAVE,R14   GET RRSAVE
      A    @DFSETD,R14   RRSAVE+DFSETD
      S    R13,R14       R14=RRC+DFSETD-DFSETN=TRR
      JLT  RRERRO
      MOV  R14,@RRSAVE   REPLACE RRSAVE WITH TRUE RR
      MOV  R13,@DFSETD  REPLACE DFSETD
RRERRO EQU  $
♦
♦♦♦♦♦♦♦♦  TEST FOR CURRENT R-R <600MS
      C    @RRSAVE,@BPM100 IS TRUE RR <600MS
      JGT  LT82
      ORI  R8,>100       SET <600MS BIT
♦
♦♦♦♦♦♦♦♦  START OF 2 X AVRR SECTION ♦♦♦♦♦♦♦♦♦♦
LT82  MOV  @AVRR,R9       GET AVRR
      SLA  R9,1           AVRR X 2
      C    @RRSAVE,R9    IS RRSAVE>=2 X AVRR
      JLT  RRLT          JUMP IF RRSAVE <
      SOC  @AVRRB,R8     SET AVRR BIT=1
♦
♦♦♦♦♦♦♦♦  START OF RR = LONG, SHORT OR NORMAL SECTION ♦♦♦♦♦♦
RRLT  SLA  R0,1          SHIFT SEQ LONG REG
      SLA  R1,1          " " " SHORT REG
      MOV  @PERFLA,@PERFLA IS PERCENTAGE CHANGED
      JNE  PERSET
      LI  R10,15         15 PER
      MOV  R10,@PERCEN  SAVE %
      MOV  @AVRR,R9     GET AVRR
PERSET MPY  @PERCEN,R9   % X AVRR
      DIV  @HUND,R9     AVRR X %/100=R9
      MOV  @AVRR,R10    GET AVRR
      A    R9,R10       AVRR + IER=RR TOLERANCE
      C    @RRSAVE,R10  IS RR TOLERANCE>RRSAVE
      JGT  RRLONG
      S    R9,R10       R9=AVRR
      S    R9,R10       AVRR - IER=RR TOLERANCE
      C    @RRSAVE,R10  IS RRSAVE < RR TOLERANCE
      JNE  SAVEMF       JUMP IF NOT (IE NORMAL RR)
      SOC  @RRSB,R8     SET SHORT BIT=1
      SOC  @SEQB,R1     SET SEQ SHORT BIT=1
      JMP  SAVEMF
RRLONG SOC  @RRLB,R8    SET LONG BIT=1
      SOC  @SEQB,R0     SET SEQ LONG BIT=1
♦
♦♦♦♦♦♦♦♦  SAVE MF1 ♦♦♦♦♦♦♦♦♦♦
SAVEMF EQU  $
      MOV  R8,@MF1      SAVE MF1
      B    @MONS41      GO TO NEXT MONITORING MODULE
      END

```

MONITOR SEQUENCE SEARCH SECTION

SYSTEM 2

1. DESCRIPTION

This program is concerned with testing different sequences of R-R intervals and QRS complex widths, and placing the results in the monitoring word MF2.

At the end of this program is the updating procedures for the parameters DMIN, TDPl and AVRR, and also the procedure for alarming the condition of "no QRS detected".

The differences between this program module, and program module MONS2P is the sequence patterns which are being monitored for, and the procedure for updating AVRR. (The sequence detected by MONS2P are retained in this module, but not used at present by the Diagnosis task (DIAT2P)).

2. IDENTIFICATION

SUBROUTINE NAME	MONS4
PROGRAM MODULE	MONS4P
GENERAL DATA MODULE	G0003D
GENERAL DATA MODULE	G0004D
GENERAL DATA MODULE	G0005D
PERMANENT DATA MODULE	P0002D
PERMANENT DATA MODULE	P0010D

3. SIZE

PROGRAM MODULE 348 Bytes.

4. CALLS TO SUBROUTINE

B	@MONS41
B	@NOQRS

5. CALLS FROM SUBROUTINE

PROGRAM MODULE	MONTDP
B	@FINISH
PROGRAM MODULE	MONS3P
BL	@RRBAVR

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data for this program is supplied in registers R0, R1 and R2 of workspace area MONS1W.

The contents of these registers are :-

- (i) R0 = Long R-R interval sequence bits.
- (ii) R1 = Short R-R interval sequence bits.
- (iii) R2 = Wide QRS complex sequence bits.

6.2. OUTPUT DATA

The output from this program is the Monitoring result word MF2, the individual bits of which indicate which sequence of R-R intervals and QRS widths have been detected.

7. TIMING

The combined execution time of the monitoring modules (MONTDP, MONS3P and MONS4P) does not exceed 3.2mS.

8. AUTHOR

B.T.V. WARTON.

```

TITL 'MONITOR SEQUENCE SEARCH SECTION SYSTEM 2'
* PROGRAMME MODULE IDENT
  IDT 'MONS4P'
* TRANSFER VECTORS OR ENTRIES
  DEF MONS41, WQRS
* CALLED PROGRAM MODULES
  REF MONTDP, MONS3P
  REF FINISH, RRBVR
* LINKED DATA MODULES
  REF G0003D, G0004D, G0005D, P0002D, P0004D
  REF CDC1, CZC1, CDC2, CZC2, CZC3, CDC3, CZC4, CDC4, CZC5
  REF CZC6, CZC7, CDC5, CDC6
  REF SEQ1, SEQ2, SEQ3, SEQ4, SEQ5, SEQ6, SEQ7, SEQ8, SEQ9
  REF MF2, DIAG, DMINC, DMINO, DSTIMC, EIGHT
  REF MF1, WQRSB, QRSMB, SIX, TDP1, TEN
  REF RRC, AVRR, RRSB, RRLB, RRSVE
  REF RRBUF, RRBEND, CSNS, CSS, SEQ10, SEQ11
RORG
PSEG

```

```

***** PROGRAMME *****
* THIS NEXT SECTION SETS SEQUENCE FLAG BITS IN MF2
*
* N O T E
* R0 = LONG SEQUENCE BIT FLAGS
* R1 = SHORT  " " "
* R2 = WQRS  " " "
*****

```

```

MONS41 CLR R8          RESET MF1 REG
*
***** SEQUENCE S - S
  CDC  @CSS,R1          COMPARE FOR S-S
  JNE  SFAILA
  MOV  @SEQ11,R8       SET SEQUENCE BIT FOUND
  JMP  SFAIL
*
***** SEQUENCE S - NS
SFAILA CDC  @CSNS,R1    COMPARE FOR S-NS
  JNE  SFAIL
  MOV  @SEQ10,R8       SET SEQUENCE BIT FOUND
*
***** SEQUENCES 4(S-NS) & 4(S(WQRS)-NS)
SFAIL  CDC  @CDC1,R1    TEST SHORT SEQ S-S-S-S-
  JNE  SFAIL1
  CZC  @CZC1,R1        TEST NOT SHORT -NS-NS-NS-NS
  JNE  RETMF2
  CDC  @CDC1,R2        TEST WQRS W-W-W-W-
  JNE  FOUND1
  CZC  @CZC1,R2        TEST NOT WQRS -NW-NW-NW-NW
  JNE  FOUND1
  MOV  @SEQ2,R8        4(S(W)-NS) FLAG SET IN R8=MF2
  JMP  RETMF2
FOUND1 MOV  @SEQ1,R8    4(S-NS) FLAG SET IN R8=MF2
  JMP  RETMF2
*
***** SEQUENCES 4(S-NS-N) & 4(S(WQRS)-NS-N)
SFAIL1 CDC  @CDC2,R1    TEST SHORT S--S--S--S--
  JNE  SFAIL2
  CZC  @CZC2,R1        TEST NOT SHORT -NSNS-NSNS-NSNS-NSNS
  JNE  SFAIL2
  CZC  @CZC3,R0        TEST NOT LONG --NL--NL--NL--NL

```

```

JNE SFAIL2
CDC @CDC2,R2 TEST WQRS W--W--W--W--
JNE FOUND2
CZC @CZC2,R2 TEST NOT WQRS -NWNW-NWNW-NWNW-NWNW
JNE FOUND2
MOV @SEQ4,R8 SET 4(S(W)-NS-N) FLAG BIT=1
JMP RETMF2
FOUND2 MOV @SEQ3,R8 SET 4(S-NS-N) FLAG BIT=1
JMP RETMF2

```

```

♦
♦♦♦♦♦♦ SEQUENCES S-NS-S & S-S-S(WQRS)
SFAIL2 CDC @CDC3,R1 TEST SHORT S-S
JNE SFAIL3
CZC @CZC4,R1 TEST NOT SHORT -NS-
JNE FAIL6
MOV @SEQ5,R8 SET S-NS-S FLAG BIT =1
JMP RETMF2
FAIL6 CDC @CDC5,R2 TEST WQRS --W
JNE SFAIL3
CZC @CZC5,R2 TEST NOT WQRS NWNW-
JNE SFAIL3
MOV @SEQ7,R8 SET S-S-S(W) FLAG BIT=1
JMP RETMF2

```

```

♦
♦♦♦♦♦♦ SEQUENCES S-NS-N-NL & S-NS-N-L
SFAIL3 CDC @CDC4,R1 TEST SHORT S---
JNE SFAIL4
CZC @CZC5,R1 TEST NOT SHORT -NSNS-
JNE SFAIL4
CZC @CZC6,R0 TEST NOT LONG --NLNL
JNE SFAIL5
MOV @SEQ6,R8 SET S-NS-N-NL FLAG=1
JMP RETMF2
SFAIL5 CZC @CZC7,R0 TEST NOT LONG --NL-
JNE SFAIL4
CDC @CDC5,R0 TEST LONG ---L
JNE SFAIL4
MOV @SEQ9,R8 SET S-NS-N-L FLAG BIT=1
JMP RETMF2

```

```

♦
♦♦♦♦♦♦ SEQUENCE S-NS-L
SFAIL4 CDC @CDC6,R1 TEST SHORT S--
JNE RETMF2
CZC @CZC7,R1 TEST NOT SHORT -NS-
JNE RETMF2
CDC @CDC5,R0 TEST LONG --L
JNE RETMF2
MOV @SEQ8,R8 SET S-NS-L FLAG BIT=1
RETMF2 MOV R8,@MF2 SAVE MF2

```

```

♦
♦♦♦♦♦♦ FINDING NEW DMIN & TD IF NEEDED
MOV @MF1,R9 GET MF1
CDC @QRSMB,R9 TEST WQRSIN MF1
JEQ AVRUD NO UP DATE
MOV @DMINO,R9 GET DMIN OLD
ABS R9 MAKE R9 +VE
JLT PD1
JEQ PD1
BL @DMINER GO TO DMIN ERROR
PD1 MPY @EIGHT,R9 DMINO X 8=R9&R10

```

SCR2.TASK.S.MONS4P 17:02:05 THURSDAY, OCT 19, 1978.

	DIV	@TEN,R9	R9&R10 / 10=DMINX0.8=R9
	MOV	R9,R8	R8=DMINO X 0.8
	MOV	@DMINC,R10	GET DMIN CURRENT
	ABS	R10	MAKE R10 +VE
	JLT	PD2	
	JEQ	PD2	
	BL	@DMINER	GO TO DMIN ERROR
PD2	SLA	R10,1	DMIN CURRENT X 2
	CLR	R9	
	DIV	@TEN,R9	R9=DMIN CURRENT X0.2
	A	R9,R8	R8=NEW DMINO
	MOV	R8,R9	
	MPY	@SIX,R9	R9 X 6
	DIV	@TEN,R9	R9= +TD
	NEG	R9	R9= -TD
	MOV	R9,@TDP1	LOAD NEW TD
	NEG	R8	MAKE R8 -VE
	MOV	R8,@DMINO	LOAD NEW DMINO

◆◆◆◆◆◆◆◆ AVRR UPDATE SECTION

AVRUD	MOV	@MF1,R9	GET MF1
	CDC	@RRSB,R9	WAS RR SHORT
	JEQ	NUD	
	CDC	@RRLB,R9	WAS IT LONG
	JEQ	NUD	
	MOV	@RRSAVE,@R15+	SAVE RRSAVE IN RR BUFFER
	CI	R15,RRBEND	IS IT THE END OF BUFFER
	JLE	GOSUM	
	LI	R15,RRBUF	RESET TO START OF BUFF
GOSUM	BL	@RRBAVR	GO TO AVERAGE RR SUB
NUD	JMP	STIM	
DMINER	RT		

◆ INSERT HERE ERROR SECTION FOR +DMIN'S

◆◆◆◆◆◆◆◆ NO QRS SECTION

NOQRS	MOV	@MF1,R9	GET MF1
	SOC	@NQRSB,R9	SET NOQRS BIT=1
	MOV	R9,@MF1	RET MF1
STIM	INC	@DSTIMC	INC DIAG STIM COUNT
	SETD	@DIAG	SET DIAG F L A G
	B	@FINISH	GO TO FINISH
	END		

DIAGNOSIS PROGRAM SYSTEM 2

1. DESCRIPTION

This program is concerned with using an alternative approach to diagnose arrhythmias, using the results supplied by the monitoring modules MONS3P and MONS4P.

2. IDENTIFICATION

SUBROUTINE NAME	DIAT2
PROGRAM MODULE	DIAT2P
GENERAL DATA MODULE	G0002D
GENERAL DATA MODULE	G0005D
GENERAL DATA MODULE	G0006D
GENERAL DATA MODULE	G0019D
PERMANENT DATA MODULE	P0005D
PERMANENT DATA MODULE	P0010D

3. SIZE

PROGRAM MODULE 196 Bytes.

4. CALLS TO SUBROUTINE

BLWP @DIAT11

5. INTERNAL DATA TRANSFERS

5.1. INPUT DATA

The input to this program are the monitoring words MF1 and MF2.

5.2. OUTPUT DATA

The output data from this program is placed in locations DF1 and DF2.

5.3. ADDITIONAL DATA CHANGES

The flags that may be effected by the execution of this program are :-

DISF, MCP, CSTIMC, DSTIMC and DIAG.

6. TIMING

The execution time of this program will not exceed 0.2mS.

7. AUTHOR

B.T.V. WARTON.

PERMANENT DATA MODULE PO0100

1. DESCRIPTION

This data module contains the comparison words used by the monitoring module MONS4P, to detect various sequences of R-R interval and QRS complex widths. Also included in this module are the comparison words used by the diagnosis program DIAT2P, along with the words used when setting the different diagnosis bits etc. in DF1.

2. IDENTIFICATION

PERMANENT DATA MODULE PO0100

3. SIZE

106 Bytes.

4. AUTHOR

B.T.V. WARTON.

```

TITL 'PERMANENT DATA MODULE P0010D'
♦ PERMANENT DATA MODULE IDENTIFIER
IDT 'P0010D'
EVEN
DEF CDC1,CDC2,CDC3,CDC4,CDC5,CDC6
DEF CZC1,CZC2,CZC3,CZC4,CZC5,CZC6,CZC7
DEF SEQ1,SEQ2,SEQ3,SEQ4,SEQ5,SEQ6,SEQ7
DEF SEQ8,SEQ9,SEQ10,SEQ11
DEF NORSB,EIGHT
DEF DOT1,DOT2,D1T1,D1T2
DEF D2T1,D2T2,D2T3,D2T4,D3T1,D3T2
DEF D4T1,D5T1
DEF ASYST,PAUSE,PBEAT,PTACH,NPBRAD,NPTACH
DEF ALARM1,ALARM2,BROAD
DEF BPM30,BPM150,BPM200,RRMAXT,CSS,CSNS
RORG
PSEG
CDC1 DATA >00AA 4(S-NS) & 4(S(W)-NS)
CZC1 DATA >0055 ''
CDC2 DATA >0924 4(S-NS-N) & 4(S(W)-NS-N)
CZC2 DATA >06DB ''
CZC3 DATA >0249 ''
CDC3 DATA >0005 S-NS-S
CZC4 DATA >2 ''
CDC4 DATA >8 S-NS-N-NL
CZC5 DATA >6 ''
CZC6 DATA >3 ''
CZC7 DATA >2 S-NS-N-L
CDC5 DATA >1 ''
CDC6 DATA >4 S-NS-L
SEQ1 DATA >1 4(S-NS)
SEQ2 DATA >2 4(S(W)-NS)
SEQ3 DATA >4 4(S-NS-N)
SEQ4 DATA >8 4(S(W)-NS-N)
SEQ5 DATA >10 S-NS-S
SEQ6 DATA >20 S-NS-N-NL
SEQ7 DATA >40 3S-W
SEQ8 DATA >80 S-NS-L
SEQ9 DATA >100 S-NS-N-L
SEQ10 DATA >200 S-NS
SEQ11 DATA >400 S-S
NORSB DATA >0200 NO QRS BIT
EIGHT DATA 8 CONSTANT
DOT1 DATA >00FC DIAGNOSIS 0 TEST 1
DOT2 DATA >0001 DIAGNOSIS 0 TEST 2
D1T1 DATA >0080 DIAGNOSIS 1 TEST 1
D1T2 DATA >007F DIAGNOSIS 1 TEST 2
D2T1 DATA >0100 DIAGNOSIS 2 TEST 1
D2T2 DATA >0400 DIAGNOSIS 2 TEST 2
D2T3 DATA >2000 DIAGNOSIS 2 TEST 3
D2T4 DATA >8000 DIAGNOSIS 2 TEST 4
D3T1 DATA >0200 DIAGNOSIS 3 TEST 1
D3T2 DATA >2000 DIAGNOSIS 3 TEST 2
D4T1 DATA >0400 DIAGNOSIS 4 TEST 1
D5T1 DATA >0200 DIAGNOSIS 5 TEST 1
ASYST DATA >0020 ASYSTOLE
PAUSE DATA >0010 PAUSE
PBEAT DATA >0008 PREMATURE BEAT
PTACH DATA >0004 PAROXYSMAL TACHYCARDIA
NPBRAD DATA >0002 NONE PAROXYSMAL BRADYCARDIA
NPTACH DATA >0001 NONE PAROXYSMAL TACHYCARDIA
ALARM1 DATA >8000 ALARM LEVEL 1 BIT

```

ALARM2 DATA >4000
BROAD DATA >2000
CSS DATA 3
CSNS DATA 2
BPM30 DATA 500
BPM150 DATA 100
BPM200 DATA 75
RRMAXT DATA 1250
END

ALARM LEVEL 2 BIT
BROAD QRS BIT
S-S
S-NS
30 BEATS / MIN
150 BEATS / MIN
200 BEATS / MIN
RR INTERVAL MAX

GENERAL DATA MODULE G0019D

1. DESCRIPTION

This data module contains the workspace area (DIAT2W) used by the diagnosis task, along with the locations where the diagnosis results words DF1 and DF2 are stored.

2. IDENTIFICATION

GENERAL DATA MODULE G0019D

3. SIZE

72 Bytes.

4. AUTHOR

B.T.V. WARTON.

```

      TITL 'GENERAL DATA MODULE 60019D'
♦ GENERAL DATA MODULE IDENTIFIER
      IDT '60019D'
      EVEN
♦ CLASS TWO
      DEF DIAT2W,DF1,DF2
      DEF RRBUF,RRBEND,PERCEN,PERFLA
DIAT2W BSS 32          DIAGNOSIS TASK WA
DF1    BSS 2          DIAGNOSIS FILE WORD 1
DF2    BSS 2          DIAGNOSIS FILE WORD 2
RRBUF  BSS 30        RR BUFFER
RRBEND BSS 2         RR BUFFER END
PERCEN BSS 2         PERCENTAGE
PERFLA BSS 2         PERCENTAGE CHANGE FLAG
      END

```


APPENDIX D

OPERATOR/NURSE PROCESSOR PROGRAM LISTING

All the programs and data modules required to produce the operator/nurse processor software system, are supplied in this appendix, in the order in which they appear in the link editor listing shown below.

PHASE 0, NURSE DRIGIN = 0000 LENGTH = 1034

MODULE	NO	DRIGIN	LENGTH
NSPTVP	1	0000	00A4
NSPIOP	2	00A4	009E
NSTHAP	3	0142	00BC
NIDQHP	4	01FE	00A2
NSUIHP	5	02A0	0202
NSPITP	6	04A2	0112
NSPOTP	7	05B4	011C
MOCPTP	8	06D0	0246
BIHEXP	9	0916	0040
ASCIIP	10	0956	0064
VDUIOP	11	09BA	00F8
P0007D	12	0AB2	000A
P0008D	13	0ABC	01B8
60009D	14	0C74	004A
60010D	15	0CBE	000E
60011D	16	0CCC	0048
60012D	17	0D14	01F8
60013D	18	0F0C	0028
60014D	19	0F34	003F
60015D	20	0F74	00C0

OPERATOR/NURSE PROCESSOR PROGRAM LABELS

D E F I N I T I O N S

NAME	VALUE	NO	NAME	VALUE	NO	NAME	VALUE	NO	NAME	VALUE	NO
ASCDAT	0AD4	13	ASCI11	0956	10	ASCNUM	0AD0	13	BIHEX1	0916	9
BUFA	0FDC	20	CL	0ABA	12	CM	0AC0	13	CP	0ABB	12
CR	0AB9	12	CR1712	0AB2	12	EM	0ABE	13	EOB	0AB3	12
ERRDR1	0AEF	13	FREE	1032	20	HEXONE	0AC6	13	HUND	0ACC	13
IHWAI	0D14	17	IHWAI2	0DB0	17	IHWAI3	0E64	17	INPUT	0A50	11
IDTF	1030	20	IDWAI	0D34	17	IDWAI2	0DDC	17	IDWAI3	0E34	17
IPFI1S	0D3A	17	IPFI2S	0E32	17	IPFI3S	0EDA	17	IPFIL1	0D89	17
IPFIL2	0E30	17	IPFIL3	0ED8	17	IPINT	0CC6	15	IPLIST	0AE4	13
IPPORT	0CAE	14	IPQS	0CEC	16	IPRTWP	0C92	14	IPSF	0CBC	14
IPSTIM	0CB2	14	IPSTRT	0CB0	14	IPRTINT	0CBE	15	IPWPT	0CAC	14
ITPCRT	0C96	14	ITRTWP	0C7A	14	ITSTRT	0C99	14	ITWPT	0C94	14
LINE	0AB6	12	MCP1P	0CBA	14	MINUS	0AD2	13	MDCINT	0CC2	15
MDCP	0CB6	14	MDCPSC	0CB8	14	MDCPT1	06D0	8	MDCPTW	0F34	19
MTPCRT	0CA2	14	MTRTWP	0C86	14	MTSTRT	0CA4	14	MTWPT	0CA0	14
NDF1	0F54	19	NDF11	0F5E	19	NDF2	0F56	19	NDF22	0F62	19
NEXTIP	0D10	16	NEXTDP	0D12	16	NIDQH1	01FE	4	NIDQH2	0256	4
NIDQH3	0226	4	NIDQH4	027C	4	NIDQHW	00CC	16	NMF1	0F5A	19
NMF11	0F6B	19	NMF2	0F5C	19	NMF22	0F6F	19	NPR	0F59	19
NPR1	0F66	19	NSPI01	00A4	2	NSPIDW	0F0C	18	NSPIT1	04A2	6
NSPDT1	05B4	7	NSTHA1	0142	3	NSTHAM	0C74	14	NSUIH1	02A0	5
NSUIH2	03F0	5	NSUIH3	03FE	5	NSUIH4	041E	5	DPBYTE	059C	6
DPERR	0C5E	13	DPFIL1	0D54	17	DPINT	0CC4	15	DPM1	0B0F	13
DPM10	0C0B	13	DPM11	0C26	13	DPM12	0C4F	13	DPM2	0B1E	13
DPM3	0B34	13	DPM4	0B5C	13	DPM5	0B70	13	DPM6	0B83	13
DPM7	0B9B	13	DPM8	0BE3	13	DPM9	0BF9	13	DPPCRT	0CA8	14
DPQS	0CFC	16	DPRAM	102C	20	DPRDM	102E	20	DPRTWP	0C9C	14
DPSTIM	0CB4	14	DPSTRT	0CAA	14	DPTEXT	0B00	13	DPTINT	0CC0	15
DPWPT	0CA6	14	DTPCRT	0C9C	14	DTRTWP	0C80	14	DTSTRT	0C9E	14
DTWPT	0C9A	14	PR	0AC2	13	PS	0AC4	13	PUART	040A	5
QIPN	0D0C	16	QDPN	0D0E	16	QUELEN	0AC8	13	RAM	0C74	14
RAM2	0C76	14	RAMEND	1034	20	RDR872	0AB4	12	RDMRAM	0CC8	15
SETEND	0CCC	15	SETIME	059E	6	SETNEG	0CC8	15	SETONE	0CBE	15
SETPC	0F2E	18	SETPC1	0F32	18	SETWP	0F2C	18	SETWP1	0F30	18
SM	0ABC	13	SPACE	0AD3	13	TASKAN	0C7E	14	TEN	0ACA	13
THDU	0ACE	13	VDUF	0CDA	15	VDUID1	09BA	11	VDUID2	09BE	11
VDUIDW	0F74	20	VDUDBA	0FB4	20	VDUIDW	0F94	20			

NURSE STATION PROCESSOR TRANSFER

VECTOR PROGRAM MODULE

1. DESCRIPTION

This program module defines the interrupt and XOP transfer vectors used by the Nurse Station Processor. Interrupt level 2 and XOP level 15 have been initialised to their appropriate values for the 990/4 Monitor Software.

2. IDENTIFICATION

SUBROUTINE NAME	NSPTV
PROGRAM MODULE	NSPTVP
GENERAL DATA MODULE	G0012D

3. SIZE

PROGRAM MODULE	164	Bytes.
----------------	-----	--------

4. CALLS FROM SUBROUTINE

INTERRUPT LEVEL	0	NSPI01
INTERRUPT LEVEL	3	NSUIH1
INTERRUPT LEVEL	4	NSUIH1
INTERRUPT LEVEL	5	NSUIH1

5. AUTHOR

B.T.V. WARTON.

TITL 'NURSE STATION PROCESSOR TRANSFER VECTOR PROGRAM MODULE'

◆ PROGRAM MODULE IDENTIFIER
IDT 'NSPTVP'
◆ CALLED PROGRAM MODULES
REF NSPI0P,NSUIHP
REF NSPI01,NSUIH1
◆ LINKED DATA MODULES
REF IHWA1,IHWA2,IHWA3
RORG
PSEG

◆◆◆◆◆◆◆◆◆◆ P R O G R A M M E ◆◆◆◆◆◆◆◆◆◆

DATA IHWA1,NSPI01	INTERRUPT 0
DATA 0,0	1
DATA 0,>5D26	2 REQUIRED BY MONITOR
DATA IHWA3,NSUIH1	3
DATA IHWA2,NSUIH1	4
DATA IHWA1,NSUIH1	5
DATA 0,0,0,0,0,0,0,0,0,0,0	6 TO 10
DATA 0,0,0,0,0,0,0,0,0,0,0	11 TO 15
DATA 0,0,0,0,0,0,0,0,0,0,0	XOP TRANSFER VECTORS
DATA 0,0,0,0,0,0,0,0,0,0,0	XOP TRANSFER VECTORS
DATA 0,0,0,0,0,0,0,0,0,0,0	XOP TRANSFER VECTORS
DATA >77D2,>604E	XOP 15 FOR MONITOR
BSS 32	WORKSPACE FOR MONITOR
ENTRY1 BLWP 30	EMULATE INT 0
END ENTRY1	

NURSE STATION PROCESSOR INITIALISATION PROGRAM

1. DESCRIPTION

This program runs at system start-up time to initialise the contents of RAM. The initialisation that is performed is as follows :-

- (1) Clearing of all RAM used.
- (2) Initialisation of software flags to +1 or -1 as required.
- (3) Initialisation of workspace register contents as required.
- (4) Initialisation of hardware, i.e. programming of UART's etc.

2. IDENTIFICATION

SUBROUTINE NAME	NSPIO
PROGRAM MODULE	NSPIOP
GENERAL DATA MODULES	G0009D
GENERAL DATA MODULES	G0010D
GENERAL DATA MODULES	G0012D
GENERAL DATA MODULES	G0015D

3. SIZE

PROGRAM MODULE	158	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

INTERRUPT LEVEL	0	NSPI01
-----------------	---	--------

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	NSTHAP
BLWP	@NSTHA1

SUBROUTINE NAME	VDUIOP
BLWP	@VDUIO1
SUBROUTINE NAME	NSUIHP
BL	@PUART

6. AUTHOR

B.T.V. WARTON.

```

        TITL 'NURSE STATION PROCESSOR INITIALISATION PROG'
♦ PROGRAMME MODULE IDENT
        IDT 'NSPIOP'
♦ TRANSFER VECTORS OR ENTRIES
        DEF NSPI01
♦ CALLED PROGRAM MODULES
        REF VDUIOP,NSTHAP,NSUIHP
        REF VDUIO1,NSTHA1,PUART
♦ LINKED DATA MODULES
        REF G0009D,G0010D,G0012D,G0015D
        REF RAM,RAM2,RAMEND,SETONE,SETNEG,SETEND
        REF IHWA1,IDWA1,OPTEXT,VDUOBA,NSTHAW
        REF IHWA2,IDWA2
        REF IHWA2,IDWA2
        REF IHWA3,IDWA3
        RORG
        PSEG

```

♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦

```

NSPI01 LWPI RAM          LOAD WP AT START OF RAM
        LI R0,RAM2      GET ADDRESS OF SECOND RAM WORD
CLEAR  CLR  *R0+        CLEAR RAM
        CI R0,RAMEND    IS IT END OF RAM
        JNE CLEAR
        LI R0,SETONE    GET SET ONE FLAG ADDRESS
SET     INC  *R0+        SET FLAGS TO +1
        CI R0,SETNEG    IS IT END OF +1 FLAG SECTION
        JNE SET
SET1    SETD *R0+       SET FLAGS TO -1
        CI R0,SETEND    IS IT END OF -1 FLAG SECTION
        JNE SET1

```

♦♦♦♦♦♦♦♦ UART 1 WA INITIALISATION

```

        LWPI IHWA1      LOAD INT HANDLER WP
        LI R6,IDWA1     I/P O/P WA
        LI R12,>1880    UART CRU BASE
        BL  *PUART      GO PROGRAM UART
        LWPI IDWA1      GET I/P O/P WP
        LI R10,IHWA1    LOAD R10 WITH IHWA1 ADDRESS
        LI R12,>1880    UART CRU BASE

```

♦♦♦♦♦♦♦♦ UART 2 WA INITIALISATION

```

        LWPI IHWA2      LOAD INT HANDLER WP
        LI R6,IDWA2     I/P O/P WA
        LI R12,>1900    UART CRU BASE
        BL  *PUART      GO PROGRAM UART
        LWPI IDWA2      LOAD I/P O/P WP
        LI R10,IHWA2    LOAD R10 WITH IHWA2 ADDRESS
        LI R12,>1900    LOAD UART CRU BASE

```

♦♦♦♦♦♦♦♦ UART 3 WA INITIALISATION

```

        LWPI IHWA3      LOAD INT HANDLER WP
        LI R6,IDWA3     I/P O/P WA
        LI R12,>1840    UART CRU BASE
        BL  *PUART      GO PROGRAM UART
        LWPI IDWA3      LOAD I/P O/P WP
        LI R10,IHWA3    LOAD R10 WITH IHWA3 ADDRESS
        LI R12,>1840    LOAD UART CRU BASE

```

♦♦♦♦♦♦♦♦ O/P SYSTEM READY MESSAGE & INITIALISE HARDWARE

```

        LWPI NSTHAW     LOAD TASK HANDLER WP
        LI R0,OPTEXT    GET O/P TEXT ADDRESS
        MOV R0,VDUOBA   SAVE ADDRESS AT VDUOBA
        BLWP *VDUIO1    GOTO VDU PROG
        CLR R0

```

SCR2.PROG.S.NSPIOP 12:26:00 FRIDAY, OCT 20, 1978.

```
      CLR  RAM
      LI   R12,>100          LOAD 9901 CRU BASE
***** ENABLING UART INTERRUPTS
      SBD  3          ENABLE INT 3
      SBD  4          ENABLE INT 4
      SBD  5          ENABLE INT 5
UP    BLWP 0NSTHA1     GO TO TASK HANDLER
      JMP  UP
      END
```


NURSE STATION PROCESSOR TASK HANDLER

1. DESCRIPTION

This program is concerned with scheduling active tasks in their order of priority. Before this program passes control to the highest priority active task, it tests whether the task is in the suspended state. If this is found to be the case, control is passed back to the task at the point at which it was interrupted. If the task is not in the suspended state, control is passed to it at its starting point.

2. IDENTIFICATION

SUBROUTINE NAME	NSTHA
PROGRAM MODULE	NSTHAP
GENERAL DATA MODULES	G0009D
GENERAL DATA MODULES	G0010D
GENERAL DATA MODULES	G0015D

3. SIZE

PROGRAM MODULE	188	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

BLWP	@NSTHA1.
------	----------

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	NSPITP
BLWP	@NSPIT1
SUBROUTINE NAME	NSPOTP
BLWP	@NSPOT1
SUBROUTINE NAME	MOCPTP
BLWP	@MOCPT1

SUBROUTINE NAME	VDUIOP
BLWP	@VDUIO1
BLWP	@INPUT

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data to this program is the task active and interrupt software flags,

IPSTIM, OPSTIM, MOCP, IOTF,
IPTINT, OPTINT, MOCINT, IPINT, OPINT.

6.2. OUTPUT DATA

The output data from this program is the task active number, which is placed in R5 of workspace area NSTHAW, and which can be referred to as TASKAN.

7. EXTERNAL DATA TRANSFERS

PERIPHERAL CRU INTERFACE

7.1. OUTPUT (TEST FACILITY)

CRU BASE ADDRESS		>1DE0
CRU LINE	0	INPUT TASK ACTIVE
CRU LINE	1	OUTPUT TASK ACTIVE
CRU LINE	2	MOCP TASK ACTIVE

8. TIMING

The execution time of this program is not in excess of 0.2mS.

9. AUTHOR

B.T.V. WARTON.

```

    TITL 'NURSE STATION PROCESSOR TASK HANDLER'
♦ PROGRAMME MODULE IDENT
    IDT 'NSTHAP'
♦ TRANSFER VECTORS OR ENTRIES
    DEF NSTHA1
♦ CALLED PROGRAM MODULES
    REF NSPITP,NSPOTP,MOCPTP,VDUIOP
    REF NSPIT1,NSPOT1,MOCPT1,INPUT,VDUIO1
♦ LINKED DATA MODULES
    REF 60009D,60010D,60015D
    REF NSTHAW,ITRTWP,OTRTWP,MTRTWP,IPRTWP,OPRTWP
    REF IPSTIM,OPSTIM,MOCPT,IPTINT,OPTINT,MOCINT,IPINT
    REF OPINT,IOTF
    RORG
    PSEG

```

♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦

```

NSTHA1 DATA NSTHAW, START
START CLR R5 RESET TASK NUMBER
      LIM1 7 OPERATING SYSTEM TEST IF UART ACTIVE
      LIM1 0 OPERATING SYSTEM PRIVILEGE INT MASK
      LWPI NSTHAW LOAD TASK HANDLER WP
      LI R12,>1DE0 LOAD TASK ACTIVATION CRU BASE
      MOV @IPSTIM,R0 IS I/P TASK ACTIVE
      JNE BIPT
      MOV @OPSTIM,R0 IS O/P TASK ACTIVE
      JNE BOPT
      MOV @MOCPT,R0 IS MOCPT TASK ACTIVE
      JNE BMOCPT
      MOV @IOTF,R0 VDU O/P ACTIVE
      JNE BVDUOP
      LI R5,5 SET TASK ACTIVE NUMBER TO 4
      ABS @IPINT WAS VDU I/P INTERRUPTED
      JGT BIP
      LWPI IPRTWP LOAD WP FOR VDU I/P TASK RETURNS
      RTWP
BIP LIM1 7 UNMASK ALL INTERRUPTS
   BLWP @INPUT GO TO VDU I/P TASK
   JMP START
BIPT LI R5,1 SET TO TASK 1
     ABS @IPTINT WAS I/P TASK INTERRUPTED
     JGT BIPT1 JUMP IF NO
     LWPI ITRTWP LOAD WP FOR INPUT TASK RETURNS
     RTWP
BIPT1 LIM1 7 UNMASK ALL INTS
      SB0 0 SET I/P TASK ACTIVE CRU BIT
      BLWP @NSPIT1 GO TO INPUT TASK
      SBZ 0 RESET I/P TASK ACTIVE CRU BIT
      JMP START
BOPT LI R5,2 SET TO TASK 2
     ABS @OPTINT WAS O/P TASK INTERRUPTED
     JGT BOPT1
     LWPI OTRTWP LOAD WP FOR OUTPUT TASK RETURNS
     RTWP RET TO INTERRUPTED TASK
BOPT1 LIM1 7 UNMASK ALL INTS
      SB0 1 SET O/P TASK ACTIVE CRU BIT
      BLWP @NSPOT1 GO TO OUTPUT TASK
      SBZ 1 RESET O/P TASK ACTIVE CRU BIT
      JMP START

```

SCR2.TASK.S.NSTHAP 12:31:04 FRIDAY, OCT 20, 1978.

```
BMOCP  LI  R5,3          SET TO TASK 3
        ABS  @MOCINT     WAS MOCP INT
        JGT  BMOCP1
        LWPI MTRTWP      LOAD WP FOR MOCP TASK RETURNS
        RTWP             RET TO INTERRUPTED TASK
BMOCP1  LIM1 7          UNMASK ALL INTS
        SBO  2          SET MCP ACTIVE CRU BIT
        BLWP @MOCPT1    GO TO MOCP TASK
        SBZ  2          RESET MCP ACTIVE CRU BIT
        JMP  START
BVDUOP  LI  R5,4          SET TO TASK 4
        ABS  @OPINT     WAS VDU O/P INTERRUPTED
        JGT  BOP
        LWPI OPRTWP      LOAD WP FOR VDU O/P TASK RETURNS
        RTWP             RET TO INTERRUPTED TASK
BOP     LIM1 7          UNMASK ALL INTS
        BLWP @VDUID01   GO TO VDU OUTPUT TASK
        JMP  START
        END
```

NURSE STATION I/O QUEUE HANDLER

1. DESCRIPTION

This program is concerned with placing the various inter-processor communications UARTs in input or output queues as required, and activating the input and output tasks accordingly. The program then when requested, supplies the next UART in the input queue to the input task or, the next UART in the output queue to the output task.

If the program finds that there are no more UARTs in the input queue, the input task is de-activated, and similarly if there are no more UARTs in the output queue, the output task is de-activated.

2. IDENTIFICATION

SUBROUTINE NAME	NIOQH
PROGRAM MODULE	NIOQHP
GENERAL DATA MODULE	G0009D
GENERAL DATA MODULE	G0011D
PERMANENT DATA MODULE	P0008D

3. SIZE

PROGRAM MODULE	162	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

B	@NIOQH1
B	@NIOQH2
B	@NIOQH3
B	@NIOQH4

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	NSTHAP
BLWP	@NSTHA1

SUBROUTINE NAME	NSUIHP
(SEE PROGRAM)	NSUIH3

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data to this program is supplied in locations QIPN and QOPN, where :-

QIPN = workspace area address to be placed in the input queue, to be used later by the input task. Register R12 in this workspace contains the CRU base address for the UART to be used.

QOPN = workspace area address to be placed in output queue, to be used later by the output task. Register R12 in this workspace contains the CRU base address for the UART to be used.

6.2. OUTPUT DATA

The output data from this program is placed in locations NEXTIP and NEXTOP where :-

NEXTIP = the address of the next workspace area to be used by the Input Task.

NEXTOP = the address of the next workspace area to be used by the Output Task.

6.3. ADDITIONAL DATA CHANGES

The values supplied to this program at location QIPN and QOPN are placed in the queues IPQS and OPQS respectively.

The program also sets flags IPSTIM and OPSTIM to activate the Input Task or Output Task as required.

7. TIMING

The execution time of this program will not exceed 0.15ms.

8. AUTHOR

B.T.V. WARTON.

```

TITL 'NURSE STATION I/O QUEUE HANDLER'
♦ PROGRAMME MODULE IDENT (PROG)
  IDT 'NIDQHP'
♦ TRANSFER VECTORS OR ENTRIES
  DEF NIDQH1,NIDQH2,NIDQH3,NIDQH4
♦ CALLED PROGRAM MODULES
  REF NSTHAP,NSUIHP
  REF NSTHA1,NSUIH3
♦ LINKED DATA MODULES
  REF G0011D,G0009D,P0003D
  REF NIDQHW,QIPN,IPQS,NEXTIP,QUELEN,IPSTIM
  REF OPSTIM,QOPN,QPOS,NEXTOP
  RORG
  PSEG

```

♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦

```

♦♦♦♦♦♦ INPUT QUEUE SECTION
NIDQH1 LWPI NIDQHW           I/O QUEUE HANDLER WA
        MOV  @QIPN,@IPQS(R2)  PUT NUMBER IN QUEUE
        INCT R2              INC TO NEXT LOCATION IN QUEUE
        C    R2,@QUELEN      IS R2 = QUEUE LENGTH
        JLE  SETIP
        CLR  R2              RESET POINTER
SETIP   MOV  @IPSTIM,R7      IS IPTASK ACTIVE
        JNE  OUT
        SETD @IPSTIM        STIM I/P TASK
        MOV  @IPQS(R1),@NEXTIP GET NEXT I/P UART WA
OUT     BLWP @NSTHA1        GO TO YASK HANDLER
♦

```

```

♦♦♦♦♦♦ ENTRY TO QUEUE HANDLER TO GET NEXT I/P
NIDQH3 LWPI NIDQHW           LOAD QUEUE WP
        MOV  @IPQS(R1),R13    SAVE LAST IDWA
        INCT R1              TO NEXT IN QUEUE
        C    R1,@QUELEN      IS R1=QUEUE LENGTH
        JLE  R1OK
R1OK    CLR  R1              RESET POINTER
        C    R1,R2           IS START=END
        JNE  GETIP
        CLR  @IPSTIM         DEACTIVATE I/P TASK
        CLR  @NEXTIP        RESET NEXT I/P REG
        JMP  ST
GETIP   MOV  @IPQS(R1),@NEXTIP GET NEXT I/P IN QUEUE
ST      RI   R13,-32        CAL UART WA
        LI   R14,NSUIH3     LOAD NSUIHP RET
        BLWP R13           GOTO INT HANDLER TO TEST SUSPEND
♦

```

```

♦♦♦♦♦♦ OUTPUT QUEUE SECTION
NIDQH2 LWPI NIDQHW           LOAD QUEUE HANDLER WP
        MOV  @QOPN,@QPOS(R5)  PUT O/P IN QUEUE
        INCT R5              NEXT LOCATION IN QUEUE
        C    R5,@QUELEN      IS R5 > QUEUE LENGTH
        JLE  SETOP
        CLR  R5              RESET POINTER
SETOP   MOV  @OPSTIM,R7      IS I/P ACTIVE
        JNE  OUT
        MOV  @QPOS(R4),@NEXTOP GET NEXT O/P
        SETD @OPSTIM        ACTIVATE O/P TASK
        JMP  OUT
♦

```

```

♦♦♦♦♦♦ ENTRY TO GET NEXT O/P ♦♦♦♦♦♦
NIDQH4 LWPI NIDQHW           LOAD QUEUE WP

```


SCR2.PROG.S.NIDQHP 12:36:16 FRIDAY, OCT 20, 1978.

	INCT R4	INC POINTER
	C R4, @QUELEN	IS R4 > QUEUE LENGTH
	JLE R4OK	
	CLR R4	RESET POINTER
R4OK	C R4, R5	IS START=END OF QUEUE
	JNE GETOP	
	CLR @OPSTIM	DEACTIVATE O/P TASK
	CLR @NEXTOP	CLEAR NEXT O/P REG
	JMP OUT	
GETOP	MOV @OPQS(R4), @NEXTOP	GET NEXT O/P
	JMP OUT	
	END	

NURSE STATION UART INTERRUPT HANDLER

1. DESCRIPTION

This program is an operating system program and is concerned with the interrupts generated by the UARTs used for inter-processor communication.

The functions performed by this program are :-

- (1) The handling of the interrupts due to the UART interval timer.
- (2) The transmission and reception of "Start of Heading" (SOH) characters "Acknowledge" (ACK) or "Negative Acknowledge" (NAK) characters for the correct start up of communication between processors.
- (3) The furnishing of workspace area addresses to the Input/Output Queue Handler, for use by the Input or Output Tasks as required.
- (4) The removal of unsuccessful communicating UARTs, from the input or output queues, and the possible indication of the errors to the operator if necessary.
- (5) The programming of all UARTs.

This operating system program is allowed the privilege of running under the interrupt mask of level 0.

2. IDENTIFICATION

SUBROUTINE NAME	NSUIH
PROGRAM MODULE	NSUIHP
GENERAL DATA MODULES	G0009D

GENERAL DATA MODULES	G00100
GENERAL DATA MODULES	G00110
GENERAL DATA MODULES	G00150
PERMANENT DATA MODULES	P00080

3. SIZE

PROGRAM MODULE 514 Bytes.

4. CALLS TO SUBROUTINE

INTERRUPT LEVEL	3	@NSUIH1	IHWA3
INTERRUPT LEVEL	4	@NSUIH1	IHWA2
INTERRUPT LEVEL	5	@NSUIH1	IHWA1
	B	@NSUIH2	
	B	@NSUIH3	
	B	@NSUIH4	
	BL	@PUART	

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	NSTHAP
BLWP	@NSTHA1
SUBROUTINE NAME	NIOQHP
B	@NIOQH1
B	@NIOQH2

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The three return vectors stored in R13, R14 and R15 of the workspace area used, are stored in the required locations for the currently active task.

6.2. OUTPUT DATA

During the operation of this program, the software flag which indicates that the task has been interrupted (i.e. IPTINT, OPTINT, MOCINT, IPINT, OPINT) is set accordingly.

7. EXTERNAL DATA TRANSFERS

PERIPHERALS TMS 9902 UARTs.

7.1. INPUT

INTERRUPT LEVEL	3
CRU BASE	>1840
INTERRUPT LEVEL	4
CRU BASE	>1900
INTERRUPT LEVEL	5
CRU BASE	>1880

CRU BIT Functions as specified in the TMS 9902
Data Sheets.

7.2. OUTPUT

CRU BASES AS ABOVE.

8. TIMING

The execution time for this program is of the
order of 0.2mS in normal communication situations.

9. AUTHOR

B.T.V. WARTON.

```

TITL 'NURSE STATION UART INT HANDLER'
♦ PROGRAMME MODULE IDENT (TASK)
  IDT 'NSUIHP'
♦ TRANSFER VECTORS OR ENTRIES
  DEF NSUIH1,NSUIH2,NSUIH3,NSUIH4,PUART
♦ CALLED PROGRAMME MODULES
  REF NSTHAP,NIDQHP
  REF NSTHA1,NIDQH1,NIDQH2
♦ LINKED DATA MODULES
  REF G0009D,G0010D,G0011D,G0015D,P0008D
  REF QOPN,QIPN,IOTF,OPERR,VDUOBA,ROMRAM
  REF ITWPR,ITPRT,ITSTR,OTWPR,OTPRT,OTSTR
  REF MTWPR,MPRT,MTSTR,IPWPR,IPRT,IPSTR
  REF IPTINT,OPTINT,MOCINT,IPINT,NSTHAM,TASKAN
  REF OPWPR,OPPRT,OPSTR,OPINT
  REF IPQS,OPQS,NEXTOP,NEXTIP,QUELEN
  RORG
  PSEG

```

```

♦
SOHD EQU >0100
ACKD EQU >0600
NAKD EQU >1500
♦

```

♦♦♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦

```

♦
NSUIH1 LIM1 0 OPERATING SYSTEM PROG
      BL @STRR SUSPEND TASK ,SAVE RETS
      TB 19 TIMINT
      JEQ TIMELP IF EQU GOTO TIMER ELAPS SECTION
      MOV R7,R7 I/P D/P MODE FLAG
      JLT IPMODE IF -VE = I/P MODE
      JGT OPMODE IF +VE = D/P MODE
      STCR R4,8 GET DATA
      MOV R0,R0 IS D/P RESP EXPECTED
      JNE OPYES
      CI R4,SOHD SOH ?
      JNE SOHND
      TB 9 P,F,D ERROR ?
      JEQ OPNAK
OPACK LI R4,ACKD ACK
      BL @OP D/P ACK
      SETD R1 SET SOH RECEIVED FLAG
      SETD R2 SET I/P FLAG
      CLR R10 ERROR COUNT
      BL @SETIME GO SET UART TIMER
BOUT BLWP @NSTHA1 GO TO TASK HANDLER
♦

```

♦♦♦♦♦♦ OUTPUT CHAR SECTION

```

OP SBD 18 RIENB
  SBD 16 TRANSMITTER ON
  LDCR R4,8 OUTPUT CHAR
  SBZ 16 TRANSMITTER OFF
  RT
♦

```

```

♦
TRYNAK CI R4,NAKD IS CHAR NAK ?
      JEQ OPSOH
      BL @NSUIH4 GO ENABLE NSUIHP PROG
      SETD R3 SET D/P SUSPEND FLAG
      BL @SETIME GO SET UART TIMER
      JMP BOUT
♦

```

```

OPYES  CI   R4,ACKD           ACK ?
        JNE  TRYNAK
        CLR  R7               RESET I/O MODE
        INC  R7               SET O/P MODE
        CLR  R0               RESET O/P RESP FLAG
        CLR  R10              ERROR COUNT
OPMODE  SBZ  18               INHIBIT INT RBRL
        BL   @SETIME          GO SET UART TIMER
        SBZ  20               INHIBIT TIMER INT
        MOV  R6,@QOPN         GIVE QUEUE NUMBER TO HANDLER
        B    @NIDQH2          GO TO PUT IN O/P QUEUE
SOHNO   MOV  R1,R1           IS SOH FLAG SET
        JEQ  OPNAK
        SETO R7               SET I/P MODE
        CLR  R1               SOH FLAG
        CLR  R10              CLEAR ERROR COUNT
♦
♦♦♦♦♦♦ INPUT MODE SECTION
♦ SET TIME TO TIME TILL CHAR IS USED BY IPTASK
IPMODE  SBZ  18               INHIBIT RBRL INT
        BL   @SETIME          GO SET UART TIMER
        SBZ  20               INHIBIT TIMER INT
        MOV  R6,@QIPN         GIVE QUEUE NUMBER
        B    @NIDQH1          GO TO QUEUE HANDLER
OPNAK   CI   R4,NAKD         WAS CHAR NAK
        JEQ  NAKER           DO NOT SEND NAK IF NAK RECEIVED
        BL   @PUART           GO PROGRAM UART
        LI   R4,NAKD         NAK
        CLR  R2               RESET I/P FLAG
        BL   @OP              O/P NAK
NAKER   BL   @ERROR          GO TO ERROR SECTION
        BL   @NSUIH4          GO ENABLE NSUIHP PROG
        JMP  BOUT
♦
♦♦♦♦♦♦ ERROR SECTION
ERROR   INC  R10              ERROR COUNT
        CI   R10,100         IS THERE 100 ERRORS
        JLT  RETS
♦ INDICATE ERROR
        CLR  R10              CLEAR ERROR COUNT
        MOV  @IOTF,@IOTF     IS VDU IN USE
        JNE  RETS
        LI   R10,OPERR        ERROR O/P ADDRESS
        MOV  R10,@VDUOBA      SAVE ADDRESS AT VDUOBA
        SETO @IOTF            SET VDU ACTIVE
        SETO @ROMRAM          SET NOT MIXED
RETS    RT
♦
♦♦♦♦♦♦ INTERVAL TIMER INTERRUPT SECTION
TIMELP  SBZ  20               INHIBIT TIMER
        MOV  R7,R7           TEST I/O MODE
        JEQ  ION0
        JGT  KILLOP
        LI   R8,IPQS          GET IPQS ADDRESS
KILL1   MOV  R8,R5
        A    @QUELEN,R5       CAL END
        JMP  KILL
KILLOP  LI   R8,OPQS          GET OPQS ADDRESS
        JMP  KILL1
KILL    C    R6,*R8           IS IT THIS UART IN QUEUE

```

```

        JEQ  KILLIT
KILL2  INCT R8
        C   R8,R5          IS IT AT END
        JLE KILL
        JMP OVER
KILLIT CLR  *R8           REMOVE FROM QUEUE
        JMP KILL2
OVER   C   R6,@NEXTOP    IS NEXT THIS UART
        JNE TESTIP
        CLR @NEXTOP      REMOVE FROM NEXTOP
TESTIP C   R6,@NEXTIP    IS NEXT THIS UART
        JNE CLRWA
        CLR @NEXTIP      REMOVE FROM NEXTIP
CLRWA  CLR  *R6           RESET BLIST POINTER
IOND   MOV  R0,R0        IS D/P RESPONSE EXPECTED
        JNE OPSOHE
        MOV  R7,R7        WAS D/P ACTIVE
        JGT OPSOH        GO D/P SOH IF YES
        BL  @NSUIH4      RESET FLAGS
        MOV  R3,R3        IS D/P SUSPENDED
        JNE OPSOH
        BL  @PUART       PROGRAM UART
        JMP BOUT
OPSOHE BL  @ERROR        GO TO ERROR SECTION
        JMP OPSOH
♦
♦♦♦♦♦♦♦ SET UART TIMER SECTION
SETIME SBD  13           LDIR SET
        LI  R5,>FA00     16 MS
        LDCR R5,8
        SBD  20           ENABLE TIMER INT
        RT
♦
OPSOH  LI  R4,SOHD       SOH
        BL  @OP          SET D/P RESP
        SETD R0           RESET SOH
        CLR  R1           " I/P FLAG
        CLR  R2           " D/P "
        CLR  R3           " I/O MODE
        CLR  R7
        BL  @SETIME
        BLWP @NSTHA1     GO TO TASK HANDLER
♦ D/P REQUEST
NSUIH2 LIM1 0
        MOV  R2,R2       IS IT INPUTING
        JEQ  OPSOH
        SETD R3           D/P SUSPENDED FLAG
        BLWP @NSTHA1     GO TO TASK HANDLER
♦
♦♦♦♦♦♦♦ D/P SUSPENDED TEST SECTION
NSUIH3 LIM1 0           PRIVILEGE MASK
        MOV  R3,R3       IS D/P SUSPENDED
        JNE NSUIH2      JUMP IF YES
        BLWP @NSTHA1     GO TO TASK HANDLER
♦
♦♦♦♦♦♦♦ PROGRAMMING UART SECTION
PUART  SBD  31           RESET UART
        LI  R8,>6300     GET UART CHAR FORMAT
        LDCR R8,8        LOAD FORMAT
        SBZ  13           RESET TIMER

```


NURSE STATION PROCESSOR INPUT TASK

1. DESCRIPTION

This program has been written as a multi input re-entrant task, and is concerned with receiving characters from all of the inter-processor communicating UARTs. The task has six main sections, the first of which is concerned with obtaining the workspace area it is to use, which contains the required UART CRU base address, and the current state of the input communication protocol. The remaining five sections are concerned with :-

- (1) Receiving the input instruction.
- (2) Receiving the inverse of the input instruction.
- (3) Receiving input data.
- (4) Receiving the Block Check Character (BCC), and
- (5) Receiving the End of Transmission Character (EOT).

2. IDENTIFICATION

SUBROUTINE NAME	NSPIT
PROGRAM MODULE	NSPITP
GENERAL DATA MODULE	G0009D
GENERAL DATA MODULE	G0011D
GENERAL DATA MODULE	G0013D

3. SIZE

PROGRAM MODULE	274	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

BLWP	@NSPIT1
------	---------

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	NSUIHP
BL	@NSUIH4
SUBROUTINE NAME	NIOQHP
B	@NIOQH3

6. INTERNAL DATA TRANSFER

6.1. OUTPUT DATA

The characters received by this task are placed in the input files associated with each UART. The position of the input file is found by adding 86 to the address of the workspace pointer being used.

6.2. ADDITIONAL DATA CHANGES

Register R0 in each of the input/output workspace areas is used as a Branch List Pointer, and is set to the next address to be used in the list when this task is next executed for that UART.

Having received the characters and placed them in an input file the task activates the MOCPC task by setting flags MOCPC and MCPIC, and incrementing the MOCPC activation counter MOCPCSC.

7. EXTERNAL DATA CHANGES

PERIPHERAL TMS 9902 UART

7.1. INPUT/OUTPUT

The CRU base address of the UART to be used is provided in the workspace area register R12 supplied to the Input Task.

8. TIMING

The execution time of this task is of the order

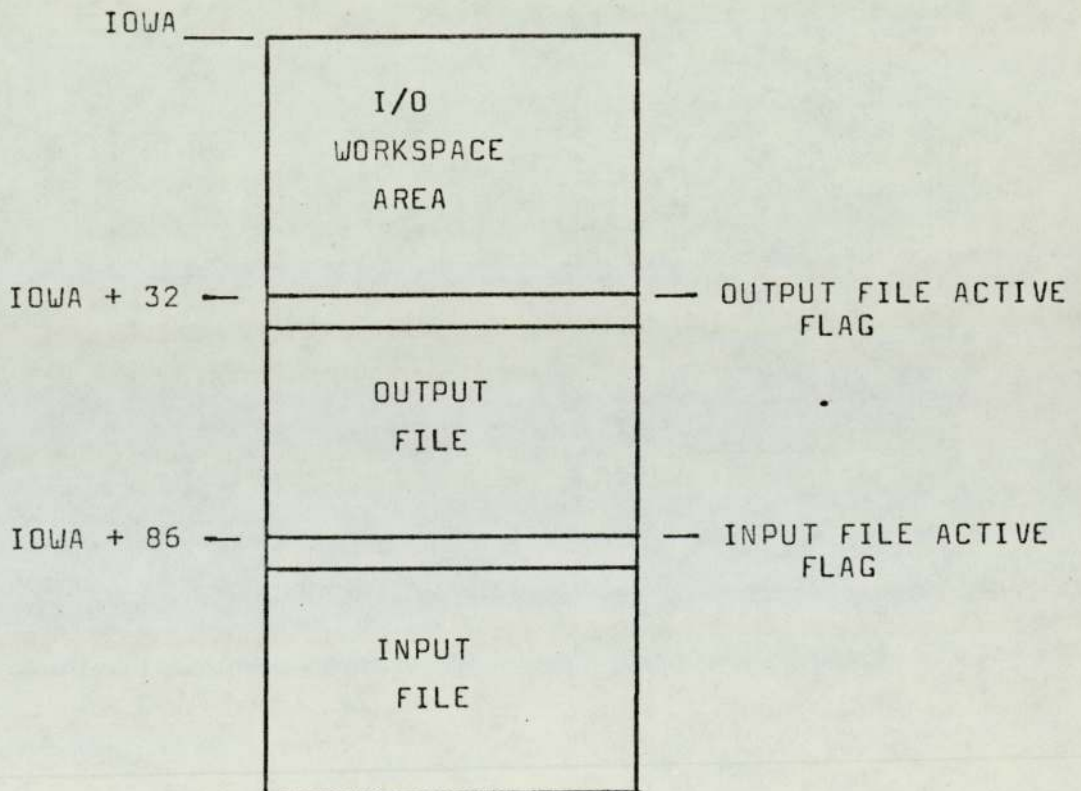
of 0.2mS.

9. AUTHOR

B.T.V. WARTON.

10. NOTE

The file memory structure is an important feature of the operation of this program. The input/output file structure for each UART is shown below.



```

        TITL 'NURSE STATION PROCESSOR I/P TASK'
♦ PROGRAMME MODULE IDENT (PROG)
        IDT 'NSPITP'
♦ TRANSFER VECTORS OR ENTRIES
        DEF NSPIT1,OPBYTE,SETIME
♦ CALLED PROGRAM MODULES
        REF NSUIHP,NIOQH3
        REF NSUIH4,NIOQH3
♦ LINKED DATA MODULES
        REF 60013D,60011D,60009D
        REF NSPIDW,NEXTIP,SETWP,SETPC,MDCP,MDCPSC,MCPJP
        REF NSTHAW
        RORG
        PSEG

```

♦♦♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦

```

ACKOP EQU >0600
END EQU >0500
NAKOP EQU >1500

```

```

♦
NSPIT1 DATA NSPIDW,START
START MOV @NEXTIP,@SETWP          GO GET NEXT I/P UART
      JEQ GONEXT                  IF = 0 GO GET NEXT
      LI R7,ADDRESS              GET ADDRESS
      MOV R7,@SETPC              MOV ADDRESS TO SETPC
      BLWP @SETWP                GET I/P WA
ADDRESS TB 25                    TEST TIME/P
      JEQ TIMER                  JUMP IF TIME ELAPS
      LI R1,BLIST                GET BRANCH LIST ADDRESS
      A R0,R1                    CAL BLIST POINTER
      MOV *R1,R1                 GET BRANCH FROM POINTER
      B *R1                      BRANCH

```

♦♦♦♦♦♦♦♦ I/P INSTRUCTION SECTION

```

IPINST STWP R2
      AI R2,86                   GET I/P FILE ADDRESS
      STCR *R2,8                 GET INST
      LI R4,END                 LOAD END CHAR
      BL @OPBYTE                D/P END
      BL @SETIME                GO SET TIMER
      LI R0,2                    SET BLIST POINT TO IPINVI
      JMP GONEXT

```

♦♦♦♦♦♦♦♦ RECEIVE INV INSTRUCTION

```

IPINVI SETO R5                   MACK R5 =-1
      STCR R5,8                 I/P CHAR
      AB *R2,R5                 ADD INST TO R5
      INC R5                    INST+INVINST+1=0
      JNE OPNAK                 R5 SHOULD=0 FOR CORRECT INST
      LI R4,ACKOP              LOAD ACK
      BL @OPBYTE                D/P ACK
      BL @SETIME                GO SET TIMER
      MOVB *R2+,R5             GET INST IS IT +VE
      JLT NEGINS                SET BLIST POINT TO EOT
      LI R0,8
      JMP GONEXT
NEGINS LI R9,50                 LOAD 50 BYTE COUNTER
      CLR R8                    BCC SUM
      LI R0,4                    SET BLIST POINT TO IPDATA
      JMP GONEXT
OPNAK LI R4,NAKOP              LOAD NAK

```

```

LIMI 0          ◆◆◆ MASK BEFOR LEAVING TASK ◆◆
BL  00PBYTE    D/P NAK
CLR  R0        RESET BLIST POINT
LI   R11,CHWP  LOAD R11 WITH RET
BLWP R10      GET WA
CHWP BL  0NSUIH4  ENABLE INT HANDLER
      JMP  GONEXT

```

◆◆◆◆◆◆◆◆ I/P DATA SECTION

```

IPDATA STOR R5,8  STORE CHAR
      AB  R5,R8   BCC SUM
      MOVB R5,♦R2+ PUT DATA IN I/P FILE
      LI  R4,END  LOAD END CHAR
      BL  00PBYTE D/P END
      BL  0SETIME SET TIMER
      DEC R9      DEC BYTE COUNT
      JNE GONEXT
      LI  R0,6    SET BLIST POINT TO IPBCC
      JMP GONEXT

```

◆◆◆◆◆◆◆◆ I/P BCC & CHECK SECTION

```

IPBCC STOR R5,8  I/P CHAR
      CB  R5,R8  ARE BCC SAME
      JNE OPNAK
      LI  R4,ACKDP LOAD ACK CHAR
      BL  00PBYTE D/P ACK
      BL  0SETIME SET TIMER
      LI  R0,8    SET BLIST POINT TO IPEOT
      JMP  GONEXT

```

◆◆◆◆◆◆◆◆ I/P EOT SECTION

```

IPEOT SETO 0MOCP  STIM MOCP
      INC  0MOCPSC INC MOCP STIM COUNT
      SETO 0MCPIP  ACTIVATE MOCP TASK
      CLR  R0      RESET BLIST
      STWP R2      SAVE WP
      RI  R2,84   WP+84=I/P FILE
      SETO ♦R2    SET I/P FILE ACTIVE
      LI  R11,HERE SET R11 RET
      BLWP R10    GET NEW WP
HERE  LIMI 0      ◆◆◆◆MASK BEFOR LEAVING◆◆◆◆
      SBO  18     ENABLE REC INT
      BL  0NSUIH4 ENABL INT HANDLER
GONEXT EQU  $
      LWPI NSTHAW GET TASK HANDLER WP
      SBZ  0      RESET TASK ACTIVE BIT
      B   0NIDQH3 GO GET NEXT I/P FROM QUEUE

```

◆◆◆◆◆◆◆◆ D/P CHAR SECTION

```

OPBYTE SBO  18  RIENB
      SBO  16  TRANSMITTER ON
      LDOR R4,8  LOAD UART
      SBZ  16  TRAN OFF
      RT

```

◆◆◆◆◆◆◆◆ TIMELP HANDLER

```

TIMER CLR  R0    RESET BLIST
      LI  R11,HERE SET R11 RET
      BLWP R10    ABANDON I/P

```

SCR2.PROG.S.NSPITP 13:14:14 FRIDAY, OCT 20, 1978.

```
***** SET UART TIMER SECTION
SETIME SBO 13          ENABLE UART TIMER
      LI  R5,>FA00     LOAD R5 WITH COUNT
      LDCR R5,8        LOAD UART WITH COUNT
      SBO 20          ENABLE INT
      RT
```

```
◆
***** BRANCH LIST VALUES
BLIST DATA IPINST,IPINVI,IPDATA,IPBCC,IPEDT
      END
```

NURSE STATION PROCESSOR OUTPUT TASK

1. DESCRIPTION

This program has been written as a multi output re-entrant task, and is concerned with transmitting characters via the inter-processor communicating UARTs. The task has seven main sections, the first of which is concerned with obtaining the workspace area it is to use, which contains the UART CRU base address required, and the current state of the output communication protocol.

The remaining six sections are concerned with :-

- (1) Transmitting instruction.
- (2) Transmitting inverse of instruction.
- (3) Testing that the "Acknowledge" character (ACK) is received, and transmission of EOT character.
- (4) Transmitting data.
- (5) Transmitting block check character (BCC).
- (6) Testing that the "Acknowledge" character (ACK) is received.

2. IDENTIFICATION

SUBROUTINE NAME	NSPOT
PROGRAM MODULE	NSPOTP
GENERAL DATA MODULE	G0013D

3. SIZE

PROGRAM MODULE	284	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

BLWP @NSPOT1

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	NIOQHP
B	@NIOQH4
SUBROUTINE NAME	NSUIHP
BL	@NSUIH4
SUBROUTINE NAME	NSPITP
BL	@OPBYTE
BL	@SETIME

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The characters which are to be transmitted by this task are present in the Output files associated with each UART. The position of the output file is found by adding 34 to the address of the workspace pointer being used.

6.2. ADDITIONAL DATA CHANGES

Register R0 in each of the input/output workspace areas is used as a Branch list pointer, and is set to the next address to be used in the list, when this task is next executed for that UART.

7. EXTERNAL DATA CHANGES

PERIPHERAL TMS 9902 UART.

7.1. INPUT/OUTPUT

The CRU base address for the UARTs to be used is provided in the workspace area register R12 supplied to the Output Task.

8. TIMING

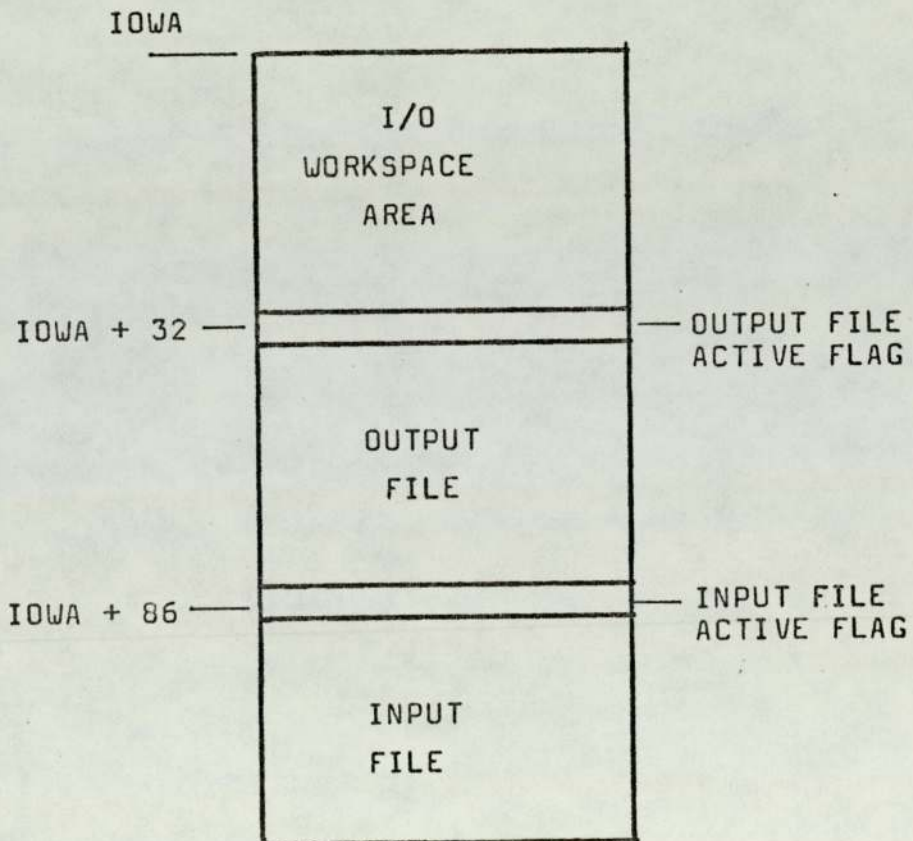
The execution time of this task is of the order of 0.2mS.

9. AUTHOR

B.T.V. WARTON.

10. NOTE

The file memory structure is an important feature of the operation of this program. The input/output file structure for each UART is shown below.



```

        TITL 'NURSE STATION PROCESSOR O/P TASK'
♦ PROGRAMME MODULE IDENT (PROG)
        IDT 'NSPOTP'
♦ TRANSFER VECTORS OR ENTRIES
        DEF NSPOT1
♦ CALLED PROGRAM MODULES
        REF NIOQHP,NSUIHP,NSPITP
        REF NIOQH4,NSUIH4,OPBYTE,SETIME
♦ LINKED DATA MODULES
        REF 60013D
        REF NSPIOW,NEXTOP,SETWP1,SETPC1
        REF NSTHAW
        RORG
        PSEG

```

♦♦♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦

```

EDT    EQU    >0400
ACK    EQU    >0600
NAK    EQU    >1500

```

```

♦
NSPOT1 DATA NSPIOW,START
START  MOV  @NEXTOP,@SETWP1    GET WP
      JEQ  GONEXT
      LI  R7,LOCATE           GET PG
      MOV R7,@SETPC1          SAVE PC RET
      BLWP @SETWP1            GET NEW WP
LOCATE TB  25                 TIMELP
      JEQ  TIMER              JUMP IF TIMER ELAPST
      LI  R1,BLIST1           GET BRANCH LIST ADDRESS
      A   R0,R1               CAL BLIST POINTER
      MOV *R1,R1              GET BRANCH POINT
      B   *R1                 BRANCH

```

♦♦♦♦♦♦ D/P INSTRUCTION SECTION

```

OPINST STWP R2                SAVE WP
      AI  R2,34                WP +34 =O/P FILE ADDRESS
      MOVB *R2+,R4             GET INST IN FILE
      BL  @OPBYTE              D/P INST
      BL  @SETIME              SET UART TIMER
      LI  R0,2                 SET BLIST POINT TO OPINVI
      JMP GONEXT

```

♦♦♦♦♦♦ D/P INVERSE OF INSTRUCTION

```

OPINVI INV  R4                INVERT INST
      BL  @OPBYTE              D/P INV INST
      BL  @SETIME              SET TIMER
      LI  R0,4                 SET BLIST POINT TO ACK1
      JMP GONEXT

```

♦♦♦♦♦♦ CHECK REPLY IS ACK

```

ACK1   STCR R5,8              I/P REPLY
      CI  R5,ACK                IS IT ACK
      JNE TRYNAK              JUMP IF NO
      INV R4                    IS INST +VE
      JLT NEGINS              JUMP TO O/P DATA
OPEOT  LIMB 0                  ♦♦♦♦ MASK BEFOR EDT EXIT ♦♦♦♦
      LI  R4,EDT                LOAD EDT CHAR
      BL  @OPBYTE              D/P EDT
      CLR R0                    RESET BLIST POINTER
      STWP R2                    SAVE WP
      AI  R2,32                WP + 32 =O/P FILE FLAG

```

```

                CLR  *R2                RESET O/P FILE ACTIVE FLAG
                LI   R11,CHWP1         LOAD R11 RET
                BLWP R10                GET NEW WA
CHWP1 EQU %
                BL   @NSUIH4           GO ENABLE INT HANDLER
♦
♦♦♦♦♦♦ EXIT FROM O/P TASK TO QUEUE HANDLER
GONEXT EQU %
                LWPI NSTHAW            GET TASK HANDLER WP
                SBZ  1                 RESET O/P TASK ACTIVE FLAG
                B    @NIDQH4           GO TO QUEUE HANDLER
♦
♦♦♦♦♦♦ O/P OF DATA SECTION ( 50 BYTES)
NEGINS LI R9,50                       SET BYTE COUNTER TO 50
                CLR  R8                BCC
                MOVW *R2,+R4           GET DATA
                AB   R4,R8             BCC SUM
                DEC  R9                DEC BYTE COUNTER
                BL   @OPBYTE           O/P DATA
                BL   @SETIME           SET TIMER
                LI   R0,6              SET BLIST POINT TO OPDATA
                JMP  GONEXT
♦
♦♦♦♦♦♦ TEST FOR NAK REPLY
TRYNAK CLR R0                          RESET BLIST POINT
                CI   R5,NAK            IS REPLY NAK
                JNE  TOUT              JUMP IF NO ?
                LI   R11,CHWP2         LOAD R11 RET
                BLWP R10                GET NEW WP
CHWP2 LIM1 0                             ***MASK BEFOR EXIT***
                BL   @NSUIH4           GET INT HANDLER TO RETX SOH
                LI   R4,>0100          SOH
                BL   @OPBYTE           O/P SOH AGAIN
                BL   @SETIME           SET TIMER
                SETD R0                SET RESP FLAG
                JMP  GONEXT
♦
♦♦♦♦♦♦ TIMING OUT ERROR SECTION
TOUT LI R11,CHWP3                       LOAD R11 RET
                BLWP R10                GET NEW WP
CHWP3 LIM1 0                             ***MASK BEFOR EXIT***
                BL   @NSUIH4           TIME OUT RESTART
                BL   @SETIME           SET TIMING OUT TIME
                SETD R3                SET O/P SUSPENDED
                JMP  GONEXT
♦
♦♦♦♦♦♦ O/P DATA SECTION
OPDATA MOVW *R2+,R4                       GET DATA
                AB   R4,R8             BCC SUM
                BL   @OPBYTE           O/P DATA
                BL   @SETIME           SET UART TIMER
                DEC  R9                DATA COUNT
                JNE  GONEXT
                LI   R0,8              SET BLIST POINT TO OPBCC
                JMP  GONEXT
♦
♦♦♦♦♦♦ O/P BLOCK CHECK CHARACTER (BCC) SECTION
OPBCC MOVW R3,R4                          GET BCC
                BL   @OPBYTE           O/P BCC
                BL   @SETIME           SET TIMER

```

SCR2.PROG.S.NSPOTP 14:36:01 FRIDAY, OCT 20, 1978.

```

      LI   R0,10           SET BLIST POINT TO ACK2
      JMP  GONEXT

♦
♦♦♦♦♦♦ RECEIVE ACK 2
ACK2   STCR R5,8           I/P REPLY
      CI   R5,ACK          IS IT ACK
      JNE  TRYNAK         JUMP IF NOT
      JMP  DPEOT

♦
♦♦♦♦♦♦ UART TIMER ELAPS SECTION
TIMER  CLR  R0             RESET BLIST POINTER
      LI  R11,CHWP2        LOAD R11 RET
      BLWP R10            GO O/P SOH AGAIN

♦
♦♦♦♦♦♦ BRANCH LIST VALUES
BLIST1 DATA OPINST,OPINVI,ACK1,OPDATA,OPBCC,ACK2
      END
```

MICRO/OPERATOR COMMUNICATION PACKAGE

1. DESCRIPTION

This program is concerned with interpreting and/or generating the communication information which passes between processors or the operator dedicated processor and the operator. For example this task will interpret on input instruction from the operator (via the VDU), and generate the command to be sent to the required patient dedicated processor.

2. IDENTIFICATION

SUBROUTINE NAME	MOCPT
PROGRAM MODULE	MOCPTP
GENERAL DATA MODULE	G0008D
GENERAL DATA MODULE	G0009D
GENERAL DATA MODULE	G0012D
GENERAL DATA MODULE	G0014D
GENERAL DATA MODULE	G0015D
PERMANENT DATA MODULE	P0008D

3. SIZE

PROGRAM MODULE 582 Bytes.

4. CALLS TO SUBROUTINE

BLWP @MOCPT1.

5. CALLS FROM SUBROUTINE

SUBROUTINE NAME	NSUIHP
B	@NSUIH2
SUBROUTINE NAME	VDUIOP
BLWP	@VDUIO2

SUBROUTINE NAME	ASCIIP
BL	@ASCI11
SUBROUTINE NAME	BIHEXP
BL	@BIHEX1

6. INTERNAL DATA TRANSFERS

6.1. INPUT DATA

The input data to this program is supplied in the VDU input buffer (BUFA) or any of the UART input files (IPFI1S, IPFI2S, IPFI3S).

6.2. OUTPUT DATA

The output data from this program for the VDU is an address where the output to the VDU can be found (VDUOBA). The output data to be sent to patient processors is placed in the required UART output files (OPFIL1 etc.).

6.3. ADDITIONAL DATA CHANGES

The software flags which may be changed by the operation of this program are :-

MCPIP, IPSF, MOSPSC, MOCP, ROMRAM, IOTF,
OPFIL1, IPFIL1, IPFIL2, IPFIL3.

7. TIMING

The execution time of this program is dependent on the input instruction which it has received.

8. AUTHOR

B.T.V. WARTON.

```

        TITL 'MICRO/OPERATOR COMMUNICATION PACKAGE'
♦ PROGRAMME MODULE IDENT (TASK)
        IDT 'MOCPTP'
♦ TRANSFER VECTORS OR ENTRIES
        DEF MOCPT1
♦ CALLED PROGRAM MODULES
        REF NSUIHP,VDUIDP,ASCIIP,BIHEXP
        REF NSUIH2,VDUID2,ASCI11,BIHEX1
♦ LINKED DATA MODULES
        REF G0008D,G0009D,G0012D,G0014D,G0015D,P0008D
        REF MOCPTW,MOCPIP,IPSF,BUFA,SM,EM,CM
        REF ERROR1,MOCPSO,MOCOP,IPLIST,OPM1,OPM2,OPM3,OPM4
        REF OPM5,OPM6,OPM7,OPM8,OPM9,OPM10,OPM11,OPM12
        REF VDUIDBA,ROMRAM,IOTF,HEXONE,IHWA1,OPFIL1
        REF OPROM,OPRAM,NDF1,NDF11,NDF2,NDF22,NPR,NPR1
        REF NMF1,NMF11,NMF2,NMF22,PR,PS
        REF IPFIL1,IPFI1S
        REF IPFIL2,IPFI2S
        REF IPFIL3,IPFI3S
        RORG
        PSEG

```

♦♦♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦

```

MOCPT1 DATA MOCPTW,START
START  MOV  @MOCPIP,R0          IS IT MICRO TO MICRO I/P
      JLT  MINPUT
TESTIP ABS  @IPSF              IS IT OPERATOR I/P
      JLT  DINPUT
      CLR  @MOCPSO            CLEAR MOCOP STIM COUNT
      CLR  @MOCOP            CLEAR MOCOP ACTIVE FLAG
      RTWP

```

```

♦♦♦♦♦♦ MICRO TO MICRO COMMUNICATION INTERPRETER
MINPUT MOV  @IPFIL1,R0        IS I/P FILE 1 ACTIVE
      JLT  IPA1
      MOV  @IPFIL2,R0        IS I/P FILE 2 ACTIVE
      JLT  IPA2
      MOV  @IPFIL3,R0        IS I/P FILE 3 ACTIVE
      JLT  IPA3

```

♦ EXTEND THIS IF MORE I/P FILES AVAILABLE

```

      CLR  @MOCPIP
      JMP  TESTIP

```

♦♦♦♦♦♦ GET FILE ADDRESS SECTION

```

IPA1  LI   R1,IPFI1S          GET START OF I/P FILE
      BL   @DECODE           DECODE MESSAGE
      CLR  @IPFIL1           CLEAR IPFIL1 FLAG
      JMP  OUT
IPA2  LI   R1,IPFI2S          GET START OF I/P FILE
      BL   @DECODE           DECODE MESSAGE
      CLR  @IPFIL2           CLEAR IPFIL2 FLAG
      JMP  OUT
IPA3  LI   R1,IPFI3S          GET START OF I/P FILE
      BL   @DECODE           DECODE MESSAGE
      CLR  @IPFIL3           CLEAR IPFIL3 FLAG
      JMP  OUT

```

♦ EXTEND THIS IF MORE I/P FILES AVAILABLE

♦♦♦♦♦♦ OPERATOR I/P INTERPRETER

```

DINPUT LI   R7,BUFA          GET VDU BUFFER

```

	C	@SM, *R7	IS IT START MONITORING
	JEQ	DOSM	
	C	@EM, *R7	END MONITORING ?
	JEQ	DOEM	
	C	@CM, *R7	CONTINUE MONITORING
	JEQ	DOCM	
	C	@PR, *R7	PULSE RATE
	JEQ	DOPR	
	C	@PS, *R7	PATIENT STATUS
	JEQ	DOPS	
ERRORM	LI	R2, ERROR1	I/P COMMAND ERROR
	BL	@VDUOP	O/P MESSAGE
*****	EXIT	FROM PROGRAMME IF	NO STIMS SECTION
OUT	DEC	@MOCPSC	DEC MOCP STIM COUNT
	JNE	GO	JUMP IF NOT = 0
	CLR	@MCPPI	RESET MICRO I/P FLAG
	CLR	@MOCP	RESET MOCP ACTIVE FLAG
	RTWP		RETURN TO TASK HANDLER
GO	MOV	@MOCPSC, R2	GET MOCP STIM COUNT
	CI	R2, 1	IS IT = 1
	JNE	AGAIN	JUMP IF NO
	MOV	@IPSF, R2	IS OPERATOR FLAG SET
	JGT	AGAIN	JUMP IF IPSF +VE
	CLR	@MCPPI	RESET MICRO I/P FLAG
AGAIN	B	@START	GO TO START OF THIS TASK
♦	*****	MICRO TO MICRO MESSAGE	GENERATION SECTION
DOSM	INCT	R7	POINT R7 TO NEXT WORD IN BUFA
	BL	@WHICHU	GO FIND WHICH PATIENT UART
WA1	LI	R6, >5000	>50=BYTE CODE FOR START MONITOR
	MOVB	R6, *R8	PUT IN O/P FILE
	LI	R10, DSTIM	SET R10 FOR RET
	BLWP	R9	GET IHWA REQUIRED
*****	TASK	STIM TEST	
DSTIM	DEC	@MOCPSC	DEC MOCP STIM COUNT
	JNE	BRANCH	
	CLR	@MOCP	DEACTIVATE TASK
	CLR	@MCPPI	MCP I/P FLAG
BRANCH	B	@NSUIH2	GO TO NSUIHP TO ACTIVATE O/P FROM UA
♦	DOEM	INCT R7	POINT TO NEXT WORD IN BUFA
	BL	@WHICHU	WHICH PATIENT
	LI	R6, >5300	>53=END MONITORING
	MOVB	R6, *R8	SAVE IN O/P FILE
	LI	R10, DSTIM	SET R10 TO RET
	BLWP	R9	
♦	DOCM	INCT R7	INC BUFA POINTER
	BL	@WHICHU	WHICH PATIENT
	LI	R6, >5500	>55=CONTINUE MONITORING
	MOVB	R6, *R8	SAVE IN O/P FILE
	LI	R10, DSTIM	SET R10 TO RET
	BLWP	R9	
♦	DOPR	INCT R7	INC BUFA POINTER
	BL	@WHICHU	WHICH PATIENT
	LI	R6, >5000	PR CODE
	MOVB	R6, *R8	PUT IN FILE
	LI	R10, DSTIM	SET R10 TO RET
	BLWP	R9	


```

♦
DOPS   INCT R7           INC BUFA POINTER
       BL   @WHICHU      WHICH PATIENT
       LI   R6,>5600     PS CODE
       MOVB R6,♦R8       SAVE IN O/P FILE
       LI   R10,DSTIM    SET R10 TO RET
       BLWP R9
    
```

```

♦
♦♦♦♦♦ MICRO TO MICRO MESSAGE DECODER
DECODE EQU $
MOV   R11,R12           ♦♦♦♦♦SAVE RET ♦♦♦♦♦
LI    R5,IPLIST        GET ADDRESS OF COMMAND STRING
CB    ♦R5+,♦R1
JEQ   MON              JUMP IF MONITORING COMMAND
CB    ♦R5+,♦R1
JEQ   MONOK           MONITOR OK
CB    ♦R5+,♦R1
JEQ   MONFAI         MONITOR FAIL
CB    ♦R5+,♦R1
JEQ   EMJMP          MONITOR END
CB    ♦R5+,♦R1
JEQ   CONMON         CONTINUING MONITORING
CB    ♦R5+,♦R1
JEQ   ERM            ERROR MESSAGE
CB    ♦R5+,♦R1
JEQ   ALREMO        ALREADY MONITORING
CB    ♦R5+,♦R1
JEQ   NOTMON        NOT MONITORING
CB    ♦R5+,♦R1
JEQ   DIAG          DIAGNOSIS
CB    ♦R5+,♦R1
JEQ   PRD           PULSE RATE DATA
CB    ♦R5+,♦R1
JEQ   PSD           PATIENT STATUS DATA
♦ ETC ( INSERT MORE COMMANDS HERE AS REQUIRED)
B     ♦R12          RET USING SAVED RET
MON   LI   R2,OPM1   MONITORING
      JMP  STIMG0
MONOK LI   R2,OPM2   MONITOR START UP OK
      JMP  STIMG0
MONFAI LI  R2,OPM3   MON S.U FAIL
      JMP  STIMG0
EMJMP  LI  R2,OPM4   END OF MONITORING
      JMP  STIMG0
CONMON LI  R2,OPM5   CONTINUE MON
      JMP  STIMG0
ERM     LI  R2,OPM6   ERROR MESSAGE
      JMP  STIMG0
ALREMO LI  R2,OPM8   ALREADY MON MESSAGE
      JMP  STIMG0
NOTMON LI  R2,OPM9   NOT MON
STIMG0 BL  @VDUOP
      B    ♦R12          RET USING SAVED RET
    
```

```

♦
♦♦♦♦♦ PROCESSING OF DIAGNOSIS DATA
DIAG  INCT R1         INC FILE POINTER
      MOV  ♦R1+,@NDF1  SAVE DF1
      MOV  ♦R1+,@NDF2  SAVE DF2
      BL  @BIHEX1     GO TO BINARY TO HEX CONVERTER
      DATA NDF1,NDF11,NDF2,NDF22
    
```

```

DATA >FFFF                END OF DATA MARKER
LI R2,OPM10                DIAGNOSIS MESSAGE
LI R3,NDF11                DIAGNOSIS MESSAGE
BL @MVDUOP                 D/P MESSAGE
B *R12                     RET USING SAVE RET
♦
♦ PROCESSING OF PULSE RATE DATA
PRD INCT R1                 INC FILE POINTER
MOV *R1+,@NPR              GET PR DATA
BL @ASCII1                 GO TO BINARY TO ASCII SUB
DATA NPR,NPR1,>FFFF
LI R2,OPM12                PULSE RATE
LI R3,NPR1
JMP STIMRR
♦
♦♦♦♦♦ PROCESSING OF PATIENT STATUS DATA
PSD INCT R1                 INC FILE POINTER
MOV *R1+,@NPR              GET PULSE RATE DATA
MOV *R1+,@NDF1             GET DIAGNOSIS WORD 1
MOV *R1+,@NDF2             GET DIAGNOSIS WORD 2
MOV *R1+,@NMF1             GET MONITORING WORD 1
MOV *R1+,@NMF2             GET MONITORING WORD 2
BL @BIHEX1                 GO TO BINARY TO HEX CONVERTER
DATA NPR,NPR1,NDF1,NDF11,NDF2,NDF22
DATA NMF1,NMF11,NMF2,NMF22,>FFFF
LI R2,OPM11                D/P MESSAGE 11
LI R3,NDF11                D/P DATA
STIMRR BL @MVDUOP          GO TO VDU D/P
B *R12                     RET USING SAVED RET
♦ ETC
♦
♦♦♦♦♦ VDU NOT ROMRAM MIX OUTPUT
VDUOP MOV R2,@VDUOBA        GIVE OUT PUT ADDRESS TO VDU PROG
SETD @ROMRAM               NOT MIXED
BLWP @VDUID2               GO DIRECT TO VDU TASK
RT
♦
♦♦♦♦♦ VDU ROM/RAM MIXED D/P
MVDUOP MOV R2,@OPROM        SET PROM RESIDENT TEXT ADDRESS
MOV R3,@OPRAM              SET RAM RESIDENT TEXT ADDRESS
ABS @ROMRAM                MIXED DATA
BLWP @VDUID2               GO DIRECT TO VDU TASK
RT
♦
♦♦♦♦♦ WHICH UART SECTION
WHICHU C *R7,@HEXONE       IS IT PATIENT ONE
JEQ UART1
♦ INSERT PROGRAM HERE AS MORE PATIENT PROCESSORS
♦ BECOME AVAILABLE
B @ERRORM
UART1 LI R8,OPFIL1         LOAD R8 WITH OPFIL1 ADDRESS
MOV *R8,R0                 IS D/P FILE ACTIVE
JEQ FILEOK
LI R2,OPM7                 TELL OPERATOR D/P ACTIVE
BL @STIMGO                 D/P MESSAGE
B @OUT
FILEOK SETD *R8+           SET OPFILE ACTIVE
LI R9,IHWA1                LOAD R9 WITH IHWA1 TO BE USED
RT
END

```

BINARY TO HEX CONVERTER

1. DESCRIPTION

This program is concerned with converting a 16 bit binary word into the four ASCII character hexadecimal value of the word, needed for later transmission to a VDU terminal.

2. IDENTIFICATION

SUBROUTINE NAME	BIHEX
PROGRAM MODULE	BIHEXP
PERMANENT DATA MODULE	P0008D

3. SIZE

PROGRAM MODULE 64 Bytes.

4. CALLS TO SUBROUTINE

BL @BIHEX1

5. INTERNAL DATA TRANSFERS

5.1. INPUT DATA

The input data for this subroutine is supplied after the BL @BIHEX1 statement by using the following statement,

DATA a, b, a, b, >FFFF

where a = address of word to be converted

 b = address where results are to be saved, and

>FFFF = end of data marker.

5.2. OUTPUT DATA

As stated above, the output results from this program are saved at the addresses specified by "b" words in the input data format.

5.3. ADDITIONAL DATA CHANGES

The last character of each of the group of 4 hexadecimal characters is made negative as an end of string indicator.

This program makes use of register R2, R3, R4, R5 and R11 in the currently active workspace area.

6. TIMING

The executing time of this program is dependent on the number of words to be converted.

7. AUTHOR

B.T.V. WARTON.

SCR2.TASK.S.BIHEXP 16:15:46 FRIDAY, OCT 20, 1978.

```
TITL / BINARY TO HEX CONVERTER /
♦ PROGRAMME MODULE IDENT (TASK)
  IDT 'BIHEXP'
♦ TRANSFER VECTORS OR ENTRIES
  DEF BIHEX1
♦ LINKED DATA MODULES
  REF P0008D
  REF ASCDAT
  RORG
  PSEG
♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦
BIHEX1 MOV  ♦R11+,R2
        CI   R2,>FFFF           IS IT END OF DATA
        JEQ  OVER
        MOV  ♦R2,R2             GET DATA
        CLR  R3                 COUNT
        MOV  ♦R11+,R4          GET ADDRESS TO PUT DATA
BYTE   MOVB  R2,R5             GET FIRST BYTE OF WORD
        SRL  R5,12             GET MOST SIG 4 BITS
        AI   R5,ASC DAT       R5 + ASCDAT ADDRESS
        MOVB ♦R5,♦R4+         SAVE DATA
        MOVB R2,R5             GET FIRST BYTE AGAIN
        ANDI R5,>0F00         GET LS 4BITS MS BYTE
        SRL  R5,8             MAKE INTO WORD
        AI   R5,ASC DAT
        MOVB ♦R5,♦R4+         SAVE DATA
        INCT R3                 COUNT
        CI   R3,4             IS WORD CONVERTED
        JEQ  NEG
        SWPB R2                 SWAP BYTE IN CONVERSION WORD
NEG    JMP  BYTE
        DEC  R4                 BACK 1 CHAR
        CLR  R2
        MOVB ♦R4,R2           GET CHAR
        NEG  R2                 MACK -VE
        MOVB R2,♦R4           RET CHAR
OVER   JMP  BIHEX1
        RT
        END
```

BINARY TO ASCII DECIMAL

1. DESCRIPTION

This program is concerned with converting a 16 bit word into the ASCII characters required to display the decimal value of the word on a VDU.

2. IDENTIFICATION

SUBROUTINE NAME	ASCII
PROGRAM MODULE	ASCIIP
PERMANENT DATA MODULE	P0008D

3. SIZE

PROGRAM MODULE 100 Bytes.

4. CALLS TO SUBROUTINE

BL @ASCI11

5. INTERNAL DATA TRANSFERS

5.1. INPUT DATA

The input data for this subroutine is supplied after the BL @ASCI11 statement by using the following statement,

DATA a, b, a, b, >FFFF

where a = address of word to be converted

b = address where results are to be saved

and >FFFF = end of data marker.

5.2. OUTPUT DATA

As stated above the output results from this

program are stored at the address specified by the "b" words in the input data format.

5.3. ADDITIONAL DATA CHANGES

The last ASCII character expressing the value of the word converted, is made negative as an end of string indicator.

This program makes use of registers R4, R5, R7, R8, R9 and R11 in the currently active workspace area.

6. TIMING

The executing time of this program is dependent on the number of words to be converted.

7. AUTHOR

B.T.V. WARTON.

SCRE.TASK.S.ASCIIP 16:18:58.FRIDAY, OCT 20, 1978.

```

      TITL  ' BINARY TO ASCII DECIMAL '
♦ PROGRAMME MODULE IDENT (TASK)
      IDT  'ASCIIP'
♦ TRANSFER VECTORS OR ENTRIES
      DEF  ASCII1
♦ LINKED DATA MODULES
      REF  P0008D
      REF  MINUS,SPACE,THOU,HUND,TEN,ASCNUM
♦♦♦♦♦♦♦♦♦♦ P R O G R A M M E ♦♦♦♦♦♦♦♦♦♦
ASCII1  MOV  R11,R8          SAVE DATA ADDRESS
NEXTV   CLR  R4
        MOV  *R8+,R5        GET DATA ADDRESS
        CI   R5,>FFFF      IS IT END OF DATA
        JEQ  OVER1
        MOV  *R8+,R9        GET DATA RET
        MOV  *R5,R5        GET DATA
        ABS  R5            IS IT NEG
        JGT  DOSPAC
        JEQ  DOSPAC
        MOVB @MINUS,*R9+    D/P MINUS
        JMP  DODIV
DOSPAC  MOVB @SPACE,*R9+    INSERT A SPACE
DODIV   DIV  @THOU,R4      R4/1000
        CLR  R7            ZERO SUP FLAG
        BL  @TZERO        GO TEST FOR ZERO
        DIV  @HUND,R4     R4/100
        BL  @TZERO        GO TEST FOR ZERO
        DIV  @TEN,R4      R4/10
        BL  @TZERO        GO TEST FOR ZERO
        A    @ASCNUM,R5    R5->30
        SWPB R5
        NEG  R5            MAKE LAST CHAR -VE
        MOVB R5,*R9        SAVE
        JMP  NEXTV
OVER1   B    *R8            RETURN
TZERO   MOV  R7,R7        TEST FLAG
        JNE  L1
        MOV  R4,R4        TEST R4
        JNE  L1
        MOVB @SPACE,*R9+    INSERT A SPACE
        JMP  CONTA
L1      SETD R7            SET FLAG
        A    @ASCNUM,R4    R4->30
        SWPB R4
        MOVB R4,*R9+        SAVE
CONTA   CLR  R4            RESET R4
        RT
        END

```


VDU INPUT/OUTPUT PROGRAM

1. DESCRIPTION

This is the lowest priority level task in the operator dedicated processor system. If the system has no other tasks active, control is passed to the VDU input routine. The output routine of the VDU program can be entered in two ways. The first is by activating the output routine as a task, which will be scheduled by the task handler program. The second method is direct entry to the VDU output routine, as is sometimes performed by the MOCP task. The second method is quicker, and does not require the de-activation of the MOCP task before the VDU output routine will run.

2. IDENTIFICATION

SUBROUTINE NAME	VDUIO
PROGRAM MODULE	VDUIOP
GENERAL DATA MODULE	G0008D
GENERAL DATA MODULE	G0013D
PERMANENT DATA MODULE	P0007D

3. SIZE

PROGRAM MODULE	248	Bytes.
----------------	-----	--------

4. CALLS TO SUBROUTINE

BLWP	@VDUIO1
BLWP	@VDUIO2
BLWP	@INPUT

5. INTERNAL DATA TRANSFERS

5.1. INPUT DATA

The input data to this program is the address where the output string of characters can be found, plus software flags indicating if the characters are in both ROM and RAM memory (flag ROMRAM). If the output string is resident in only RAM or ROM the address is supplied in location VDUOBA. If both types of memory contain the output string, the addresses of their locations are given at locations OPRAM and OPRAM.

5.2. OUTPUT DATA

The characters received from the VDU are stored in buffer BUFA.

5.3. ADDITIONAL DATA CHANGES

On leaving this program, the task active flag IOTF is reset.

6. EXTERNAL DATA TRANSFERS

PERIPHERAL VDU

6.1. INPUT

CRU BASE > 1000
TMS 9902 UART used in interface.

6.2. OUTPUT

AS ABOVE.

7. TIMING

The execution time of this program is dependent on the length of the character string to be output.

8. AUTHOR

B.T.V. WARTON.

```

TITL 'VDU I/O PROGRAMME'
♦ PROGRAMME MODULE IDENT (PROG)
  IDT 'VDUIOP'
♦ TRANSFER VECTORS OR ENTRIES
  DEF VDUID1,VDUID2,INPUT
♦ LINKED DATA MODULES
  REF 60015D,60008D,P0007D
  REF VDUIDW,VDUF,CR1712,RDR872,VDUOBA,CR,BUFA
  REF CL,CP,LINE,EDB,IOTF,DCPF,IPSF,VDUIDW
  REF OSTIME,EDS,FREE
  REF ROMRAM,OPRAM,OPROM,MDCP,MDCPSC
  RORG
  PSEG

```

```

♦♦♦♦♦♦♦♦♦♦ PROGRAMME ♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦♦
VDUID1 DATA VDUIDW,START ENTRY POINT FROM TASK HANDLER
VDUID2 DATA VDUIDW,START DIRECT ENTRY POINT
♦♦♦♦♦♦ OUTPUT SECTION
START ABS @VDUF TEST VDU FLAG
  JGT LOADA
  LI R12,>1000 LOAD CRU BASE
  SBO 31 RESET COMMAND
  LDCR @CR1712,8 LOAD COUNT & RESET LDCTRL
  SBZ 20 INHIBIT TIMER
  SBZ 13 RESET LDIR
  LDCR @RDR872,11 LOAD RDR & RESET LRDR
  LDCR @RDR872,12 LOAD XDR & RESET LXDR
  LWPI VDUIDW LOAD OTHER WP
  LI R12,>1000 LOAD CRU BASE
  LWPI VDUIDW RET TO FIRST WP
  CLR R4 CHAR REG
LOADA EQU $
  MOV @ROMRAM,@ROMRAM IS IT MIXED
  JGT MIXED
  MOV @VDUOBA,R0 GET ADDRESS OF O/P TEX
  CLR R5
NEXT CB @R0,@EDB IS CHAR END OF BUFFER MARKER
  JEQ FOUND
  MOVEB @R0+,R4 GET CHAR
  MOVEB R4,R9 SAVE CHAR
  BL @PRINT O/P CHAR
  MOVEB R9,R9 WAS CHAR -VE
  JGT NEXT
  INCT R5
  MOV @VDUOBA(R5),R0 GET NEXT ADDRESS
  JMP NEXT
♦
♦♦♦♦♦♦ MIXED DATA SECTION
MIXED MOV @OPROM,R0 GET ROM TEXT ADDRESS
  MOV @OPRAM,R1 GET RAM TEXT ADDRESS
MIXED1 CB @R0,@EDB IS CHAR END OF BUFFER
  JEQ FOUND
  MOVEB @R0+,R4 GET CHAR
  MOVEB R4,R9 SAVE CHAR
  BL @PRINT O/P CHAR
  MOVEB R9,R9 WAS CHAR -VE
  JGT MIXED1
NEXT1 MOVEB @R1+,R4 GET CHAR
  MOVEB R4,R9 SAVE CHAR
  BL @PRINT O/P CHAR
  MOVEB R9,R9 WAS CHAR -VE

```

```

        JGT  NEXT1
        JMP  MIXED1
♦
♦♦♦♦♦♦ OUTPUT CHAR SECTION
PRINT  SBO  16          TURN ON TRANSMITTER
XBRE   TB   22          WAIT FOR XBRE=1
        JNE  XBRE
        ABS  R4
        LDICR R4,8      MAKE CHAR +VE
        SBZ  16          LOAD CHAR
        RT              TURN OFF TRAN
♦
♦♦♦♦♦♦ EXIT FROM TASK
FOUND  CLR  @IOTF      RESET IOTF FLAG
        RTWP
♦
♦♦♦♦♦♦ I N P U T   S E C T I O N
INPUT  DATA VDUIOW,INPUTS
INPUTS LWPI VDUIOW
        LIM1 7
        CLR  @FREE      FREE TIME COUNTER
        CLR  R2         CHAR COUNTER
        LI   R3,BUFA    GET I/P BUFFER ADDRESS
RCVLP  INC  @FREE      INC FREE TIME COUNT
        TB  21          TEST RCVLP
        JNE  RCVLP     JUMP IF CHAR NOT REC
        STCR R4,8      STORE CHAR
        SBZ  18          RESET REC
        BL  @PRINT     ECHO CHAR
        CB  R4,@CL     IS IT CLEAR LINE
        JEQ  INPUTS    IS IT CLEAR PAGE
        CB  R4,@CP
        JEQ  INPUTS
        MOVB R4,@R3    PUT CHAR IN BUFFER
        INC  R2         INC CHAR COUNT
        CB  R4,@CR     IS CHAR CR
        JEQ  EXITLF    IS CHAR COUNT=LINE
        C   R2,@LINE
        JEQ  EXIT
        INC  R3         INC BUF ADDRESS
        JMP  RCVLP
EXIT   SETO  @MOCP     SET MOCP TASK FLAG
        INC  @MOCPSC   STIM MOCP COUNTER
        SETO  @IPSF    SET IPSF FLAG FOR MOCP
        CLR  @IOTF     RESET IOTF FLAG
        RTWP          RET TO S5TH
♦ LINE FEED SECTION
EXITLF LI  R4,>0A00    =LF
        BL  @PRINT     O/P LF
        JMP  EXIT
        END

```

PERMANENT DATA MODULE P00070

1. DESCRIPTION

This data module contains VDU, UART programming data and control characters.

2. IDENTIFICATION

PERMANENT DATA MODULE P00070

3. SIZE

10 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

      TITL 'PERMANENT DATA MODULE P0007D'
♦ PERMANENT DATA MODULE IDENTIFIER
      IDT  'P0007D'
      EVEN
      DEF  CR1712,RDR872,LINE,EOB,CR,CL,CP
      RDRG
      PSEG
CR1712 DATA >6200          CONTROL REG
RDR872 DATA >34           9600
LINE   DATA 80           80 CHAR PER LINE
EOB    BYTE >80           END OF BUFFER
CR     BYTE >0D           CARRAGE RET
CL     BYTE >18           CLEAR LINE
CP     BYTE >0C           CLEAR PAGE
      END

```

PERMANENT DATA MODULE P0008D

1. DESCRIPTION

This data module contains lists of allowed operator input instructions, inter-processor instructions, and a list of output messages for the VDU.

2. IDENTIFICATION

PERMANENT DATA MODULE P0008D

3. SIZE

440 BYTES.

4. AUTHOR

B.T.V. WARTON.


```
OPM10  BYTE >0A,>0D,>80
        TEXT -'DIAGNOSIS CODE DF1='
        TEXT -' DF2='
        BYTE >0A,>0D,>80
OPM11  TEXT -'PATIENT STATUS DF1='
        TEXT -' DF2='
        TEXT -' PR='
        TEXT -' MF1='
        TEXT -' MF2='
        BYTE >0A,>0D,>80
OPM12  TEXT -'PULSE RATE ='
        BYTE >0A,>0D,>80
OPERR  TEXT 'COMMUNICATION ERROR'
        BYTE >0A,>0D,>80
        END
```

GENERAL DATA MODULE G0009D

1. DESCRIPTION

This data module must be the first in RAM as it contains the label RAM used by the initialisation program (NSPIOP). It contains the Task Handler workspace area, the stack of storage locations for return vectors and task active flags.

2. IDENTIFICATION

GENERAL DATA MODULE G0009D

3. SIZE

CLASS TWO : 74 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'GENERAL DATA MODULE 60009D'
♦ GENERAL DATA MODULE IDENTIFIER
        IDT '60009D'
        EVEN
♦ CLASS TWO
        DEF RAM, RAM2, NSTHAW, ITRTWP, DTRTWP, MTRTWP, IPRTWP
        DEF ITWPRT, ITPCRT, ITSTRT, DTWPRT, DTPCRT, DTSTRT
        DEF MTWPRT, MTPCRT, MTSTRT, IPWPRT, IPPCRT, IPSTRT
        DEF IPSTIM, OPSTIM, MOCP, MOCPSC, MCP, IP, IPSF, TASKAN
        DEF DPRTWP, DPWPRT, DPPCRT, DPSTRT
        RORG
        PSEG
RAM      EQU    $           START OF RAM
RAM2     EQU    $+2        SECOND WORD OF RAM
TASKAN   EQU    $+10      TASK ACTIVE NUMBER
NSTHAW   BSS    6         TASK HANDLER WA
ITRTWP   BSS    6         I/P TASK WP FOR RET
DTRTWP   BSS    6         D/P TASK WP FOR RET
MTRTWP   BSS    6         MCP TASK WP FOR RET
DPRTWP   BSS    6         VDU D/P TASK WP FOR RET
IPRTWP   BSS    2         VDU I/P TASK WP FOR RET
♦ I/P TASK RETURNS
ITWPRT   BSS    2         I/P TASK WP RET
ITPCRT   BSS    2         I/P TASK PC RET
ITSTRT   BSS    2         I/P TASK ST RET
♦ D/P TASK RETURNS
DTWPRT   BSS    2         D/P TASK WP RET
DTPCRT   BSS    2         D/P TASK PC RET
DTSTRT   BSS    2         I/P TASK ST RET
♦ MCP TASK RETURNS
MTWPRT   BSS    2         MCP TASK WP RET
MTPCRT   BSS    2         MCP TASK PC RET
MTSTRT   BSS    2         MCP TASK ST RET
♦ VDU D/P TASK RETURNS
DPWPRT   BSS    2         VDU D/P TASK WP RET
DPPCRT   BSS    2         VDU D/P TASK PC RET
DPSTRT   BSS    2         VDU D/P TASK ST RET
♦ VDU I/P TASK RETURNS
IPWPRT   BSS    2         VDU I/P TASK WP RET
IPPCRT   BSS    2         VDU I/P TASK PC RET
IPSTRT   BSS    2         VDU I/P TASK ST RET
♦
IPSTIM   BSS    2         I/P TASK ACTIVE FLAG
OPSTIM   BSS    2         D/P TASK ACTIVE FLAG
MOCP     BSS    2         MCP TASK ACTIVE FLAG
MOCPSC   BSS    2         MCP STIM COUNTER
MCP      BSS    2         MICRO TO MICRO I/P MCP FLAG
IP       BSS    2         OPERATOR MCP FLAG
        END

```

GENERAL DATA MODULE G0010D

1. DESCRIPTION

This data module contains software flags which must be initialised to +1 or -1, at system start up time.

2. IDENTIFICATION

GENERAL DATA MODULE G0010D

3. SIZE

CLASS TWO : 14 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'GENERAL DATA MODULE 60010D'
♦ GENERAL DATA MODULE IDENTIFIER
        IDT '60010D'
        EVEN
♦ CLASS TWO
        DEF SETONE,SETNEG,SETEND,IPTINT,OPTINT,MOCINT
        DEF IPINT,ROMRAM,VDUF,OPINT
        RORG
        PSEG
♦ FLAGS TO BE INITIALISED TO +1
SETONE EQU $
IPTINT BSS 2          I/P TASK INT FLAG
OPTINT BSS 2          O/P TASK INT FLAG
MOCINT BSS 2          MDCP TASK INT FLAG
OPINT  BSS 2          VDU O/P TASK INT FLAG
IPINT  BSS 2          VDU I/P TASK INT FLAG
♦ FLAGS TO BE INITIALISED TO -1
SETNEG EQU $
ROMRAM BSS 2          VDU ROM RAM MIX FLAG
VDUF   BSS 2          VDU FLAG
SETEND EQU $
        END

```

GENERAL DATA MODULE GO011D

1. DESCRIPTION

This data module contains the Queue Handler program workspace area, input and output queues etc.

2. IDENTIFICATION

GENERAL DATA MODULE GO011D.

3. SIZE

CLASS TWO : 72 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'GENERAL DATA MODULE 60011D'
♦ GENERAL DATA MODULE IDENTIFIER
        IDT '60011D'
        EVEN
♦ CLASS TWO
        DEF NIOQHW, IQOS, OPOS, QIPN, QOPN, NEXTIP, NEXTOP
        RORG
        PSEG
NIOQHW BSS 32          QUEUE HANDLER WA
IQOS   BSS 16          I/P QUEUE
OPOS   BSS 16          O/P QUEUE
QIPN   BSS 2           QUEUE I/P VALUE
QOPN   BSS 2           QUEUE O/P VALUE
NEXTIP BSS 2           NEXT VALUE FOR I/P TASK
NEXTOP BSS 2           NEXT VALUE FOR O/P TASK
        END

```

GENERAL DATA MODULE G00120

1. DESCRIPTION

This data module contains the Interrupt Handler workspace areas, Input/Output workspace areas, and input and output files, necessary for the number of inter-processor communications UARTs connected to the system (in this case 3).

2. IDENTIFICATION

GENERAL DATA MODULE G00120

3. SIZE

CLASS TWO : 504 BYTES.

4. AUTHOR

B.T.V. WARTON.


```

        TITL 'GENERAL DATA MODULE 60012D'
♦ GENERAL DATA MODULE IDENTIFIER
        IDT '60012D'
        EVEN
♦ CLASS TWO
        DEF IHWA1, IDWA1, OPFIL1, IPFIL1, IPFI1S
        DEF IHWA2, IDWA2, IPFIL2, IPFI2S
        DEF IHWA3, IDWA3, IPFIL3, IPFI3S
        RORG
        PSEG
IHWA1  BSS  32          UART CRU BASE 1880  INT 5
IDWA1  BSS  32          //      //
OPFIL1 BSS  52          //      //
IPFIL1 BSS  52          //      //
IPFI1S EQU  IPFIL1+2    //      //
♦
IHWA2  BSS  32          UART CRU BASE 1900  INT 4
IDWA2  BSS  32          //      //
OPFIL2 BSS  52          //      //
IPFIL2 BSS  52          //      //
IPFI2S EQU  IPFIL2+2    //      //
♦
IHWA3  BSS  32          UART CRU BASE 1840  INT 3
IDWA3  BSS  32          //      //
OPFIL3 BSS  52          //      //
IPFIL3 BSS  52          //      //
IPFI3S EQU  IPFIL3+2    //      //
        END

```

GENERAL DATA MODULE G0013D

1. DESCRIPTION

This data module contains the Input/Output task workspace area, and the locations used by these tasks when swopping to new workspace areas.

2. IDENTIFICATION

GENERAL DATA MODULE G0013D

3. SIZE

CLASS TWO : 40 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

      TITL 'GENERAL DATA MODULE 60013D'
♦ GENERAL DATA MODULE IDENTIFIER
      IDT '60013D'
      EVEN
♦ CLASS TWO
      DEF NSPIOW,SETWP,SETPC,SETWP1,SETPC1
      RORG
      PSEG
NSPIOW BSS 32          I/P O/P TASK WA
SETWP  BSS  2          WP SETTING ADDRESS
SETPC  BSS  2          PC SETTING ADDRESS
SETWP1 BSS  2          WP1 SETTING ADDRESS
SETPC1 BSS  2          PC1 SETTING ADDRESS
      END

```

GENERAL DATA MODULE G0014D

1. DESCRIPTION

This data module contains the MOCP workspace area, and the locations used by the MOCP task to store received data.

2. IDENTIFICATION

GENERAL DATA MODULE G0014D

3. SIZE

CLASS TWO : 63 BYTES.

4. AUTHOR

B.T.V. WARTON.

```

          TITL 'GENERAL DATA MODULE 60014D'
♦ GENERAL DATA MODULE IDENTIFIER
          IDT  '60014D'
          EVEN
♦ CLASS TWO
          DEF  MOCPTW,NDF1,NDF2,NPR,NDF11,NDF22
          DEF  NPR1,NMF1,NMF2,NMF11,NMF22
          RORG
          PSEG
MOCPTW BSS 32          MOCPTW TASK WORK SPACE
NDF1   BSS 2          DF1 STORE
NDF2   BSS 2          DF2 STORE
NPR    BSS 2          PULSE RATE STORE
NMF1   BSS 2          MF1 STORE
NMF2   BSS 2          MF2 STORE
NDF11  BSS 4          DF1 VDU O/P
NDF22  BSS 4          DF2 VDU O/P
NPR1   BSS 5          PR VDU O/P
NMF11  BSS 4          MF1 VDU O/P
NMF22  BSS 4          MF2 VDU O/P
          END

```

GENERAL DATA MODULE G00150

1. DESCRIPTION

This data module contains VDU workspace areas and buffers.

This must be the last data module in RAM as it contains the RAMEND label used by the system initialisation task.

2. IDENTIFICATION

GENERAL DATA MODULE G00150

3. SIZE

CLASS TWO : 192 Bytes.

4. AUTHOR

B.T.V. WARTON.

```

        TITL 'GENERAL DATA MODULE 60015D'
♦ GENERAL DATA MODULE IDENTIFIER
        IDT '60015D'
        EVEN
♦ CLASS TWO
        DEF VDUIOW,VDUOBA,BUFA,OPROM,OPRAM
        DEF RAMEND,IOTF,FREE,VDUOIW
        RDRG
        PSEG
VDUIOW BSS 32          VDU TASK HANDLER ENTRY WA
VDUOIW BSS 32          VDU TASK DIRECT ENTRY WA
VDUOBA BSS 40          VDU O/P BUFFER ADDRESSES
BUFA   BSS 80          I/P BUFFER
OPRAM  BSS 2           O/P RAM ADDRESS
OPROM  BSS 2           O/P ROM ADDRESS
IOTF   BSS 2           VDU TASK ACTIVE FLAG
FREE   BSS 2           FREE TIME COUNTER
RAMEND EQU $          ***** END OF RAM *****
        END

```

A DISTRIBUTED MICROPROCESSOR SYSTEM FOR THE DETECTION AND DIAGNOSIS OF
CARDIAC ARRHYTHMIAS

H. A. Barker, TD, BSc, PhD, AFIMA, MInstMC, CEng, FIEE*

B. T. V. Warton, MSc, AMIEE*

Summary

The paper describes a system for the real-time monitoring of patients in coronary care units. A distributed approach allows the allocation of a microprocessor to each patient for the purposes of electrocardiogram analysis. The functions performed by these microprocessors include digital filtering of the electrocardiogram, detection and measurement of each heart beat complex, and diagnosis of arrhythmias by decision tables. The patient-connected microprocessor systems may be operated as stand-alone units, or may be connected to a further microprocessor system for the centralisation of information storage and display and operator control of the distributed system.

1. Introduction

In coronary care units (CCUs), the patients' heart rhythms are the principal indicators of their state of health. The detection and diagnosis of abnormalities in these rhythms, commonly known as arrhythmias, are therefore of prime importance in such units.

The most common method for measuring heart rhythms is by amplification of the small potential differences associated with heart action, which occur on the surface of the chest, to provide electrical signals in the form of electrocardiograms (ECGs). In the past, conventional computers have been used to assist in the detection and diagnosis of arrhythmias in ECG data (ref. 1-8). The high cost of on-line systems for this purpose, however, has precluded their widespread use in CCUs.

The advent of the microprocessor has now provided the possibility of providing a cheaper and more flexible system, not only by a direct reduction in the cost of information processing, but also by the concomitant possibility of distributing this processing throughout the system. The design and development of such a system is described here. Its object is to exploit the advantages which microprocessors can provide, and its results should benefit those whose dependence on the system may be literally a matter of life or death.

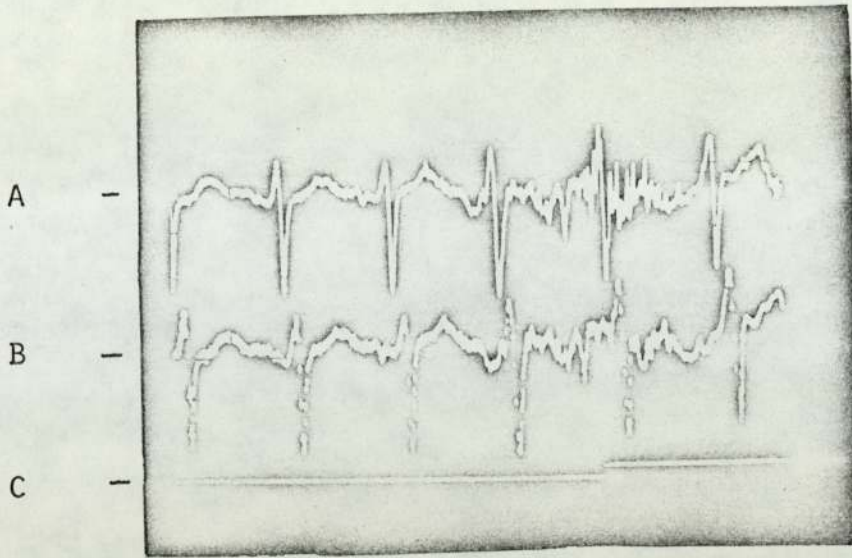
2. Analysis of system function

The overall function of the system may be sub-divided into a number of distinctly different types of function, broadly classified as follows:

Signal acquisition: this function is concerned with the generation of a primary ECG signal (Fig. 1), by amplifying the chest electrode potentials. It is a function which is performed satisfactorily by analogue equipment in common 'bedside' use in CCUs, and will not be considered in detail here.

Signal conditioning: this function is concerned with the processing of a primary ECG signal, to obtain a conditioned signal (Fig. 1) from which measurements may be taken with an appropriate degree of confidence. The advantages of digital methods for this purpose are such that this function is best performed by a microprocessor, and the approach adopted here is described in Section 4.1.

* Department of Electrical Engineering, University of Aston in Birmingham



- A PRIMARY ECG SIGNAL
- B CONDITIONED ECG SIGNAL
- C NOISE DETECTION INDICATOR

FIGURE 1 ECG SIGNALS

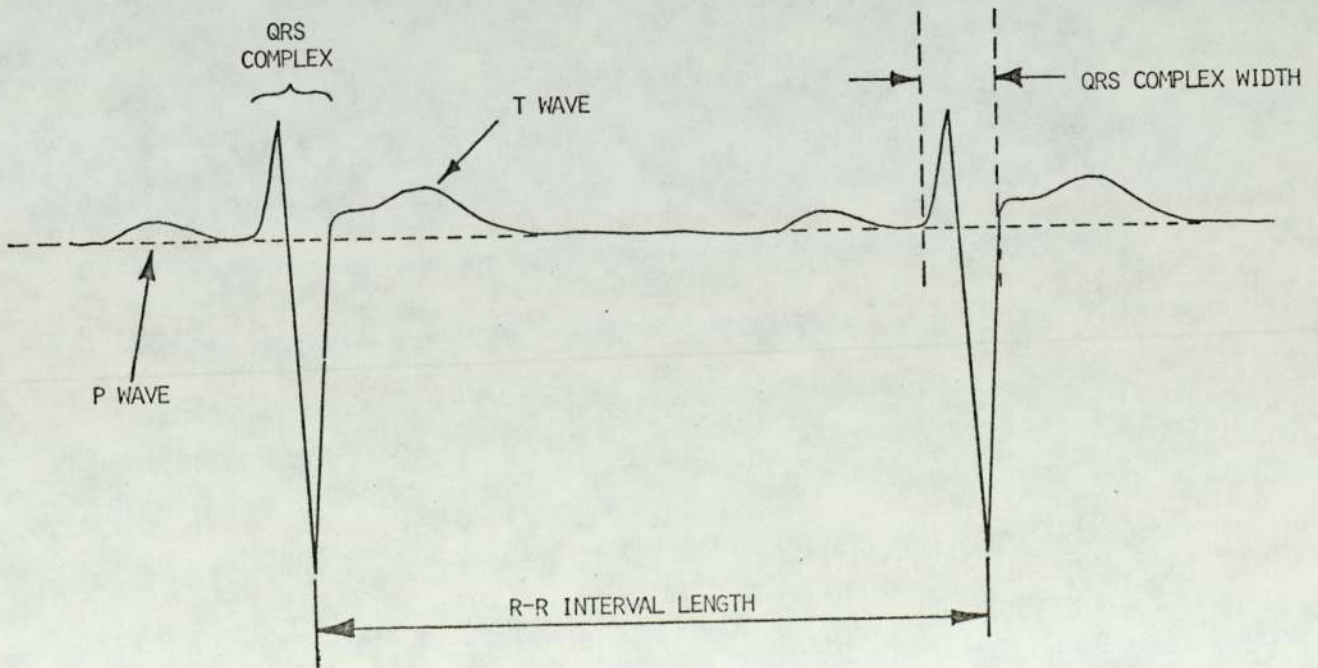


FIGURE 2 ECG CHARACTERISTICS

Signal monitoring: this function is concerned with the extraction of parameter measurements from a conditioned ECG signal. Attention here is focussed principally on the length of the R-R interval and the width of the QRS complex (Fig. 2), as described in Section 4.2.

Diagnosis: this function is concerned with the assessment of results obtained by monitoring. A decision table approach is used here, as described in Section 4.3.

Display: this function is concerned with the presentation of information, such as ECG data, parameter values, diagnoses and trends, to an operator.

Storage: this function is concerned with the retention of information concerned with display, using appropriate media.

In addition to these specific functions, the general functions of communication and control are pervasive throughout the system.

3. System structure

In order to determine a suitable structure for the system, it is necessary to examine the functions outlined in Section 2, and the information flows between them, as shown in Fig. 3. Only the signal acquisition function is of necessity distributed in the system, since this must be allocated on a one-per-patient basis. The remaining functions may be structured as required. Since the highest rates of data transfer occur permanently between the signal acquisition, conditioning and monitoring functions, the greatest benefits of distributed processing are obtained if each of these functions is allocated on a one-per-patient basis, and this arrangement is therefore adopted as the foundation of the system structure.

Within this arrangement, the allocation of processors to functions, or vice-versa, is not a procedure capable of simple or precise quantification. Some indication of an appropriate form of solution may however be obtained by assessing the degree of utilisation of a typical modern microprocessor in the performance of each function. With this approach, a particularly simple form of solution is obtained because the assessments show that, for a single patient, total performance of all the functions shown in Fig. 3 is well within the capability of a TMS 9900 16-bit microprocessor. These considerations therefore indicate that a system completely distributed on the basis of one such processor per patient is the most suitable structure for this application.

A structure in which all functions are distributed on a one-per-patient basis has the obvious advantage of flexibility, and for this reason each processor in the system is provided with the capability of operating in a stand-alone mode. There are, however, other factors which militate against complete distribution of the display and storage functions; these include the cost of peripheral devices associated with these functions and the management requirement for centralisation of the facilities which these functions provide.

In the final system structure, therefore, all functions, except those concerned with centralised display and storage, are distributed to patient-dedicated processor systems. These systems, although capable of stand-alone operation if required, normally perform only those functions upto and including diagnosis, and the information obtained from their operation is communicated to the centralised display and storage facilities under the control of an operator-dedicated processor system (Fig. 4).

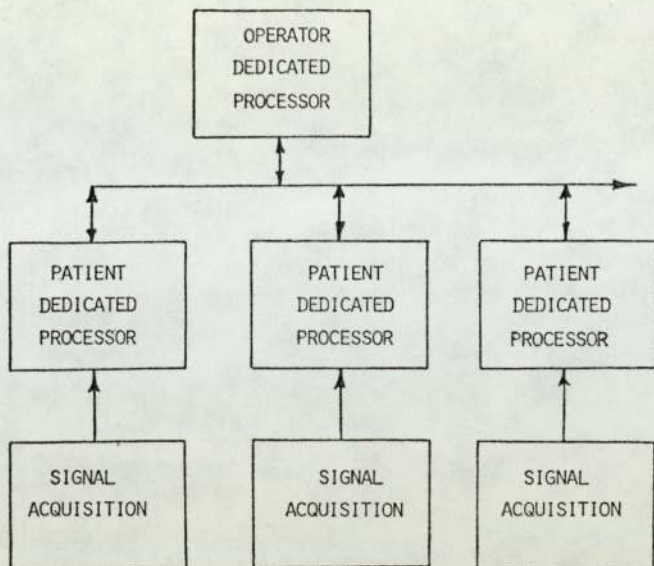


FIGURE 4 STRUCTURE OF DISTRIBUTED SYSTEM

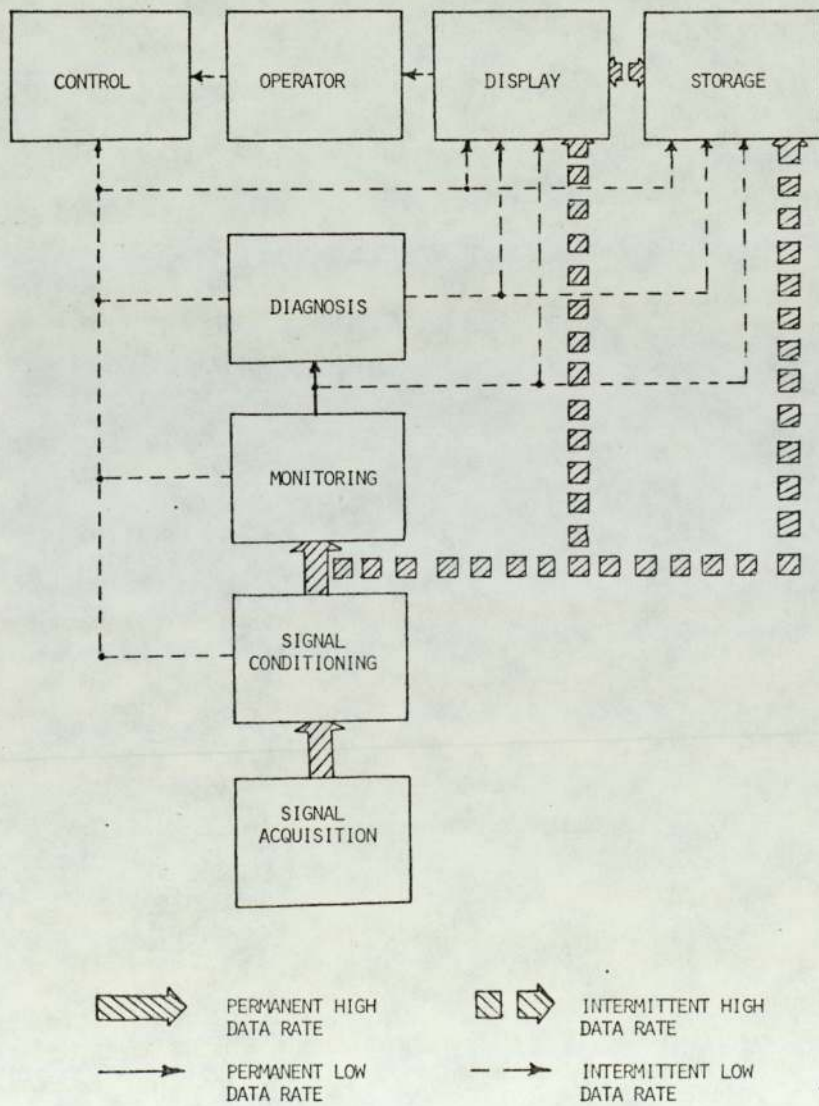


FIGURE 3 SYSTEM FUNCTIONS AND INFORMATION FLOWS

4. Patient-dedicated processor system design

Each patient-dedicated processor system performs the functions of signal conditioning, monitoring, diagnosis and communication, under the control of an operating system in the form of a real-time scheduler. The only function in any way dependent on the structure of the remainder of the system is that of communication; this is normally concerned with inter-processor communication, but must be concerned with operator communication when in the stand-alone mode.

4.1 Signal conditioning

The purpose of signal conditioning is to improve the consistency of subsequent signal monitoring, by the removal of very low frequency components (d.c. and base-line drift), and the reduction of intermittent high frequency components (artifact), from the primary ECG signal. A sketch of the normal ECG spectrum, as obtained by Golden et. al. (ref. 9) is shown in Fig. 5.

The required signal conditioning is accomplished by an adaptive digital filtering algorithm, applied to samples of the primary ECG signal which are obtained, as recommended by Wartak et. al. (ref. 10), at a rate of 250 Hz with 8-bit resolution. A block diagram of the digital filter is shown in Fig. 6. The d.c. and base-line drift is removed by a second-order high-pass filter with 0.5 Hz cut-off frequency, and the artifact is reduced by an adaptive arrangement in which the parameter settings have been determined experimentally. The presence of artifact is detected when the output of a second-order high-pass filter with 60 Hz cut-off frequency exceeds a threshold, in which case the output of a second-order low-pass filter with 25 Hz cut-off frequency is used in preference to an unfiltered signal. This approach allows the detection of artifact to be indicated (Fig. 1) through the diagnosis function to the operator, to show in a simple fashion that a temporary decrease in diagnosis confidence might be expected.

The delays of N and n samples, shown in Fig. 6, are chosen to equalise the total delays through the 25 Hz low-pass filter and the direct path, and also to ensure that the filtered signal is introduced just prior to the occurrence of the artifact to be reduced. The delayed hold ensures that the low-pass filter remains in continuous operation when rapid bursts of artifact are present. The filtering algorithm execution time is 1 ms, which is well within the 4 ms sampling period. A short execution time, together with a relatively simple programme, are due mainly to the availability of a single instruction for a 16-bit multiplication operation with the TMS 9900 microprocessor.

4.2 Monitoring

Measurements are performed on the conditioned ECG signal after the detection of each QRS complex (Fig. 2), which is accomplished by a delayed-difference threshold method. A signal is obtained as the difference between samples which are separated by 6 sample periods (24 ms), and compared with a threshold which is 60% of the average minimal negative value of the signal (Fig. 7), as suggested by Van Eyll et.al. (ref. 11). The measurements which are then performed are those necessary for the subsequent diagnosis of certain arrhythmias, using the method of Rabin et.al. (ref. 8). Although their particular approach has been adopted here, the scope of the measurements could easily be extended to provide the data for any diagnostic method.

In this case, the primary measurements are the length of the R-R interval and the width of the QRS complex (Fig. 2). The R-R interval length is compared with the average R-R interval, relative to which it is classified

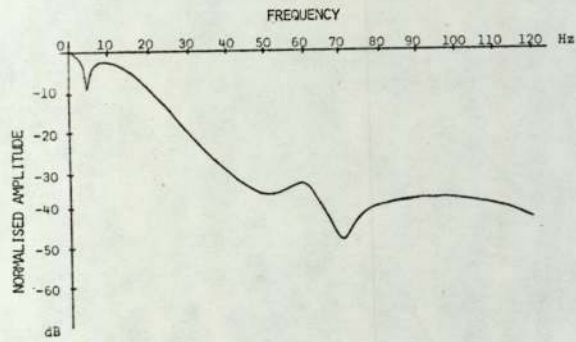


FIGURE 5 ECG SPECTRUM

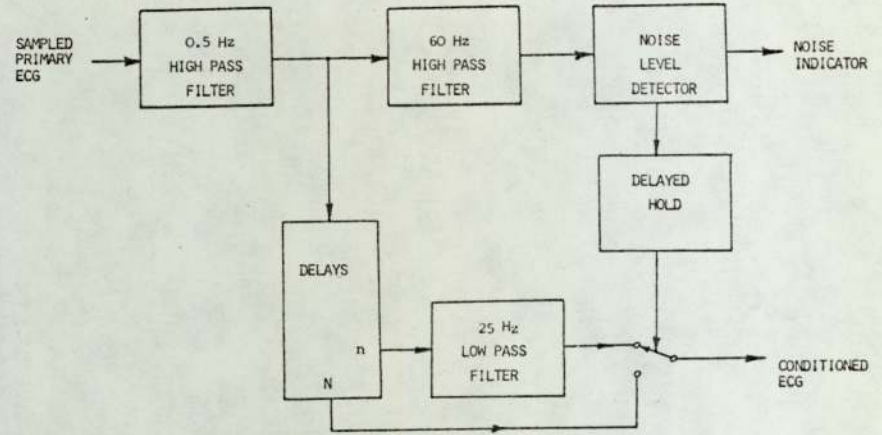


FIGURE 6 BLOCK DIAGRAM OF ADAPTIVE DIGITAL FILTER

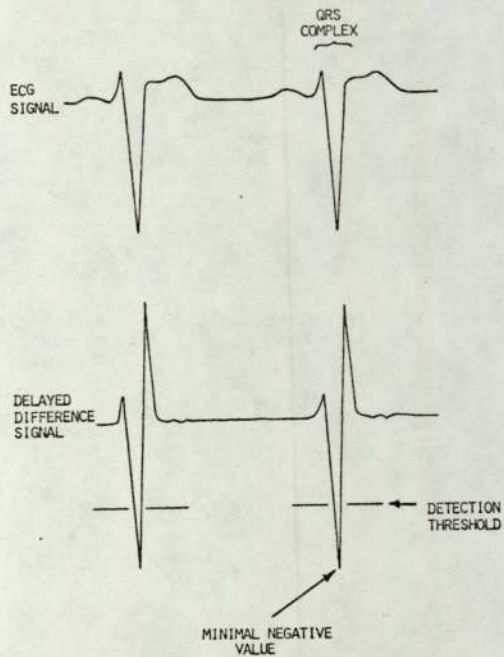


FIGURE 7 DELAIED-DIFFERENCE DETECTION OF QRS COMPLEX

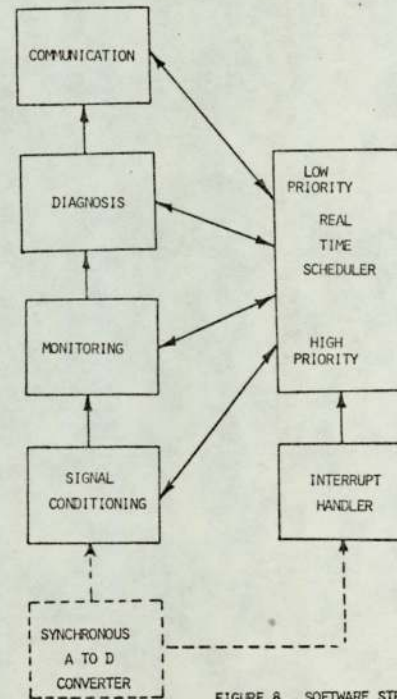


FIGURE 8 SOFTWARE STRUCTURE OF PATIENT DEDICATED PROCESSOR

as normal (N), short (S) or long (L). Normal R-R interval lengths are used to update the R-R interval average, which is compared with standard intervals corresponding to various pulse rates. The QRS complex width is compared with a standard interval of 120 ms, relative to which it is classified as wide (WQRS) or normal.

The measurements are used, together with previous measurements, in a number of tests, as shown in Table 1. Each test has either a true or false result, corresponding to which bits are set or reset in two 16-bit words for subsequent use in the diagnosis function. A shorthand notation is used to specify certain sequence tests; for example, a sequence consisting of an R-R interval which is short, followed by a QRS complex which is wide, followed by an R-R interval which is not short, all repeated 4 times, is written $4[S \rightarrow WQRS \rightarrow \bar{S}]$.

4.3 Diagnosis

Diagnosis is concerned with the recognition of specific arrhythmia conditions from the bit patterns of the words obtained by monitoring. The approach adopted here is to use decision tables (ref. 12), and an example of one of the tables used is shown in Table 2. The actual testing of bit patterns in a word is very simple with the TMS 9900 microprocessor, because of the availability of a single instruction (COC) for testing a word for a pattern of bits required to be set, and a single instruction (CZC) for testing a word for a pattern of bits required to be reset. To diagnose Bradycardia, a slow pulse rate condition, for example, the decision table in Table 2 defines the pattern required and it is only necessary to compare the first monitored word in Table 1 with CO_{16} , using the COC instruction, and with $3F_{16}$, using the CZC instruction, and if both tests are satisfied the diagnosis is established. On completion of a diagnosis such as this, other decision tables are then used to test for other possible diagnoses.

4.4 Communication

The communication function is concerned with the transfer of the information shown in Fig. 3, either to the operator-dedicated processor system in normal operation, or to the display and storage facilities directly in the stand-alone mode. In both cases an asynchronous serial data channel is used, and the receiver-transmitter is implemented by a dedicated TMS 9902 asynchronous communications controller specifically designed for use with the TMS 9900 microprocessor.

4.5 Control

All patient-dedicated functions operate under the control of a real-time scheduler. The operating priority of a function is the inverse of its position in the system hierarchy, and the signal conditioning function, which occupies the lowest position in the system hierarchy, therefore has the highest operating priority. This function is activated by an interrupt from the analogue-digital converter as each ECG sample is obtained, and each remaining function is then activated by the next highest priority function as the data flows through the system (Fig. 8). The real-time scheduler, however, suspends the operation of lower priority functions when a higher priority function is active, so each higher priority function is allowed to run to completion before the lower priority function is commenced.

EVENT		WORD 1 SET BIT
PULSE RATE IS GREATER THAN 140 BEATS PER MINUTE		0
PULSE RATE IS GREATER THAN 110 BEATS PER MINUTE		1
PULSE RATE IS GREATER THAN 100 BEATS PER MINUTE		2
PULSE RATE IS GREATER THAN 90 BEATS PER MINUTE		3
PULSE RATE IS GREATER THAN 80 BEATS PER MINUTE		4
PULSE RATE IS GREATER THAN 60 BEATS PER MINUTE		5
PULSE RATE IS GREATER THAN 40 BEATS PER MINUTE		6
PULSE RATE IS GREATER THAN 20 BEATS PER MINUTE		7
		8
A QRS COMPLEX HAS OCCURRED DURING THE LAST 6 SECONDS		9
CURRENT R-R INTERVAL IS NOT LESS THAN TWICE THE AVERAGE		10
CURRENT R-R INTERVAL IS LONG		11
CURRENT R-R INTERVAL IS SHORT		12
CURRENT QRS COMPLEX IS WIDE		13
MORE THAN 82% OF PREVIOUS QRS COMPLEXES ARE WIDE		14
		15
EVENT		WORD 2 SET BIT
A SEQUENCE 4 [S→ \bar{S}]	HAS OCCURRED	0
A SEQUENCE 4 [S→WQRS→ \bar{S}]	HAS OCCURRED	1
A SEQUENCE 4 [S→ \bar{S} →N]	HAS OCCURRED	2
A SEQUENCE 4 [S→WQRS→ \bar{S} →N]	HAS OCCURRED	3
A SEQUENCE S→ \bar{S} →S	HAS OCCURRED	4
A SEQUENCE S→ \bar{S} →N→ \bar{L}	HAS OCCURRED	5
A SEQUENCE 3 [S]→WQRS	HAS OCCURRED	6
A SEQUENCE S→ \bar{S} →L	HAS OCCURRED	7
A SEQUENCE S→ \bar{S} →N→L	HAS OCCURRED	8
		9
		10
		11
		12
		13
		14
		15

TABLE 1 TESTS PERFORMED IN ECG MONITORING

EVENT	WORD 1 BIT	TRUE				ELSE
		F	F	F	F	
PULSE RATE 140	0	F	F	F	F	-
PULSE RATE 110	1	F	F	T	F	-
PULSE RATE 80	4	F	F	T	T	-
PULSE RATE 60	5	F	F	T	T	-
PULSE RATE 40	6	T	F	T	T	-
PULSE RATE 20	7	T	T	T	T	-
QRS IN LAST 6 SECONDS	9	-	-	-	F	-
BRADYCARDIA		X				
IDIOVENTRICULAR RHYTHM			X			
SUPRAVENTRICULAR RHYTHM				X		
LOST SIGNAL					X	
NEXT TABLE		X	X	X	X	X

TABLE 2 EXAMPLE OF DECISION TABLE DIAGNOSIS

5. Operator-dedicated processor system design

When the display and storage functions are centralised, an operator-dedicated processor system is required to act as a centre for communication and control between the patient-dedicated processor systems, and the display and storage facilities. As the majority of processing in the system is distributed, the data flows in the operator-dedicated system are low and consist mainly of routine information such as pulse rates and arrhythmia diagnoses. During normal operation, this information is simply repeated by the operator-dedicated system to a visual display unit, where it may be viewed by an operator.

There is, however, the requirement for information storage in the system, and although this function has not yet been implemented, its general characteristics may be described. A particular requirement is for the storage of those parts of the ECG signals which contain significant arrhythmia events. The data rates required for this are somewhat higher than those concerned with routine information, but the occurrence of such events is normally intermittent. Therefore a serial data transmission channel to the appropriate magnetic media, under the control of the operator-dedicated system, will be a suitable implementation for this function.

When the storage function is implemented, the control function will be extended to allow the recall of stored data to the visual display unit by an operator. At this stage it may be necessary to re-appraise the method of system management by the operator-dedicated system. It is not, however, envisaged that more than one TMS 9900 microprocessor will be required in the operator-dedicated system to service all the patient-dedicated systems in a normal CCU.

6. Conclusions

In an on-line system for the detection and diagnosis of arrhythmias in the ECGs of patients in CCUs, the use of microprocessors allows the data processing to be distributed as required. Examination of the functions and information flows within the system, in the context of modern microprocessor capability, indicates that in the preferred system structure the majority of functions are allocated to patient-dedicated 16-bit microprocessor systems, with the display and storage functions centralised in an operator-dedicated 16-bit microprocessor system.

The design of a system with this structure has been described in this paper. Methods for realising each function have been examined, and the nature of a microprocessor implementation discussed. In particular, the advantages of the powerful instruction set associated with a 16-bit microprocessor has been demonstrated.

The system is shown to be flexible, not only in respect of the hardware configuration, which allows each patient-dedicated system to operate on a stand-alone basis if required, but also in respect of the software functions. Although a particular diagnostic method has been adopted in the system described, the implementation of other diagnostic methods, involving further monitoring measurements, could be implemented in new software fairly easily.

7. Acknowledgments

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