# Functionalisation of graphene as a tool for developing nanomaterials with predefined properties

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#### **Abstract**

Graphene based nanomaterials (GBN) have been recently applied in a broad range of science and technology fields such as nanobiomedicine, electronics, energy storage and power generation exploiting their unique electronic structure, physical properties, and opportunities for modifying their surface using covalent and non-covalent interactions. In the present review we systematised the origins of GBN functionalisation using organic and inorganic molecules, polymers, biomolecules, and anticancer drugs. We show that varying the procedure of GBN functionalisation allows to obtain nanomaterials with desired properties that can be applied to the development of materials with enhanced physicochemical properties, nanoplatforms for drug delivery, nanobiosensors for detection of various biomolecules, as well as nanomaterials for bioimaging and diagnostics. The review can be useful for experts in the fields of material science and nanobiomedicine.

*Keywords:* graphene, graphene oxide, functionalization, nanobiomaterials, drug delivery, nanobiosensors, bioimaging.

#### 1. Introduction

Graphene based nanomaterials (GBN) such as graphene oxide (GO), graphene, and reduced graphene oxide (rGO) have been at the forefront of research due to their unique structure and distinguished physico-chemical properties (Table 1). One of the most important application of GBN is biomedicine: tissue engineering [1], bioimaging [2,3] targeted anticancer drug delivery [4–9], biosensors [10–12], development of antiviral [13–16], antibacterial [17–20], antifungal materials [21,22], as well as the delivery of biomolecules such as enzymes [23,24], proteins [25–27], genes [28–30], RNA [31,32], and DNA [33,34]. In addition, GBN were used as materials for energy applications (fuel cells [35,36], batteries [37,38], solar cells [39,40]), for manufacturing smart materials [41], nano-enhancers to design heat transfer media with better thermal performance [42–44] and for water disinfection and desalination [45–47]. Fig. 1 summarises the publications distribution in these research areas.

GBN can be functionalised through covalent [48–52] and non-covalent [53–57] interactions. Functionalisation of GBN leads to the enhancement of their electrical [58,59], optical [60,61], thermal [62,63], electronic [64–66], and mechanical [67,68] properties. Graphene is a monolayer carbonaceous material [69] that can be prepared in the form of single or multilayered flakes depending on the method of preparation [70]. It can be synthesised using various methods such as chemical vapour deposition (CVD) [71–77], electrochemical exfoliation of graphite [78–83], mechanochemical exfoliation of graphite [84] as well as chemical and thermal reduction of GO resulting in the formation of rGO [85–91].

Graphene is composed of sp<sup>2</sup>-hybridised hexagonal carbon atoms forming twodimensional nanolayers, while GO contains various oxygen functional groups distributed on the surface such as carboxyl, carbonyl, and lactol at the edges of GO layers in addition to epoxy and hydroxyl groups on the basal plane [92–97], (Fig. 2). rGO is a form of GO in which most of the oxygen-containing functional groups are reduced by such agents as hydrazine hydrate or biomolecules [98,99].

A single layer of graphene was isolated in 2004 by Andrei Geim and Konstantin Novoselv [100], while GO was synthesised for the first time in 1859 by Benjamin Brody by oxidising graphite using a mixture of oxidising agents potassium chlorate and fuming nitric acid [101]. However, the most efficient method was developed by William Hummers and Richard Offeman in 1957 using the oxidising mixture of sulphuric acid, sodium nitrate, and potassium permanganate [102].

This review summarises approaches for the covalent and non-covalent functionalisation of GBN. Due to multifunctional groups located on the GO surface as well as the presense of sp<sup>2</sup>-hybridised carbon atoms, further functionalisation of GBN can be conducted with the molecules of various nature. A multitude of organic reactions (Fig. 3) can be carried out: amidation, esterification, 1,3-dipolarcycloaddition, halogenations, as well as hydrogen bonding,  $\pi$ – $\pi$  stacking interactions, and hydrophobic interactions.

These reactions allow to obtain unique materials for biomedical applications, such as cancer treatment [103], drug and biomolecules delivery [104,105], development of biosensors [106] and materials with antiviral [107], antibacterial [108], and antifungal properties [109]. This review demonstrates that among GBN, GO has the highest potential for the applications in nanomedicine due to the following reasons. (*i*) GO consists of various functional groups which allow to perform further functionalisation of the surface. (*ii*) The functionalisation of GO increases its biocompatibility. (*iii*) The presence of oxygen-containing functional groups provides the stability of GO aqueous dispersions.

#### 2. Functionalisation of GBN

## 2.1 Graphene conjugation with organic molecules

Graphene structure can be covalently or non-covalently functionalised with organic molecules using amidation, esterification, and halogenation reactions. Hossain et al. [110] studied the diazotisation of graphene obtained by epitaxial growth method (G-epitaxial) on SiC. The authors demonstrated that the basal plane of graphene can be functionalised with such organic molecule as 2-aminoethanethiol (HS-C<sub>2</sub>H<sub>4</sub>-NH<sub>2</sub>) using diazotisation reaction. In addition, it was found that amine diazonium salts undergo spontaneous reduction resulting in functionalisation of the graphene surface with HS-C<sub>2</sub>H<sub>4</sub> residues leading to G-thioethyl (GT). In their further work [111] Hossain et al. performed the covalent immobilisation of AuNPs on the surface of GT. The -SH-groups of GT were treated with HAuCl<sub>4</sub> with subsequent reduction by NaBH<sub>4</sub>. Thus, Au was covalently attached to graphene through -S-Au bond. Then, the immobilised AuNPs were modified with such sulphur-containing molecules as hexanedithiol (HSC<sub>6</sub>H<sub>12</sub>SH). The resulting assembly with graphene can be used for loading various sulphur-containing biomolecules through the formation of an Au-S linkage (Fig.4).

Wang et al. [112] developed a covalent functionalisation with 3-aminopropyltriethoxysilane (APTS) through the hydroxyl groups on the graphene surface using DCC as a catalyst (Fig. 5). De Sousa et al. [113] presented the covalent functionalisation of GO with mannosylated ethylenediamine, the reaction proceeded through EDC/NHS coupling (Fig. 6). Shang et al. reported that GO was covalently functionalised with N-heterocyclic carbene–palladium complex (NHC-Pd<sup>2+</sup>) for the application as an efficient catalyst for Suzuki–Miyaura coupling reactions [114].

Qian et al. presented the procedures of covalent functionalisation for graphene quantum dots where graphene surface was functionalised with organic molecules including dialcohols, diamines, and dithiols for bioimaging applications [115]. Yu et al. performed DFT study of non-covalent interaction between graphene and some aromatic molecules including thiophene (T), benzene (B) and pyridine (P). According to the study the aromatic rings of these molecules were placed on the top of the graphene surface at the height of 0.35 nm in parallel or vertical orientation. The results demonstrated that the interaction between the two polar molecules (T, P) and graphene is weaker than that of the nonpolar molecule (B). In addition, the non-covalent interactions between the aromatic molecules and graphene surface mainly originates from the  $\pi$ –  $\pi$  stacking between the  $\pi$  electrons of aromatic compound and graphene [116].

#### 2.2 Graphene conjugation with inorganic molecules

Graphene surface can be functionalised with inorganic molecules including metal and metal oxide nanoparticles. Poh et al. [117] developed a method of graphene's halogenation (Fig. 7) through the covalent attachment of chlorine, bromine, or iodine. In this method graphite oxide (GrO) was prepared from graphite by oxidation followed by the thermal exfoliation of GrO with the formation of rGO (TRGO). The obtained nanomaterials can be used in the development of electronic and electrochemical devices.

Lai et al. [118] presented the synthesis of brominated graphene via electrophilic substitution reaction using N-bromosuccinimide (NBS) in aqueous solution of sulfuric acid to stimulate the decomposition of NBS and facilitate the formation of bromine cations. Then, these cations acted as electrophiles and covalently bonded to the defect sites of rGO (mostly sp<sup>2</sup> C–H) located at the edges of graphene flakes. The authors introduced a reaction mechanism based on the electron exchange reaction. It is well known that carbon atoms of the rGO lattice are

electron-rich due to sp<sup>2</sup> -hybridisation and they possess negative partial charge while bromine cations are electron-deficient and therefore possess partial positive charge. Thus, the generated bromine cations could be covalently attached to the defects of rGO (Fig. 8).

Dong et al. demonstrated the possibility of the reaction between GO and FeCl<sub>3</sub> [119]. Coordination bonds were formed between Fe<sup>3+</sup> and hydroxyl groups of GO at the edges of the flake (Fig. 9). Literature analysis shows that GBN were non-covalently functionalised with metal nanoparticles for biosensing and antibacterial applications, for instance, silver nanoparticles (AgNp) [120–128], gold nanoparticles (AuNp) [129–136], and platinum nanoparticles (PtNp) [137–142]. In addition, the non-covalent functionalisation of GBN with metal oxide nanoparticles (ZnO [143–146], CuO [147,148] allows to obtain nanomaterials for the development of antimicrobial pharmaceutics and biochemical sensors for single stranded RNA detection. At the same time, covalent and non-covalent functionalisation of GBN with Fe<sub>3</sub>O<sub>4</sub> magnetic nanoparticles allow to obtain nanomaterials for drug delivery and cancer sensing [149–154] (see Table 2).

## 2.3 Graphene conjugation with polymers

Graphene and GO can be functionalised with various polymers through covalent [155] and non-covalent interactions [55]. The obtained nanomaterials can be used in energy applications, catalysis, and biomedicine [156–158]. Fang et al. [159] performed the covalent functionalisation of graphene nanosheets with linear polystyrene (PS, M= 60 kDa) for preparing nanocomposites with enhanced mechanical properties (increased tensile strength and Young's modulus by 70% and 57% in comparison with individual PS). At first, the authors prepared GO using modified Hummers and Offeman's method then reduced it using hydrazine hydrate to rGO sheets. Then, hydroxylated graphene (G-OH) was synthesised *via* diazonium addition reaction in

the presence of 2-(4-aminophenyl) ethanol and isoamyl nitrite. The obtained G-OH was treated with triethanolamine and 2-bromopropionyl bromide to prepare graphene-based initiator. Finally styrene was added to the graphene-based initiator in the presence of methyl-2-bromopropionate (MBP), CuBr and N,N,N',N',N''-pentamethyl-diethylenetriamine (PMDETA) to synthesise polystyrene covalently functionalised with graphene nanosheets (Fig. 10).

Cano et al. [160] demonstrated the possibility of covalent functionalisation of GO with poly(vinyl alcohol) (PVA) for enhancing the mechanical properties of PVA. As a result, the authors demonstrated 60% improved Young's moduli and 400% tensile strength compared to non-modified PVA. The authors performed carbodiimide coupling of GO with (PVA, M= 6-500 kDa) using N,N'-dicyclohexylcarbodiimide (DCC) and 4-dimethylaminopyridine (DMAP) to produce GO-PVA conjugate (Fig. 11). Wan et al. [161] performed the covalent functionalisation of GO surface with diglycidyl ether of bisphenol-A (DGEBA) (Fig. 12), resulting in the formation of (DGEBA–GO) polymers with improved thermal stability and mechanical properties such as enhanced tensile strength (61–75% increase) and fracture toughness (29–41% increase) compared to non-modified DGEBA.

Xu et al. [162] demonstrated the covalent functionalisation of GO with 6-armed PEG-NH<sub>2</sub>. At first the authors converted 6-armed PEG-OH to 6-armed PEG with six amino end groups (6-armed PEG-NH<sub>2</sub>) according to the protocol applied by Mei et al. [163] with subsequent covalent functionalisation of GO surface by 6-armed PEG-NH<sub>2</sub> through amidation reaction using EDC·HCl as a coupling agent. The obtained nanomaterial GO-PEG-NH<sub>2</sub> was applied as a drug delivery system for paclitaxel (PTX). The cytostatic was attached by non-covalent functionalisation through  $\pi$ - $\pi$  stacking and hydrophobic interactions (Fig. 13). In

addition to these covalent conjugates, GBN was applied as additives to various nanocomposite materials.

Yu et al. performed the modification of polystyrene (PS) with 2 wt % GO and obtained materials with superior anti-corrosion properties (protection efficiency against corrosion increased from 37.90% to 99.53% in comparison to PS), increased thermal stability (from 73 for PS to 372 °C for GO-PS) and enhanced mechanical properties (the storage modulus increased from 1808.76 MPa for PS to 2802.36 MPa for GO-PS) [164]. Deshmukh et al. carried out the synthesis of a nanocomposite based on polyvinylchloride (PVC) modified with GO (the quantity of GO varied from 0.5 to 2.5 wt %). It was demonstrated that the incorporation of GO to PVC leads to decrease in surface roughness through improving the values of contact angle [165]. Ovcharenko et al. demonstrated that GO-poly(carbonate-urea)urethane nanocomposite can be applied in the development of artificial heart valves due to its superior mechanical properties, hemocompatibility, and calcific resistance of nanocomposites [166]. Kumar et al. revealed that the nanocomposite based on sulfonated GO and sulfonated polyether ether ketone (SGO-SPEEK) demonstrated high proton conductivity of 0.055 S cm<sup>-1</sup> at 80<sup>o</sup>C and 30% RH compared to the non-modified SPEEK (0.015 S cm<sup>-1</sup>). Thus, the obtained nanomaterial can be used for the development of fuel cells [167].

#### 2.4 Graphene conjugation with anticancer drugs

Literature shows that GBN was conjugated with anticancer drugs through noncovalent interaction of the drug with graphene surface. Zhang et al. [168] reported that covalent functionalisation of GO with sulfonic acid groups and folic acid (GO-SO<sub>3</sub>H-FA) allowed to increase the specificity towards MCF-7 cells (human breast cancer cell line). Addition of anticancer drugs (doxorubicine (DOX) and camptothecin (CPT)) through non-covalent

functionalisation (due to  $\pi$ – $\pi$  stacking and hydrophobic interactions between the drugs and the GO surface) significantly increase the therapeutic efficacy in comparison with individual drugs. The amount of CPT and DOX on GO-SO<sub>3</sub>H-FA-CPT-DOX was calculated to be 4.5 % and 400% respectively.

Wang et al. [104] demonstrated that the covalent functionalisation of GO with chlorotoxin (CTX) increases the drug delivery to C6 glioma cells. At the same time, non-covalent attachment of DOX with the capacity of 570 mg DOX per gram CTX-GO significantly increases the efficiency of the conjugate (the release of the drug was pH dependent). Fan et al. [169] synthesised covalent conjugate based on GO with adipic acid dihydrazide and sodium alginate (SA). Then, DOX·HCl was non-covalently attached to GO-SA, the maximum capacity of DOX on GO-SA was 1.8 mg/mg GO-SA with the best drug release rate at pH 5.0. The cytotoxicity measurements demonstrated that GO-SA conjugate did not bear toxicity while GO-SA/DOX showed cytotoxicity towards HeLa (human cervical carcinoma cell line) through specific targeting of CD44 receptors.

Qin et al. [170] prepared GO non-covalently conjugated with polyvinylpyrrolidone (PVP, M=30 kDa) and then folic acid (FA) was covalently attached to COOH groups of GO through amide bond formation followed by the non-covalent attachment of DOX to the surface of FA–GO–PVP (through  $\pi$ – $\pi$  stacking and hydrophobic interactions). The load ratio of DOX on FA–GO–PVP was calculated to be 107.5 wt%. The obtained conjugate demonstrated high anticancer efficacy on HeLa cells. Huang et al. [171] described the ability of GO functionalised with FA to efficiently load chlorin e6 photosensitiser for targeted photodynamic therapy. Tiwari et al. [172] used GO-PVP non-covalent conjugate for the dual non-covalent attachment of quercetin (QS) and gefitinib (GF) and compared it with the GO-PVP-QS and GO-PVP-GF conjugates. The

authors found that the combined drug loading had high cytotoxicity against PA-1 cells (ovarian cancer cell line) compared with the individual drugs and the free drugs. The amount of QS and GF in GO-PVP-QS-GF was equal to 20 and 46% respectively.

GO was functionalised with polyethylene glycol, FA, and CPT by non-covalent  $\pi$ – $\pi$  stacking interactions (CPT percentage was 45%) and achieved 76% cytotoxicity towards MCF-7 (breast cancer cell line) at the highest applied concentration (100 μg·ml<sup>-1</sup>) [173]. In addition, magnetic GO surface was grafted by β-cyclodextrin (β-CD, M=1.1 kDa) for the delivery of DOX and methotrexate (MTX). The cytotoxicity results on K562 cells (leukemia cell line) showed decreasing cell viability by 65% and 55% at the concentration of 16 μg·ml<sup>-1</sup> for GO-Fe<sub>3</sub>O<sub>4</sub>-β-CD-DOX (37.4% of DOX ) and GO-Fe<sub>3</sub>O<sub>4</sub>-β-CD-MTX (23.4% of MTX ), respectively [174].

GO was functionalised with natural polymer chitosan (CS) and FA for the delivery of CPT and 3,3'-diindolylmethane (DIM). The obtained conjugate (GO-CS-FA-CPT-DIM) demonstrated increased cytotoxicity against MCF-7 cell line using MTT assay (95.67 % decrease of the cell viability) that was significantly higher in comparison with the pure drugs DIM (42.4 %) and CPT (52.59 %) [175]. Pei et al. revealed that the simultaneous attachment of Pt and DOX to GO surface functionalized with PEG (pGO) (pGO-Pt-DOX, weight ratio: 1:0.376:0.376) leads to enhanced cytotoxicity against both Cal-27 (human squamous cell carcinoma cell line) and MCF-7 (breast cancer cell line). The authors observed a higher inhibition rate for the pGO-CP-DOX conjugate in comparison with individual drugs: IC<sub>50</sub> (MCF-7) =14.5 μg·ml<sup>-1</sup> for pGO-Pt-DOX, 22.5 μg·ml<sup>-1</sup> for pGO-DOX and 22 μg·ml<sup>-1</sup> for pGO-CP [176]. Bullo et al. demonstrated the possibility of GO functionalisation with PEG, FA, and anticancer drugs protocatechuic acid (23.47% PCA) and chlorogenic acid (18.33% CA-). The authors studied the conjugate GO-PEG-FA-PCA-CA against two cancer cells HT29 (colon cancer cells) and HePG2 (human liver cancer

cells). Cytotoxicity experiments revealed the following results: IC<sub>50</sub> (HT29) = 50.69 μg·ml<sup>-1</sup>, IC<sub>50</sub> (HepG2) = 40.39 μg·ml<sup>-1</sup>[177]. Gong et al. demonstrated that fluorinated graphene (FG) was used to load the mixture of DOX and CPT after covalent functionalisation with CS; the load of DOX and CPT was equal to 110% and 25%, respectively. The obtained conjugate FG-CS-DOX-CPT demonstrated the decrease of cell viability towards HeLa cell line by 60 and 75% under laser irradiation at 808 nm [178]. Gong et al. in another study showed the possibility of carrying out non-covalent conjugation of FG with DOX (at 200%). FG-DOX conjugate at the concentration of 30 μg·ml<sup>-1</sup> significantly decreased the cell viability of HeLa cancer cell line up to 94 % after 48 h incubation [179].

Shim et al. revealed in *in-vivo* study that rGO functionalised with low-molecular-weight heparin (LHT7) acted as a tumor-targeting molecule for the delivery of DOX. The conjugate rGO-LHT7-DOX with rGO:DOX weight ratios 2, 1, 0.5, 0.1, demonstrated high anti-tumor effect against human KB carcinoma cells (61.1 % decrease of cell viability) as well as significant reducing of tumor size by  $(92.5 \pm 3.1)\%$  [180]. Table 3 summarises examples of conjugation between anticancer drugs and the surface of GBN.

## 2.5 Graphene conjugations with biomolecules

Graphene and GO were conjugated with short chain peptides, enzymes, and proteins by covalent or non-covalent attachment. These molecules can react with the surface of graphene or the various oxygen functional groups of GO (carboyxyl, hydroxyl, epoxy, and carbonyl groups), for example by forming amide bond between the carboxylic group of GO and the NH<sub>2</sub> group of the enzyme or the protein. Also, the non-covalent attachment can take place through hydrophobic, electrostatic, or  $\pi$ – $\pi$  interactions [181,182].

Wang et al. [183] showed the possibility of covalent conjugation of GO with antibodies (Ab) using bifunctional PEG (NH<sub>2</sub>–PEG–COOH) as a linker. The carboxylic groups of GO linked with the amino groups of PEG by EDC coupling forming amide bonds and then the COOH groups of PEG were coupled with NH<sub>2</sub> groups of the antibody forming GO-PEG-Ab by the same reaction. The obtained material can be used as sensors with high sensitivity towards small molecules as antigens. Jokar et al. [184] performed covalent functionalisation of GO with polyethylene glycol (M = 1 KDa) and HSA with subsequent non-covalent  $\pi$ – $\pi$  interactions with PTX for drug delivery (the PTX-loading was equal to 22%). The authors pointed out that the release rate of PTX was faster in the acidic mediums (at pH values of 5 and 6.8).

Kim et al. [185] showed that GO can be covalently conjugated with polyethylenimine (M= 1.8 kDa) as a gene delivery cationic vector through  $\pi$ – $\pi$  stacking interactions with GO surface. At the same time, the conjugate acted as a bioimaging material due to its excellent photoluminescence properties. In our group GO was covalently functionalised with L-methionine [186] and L-cysteine [187] through amidation reaction. Moreover, we demonstrated the high biocompatibility of these materials, in particular hemocompatibility without cyto- or genotoxicity.

The authors of [188–190] performed covalent and non-covalent conjugation of GBN with biomolecules such as DNA, peptides, proteins, enzymes, carbohydrates, and viruses for various applications, for example, drug delivery, cancer treatment, tissue engineering, bioimaging as well as the development of biosensors for detecting very low concentrations of biomolecules such as antibodies, nucleic acids, enzymes, or proteins especially for early diagnosis of diseases [191–196]. Wang et al. [193] demonstrated that graphene covalently modified by antibodies can detect in earlier stages the disease markers such as hormones, enzymes, proteins, sugars, peptides, and

disease related genes. Zhang et al. [181] demonstrated that GO covalently and non-covalently linked with proteins (as BSA and trypsin), enzymes and peptides, can be applied as a platform for further immobilisation of Au nanoparticles for the application to biosensors and synthesising novel graphene-based nanoarchitectures. Lu et al. [197] performed the covalent functionalisation of amino-modified DNA with GO through amidation reaction using EDC coupling for the purpose of detecting heavy metals.

## 3. Biocompatibility of GBN

Biocompatibility investigations of new materials usually include the study of haemolysis, thrombocyte aggregation, binding to human serum albumin (HSA), genotoxicity, cytotoxicity, and plasma-coagulation haemostasis.

## 3.1 Haemolysis

Literature analysis reveals that the functionalisation of graphene surface leads to decreasing the haemolysis and thus increasing haemocompatibility. Liao et al. [198] showed that GO has dose dependent hemolytic activity with  $TC_{50} = 20.2$ -49.6 µg·ml<sup>-1</sup> which is the concentration of GO that causes 50% haemolysis, while graphene sheets showed insignificant hemolysis ( $TC_{50} > 200 \,\mu\text{g·ml}^{-1}$ ). At the same time, the noncovalent functionalisation of GO with chitosan didn't demonstrate any hemolytic activity pointing out that the functionalisation can protect erythrocytes. Pinto et al. [199] showed that the noncovalent functionalisation of graphene surface by polymers (poly(vinyl alcohol), poly(ethylene glycol), poly(vinyl pyrrolidone), hydroxyethyl cellulose, chondroitin, glucosamine, and hyaluronic acid resulted in decreasing haemolysis to less than 1.7 % for all materials at concentrations up to 500 µg·ml<sup>-1</sup>. In our previous works GO enriched by oxygen containing groups (EOGO) as well as GO functionalised

with L-methionine (GFM) and L-cysteine (GFC) did not cause erythrocyte membrane damage at up to 25 μg·ml<sup>-1</sup> [98,186,200].

# 3.2 Thrombocyte aggregation

Singh et al. [201,202] demonstrated that GO ( $C = 2 \, \mu g \cdot ml^{-1}$ ) induced platelet aggregation. The functionalisation of GO with amine functional groups did not activate platelet aggregation at the same concentration range. The authors showed that the aggregation caused by GO was even stronger than that initiated by thrombin. Podolska et al. [203] determined that GO, rGO, and rGO-PEG ( $C = 50 \, \mu g \cdot ml^{-1}$ ) did not stimulate platelet aggregation in the presence of 2  $\mu mol \cdot ml^{-1}$  of adenosine diphosphate (ADP). GFC (up to 25  $\mu g \cdot l^{-1}$ ) did not stimulate the ADP-induced aggregation of platelets while GFM and EOGO demonstrated anti-aggregation activity up to 25  $\mu g \cdot l^{-1}$  and 100  $\mu g \cdot l^{-1}$  respectively, in the experiments of ADP and collagen induced aggregation.

### 3.3 Binding to human serum albumin

Ding et al. [204] revealed that GO (100  $\mu$ g ml<sup>-1</sup>) can interact with HSA through various types of interactions (covalent bonds, hydrogen bonds, electrostatic forces, hydrophobic and  $\pi$ – $\pi$  stacking interactions). The interaction between GO and HSA led to malfunctioning of HSA and its inability to remove toxins due to conformational changes, meaning that GO is potentially toxic. The functionalisation of GO surface by carboxylic groups (GO-COOH, 100  $\mu$ g ml<sup>-1</sup>) showed increasing biocompatibility as it didn't cause functional changes of HSA. In contrast, Taneva et al. [205] demonstrated that GO (8 mg ml<sup>-1</sup>) interaction with HSA did not cause toxic effect for HSA in the blood plasma due to the low affinity of GO to HSA.

Ding et al. [204] determined the values of the dissociation constant (the reciprocal of the binding constant) of the HSA complex with GO ( $K_d$ = 27.5  $\mu$ g·ml<sup>-1</sup>). The authors proposed that the formation of covalent bonds is due to the interaction of GO epoxy groups and free amino

groups of Lys and Arg of HSA by the nucleophilic addition mechanism and hydrogen bonding. In turn, the interaction of modified GO with HSA mainly occurs due to the formation of hydrogen bonds because the epoxy groups are blocked by the carboxyl groups: the dissociation constant value for the interaction between GFM, GFC, and HSA are equal to 185.2 [186] and 1600 [98] µg·ml<sup>-1</sup>, respectively.

#### 3.4 Genotoxicity

Liu at al. [206] revealed that GO at concentrations up to 100 µg ml<sup>-1</sup> induced mutagenesis due to interfering with DNA replication and altering gene expression patterns. Wang et al. [207] reported that GO (up to 100 µg ml<sup>-1</sup>) possessed significant genotoxicity to human lung fibroblast (HLF) cells due to DNA damage through the generation of reactive oxygen species and surface charge of GO. After functionalisation of GO surface with PEG and lactobionic acid, the genotoxicity was significantly decreased.

Akhavan et al. [208] demonstrated that the genotoxicity is dependent on lateral size dimensions of graphene: the rGO nanoparticles with average lateral dimensions of 11±4 nm were able to penetrate into the nucleus of the human mesenchymal stem cells (hMSCs) leading to DNA fragmentations and chromosomal aberrations at low concentrations (0.1 and 1.0 mg·ml<sup>-1</sup>) after 1 h. At the same time rGO sheets with average lateral dimensions of 3.8±0.4 μm did not exhibit genotoxicity even at 100 mg·ml<sup>-1</sup> after 24 h. Both GFM and GFC did not demonstrate genotoxicity up to 25 μg·ml<sup>-1</sup> as well as less genotoxicity recorded for EOGO up to the concentrations of 100 μg ml<sup>-1</sup>[209].

## 3.5 Cytotoxicity

Wang et al. [210] indicated that GO (10-200  $\mu g$  ml<sup>-1</sup>) cause cytotoxicity in a dose dependent manner to human multiple myeloma RPMI 8226 cells through oxidative stress mechanism.

Akhavan et al. [208] revealed that the cytotoxicity of graphene is size and concentration dependent. rGO with average lateral dimension 11 ±4 nm is cytotoxic to hMSCs at 1 μg ml<sup>-1</sup> while rGO with larger average lateral dimension of 3.8 ± 0.4 μm showed less cytotoxicity at higher concentration of 100 μg ml<sup>-1</sup>. Sun et al. [211] showed that the functionalisation of graphene surface with hydroxyl functional groups (G-OH) preserves viability of rat adipose tissue-derived stromal cells (rADSCs). Wu et al. [212] demonstrated that covalently functionalised GO with adipic acid dihydrazide (AD) and hyaluronic acid (HA) had no cytotoxic effect towards HeLa and L929 cell lines up to 200 μg·ml<sup>-1</sup>. In addition, GFM, GFC, and EOGO did not demonstrate cytotoxicity towards HEK293 cell line up to 25 mg·l<sup>-1</sup>.[98,186,209]

## 4. GBN dispersion stability

It is well known that graphene, GO, and rGO have different stability of colloid dispersions in water. Si et al. demonstrated that pristine graphene has no despersibility because it has no oxygen functional groups and due to having high density of hydrophobic sp<sup>2</sup> C=C bonds [213]. The ability of GBN to form stable dispersions in water is referred to (*i*) the high polarity and forming hydrogen bonds with water [214]; (*ii*) the presence of charged particles leading to high electrostatic repulsion between graphene flakes [215–217].

The importance of GBN dispersions stabilisation is a key point for its biomedical applications. GBN dispersions can be obtained through various approaches: (*i*) exfoliation of graphene in definite solvents without functionalisation or addition of stabilising agents (surfactants or polymers); (*ii*) covalent or noncovalent functionalisation of graphene surface which support stability of aqueous dispersions; (*iii*) using dispersing agents such as surfactants and polymers that can be adsorbed on graphene surface and increase the exfoliation, solvation

and stabilisation of graphene layers in aqueous dispersions [218]. Table 4 demonstrates the characteristics of GBN dispertions.

#### 5. Conclusion

GBN in the form of graphene, GO, and rGO are perspective nanostructures in which the surface is enriched by electrons and various oxygen-containing functional groups are present that allow to perform covalent and non-covalent functionalisation leading to various nanomaterials that are promising in applications in nanobiomedicine (Fig. 14) as targeted drug delivey, the treatment of cancer, tissue engineering, bioimaging, biosensors, developing antimicrobial and antiviral materials as well as in energy applications (batteries, solar cells, fuel cells, superconductors), textiles, and electronics. Among GBN, GO is a leading nanomaterial due to the presence of oxygen-containing functional groups along with the  $\pi$  structure that can be exploited as a nanoplatform for covalent or non-covalent loading of organic and inorganic compounds. At the same time the presence of the functional groups provides the stability of GO aqueous dispersions in contrast to graphene or rGO.

#### **6. Future remarks/recommendations**

This review summarises the results of studies on covalent and noncovalent functionalisation of graphene surface. Particular attention is paid to establishing the relationship between the type of functionalisation and the possibilities of GBN application in various fields of science and technology. Literature analysis reveals the following trends in the study of GBN:

(i) there is a large body of data on covalent and noncovalent modification of graphene surface which allows to vary the physicochemical properties of the final nanomaterial and affect the GBN dispersions stability;

- (ii) large number of scientific works are devoted to the application of GBN as nanomodifiers. The implementation of this approach makes it possible to obtain new materials with unique physicochemical and operational characteristics;
- (iii) extremely relevant direction is devoted to the application of GBN in medicine and bioanalysis. In this regard, the number of publications on the study of biocompatibility, as well as *in vitro* and *in vivo* studies of GBN is increasing annually.

At the same time, detailed analysis of the literature data reveals the following drawbacks and problems that deserve special attention:

- (i) lack of data on identification of the synthesised nanomaterial. Often, the authors do not conduct a comprehensive study of the structure and composition of the obtained materials;
- (ii) the question of reproducibility of GBN syntheses remains open;
- (iii) the literature presents a small number of studies aimed at studying the stability of GBN dispertions;
- (iv) there is no data on the metabolic pathways and toxicokinetics of GBN for biomedicinal purposes;
- (v) GBN biomedicinal studies are not comprehensive and do not allow to analyse the full profile of the possibilities of using these nanomaterials.

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Table 1. Physico-chemical properties of GBN

Properties	Graphene	rGO	GO
Mechanical properties	Stiffness: 340 N·m <sup>-1</sup> [219];	Stiffness: 22.4 N·m <sup>-1</sup> [220];	Stiffness: 145.3 N·m <sup>-1</sup> [223];
	Young's modulus: 1.0 ± 0.1TPa	Young's modulus: 0.25± 0.15	Young's modulus: $207.6 \pm 23.4$
	[219];	TPa [221];	GPa [223];
	strength: 42 N·m <sup>-1</sup> (130 GPa) [219].	strength: 293.3 MPa [222].	strength: 17.3 N·m <sup>-1</sup> (24.7 GPa)
			[224].
Electrical properties	Electrical conductivity: 6500 S·m <sup>-1</sup>	Electrical conductivity: 3032.6-	Electrical conductivity: 1.34·10 <sup>-5</sup>
	[225];	4006 S·m <sup>-1</sup> [227];	S·m <sup>-1</sup> [230];
	electron mobility: 25 m <sup>2</sup> V <sup>-1</sup> s <sup>-1</sup>	electron mobility: 26 cm <sup>2</sup> V <sup>-1</sup> s <sup>-1</sup>	electron mobility: 2-200 cm <sup>2</sup> V <sup>-1</sup>
	[226];	[228];	s <sup>-1</sup> [231];
	sheet resistance: 30 $\Omega$ per square of	sheet resistance: 1.6 K $\Omega$ /sq at	sheet resistance: 276-2024 $\Omega$ /sq
	2D area (30 Ω/sq) at 97.7 %	85% transparency [229].	at 23–77% transparency [232].
	transmittance [226].		
Thermal properties	Thermal conductivity: ranges from	Thermal conductivity: 1.3	Thermal conductivity: 8.8

	(1500-5000) W·m <sup>-1</sup> ·K <sup>-1</sup> [233].	$W \cdot m^{-1} \cdot K^{-1}[234].$	$W \cdot m^{-1} \cdot K^{-1}$ [235].
Application	Biomedicine [236], energy [156],	Biomedicine [239], energy	Biomedicine [158], energy
	electronics [237], nanocomposites	[240], electronics [241],	[243], nanocomposites [238],
	[238], nanosensors [226].	nanocomposites [238],	nanosensors [244].
		nanosensors [242].	

Table 2. Applications, properties and description of key results of nanocomposite materials.

GBN-nanocomposite type	Application	Key results and description	Reference
and composition information			
GO- AgNp	Antibacterial agent.	Inhibitory concentration of GO-AgNp towards Pseudomonas	[120]
Characteristics of	Antibacterial coatings	aeruginosa is 2.5 μg·ml <sup>-1</sup> with 100% inhibition rate after 1	
nanocomposite:	for preventing growth	h. In the case of GO the authors did not observe antibacterial	
-GO thickness: 0.7-1.2 nm;	of bacteria on	activity.	
-distribution size: 300-800 nm.	medical devices.	Role of GO: (i) stabilizing agent preventing agglomeration	
-AgNps size: 7.5 nm.		of AgNp; (ii) increasing of surface area of AgNps.	
GO-TETA-AgNps	Sensors for organic	Detection limit for <i>p</i> -aminothiophenol- $2 \cdot 10^{-8}$ M and	[123]
Characteristics of	molecules (p -	melamine- 2·10 <sup>-7</sup> M.	
nanocomposite:	aminothiophenol and	Inhibition effect (100%) against the growth of Escherichia	
-GO covalently functionalised	melamine).	$coli (E. coli)$ at $C$ (GO-TETA-Ag)= 100 $\mu$ g·ml <sup>-1</sup> .	
with N-(trimethoxysilylpropyl)	Antibacterial agents.		
ethylenediaminetriacetic acid			
trisodium salt (TETA) and			

AgNps (30-50 nm);			
-stable aqueous dispersion at C			
(GO-TETA-AgNps)=0.5			
mg·ml⁻¹.			
-uniform distribution of AgNps			
on graphene surface (according			
to SEM).			
rGO-PDA-AgNps	DNA biosensors.	Detection limit of 3.2·10 <sup>-15</sup> M.	[126]
Characteristics of		Application of rGO allows to increase electrode active area	
nanocomposite:		and enhance detection signal.	
-rGO modified with			
polydopamine-AgNps;			
-heterogeneous distribution of			
AgNps on graphene surface			
with non-uniform sizes leading			
to increasing immobilization of			

the target molecules.			
rGO-1,6 diaminohexane-	Antibacterial activity,	Disinfecting water against total and fecal coliform bacteria at	[45]
AgNp.	water disinfection.	$C=1 \text{ mg}\cdot\text{ml}^{-1}$ with 100 % inhibition rate.	
Characteristics of			
nanocomposite:			
-rGO noncovalently			
functionalised with 1,6			
diaminohexane- AgNp (by			
hydrogen bonding, electrostatic			
interactions);			
-using of single layers of			
graphene sheets (according to			
HRTEM) leads to			
homogeneous distribution of			
AgNps.			
rGO-AuNps-PNA	Biosensors for	Detection limit up to 1·10 <sup>-14</sup> M. In the absence of AuNps	[245]

Characteristics of	miRNA.	detection limit is equal to 1·10 <sup>-13</sup> M.	
nanocomposite:			
-rGO noncovalently modified			
with AuNps which in turn			
covalently functionalised with			
peptide nucleic acid probe			
(PNA);			
-the sequence of the PNA			
probe is N-			
AACCACACAACCTACTAC			
CTCA-C;			
-rGO thickness: 1.6 nm;			
-particle size of AuNps: 10 nm.			
rGO-AuNps-TGA	Sensors for detection	Detection limit up to 2.5·10 <sup>-8</sup> M.	[131]
Characteristics of	of mercury (II) ions.		
nanocomposite:			

-noncovalently functionalised			
rGO with AuNps followed by			
covalent functionalisation with			
thioglycolic acid (TGA);			
-homogenious distribution of			
AuNps (5 nm) on rGO surface			
without agglomerations.			
rGO-PtNps	Fuel cells.	High fuel cell performance of rGO-PtNps with maximum	[140]
Characteristics of		power output of 320 mW·cm <sup>-2</sup> (40% higher than for carbon	
nanocomposite:		black (Vulcan XC-72) modified with PtNps (Pt-VC)).	
-superior dispersion of PtNps		The high fuel cell performance using low loading of PtNps (	
on rGO surface;		0.25 mg cm <sup>-2</sup> ) in comparison to higher Pt loading used in	
-small particle size of rGO-		standard fuel cell electrodes (0.5 mg cm <sup>-2</sup> ).	
PtNps: 1.9 nm;		High fuel cell performance is referred to high catalytic	
surface area: 138 m <sup>2</sup> ·g;		activity due to high electrochemical surface area and small	
PtNps loading: 0.25 mg cm <sup>-2</sup> .		PtNps size.	

rGO-T-Pt	Electrocatalyst for	Higher electrocatalytic activity than Pt-VC and Pt-rGO	[142]
Characteristics of	methanol oxidation.	catalysts.	
nanocomposite:	Fuel cells.	Electrode charge transfer resistance $R_{ct}$ =158, 185 and 203 $\Omega$	
- rGO-taurine-PtNp;		for rGO-T-Pt, rGO-Pt and Pt-VC, respectively.	
-rGO modified with taurine		Catalytic enhancement mechanism of rGO-T-Pt: (i) presence	
and PtNps;		of SO <sub>3</sub> H <sup>-</sup> groups due to functionalisation of rGO with	
-thickness of rGO-T is 1.2 nm		taurine molecules;	
with lateral dimensions of		(ii) uniform and symmetrical distribution of PtNps with	
several micrometers;		particle size of 3.8 nm on rGO –T surface;	
-loading of Pt up to 80 wt%.		(iii) enhanced charge transfer ability.	
rGO-ZnO	Sensors for NO <sub>2</sub> .	rGO-ZnO sensor has higher response than ZnO sensor	[144]
Characteristics of		toward NO <sub>2</sub> gas at 200 $^{0}$ C and 250 $^{0}$ C.	
nanocomposite:		Response of the sensor rGO-ZnO to NO <sub>2</sub> gas at $C$ (NO <sub>2</sub> ) = 5	
-ZnO particle diameter: $20 \pm 2$		ppm is 1.4 times higher than that of pure ZnO sensor.	
nm;			
-lateral size dimensions of rGO			

sheets range from few			
nanometers up to some tens of			
micrometers.			
G-ZnO-PSE-ssDNA	Genosensors for ss	Detection limit is 4.3·10 <sup>-12</sup> M due to high conductivity of G-	[143]
Characteristics of	RNA detection.	ZnO ( $R_{ct}$ =1241.3 $\Omega$ .), large specific area and catalytic	
nanocomposite:		properties.	
-graphene-ZnO -single			
stranded DNA;			
-noncovalent composite of			
graphene (G)-ZnO- 1-			
pyrenebutyric acid N-			
hydroxysuccinimide ester			
(PSE) that was covalently			
functionalised with amino			
modified ssDNA probe;			
-ssDNA probe was used to			

hybridize with ssRNA target			
for detection.			
GO- CuO	Antibacterial agent.	Inhibiting the growth of <i>E. coli</i> and <i>S. typhimurium</i> bacteria	[148]
Characteristics of		in the concentration range 1-3 mg·ml <sup>-1</sup> , toxicicty for both	
nanocomposite:		bacteria after 3 h is 98% at $C$ (GO-CuO)= 3 mg·ml <sup>-1</sup> .	
-CuO loading: 40%;		Mechanism of antibacterial activity: (i) cellular uptake, (ii)	
-thickness of GO layers is 12		generation of reactive oxygen species.	
nm;			
-thickness of GO-CuO layers is			
13 nm;			
-particle size of CuO is190 nm.			
GO-CuO	Anticancer activity.	Cytotoxic activity (70%) against Human colon cancer cell	[246]
Characteristics of	Photocatalyst for dye	line (HCT-116) at 100 μg·ml <sup>-1</sup> .	
nanocomposite:	degradation.	GO-CuO led to 83.20 % degradation of methylene blue dye	
-agglomerated CuO		solution when exposed to visible light for 60 min (due to	
nanoparticles with spherical		generation of 'OH and 'O2 <sup>-</sup> radicals that oxidize methylene	

morphology.		blue).	
rGO-Fe <sub>3</sub> O <sub>4</sub>	Anticancer agents.	Anticancer activity: cytotoxicity of rGO-Fe <sub>3</sub> O <sub>4</sub> against	[150]
Characteristics of	Antibacterial agents.	erythromyeloblastoid leukemia (K562), prostate carcinoma	
nanocomposite:		(PC-3), epidermoid carcinoma (A-431), ER <sup>+</sup> breast	
-Fe <sub>3</sub> O <sub>4</sub> particle size: 6 ±3nm;		carcinoma (MDA-MB-231), colon carcinoma (COLO-205),	
-superparamagnetic properties:		ER1 breast adenocarcinoma (MCF-7), and lung carcinoma	
saturation magnetisation (Ms =		(A-549) cell lines at $C$ (rGO-Fe <sub>3</sub> O <sub>4</sub> )=50 $\mu$ g·ml <sup>-1</sup> is equal to	
20.1 emu·g <sup>-1</sup> ) and coercivity		20–40% depending on cell line	
(Hc=6.25 Oe).		Antibacterial activity: minimum inhibitory concentration of	
		rGO-Fe <sub>3</sub> O <sub>4</sub> = 1000 μg·ml <sup>-1</sup> against Gram-positive bacteria,	
		(Staphylococcus aureus, Bacillus subtilis, Streptococcus	
		mutans, and Enterococcus faecalis) and Gram-negative	
		bacteria (Salmonella typhi and E. coli).	
GO–APTES-Fe <sub>3</sub> O <sub>4</sub> -DOX	Targeted drug	Targeted delivery of DOX with loading capacity of 0.2 mg	[154]
Characteristics of	delivery. Dual in-	of DOX per 1 mg GO-Fe <sub>3</sub> O <sub>4</sub> -APTES (20 wt % loading).	
nanocomposite:	vitro fluorescence	DOX- GO-Fe <sub>3</sub> O <sub>4</sub> -APTES led to 2.5 fold higher efficacy of	

-GO covalently functionalised	and in-vivo magnetic	cytotoxicicty (62%) against HeLa cells than free DOX (	
with 3–	resonance imaging.	reducing the required dose of DOX by 8 times to have the	
aminopropyltriethoxysilane	Cancer sensing.	same value of cytotoxicity).	
(APTES) and noncovalently		The intensity ratio of emission spectra of GO-Fe <sub>3</sub> O <sub>4</sub> -APTES	
with Fe <sub>3</sub> O <sub>4</sub> and DOX;		in red (635 nm) and green (535 nm) for cancer (HeLa and	
-particle size of GO-Fe <sub>3</sub> O <sub>4</sub> -		MCF-7) and healthy cell line (HEK-293) depends on the	
APTES: 260 nm.		type of cell line and its pH value in the cell	
		microenvironment.	

Table 3. Cytotoxicity of conjugates based on GBN and non-covalently attached anticancer drugs evaluated by cell viability assay.

Type of GBN	Drug load	Cell lines or type	Applied concentrations and IC <sub>50</sub> or	Reference
		of cancer	approximate % of cytotoxicity at the	
			highest concentration	
GO-sulphonic acid	Loading of a dual drug:	MCF-7 cells	$C=$ 2 and 20 $\mu g \cdot ml^{-1}$ for (GO-SO <sub>3</sub> H-	[168]
groups- folic acid	camptothecin (CPT) (4.5	(human breast	DOX-FA), % cytotoxicity = 20% and for	
(GO-SO <sub>3</sub> H-FA);	%) and Dox (400%).	adenocarcinoma)	GO-FA-DOX (% cytotoxicity = 67%)	
GO-FA			C= 0.002, 0.02 and 0.2 μg·ml <sup>-1</sup> for (GO-	
			FA-DOX-CPT) of % cytotoxicity = 22%	
			and (GO-FA-CPT)	
			% cytotoxicity: = 26%	
GO- chlorotoxin	Loading of DOX	C6 (glioma cells)	$C= 1-5 \mu g \cdot ml^{-1}$ ;	[104]
(GO-CTX)	570 mg DOX per gm GO-		% of cytotoxicity = 60%	
	CTX.			
GO-sodium alginate	Loading of DOX 1.8	HeLa cells	C= 5 - 20 μg·ml <sup>-1</sup>	[169]
(GO-SA)	mg/mg.		% of cytotoxicity = 69%	
GONP with	Cisplatin (CP) loading was	A549 (human	C= 2.5 – 30 μg·ml <sup>-1</sup>	[247]
dimensions of 50 $\times$	not determined.	lung cancer cell	% of cytotoxicity = 90%	
50 nm <sup>2</sup>		line)		
GO-polyethylene	Camptothecin (CPT)	MCF-7 (breast	C= 20 – 100 μg·ml <sup>-1</sup>	[173]
glycol-folic acid	loading 45%.	cancer cell line)	% of cytotoxicity = 76%	
(GO-PEG-FA)				

GO-Fe <sub>3</sub> O <sub>4</sub> -β-	DOX loading 37.4 %	K562 cells	$C = 2 - 16 \mu \text{g} \cdot \text{ml}^{-1}$	[174]
cyclodextrin	MTX loading 23.4 %	(leukemia cell	% of cytotoxicity (DOX) = 65%	
		line)	% of cytotoxicity (MTX) = 55%	
GO-PEG-FA	Loading of Protocatechuic	HT29 (Colon	C= 1.56 – 100 μg·ml <sup>-1</sup>	[177]
	acid (PCA)- 23.47% and	cancer cell line);	% of cytotoxicity (HT29) = 58%	
	Chlorogenic acid (CA)-	HePG2 (human	$IC_{50} (HT29) = 50.69 \ \mu g \cdot ml^{-1};$	
	18.33%.	liver cancer cell	% of cytotoxicity (HepG2)= 61%	
		line)	$IC_{50} (HepG2) = 40.39 \ \mu g \cdot ml^{-1}$	
GO-FA- bovine	DOX	MCF-7 (human	C= 0.01– 20 μg·ml <sup>-1</sup>	[248]
serum albumin (GO-	Loading- 437.43 µg DOX /	breast cancer cell	IC <sub>50</sub> (MCF-7, 24 h) = $8.9 \pm 0.7$	
FA-BSA)	mg	line) FA-receptor-	μg·ml <sup>-1</sup>	
	(GO-FA-BSA).	positive)	$IC_{50}$ (MCF-7, 48 h) = 0.048 ± 0.010	
		A549 (human	$\mu g \cdot ml^{-1}$ (% of cytotoxicity = 83%)	
		lung cancer cell		
		line) (FA-	$IC_{50} (A549, 24 h) = 5.3 \pm 0.7$	
		receptor-negative)	μg·ml <sup>-1</sup>	
			IC <sub>50</sub> (A549, 48 h) = $0.279 \pm 0.037 \ \mu \text{g·ml}^{-}$	
			<sup>1</sup> (% of cytotoxicity = 78%)	
FA-GO-PVP	DOX loading -107.5 %.	HeLa cells	2 μg·ml <sup>-1</sup> ; 20 μg·ml <sup>-1</sup>	[170]
(folic acid-GO-			(% of cytotoxicity = 71%)	
polyvinylpyrrolidone,				
M= 30kDa)				

Fluorinated GO	loading of DOX ~200%	HeLa cells	C= 1.11 – 30 μg·ml <sup>-1</sup>	[179]
(FGO)			(% of cytotoxicity (24 h) = 70%)	
			(% of cytotoxicity (48 h) = 94%)	
Pegylated folate and	CPT loading- 90%	HeLa cells	$IC_{50} = 3.1 \ \mu M$	[249]
peptide-decorated				
graphene oxide				
PEG-FA-Pep-GO				
Graphene quantum	DOX loading is dose	blood cancer cells	C= 2- 32 μg·ml <sup>-1</sup>	[250]
dots - carboxymethyl	dependent on GQD	(K562)	With IC <sub>50</sub> values of 5.1 µg⋅ml <sup>-1</sup> GQD	
cellulose hydrogel	GQD(10%)-CMC ~ 4.5%,		(% cytotoxicity = 93%)	
(GQD - CMC)	GQD(20%)-CMC ~5.5 %			
	GQD(30%)-CMC~6 %			
GO-PVP and GO- β-	The anticancer drug SN-38	MCF-7	5 and 10 μg·ml <sup>-1</sup>	[251]
cyclodextrin (CD)	(7-ethyl-10-hydroxy		IC <sub>50</sub> (GO-PVP-SN-38) =97 μM	
	camptothecin)		( % cytotoxicity = 68% )	
	The loading:- 1 g of GO-		$IC_{50}$ (GO-β-CD-SN-38) = 170 μM	
	PVP loaded 0.17 g of SN-		(% cytotoxicity = 65%)	
	38;			
	1 g of GO-β-CD loaded			
	0.14 g of SN-38			

Table 4. Characteristics of GBN dispersions

System	Mechanism of dispersion	Characteristics of	Category of	Reference
	stabilization	dispersion	stabilization	
			process	
GO covalently functionalised by SO <sub>3</sub> H	The presence of negatively	Duration of stability	Functionalisation	[213]
groups (GO-SO <sub>3</sub> H).	charged HSO <sub>3</sub> <sup>-</sup> functional groups	investigation: one month.		
	on GO surface cause	$C(GO-SO_3H)=2 \text{ mg}\cdot\text{ml}^{-1}.$		
	electrostatic repulsion of the	pH range: 3-10.		
	graphene layers.	ζ-potential: -55-60 mV at		
		рН 6.		
Graphene noncovalently functionalised	The negatively charged CS	Duration of stability	Functionalisation	[54]
with tetrapotassium salt of coronene	molecules form noncovalent $\pi$ - $\pi$	investigation: months.		
tetracarboxylic acid (G-CS)	stacking interactions with	$C(G-CS)=0.15 \text{ mg}\cdot\text{ml}^{-1}.$		
Graphene was obtained by two	graphene surface and prevent $\pi$ -			
methods: thermal exfoliation of graphite	$\pi$ stacking interactions between			
oxide and the arc evaporation of	graphene layers stabilising the			

graphite in a hydrogen atmosphere.	dispersions of G-CS.			
				50113
Graphene functionalised with hydroxyl		Duration of stability	Functionalisation	[211]
groups (G-OH).	containing groups;	investigation: one month.		
	(ii) high negative charge density	$C(G-OH)=0.1-5 \text{ mg}\cdot\text{ml}^{-1}.$		
	of the graphene surface.	ζ-potential: -50mV.		
Graphene-SiO <sub>2</sub> .	(i) increased hydrophilicity due	Duration of stability	Functionalisation	[217]
	to the presence of SiO <sub>2</sub> groups;.	investigation: 7 days.		
	(ii) steric hinderance effect			
	provided by the SiO <sub>2</sub> groups.			
rGO non covalently functionalised with	rGO +SLS: (i) hydrophobic	Duration of stability	Functionalisation	[252]
natural polymers: sodium lignosulfonate	interaction of alkyl groups and	investigation: four months.		
(SLS, $M_{\rm w}$ =60000), sodium	aromatic rings of SLS with	C(rGO-polymer)=0.6-2		
carboxymethyl cellulose (SCMC,	graphene surface through $\pi$ - $\pi$	mg·ml⁻¹.		
$M_{\rm w}$ =250000), and pyrene-containing	stacking interaction; (ii) the			

hydroxypropyl cellulose (HPC-Py).	sulphonic groups (-SO <sub>3</sub> Na)			
	provide sufficient electrostatic			
	repulsion.			
	rGO + SCMC: electrostatic			
	repulsion of carboxylate anions.			
	rGO + HPC-Py: steric repulsion			
	caused by the long polymer			
	chains.			
rGO covalently functionalised with N-	The hydrophilic EDTA groups	Duration of stability	Functionalisation	[253]
(trimethoxysilylpropyl)	stabilized rGO-NEDTA aqueous	investigation: three		
ethylenediamine triacetic acid	dispersions.	months.		
(NEDTA).		C(rGO-NEDTA)=1		
		mg·ml <sup>-1</sup> .		
Graphene + sodium dodecylbenzene	the aqueous dispersions were	Duration of stability	Surfactant	[215]
sulfonate (SDBS).	stabilised by Coulomb repulsion	investigation: 6 weeks.	addition	

The graphene was obtained by	between the G-SDBS sheets.	Particle size: 500 nm.		
ultrasound exfoliation of graphite in		$C(G-SDBS)=0.5 \text{mg}\cdot\text{ml}^{-1}$ .		
water solution of SDBS surfactant. The		ζ-potential: -50 mV at		
final nanomaterial contained 40 % of		pH=7.		
multilayered graphene (< 5 layers), 3%				
monolayered.				
Graphene + ionic and nonionic	Addition of ionic and nonionic	Duration of stability	Surfactant	[254,255]
surfactants [P123, Tween 80,	surfactants maintained	investigation: one month.	addition	
Triton X-100, polyvinylpyrrolidone,	exfoliation between graphene	Size of graphene flakes:		
poly(sodium 4-styrenesulfonate),	layers through electrostatic	several hundred		
sodium deoxycholate, sodium	repulsion forces.	nanometers		
dodecylbenzene-sulfonate, 1-		$C(G-surfactant)=1 \text{ mg ml}^-$		
pyrenebutyric acid, sodium dodecyl		1.		
sulphate, sodium taurodeoxycholate				
hydrate, hexadecyltrimethylammonium				
bromide].				

Graphene + sodium cholate (G-SC).	Addition of amphiphilic	Duration of stability	Surfactant	[216]
	surfactant provides $\pi$ - $\pi$ stacking	investigation: one week	addition	
	interaction with graphene	$C(G-SC)=11 \text{ mg}\cdot 1^{-1}$		
	surface (through hydrophobic	ζ-potential: -45 mV.		
	domains) and stabilisation in			
	water (through hydrophilic			
	domains). At the same time the			
	electrostatic repulsion between			
	G-SC layers takes place due to			
	the presence of negatively			
	charged cholate ions on the			
	graphene surface.			
Graphene + anionic surfactant sodium	G-SDBS dispersions stabilized	Duration of stability	Surfactant	[217]
dodecyl benzene sulfonate (SDBS).	by the electrostatic repulsion	investigation: one week.	addition	
	caused by addition of SDBS that			
	increases the charge density of			

	graphene surface.			
Chemically converted graphene (CCG)	The presence of carboxylate ions	Particle size: 200 – 1000	Exfoliation	[256,257]
(synthesized by GO reduction by	on CCG-surface increases the	nm.		
hydrazine hydrate without total	electrostatic repulsion between	$C(CCG)=0.05 \text{ mg}\cdot\text{ml}^{-1}$ .		
conversion of all oxygen-containing	graphene layers.	ζ-potential is pH		
functional groups and remaining of few		dependent: -30 to -43 mV		
COOH groups).		in the pH range 6.1 to 10.		
GO	Electrostatic repulsion between	Particle size: 200 – 1000	Exfoliation	[257]
	GO layers due to presence of	nm.		
	oxygen containing functional	Highest ζ-potential -48.6		
	groups (C-OH and COOH). pH	mV at pH 10.		
	can affect the stability of	The dispersions are stable		
	colloids due to changing the	of pH= 4-11.		
	charge of nanoparticles in the			
	following processes: (i)			
	protonation of acidic groups (C-			

	OH and COOH) in acidic medium (ii) deprotonation of C-OH and COOH groups in alkaline medium leading to increase of negative charge and electrostatic repulsion.			
GO + ethylene glycol (EG);	High polarity of the solvents	Particle sizes (µm): 0.11	Exfoliation	[258]
GO + deionized water (DW);	(EG, DW and E) leads to high ζ-	(GO-DW), 22.23 (GO-		
GO + ethanol (E);	potential values of GO; nonpolar	EG), 0.33 (GO-E), 0.90		
GO + mineral oil (MO).	solvent (MO) leads to low ζ-	(GO-MO).		
	potential values of GO and	C(GO)=0.2  wt%.		
	hence decrease the stability of	ζ-potentials (mV):		
	dispersions.	-113.77 (GO-DW), 4037.1		
		(GO-EG), -39.1 (GO-E),		
		6.60 (GO-MO).		
rGO	Due to presence of residual	Duration of stability	Exfoliation	[259]

	hydrophilic groups after GO	investigation: 15 days		
	reduction such as hydroxyl,	without sedimentations		
	carboxyl, and carbonyl groups.	while the authors observed		
		sedimentation after 45		
		days		
		$C(rGO)=0.2 \text{ mg}\cdot\text{ml}^{-1}$ .		
		ζ-potential: -50.9 mV at		
		pH 12.		
GO + polar solvents (water, methanol,	Electrostatic repulsion forces	Duration of stability	Exfoliation	[260]
ethanol, DMF, THF).	due to the presence of oxygen	investigation: two months.		
	containing groups on GO surface	Size of particles: 1-10 μm.		
	(hydroxyl and carboxyl) that	$C(GO)=0.33 \text{ mg}\cdot\text{ml}^{-1}$ .		
	stabilize graphene dispersions	$\zeta$ -potential: -25 to -46		
	due to increasing of charge	mV depending on solvent		
	density.	type.		

## List of abbreviations

ADP Adenosine diphosphate

AD Adipic acid dihydrazide

Arg Arginine

APTS 3- Aminopropyltriethoxysilane

B Benzene

BT Benzothiophene

CVD Chemical vapor deposition

CCG Chemically converted graphene

DW Deionized water

DBT Dibenzothiophene

EDC 1-(3-Dimethylaminopropyl)-3-ethylcarbodiimide

DMF Dimethyl formamide

E Ethanol

EDTA Ethylenediamine triacetic acid

EG Ethylene glycol

GO-SO<sub>3</sub>H GO covalently functionalised by SO<sub>3</sub>H groups

EOGO GO, enriched by oxygen containing groups

GFC GO functionalised with L-cysteine

GFM GO functionalised with L-methionine

GBN Graphene based nanomaterials (GO, rGO, graphene)

G-OH Graphene functionalized with hydroxyl groups

G-CS Graphene noncovalently functionalised with tetrapotassium salt of

coronene tetracarboxylic acid

G-epitaxial Graphene obtained by epitaxial growth method

GO Graphene oxide

GrO Graphite oxide

HSA Human serum albumin

HA Hyaluronic acid

Lys Lysine

Man-GO Mannosylated ethylenediamine GO

MO Mineral oil

(NHC-Pd<sup>2+</sup>) N-heterocyclic carbene–palladium complex

NHS N-Hydroxysuccinimide

DCC N,N'-Dicyclohexylcarbodiimide

NEDTA N-(trimethoxysilylpropyl) ethylenediamine triacetic acid

PEG Polyethylene glycol

HPC-Py Pyrene-containing hydroxypropyl cellulose

P Pyridine

rGO Reduced graphene oxide

SCMC Sodium carboxymethyl cellulose

SC Sodium cholate

SDBS Sodium dodecylbenzene sulfonate

SLS Sodium lignosulfonate

THF Tetrahydrofuran

TRGO Thermally reduced graphene oxide

T Thiophene

Cell lines

K562 Blood cancer

MCF-7 Breast cancer

HT29 Colon cancer

COLO-205 Colon carcinoma

A-431 Epidermoid carcinoma

MCF-7 ER1 breast adenocarcinoma

MDA-MB-231 ER<sup>+</sup> breast carcinoma

K562 Erythromyeloblastoid leukemia

C6 Glioma

MCF-7 Human breast adenocarcinoma

MCF-7 Human breast cancer

KB Human carcinoma

HeLa Human cervical carcinoma

HCT-116 Human colon cancer

HEK293 Human embryonic kidney 293

HePG2 Human liver cancer

A549 Human lung cancer

HLF Human lung fibroblast

hMSCs Human mesenchymal stem

RPMI 8226 Human multiple myeloma

Cal-27 Human squamous cell carcinoma

K562 Leukemia

A-549 Lung carcinoma

PA-1 Ovarian cancer

PC-3 Prostate carcinoma

rADSCs Rat adipose tissue-derived stromal

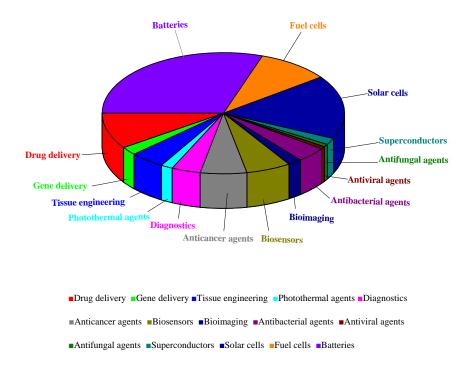


Fig. 1. Publication distribution of GBN applications in various research areas.

Fig. 2. GO structure

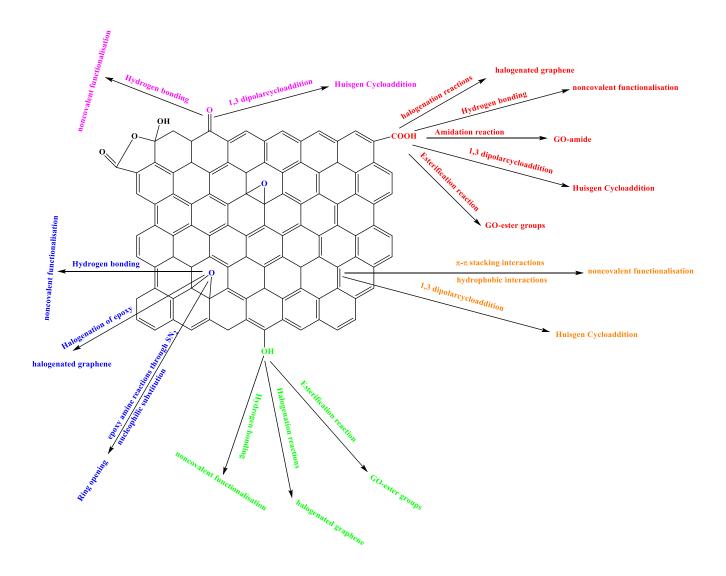


Fig. 3. Scheme showing various kinds of reactions that can happen on the graphene surface.

Fig. 4. Schematic of the reaction mechanism for spontaneous reduction of thioethyldiazonium (HS- $C_2H_4NN^+$ ) ions on graphene surface with subsequent covalent immobilisation of AuNPs on graphene followed by the reaction with dithiol molecules [111].

Fig. 5. Functionalisation of hydroxyl groups of GO with APTS through covalent bonding [112].

Fig. 6. Covalent functionalisation of GO with mannosylated ethylenediamine (in red) through EDC / NHS coupling [113].

Fig. 7. Synthesis of halogenated graphene by thermal exfoliation of graphite oxide in a halogen atmosphere [117].

Fig. 8. Proposed mechanism of the bromination of RGO using NBS through electrophilic substitution reaction [118]

Fig. 9. Schematic illustration of the formation of GO–Fe complexes through oxygen-donor coordination of GO to ferric ions [119].

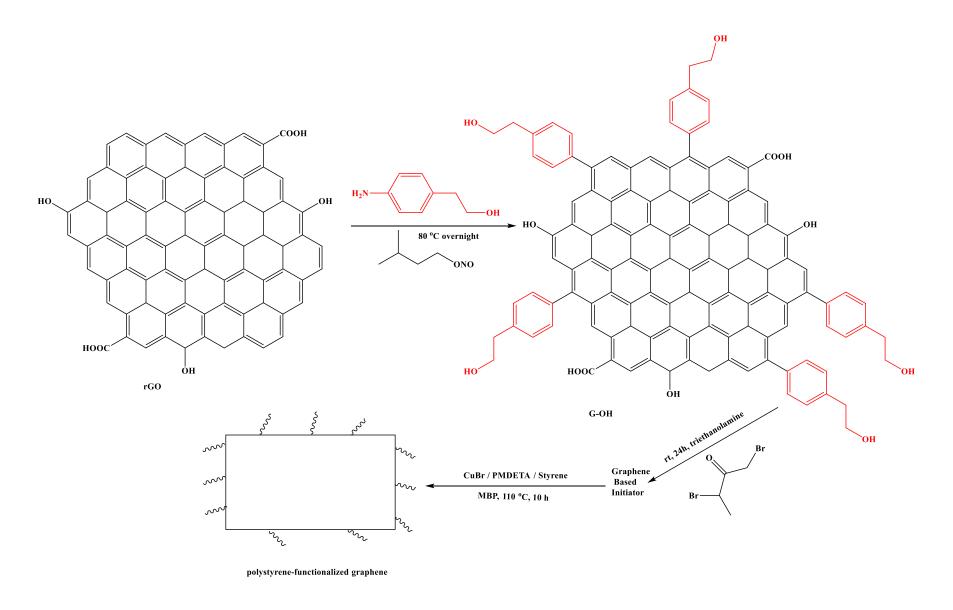


Fig. 10. Synthesis route of polystyrene-functionalised graphene nanosheets [159].

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Fig. 11. Functionalisation of GO with poly(vinyl alcohol) by a carbodiimide esterification reaction [160].

Fig. 12. Covalent functionalisation of GO with DGEBA [161].

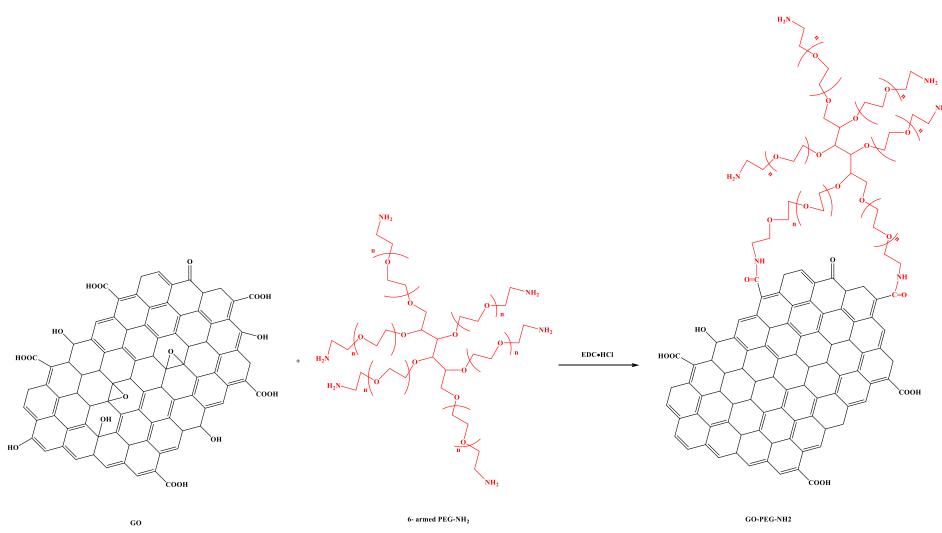


Fig. 13. Covalent functionalisation of GO with 6-armed PEG-NH<sub>2</sub> through amidation reaction [162]

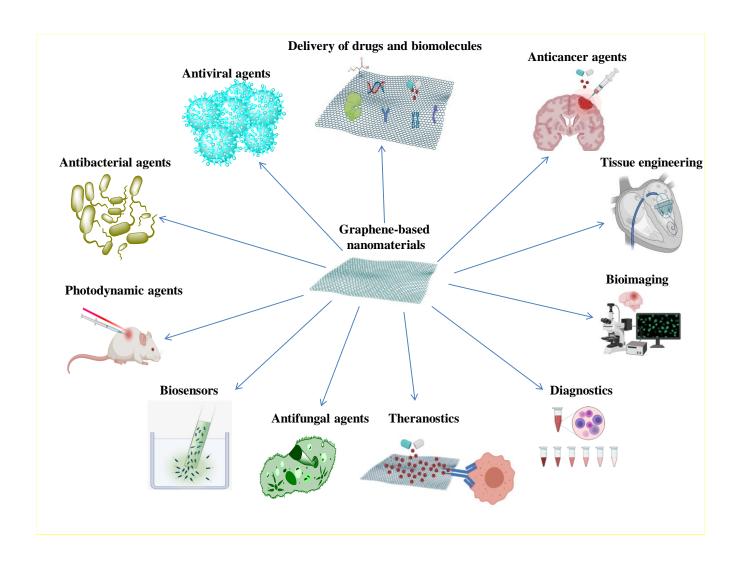


Fig. 14. The application of GBN in nanobiomedicine.