

**Title:** The Nature and Consequence of Vitronectin Interaction in the Non-Compromised Contact Lens Wearing Eye

**ABSTRACT**

*Purpose:* The aim of this work was to investigate the locus and extent of vitronectin (Vn) deposition on *ex vivo* contact lenses and to determine the influence of wear modality together with surface and bulk characteristics of the lens material.

*Methods:* The quantity and location of Vn deposition on the surfaces of contact lens materials was investigated using a novel on-lens cell attachment assay technique.

*Results:* Vn mapping showed that deposition resulted from lens-corneal interaction rather than solely from the tear film. Higher cell counts on the posterior surface of the lenses were determined in comparison to the anterior surface. Overall gross Vn deposition was greater for high water content-low modulus materials ( $117\pm 4$  average cell count per field) than low water content-high modulus materials ( $88\pm 6$  average cell count per field).

*Conclusions:* The role of Vn in plasmin regulation and upregulation is widely recognised. The findings in this paper suggest that the locus of Vn on the contact lens surface, which is affected by material properties such as modulus, is potentially an important factor in the generation of plasmin in the posterior tear film. Consequently, the potential for materials to affect Vn deposition will influence lens-induced inflammatory processes.

**Keywords:** Biomarkers; tears; deposition; fibroblast cells; post-lens tear film.

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Conflicts of interest: None

## 1 **1. Introduction**

2  
3 There is a growing interest in biomarkers related to inflammation and immunoregulation of the  
4 ocular environment in contact lens wear. One interesting candidate biomarker is vitronectin  
5 (Vn), a prominent inflammatory regulatory glycoprotein and adhesion molecule, which has  
6 been detected in tears [1, 2]. Vn is a relatively small glycoprotein of 459 amino acid residues  
7 [3] and is commonly detected in two forms; a single 75 kDa polypeptide chain and a 65 kDa  
8 subunit linked to a 10 kDa fragment by a disulphide bond [4]. This glycoprotein is involved in  
9 many physiological processes, a number of which are summarised in Table 1. Its functions are  
10 dependent on its binding to various matrix and cellular components, which in turns stabilises  
11 or activates a variety of biological macromolecules.

12  
13 One of the primary functions of Vn is to regulate the spreading and attachment of a wide variety  
14 and range of cells [32, 33]. Both Vn has an Arg-Gly-Asp (RGD) cell binding sequence that  
15 enables the individual proteins to bind integrins. The integrin family of heterodimeric proteins,  
16 which directly regulates cellular differentiation, proliferation, and migration - can influence  
17 processes such as wound healing, inflammation, and cancer [34]. Vn also inhibits complement  
18 activity [5, 35]. The concentration of Vn in tears has been shown to be dependent on the tear  
19 state; the levels in reflex, open-eye, and closed-eye tear samples have been reported to be  
20  $0.08 \pm 0.3 \mu\text{g/ml}$ ,  $0.75 \pm 0.32 \mu\text{g/ml}$  and  $3.7 \pm 2.2 \mu\text{g/ml}$  respectively [1, 2]. In terms of contact  
21 lens wear bandage lenses doped with recombinant human Vn have been shown to be effective  
22 in the enhancement of corneal epithelial wound healing on excised donor human corneas [36,  
23 37].

24  
25 Initially it was suggested that the majority of Vn came from conjunctival blood vessels [2], but  
26 Vn has since been found within the basement membrane of the corneal epithelium, which may  
27 indicate a possible endogenous source [38]. It has also been proposed that the overall elevation  
28 of protein levels during eye closure is due to an increase in vascular permeability in  
29 combination with the accumulation of leakage products resulting from a reduced tear turnover  
30 [1, 39]. The effect of vascular leakage on the ocular surface and the potential consequences of  
31 the altered overnight ocular environment are at present poorly understood. Although the  
32 parallel influx of certain components, including plasmin and complement proteins [40], are  
33 likely to be related, the anti-inflammatory properties of Vn, such as the inhibition of

34 complement lysis and plasmin-mediated inflammation, may be extremely important in  
35 controlling or co-controlling the closed eye environment.

36

37 The aim of this work was to investigate the locus and extent of Vn deposition on ex vivo contact  
38 lenses and to determine the influence of wear modality together with surface and bulk  
39 characteristics of the lens material. To detect the adsorption of Vn onto the contact lens surface,  
40 a probe to visualise and trace its presence was required. This was achieved by using fibroblast  
41 cells as a probe, taking advantage of the adhesive nature and the cell binding domain of Vn.  
42 The importance of vitronectin (and fibronectin) in the contraction process in vitro corneal  
43 wound healing studies with fibroblasts (and myofibroblasts) has been demonstrated and  
44 highlights its influence in cell interaction and movement in the ocular environment [41, 42].  
45 The value of a cell-based assay for the study of Vn in the post-lens ocular environment is  
46 demonstrated. Such studies provide a basis for understanding and potentially modulating the  
47 upregulation of plasmin in the post-lens tear film.

48

## 49 **2. Materials and methods**

50

### 51 *2.1. Reagents and immunochemicals*

52 Rabbit IgG (polyclonal); rabbit anti-human fibronectin (polyclonal); human vitronectin; human  
53 fibronectin – all Sigma Aldrich, Gillingham, UK. Rabbit anti-human vitronectin (polyclonal)  
54 (Gibco, BRL). All other reagents were obtained from Sigma Aldrich, Gillingham, UK, unless  
55 otherwise stated.

56

### 57 *2.2. Cell line*

58

59 Mouse 3T3 Swiss Albino embryo fibroblasts cells were purchased from European Collection  
60 of Cell Cultures (ECACC; Salisbury, UK) and grown in Dulbecco's Modified Eagles Medium  
61 – high glucose (DMEM), supplemented with 10% fetal bovine serum (FBS) and 1% 200 mM  
62 L-glutamine solution. Cells were incubated at 37°C in 5% CO<sub>2</sub>, and maintained for up to 10  
63 passages. 1 ml of resuspended cells was added to 19 ml HBS prior to each assay at a  
64 concentration of 5x10<sup>4</sup> cell/ml. Cell viability was determined by the standard trypan blue dye  
65 exclusion test.

66

### 67 *2.3. On-lens cell attachment assay*

68

69 All solutions and analytes were pre-heated to 37°C. A magnesium chloride stock solution  
70 (MgCl<sub>2</sub>, 50 mM), a rabbit IgG solution (300 µg/ml in HBS) and a 1% solution of glutaraldehyde  
71 in HBS were prepared. The cell assay involves the selective inhibition of the adhesion  
72 molecules, using antibody blocking techniques, to validate the significance of Vn on the lens  
73 surface. An anti-Vn antibody control diluted to 1:100 in HBS was incorporated into the assay  
74 to block the action of Vn and used as a comparison against the Vn standard control wells to  
75 assess the adhesion of Vn onto the lens. The use of an IgG antibody, at 300 µg/ml, as a control  
76 was to negate the action of an arbitrary antibody in the system. The lenses, removed from either  
77 doping solution (control lenses and unworn lenses) or saline (worn lenses), were placed  
78 individually into the appropriate test wells of a 24-well plate. Each well was rinsed with 1 ml  
79 HBS (x3). 1 ml HBS was added to the Vn positive control well, 1 ml of the prepared IgG  
80 solution was added to the antibody control well and 100 µl anti-human Vn diluted with 900 µl  
81 HBS was added to the anti-Vn control well. Each 24-well plate was incubated for 60 minutes,  
82 at 37°C and 5% CO<sub>2</sub>, and gently agitated every 10 minutes.

83

84 After incubation, the solution from each lens was aspirated by means of a pipette, with care  
85 taken not to touch the lens. 1 ml of the cell solution in HBS at a final cell count of 5x10<sup>4</sup> cells/ml  
86 was added to each well, in addition to 100 µl of MgCl<sub>2</sub> stock. The 24-well plate was then  
87 incubated for a further 60 minutes at 37°C and 5% CO<sub>2</sub>. Following this second incubation  
88 period, the cell solution from each well was removed and each well and lens was rinsed with 1  
89 ml HBS three times. All lenses were moved to a new 24-well plate and rinsed once with 1 ml  
90 HBS. The cells were fixed in 1 ml of 1% glutaraldehyde stock solution ready for counting.

91

#### 92 2.4. Cell counts

93

94 To count the surface-located cells, each *ex vivo* lens was notionally divided into two areas; the  
95 edge and the centre. The field of vision in which each individual count was taken was defined  
96 by an internal graticule in the eye piece of the microscope. The eye piece graticule measures 1  
97 cm x 1 cm which, when read under a x10 magnification, allowed a field of vision of 1 mm<sup>2</sup>.  
98 An average of the four counts at the edge and single count in centre zone are presented.

99

#### 100 2.5. In vitro control experiments

101 For the on-lens cell attachment assay, lenses (n=3) were doped with Vn to illustrate that it  
102 adsorbs out of solution on to the contact lens surface. The assay relies on the basis that Vn  
103 adheres to contact lens surfaces and that fibroblast cells with integrin receptors for Vn adhere  
104 to the contact lens using Vn as the binding ligand. An initial experiment was performed to  
105 prove that Vn adsorbed out of solution onto the contact lens surface and that it could be detected  
106 using the fibroblast cell assay. Four Group I unworn polyHEMA lenses were doped for 24  
107 hours with a 20 µg/ml solution of Vn. A duplicate set of unworn, non-doped polyHEMA lenses  
108 were assayed as a control. The choice of a Group I set of lenses in this assay was used to take  
109 the assay to the limits. Group I lenses are known to display lower levels of spoilation over  
110 various wear regimes compared to Groups II and IV and thus could be classed as the lowest  
111 threshold for all lenses to be analysed. For *in vitro* assays, human Vn at various concentrations  
112 diluted in PBS was used as the positive Vn control (Vn positive control). Prior to *in vitro* doping  
113 assays, the appropriate lenses were incubated in specific µg/ml concentration of Vn per assay  
114 requirements. The on-lens cell attachment assay was then performed.

115

#### 116 *2.6. The effect of concentration, lens water content and lens ionicity on Vn adsorption*

117

118 To study the effect of concentration polyHEMA contact lenses (n=4) were used in order to  
119 keep the lens type consistent with the initial experiment and to reduce experiment parameter  
120 variability. The four concentrations of Vn used to dope the lenses were: 1 µg/ml, 5 µg/ml, 10  
121 µg/ml and 20 µg/ml. Control non-doped lenses (n=4) were also analysed. No antibody controls  
122 were required. Two separate assays were designed to assess the influence of the lens on the  
123 adsorption of Vn to its surface. Firstly, a water content assay was performed. The lenses used  
124 were all Vistagel non-ionic lenses (n=4) with water contents of 38%, 42%, 60%, and 75%.  
125 HEMA or HEMA/NVP lenses were chosen to evaluate the effect of lens water content on cell  
126 adhesion because the material is available in a range of water contents. Secondly, an ionicity  
127 assay using non-ionic Group II (vasurfilcon A, n=2) versus ionic Group IV (etafilcon A, n=2)  
128 lenses (both are high water content lenses) was performed. All of the lenses were doped with  
129 Vn at a concentration of 10 µg/ml for 24 hours. Only the Vn positive control and antibody  
130 control lenses were tested.

131

#### 132 *2.7. Ex vivo contact lenses assays*

133

134 A range of lenses (Table 2) was worn by asymptomatic subjects in either a daily wear modality,  
135 averaging 196 hours over 2 weeks, or an extended wear modality, averaging 168 hours over 1  
136 week, as specified with each assay. Upon removal, lenses were placed in PBS and stored at  
137 4°C. A total of over 100 lenses was assayed in this study. Cell adhesion on the anterior and  
138 posterior surface of Group IV etafilcon A lenses was analysed. Lenses from 8 subjects were  
139 worn on a daily wear basis (n=8) and on an extended wear (n=8) basis. Centre versus edge  
140 analysis was analysed on Group II (vasurfilcon A, n=8) daily wear and Group IV (etafilcon A,  
141 n=8) daily wear lenses. The study was extended to include one conventional hydrogel lens  
142 material (etafilcon A) and three silicone hydrogel lens materials (lotrafilcon A, lotrafilcon B  
143 and balafilcon A) to assess material variation and lens modulus. Each lens type (n=4) was worn  
144 by the same asymptomatic subject on a daily wear basis and stored in saline solution after  
145 removal. ReNu® multipurpose solution (B&L) was used to clean the lenses where necessary.  
146 Work done previously in our laboratories found that levels of adsorbed Vn were only  
147 marginally reduced (<5%) by treatment with this care solution. This was also found to be the  
148 case with *ex vivo* lenses. The study and its protocol were approved by an Institutional Review  
149 Board in accordance with the tenets of the Declaration of Helsinki.

150

#### 151 *2.8. Assessment of the contributory role of fibronectin*

152

153 Fn is an important adhesion protein which, in addition to Vn, has been reported in tears [43].  
154 Both of these cell attachment-promoting proteins are immunologically unrelated and  
155 biochemically different but, due to the fact that their cell adhesive properties are similar, it was  
156 inadvisable to assume that Vn was solely responsible for both adsorption onto the contact lens  
157 and the cell-mediated adhesion. From a doubling dilution range of standards, a concentration  
158 of 12.5 µg/ml of Fn was selected - taking into account the requirement for a satisfactory cell  
159 count and cost effectiveness. This concentration is similar to those levels used for the Vn  
160 doping experiments, and slightly higher than those levels of Fn measured in tears (~ 4 µg/ml  
161 [44]) allowing for a marginal increase in tear levels. The designated, control, anti-Vn and anti-  
162 Fn, Group IV etafilcon A lenses were doped in 12.5 µg/ml of Fn for 24 hours. For all initial  
163 validation assays, an anti-Fn antibody at 1:100 in HBS, was also used as a direct comparison  
164 against the anti-Vn antibody and Vn standard controls. Again, this was to either eliminate or  
165 accept the role of Fn as a competitive adhesion molecule in contact lens wear and/or to further  
166 validate the dominant adhesion of Vn onto the contact lens.

167

### 168 **3. Results**

169

#### 170 *3.1. In vitro method validation*

171

172 The average cell counts on doped lenses were greatest for the Vn positive control lenses ( $59\pm 3$ )  
173 and for the antibody control lenses ( $52\pm 3$ ). The lenses blocked with anti-Vn demonstrated  
174 expected low cell counts ( $4\pm 2$ ) (Fig. 1). A set of non-doped blank lenses ( $n=3$ ) was also assayed  
175 where an average background level of  $<5$  cells was observed on all lenses; a similar cell count  
176 to the lenses treated with anti-Vn. The comparison of cell counts between the blank lenses and  
177 doped lenses shows a 20-fold increase in the average cell count per field. These results verify  
178 Vn dependant adhesion of cell fibroblasts to lenses and demonstrate the use of a cell-based  
179 assay to detect Vn. Fn demonstrated poor adsorption out of doping solution onto the contact  
180 lens, displaying low cell counts ( $10\pm 2$ ) in comparison to Vn-mediated adhesion ( $59\pm 3$ ). Anti-  
181 Fn antibodies which were also incorporated into the assay to negate the role of this adhesive  
182 glycoprotein in the attachment of the cells to the contact lens demonstrated no inhibitory  
183 influence. Thus, it could be concluded that Fn is clearly not involved in cell adhesion with these  
184 cell types and therefore does not adversely interfere with this Vn dominated cell-based assay.

185

#### 186 *3.2. The effect of Vn doping concentration, lens water content and ionicity on Vn adsorption*

187

188 The higher the concentration of Vn in the doping solution the higher the cell counts. Increasing  
189 the Vn concentration from  $1\ \mu\text{g/ml}$  to  $20\ \mu\text{g/ml}$  gave an increase in the average cell count per  
190 field from  $5\pm 0.8$  to  $37\pm 2$  (Fig. 2). All subsequent lenses doped with Vn were doped with  $10$   
191  $\mu\text{g/ml}$  as this was found to be the optimum concentration. The effect of lens water content on  
192 cell counts showed the higher the water content of the lens, the higher the Vn-mediated cell  
193 adhesion. Average cell count per field for lenses with water contents of 38% and 75% increased  
194 from  $42\pm 0.8$  to  $58\pm 1$  respectively (Fig. 3). The results illustrate the fact that water content does  
195 not have a substantial effect on these non-ionic lenses, but there is a progressive increase in  
196 adsorption with water content, with an assumed tendency to reach a plateau of adsorption. Anti-  
197 Vn antibody controls were used to validate the cell-Vn adhesion and to negate cell-lens  
198 interactions. Greater cell counts on high water content ionic Group IV lenses ( $73\pm 6$ ) were  
199 observed in comparison to high water content non-ionic Group II lenses ( $53\pm 9$ ) (Fig. 4). High  
200 water content ionic lenses were found to adsorb the greatest protein, in contrast to low water

201 content non-ionic lenses. This may suggest that the ionicity of the lens is more important than  
202 the water content with regard to Vn adsorption.

203

### 204 *3.3. Vn deposition on anterior and posterior surfaces of ex vivo lenses in daily wear and* 205 *extended wear modalities*

206

207 Higher cell counts on the posterior surface of the lenses were determined in comparison to the  
208 anterior surface, irrelevant of the modality of wear, as average cell counts per field increased  
209 by 95% from the anterior to the posterior surface in both wear modalities (Fig. 5). All further  
210 test lenses, therefore, analysed the posterior lens surface only. Greater cell counts were also  
211 detected on extended wear lenses than daily wear lenses with an average increase in cell count  
212 of 46% for both the posterior and anterior surfaces of the lenses.

213

### 214 *3.4. Vn deposition on ex vivo daily wear lenses, center versus edge*

215

216 It was noted that there was a difference in locus of Vn deposition on the posterior lens surface.  
217 Therefore, a comparison of Vn adsorption at the centre and edge of the lenses was performed.  
218 Greater Vn deposition was observed at the lens edge compared to the centre, irrespective of the  
219 lens material type. Average increases in cell counts from centre to edge (on the posterior lens  
220 surface) of 68% and 65% were observed for Group II lenses and Group IV lenses respectively  
221 (Fig. 6). The results revealed higher cell counts on the Group IV ionic material in comparison  
222 to the Group II non-ionic material, both for the lens centre with an average cell count increase  
223 of 30% and the lens edge with an average increase of 25%.

224

### 225 *3.5. Material variation and the effect of lens modulus*

226

227 The highest levels of Vn deposition was determined on the etafilcon A material ( $117 \pm 4$ ), with  
228 lotrafilcon B, balafilcon A and lotrafilcon A showing decreasing cell counts at the lens edge  
229 ( $115 \pm 4$ ,  $107 \pm 5$ ,  $88 \pm 6$  respectively) (Fig. 7). The relationship between vitronectin-mediated cell  
230 count and lens modulus in terms of water content is summarised in Table 3. The lower the  
231 modulus, the greater the deposition at the lens edge. Lotrafilcon A, a low water content high  
232 modulus material has a lower edge:center ratio of 1.3:1, whereas etafilcon A, a high water  
233 content low modulus material, has a higher edge:center ratio of 3.3:1. A comparison of two  
234 similar lenses revealed that lotrafilcon B, with a lower modulus of 1.0 MPa, had a much greater



235 edge:centre ratio in comparison to lotrafilcon A, with a higher modulus of 1.5 MPa. Lotrafilcon  
236 B, the softer material, allows more drape of the lens over the cornea, thus lens-tissue interaction  
237 is emphasised at the lens edge.

238

#### 239 **4. Discussion**

240

241 The adhesive nature of Vn and its role in fibroblast cell attachment and movement was  
242 exploited to demonstrate the interaction of this glycoprotein with contact lens surfaces and the  
243 influence of the contact lens on Vn deposition out of tears and/or the corneal tissue bed was  
244 established. *In vitro* doping of contact lenses with Vn at varying concentrations showed a direct  
245 correlation between an increase in Vn concentration and its adsorption onto the contact lens.  
246 Although a plateau was not reached within the concentration levels studied, it can be expected  
247 that a limiting plateau would ultimately be achieved after a gradual increase. However, as  
248 previously stated, Vn concentrations in the eye have been reported at  $0.75\pm 0.32$   $\mu\text{g/ml}$  in the  
249 open eye [1]. It is therefore extremely unlikely for Vn concentrations to exceed the *in vitro*  
250 experimental limits of 20  $\mu\text{g/ml}$ , in tears. These results demonstrate that cell adhesion is  
251 dependent upon Vn concentration in solution. However, concentration curves cannot be used  
252 to calculate Vn concentration against cell counts as each assay must be treated separately. It  
253 was also observed that the percentage water content of materials directly affected Vn  
254 adsorption; an increase in water content clearly exhibited a rise in the adsorbed levels of Vn.  
255 In addition, the ionicity of the lens also greatly influenced the adsorption of Vn with greater  
256 accumulation of Vn on the ionic (Group IV) versus the non-ionic (Group II) lenses.

257

258 Deposition of Vn was significantly greater on *ex vivo* lenses in comparison with lenses doped  
259 with Vn *in vitro*. Centre versus the edge of the lens analysis revealed interesting differences in  
260 Vn levels. There was a marked increase in Vn accumulation at the edge of the lens in contrast  
261 to the centre of the lens. This phenomenon was evident in both the daily wear and extended  
262 wear regimes. The fact that this preferential adsorption was evident for both wear modalities is  
263 very significant. As the name suggests, daily wear lenses are inserted and removed on a daily  
264 basis. The effect of daily handling of the lens, varying insertion and removal parameters and  
265 cleaning would be expected to change the characteristics of the deposition of Vn. However,  
266 this was not the case and the deposition profiles resembled that of the extended wear modality.  
267 The use of the multipurpose solution had little effect on Vn levels. Both wear modalities

268 appeared to create a Vn rich micro-climate at edge of the lens, which may be the site of  
269 localised inflammatory mediation.

270

271 Vn deposition was predominantly found to occur on the posterior surface of the lens in  
272 accordance with those results established in a preliminary study [45] where significantly  
273 greater levels of Vn were observed on the back surface of a worn lens in comparison with the  
274 front surface irrespective of wear modality or lens material properties. The accumulation at the  
275 posterior lens surface may reflect Vn moving out of the corneal tissue bed due to lens-tissue  
276 interactions, as opposed to simply reflecting tear derived Vn. Aggregation of Vn on the  
277 posterior surface is thought to create a particular micro climate, which due to its multifunctional  
278 nature and ability to bind to numerous ligands and proteins, could lead to the initiation of, or  
279 role in, a number of effector systems. A sliding motion of the eyelid over the lens surface will  
280 bring about fricto-mechanical stimulation [46]. This movement might be expected to stimulate  
281 a biochemical response with the potential to generate an upregulation of particular components  
282 or to activate additional pathways in response to the physical trauma of the eyelid-lens  
283 interaction – modest though that might be. Diminished tear flow at the posterior surface of the  
284 lens, in addition to a reduction in the dynamic interaction with the tissue bed, would be expected  
285 to produce a quite different level of response with the potential adsorption of specific  
286 biochemical components from the more ‘closed’ environment. The importance of anterior  
287 versus posterior lens differential in terms of biochemical interactions and physical parameters  
288 cannot be under estimated and its significance has been reviewed elsewhere [47, 48].

289

290 Greater Vn deposition was also detected on extended wear lenses compared with daily wear  
291 lenses. Taking the total wear time and lens-tissue bed contact into consideration, the cell  
292 attachment was always greater for the extended wear lenses than the daily wear lenses. The  
293 cell attachment observed at the *in vitro* concentrations equivalent to those found in tears are  
294 much lower than those found on posterior surfaces of worn lenses. This may be explained by  
295 the interaction between the ocular tissue and contact lens, with the posterior microclimate  
296 favouring Vn attachment. The investigation was extended to include Group II and Group IV  
297 material types and a comparison of Vn levels for the central and peripheral regions of the lenses  
298 was carried out on the posterior surface of the lenses. Greater Vn deposition on Group II  
299 materials in contrast with Group IV materials demonstrated that cell attachment is markedly  
300 dependent upon material type, highlighting the potential for materials effects in influencing Vn  
301 deposition and the nature of the post-lens microclimate. Again, an evaluation of the centre

302 versus the edge of the lens revealed that a greater Vn concentration resulted on the edge. The  
303 locus of Vn deposition is significant as this may influence the locus of plasmin regulation.  
304 Localised plasmin at the edge has the potential to escape into the tear film, whereas plasmin  
305 regulated at the centre of the lens may become ‘trapped’ in that region.

306

307 The edge:centre cell count ratio was clearly material dependent and it appears that the influence  
308 of modulus on cell adhesion overrides any effect of lens water content and ionicity one. The  
309 modulus of a lens describes its resistance to deformation, where modulus is equal to  
310 stress/strain. In general, it was observed that the lower the modulus, the greater the deposition  
311 of Vn at the lens edge and a low water content high modulus material, such as lotrafilcon A,  
312 has a lower edge:centre ratio compared with a high water content low modulus material, such  
313 as etafilcon A, which has a higher edge:centre ratio. Although the morphology of silicone  
314 hydrogel lenses complicates matters further, the lens modulus is a significant if not dominant  
315 factor.

316

317 The emerging patterns are clear - the presence of a contact lens concentrates Vn near the ocular  
318 tissue bed, and thus the preferential adsorption of Vn, particularly towards the edge, on to the  
319 lens surface reveals a Vn rich post-lens micro climate that can influence localised inflammation  
320 and upregulation of plasmin. Vn is involved in the regulation of fibrinolysis, a consequence of  
321 the fact that it binds and stabilises plasminogen activator inhibitor-1 (PAI-1), which thereby  
322 allows PAI-1 to inhibit the action of tissue plasminogen activator (tPA) and the fibrinolysis  
323 process as a whole [20]. If Vn is localised on a surface adjacent to the cellular site, the  
324 somatomedin B homology region of the protein binds to the active site of PAI-1, thereby  
325 generating plasminogen activator and resulting in the upregulation of plasmin [49]. Tear  
326 plasmin activity has been observed in tear fluid of subjects with corneal disorders, for example  
327 an increase in tear plasmin in particular in corneal ulcers has been demonstrated [50], leading  
328 to the implication that elevated plasmin levels are important in the pathogenesis of ocular  
329 infection and dysfunction. The view is that it is an important potential trigger of additional  
330 events leading, in extreme cases, to pathology in an otherwise healthy tissue. Plasmin, for  
331 example, can cleave Fn (an important adhesion molecule involved in corneal re-epithelisation),  
332 which is significant as Fn degradation is associated with impaired wound healing [51, 52].

333

334 Levels of tear plasmin have been shown to increase progressively in the sequence: no lens  
335 control group, daily wear soft lens group, extended wear soft lens group [53], and it has been

336 proposed that the proteolytic activity of plasmin may contribute to corneal epithelial  
337 abnormalities associated with lens wear [49, 53]. Vn localised on the lens surface adjacent to  
338 the corneal surface may remove PAI-1 leading to local upregulation of plasmin in the posterior  
339 tear film. If Vn is localised on a (synthetic) surface adjacent to the cellular site (such as a  
340 chronic wound) it removes PAI-1 from the reaction by fixing it, creating an imbalance in favour  
341 of plasminogen activator. This can result in a local upregulation of active plasmin formation,  
342 thereby controlling an important regulatory mechanism in wound repair; an increase in  
343 degradative proteolysis which may then result in a state of non-healing and excessive  
344 inflammation.

345

346 It remains unclear whether Vn binds to the lens surface to form a monolayer or whether  
347 constant protein binding continues to occur. Is there an initial layer of Vn formed which is  
348 always retained on the surface or is there constant competitive binding through some form of  
349 proteolysis or denaturation?

350

## 351 **5. Conclusions**

352

353 The potential for materials to affect Vn deposition will affect the locus of plasmin generation  
354 and thus influence lens-induced inflammatory processes. Clinical implications of this are yet  
355 to be determined, and further studies are required in order to comment on the ideal properties  
356 of a lens when considering the connection between contact lenses and the consequential  
357 inflammatory process. It can be said that an ideal lens is one that minimises protein interaction  
358 at the surface and that allows more exchange of protein at the edge. The unique conformational  
359 flexibility and multidomain structure of Vn which allows it to bind to a large repertoire of  
360 ligands makes its potential interactions with biomaterials all the more intriguing. Its versatile  
361 binding capabilities and receptor functions could, in the future, be used in the characterisation  
362 of structure-function properties and importantly in the design of new biomaterials.

363

364 The significance of this body of research must lie in the area of wound healing and the  
365 compromised anterior eye. Bandage contact lenses (BCLs) are regularly used to protect the  
366 compromised cornea from further ocular insult, to enable the relief of pain and to improve the  
367 ability of the corneal epithelium to heal. However, the use of contact lenses in therapeutics as  
368 bandage lenses is in its infancy. Lens choice appears to be influenced by convenience and  
369 availability rather than specific knowledge of their biochemistry of the healing process. Little

370 is known about the interaction of specific materials with corneal conditions and the way in  
371 which materials can promote/inhibit the healing process. The importance of lens choice is  
372 therefore apparent when evaluating the effect of material on the inflammatory process. *Ex vivo*  
373 lenses worn in the uncompromised eye only were analysed in this study. The study is currently  
374 being expanded to include lenses worn for bandage use in the compromised eye.

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## Figure Legends

Figure 1. Cell counts on Vn doped (20 µg/ml) polyHEMA lenses in vitro. The greatest cell counts were found to be on Vn positive control lenses (59±3.3) and similar levels were found as expected on the antibody control lenses (52±3). Lenses treated with the anti-Vn negative control were found to have the lowest cell counts (4±2), validating the role of Vn for cell adhesion.

Figure 2. Cell counts with varying concentrations of vitronectin on polyHEMA lenses in vitro. The higher the doping concentration of Vn, the higher the cell counts; increasing the Vn concentration from 1 µg/ml to 20 µg/ml gave an increase in the average cell count per field from 5±0 to 37±1.7.

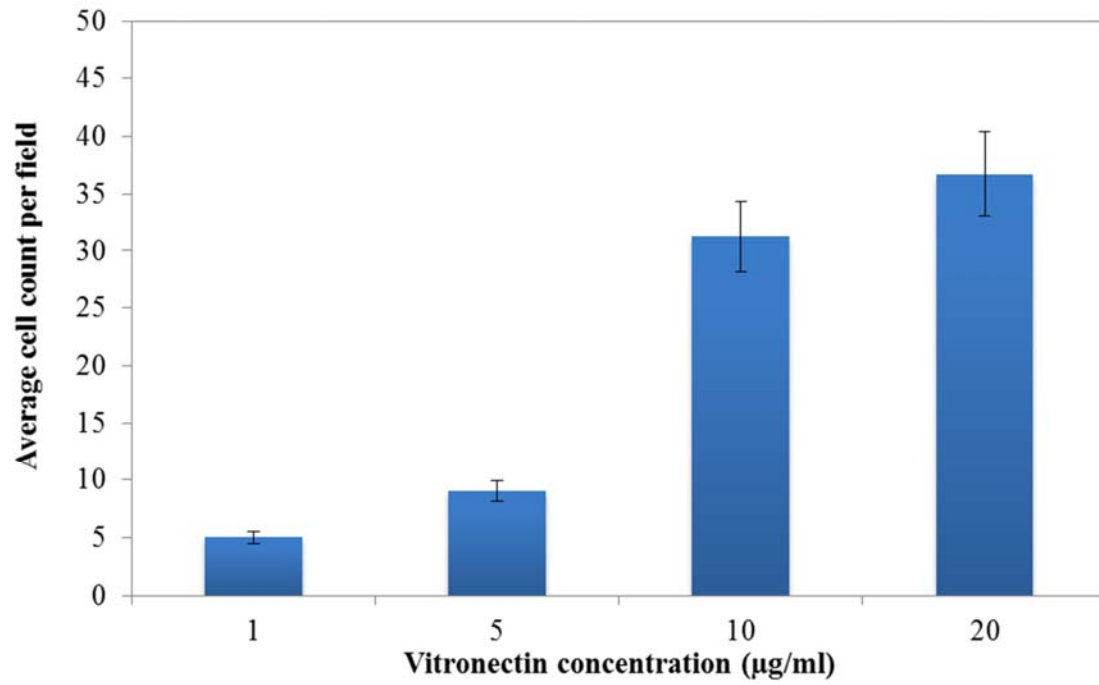
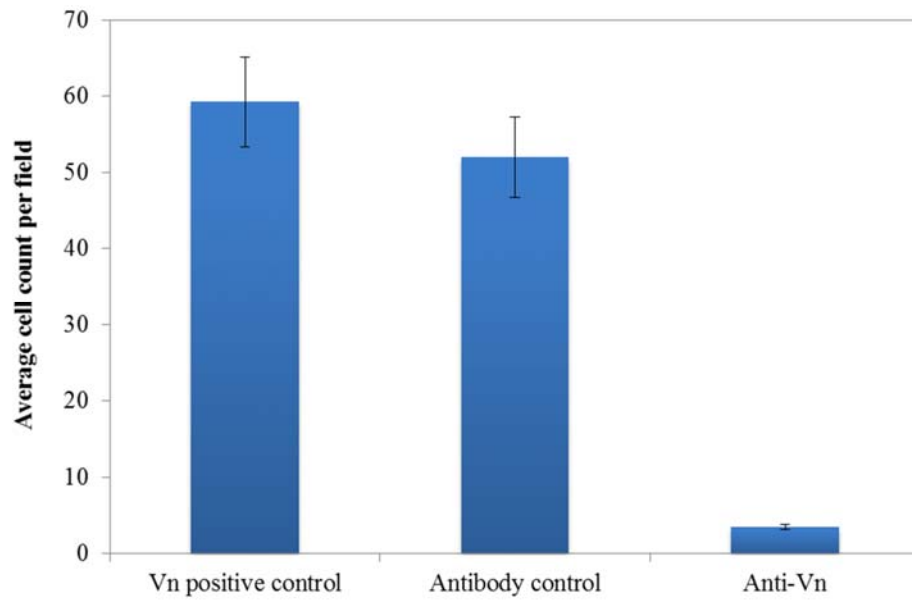
Figure 3. The relationship between Vn-mediated cell counts and lens water content. The higher the water content of the lens, the higher the Vn-mediated cell adhesion; the average cell count per field for lenses with water contents of 38% and 75% increased from 42±0.8 to 58±0.96 respectively.

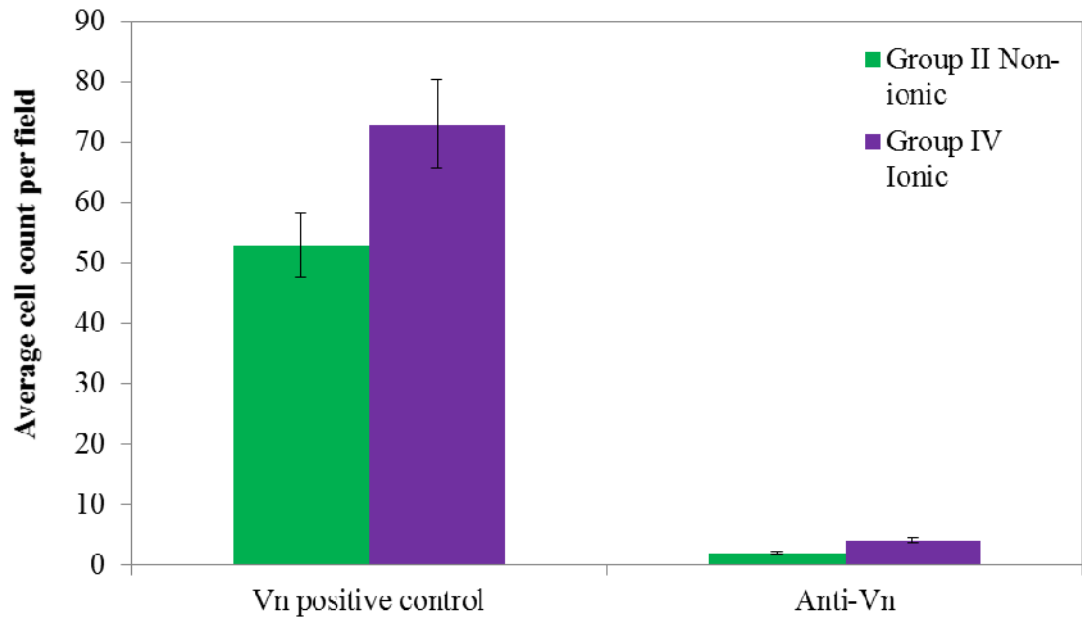
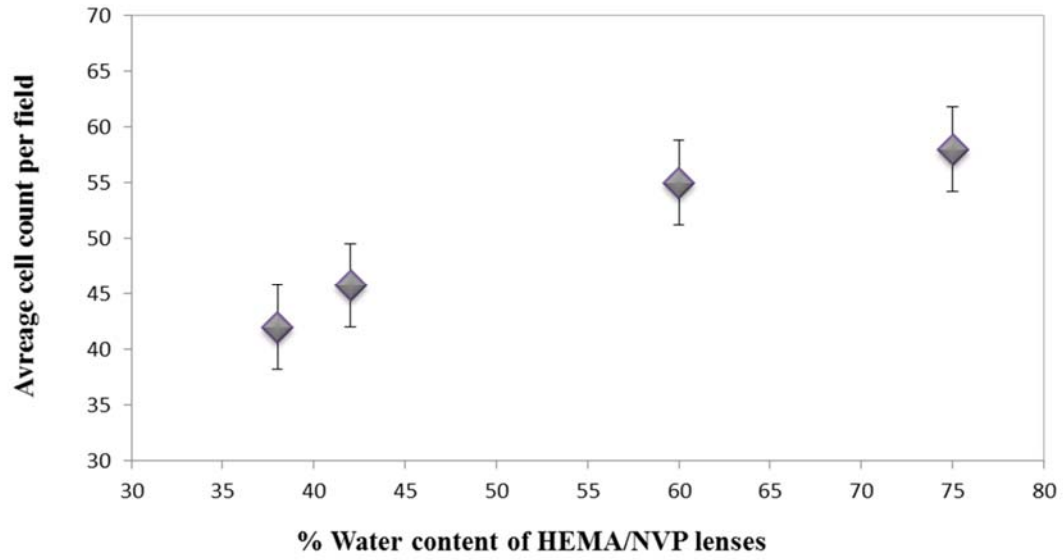
Figure 4. The relationship between Vn-mediated cell counts and lens ionicity. High water content ionic Group IV lenses had greater cell counts (etafilcon A 73±6) compared with high water content non-ionic Group II lenses (vasurfilcon A 53±9).

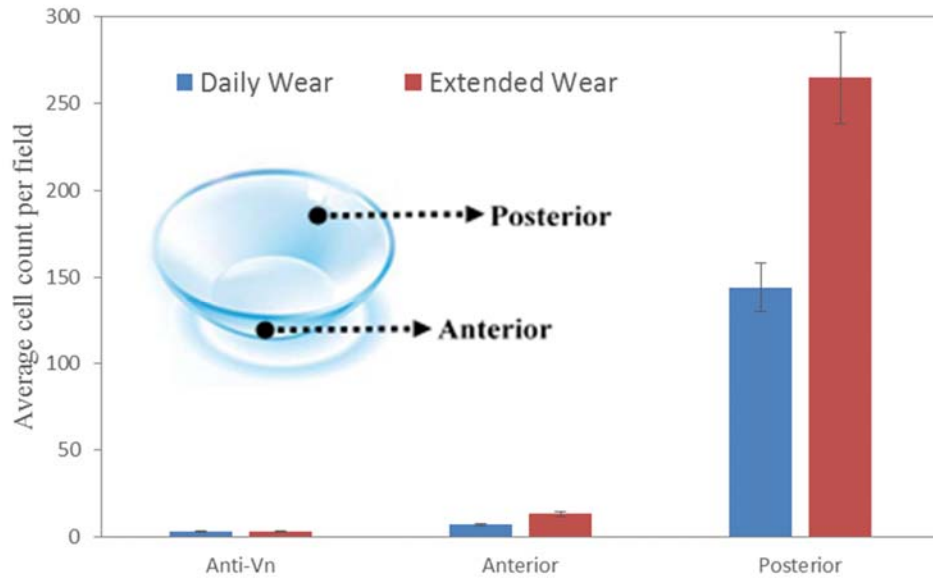
Figure 5. Comparative vitronectin-dependent cell counts on daily wear and extended wear etafilcon A lenses: anterior versus posterior. Higher cell counts were always detected on the posterior lens surface (daily wear 144±15, extended wear 265±26) than on the anterior lens surface (daily wear 7±0.3, extended wear 13±1). Greater cell counts overall were also detected on extended wear (198 hours wear) lenses in comparison to daily wear (168 hours wear) lenses.

Figure 6. Comparative vitronectin-dependent cell counts on the posterior surface of ex vivo Group II (vasurfilcon A) and Group IV (etafilcon A) contact lenses worn on a daily wear basis: centre versus edge. Cell counts on the centre and edge areas. Greater cell attachment was observed at the lens edge compared to the centre: cell counts increased from centre to edge for Group II and Group IV lenses by 68% and 65% respectively. The ionic Group IV material showed greater cell counts over the entire lens surface in comparison to the non-ionic Group II material.

Figure 7. The influence of lens material, worn on a daily wear basis, on vitronectin-mediated cell count: centre versus edge. The highest cell counts levels were found on the etafilcon A material, with lotrafilcon B balafilcon A and lotrafilcon A showing decreasing cell counts respectively at the lens edge.







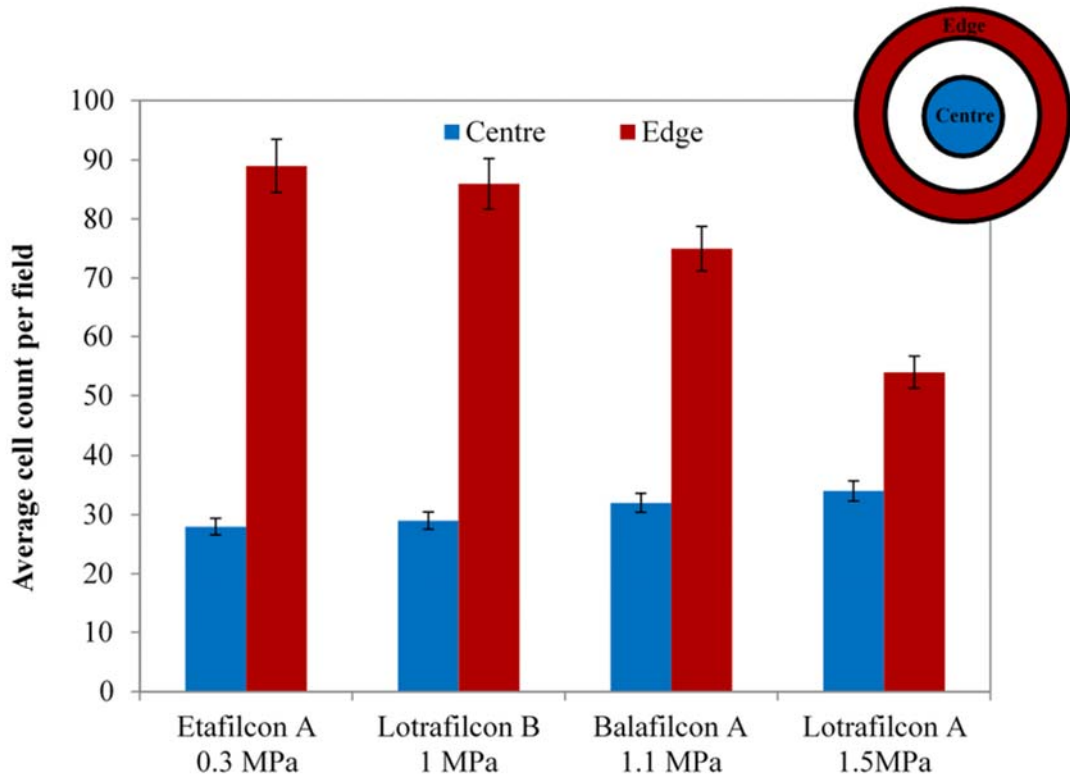
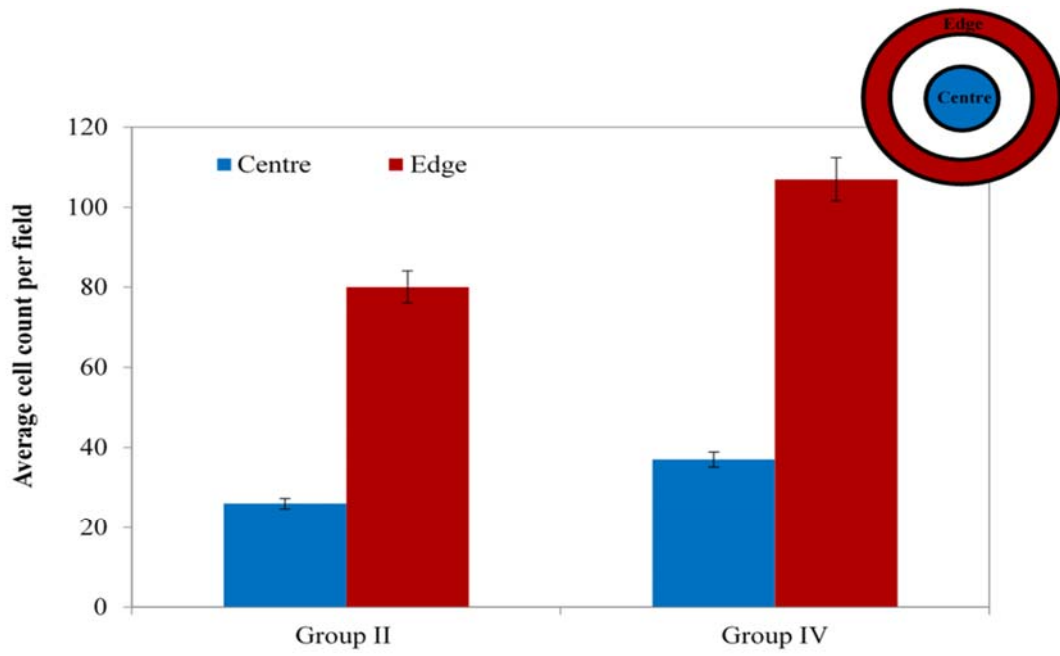


Table 1. A summary of the diverse functions of vitronectin.

<b>Process</b>	<b>Description</b>	<b>Consequences</b>
Complement regulation [5-7]	Inhibition of MAC (C5b-9)	Protection of bystander cells
T-cell cytotoxicity [8, 9]	Inhibition of cell lysis by perforin	Protection of bystander cells
Cellular adhesion [10-14]	Integrin binding	Migration, attachment and aids healing
Thrombosis [15-17]	Binds thrombin-antithrombin III	Inhibits thrombin inactivation, regulating blood coagulation
Fibrinolysis [18-21]	Stabilizes PAI-1	Anti-proteolytic activity
Inflammation [22]	Binds $\beta$ -endorphin	Pain suppressor
Binds structural macromolecules [23-26]	Heparin, collagen, heparin sulphate	For activation or adhesion to surfaces. Healing?
Growth factor interaction [27-29]	Vn-GF complexes	Promote wounding healing and cell regulation
Anti-bacterial [30, 31]	Cell-bacteria mediated interaction	Enhanced intracellular killing of surface bound bacteria

Table 3. The relationship between lens modulus, edge:centre ratio and water content.

<b>Material</b>	<b>Etafilcon A</b>	<b>Lotrafilcon B</b>	<b>Balafilcon A</b>	<b>Lotrafilcon A</b>
Modulus (MPa)	0.3	1	1.1	1.5
Edge : Centre Ratio	3.3 : 1	3.0 : 1	2.5 : 1	1.3 : 1
Water Content (%)	58	33	36	24

Table 3. The relationship between lens modulus, edge:centre ratio and water content.

Material	Etafilcon A	Lotrafilcon B	Balafilcon A	Lotrafilcon A
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