

Allocation of rhodamine-loaded nanocapsules from blood circulatory system to adjacent tissues assessed *in vivo* by fluorescence spectroscopy

Yana Tarakanchikova^{1,2,3,9}, Olga Stelmashchuk⁴, Evgeniya Seryogina⁴,
Gennadii Piavchenko^{4,5}, Evgeny Zherebtsov⁶, Andrey Dunaev⁴,
Alexey Popov^{1,7} and Igor Meglinski^{1,4,7,8}

¹ Opto-Electronics and Measurement Techniques Research Unit, University of Oulu, Oulu, Finland

² Nanobiotechnology Laboratory, St. Petersburg Academic University, St Petersburg, Russia ³

Research Institute of Pediatric Oncology, Hematology and Transplantology named by R.M.

Gorbacheva, St Petersburg, Russia

⁴ Orel State University named after I.S. Turgenev, Orel, Russia

⁵ Centre of Preclinical Research, JSC 'Retinoids', Moscow, Russia

⁶ Aston University, Aston Institute of Photonic Technologies, Birmingham, United Kingdom

⁷ Interdisciplinary Laboratory of Biophotonics, National Research Tomsk State University, Tomsk, Russia ⁸ National Research Nuclear University 'MEPhI', Institute of Engineering Physics for Biomedicine (PhysBio), Moscow, Russia

E-mail: yana.tarakanchikova@oulu.fi

Abstract

Modern fluorescent modalities play an important role in the functional diagnostic of various physiological processes in living tissues. Utilizing the fluorescence spectroscopy approach we observe the circulation of fluorescent-labelled nanocapsules with rhodamine tetramethylrhodamine in a microcirculatory blood system. The measurements were conducted transcutaneously on the surface of healthy Wistar rat thighs *in vivo*. The administration of the preparation capsule suspension with a rhodamine concentration of 5 mg kg⁻¹ of the animal weight resulted in a two-fold increase of fluorescence intensity relative to the baseline level. The dissemination of nanocapsules in the adjacent tissues via the circulatory system was observed and assessed quantitatively. The approach can be used for the transdermal assessment of rhodamine-loaded capsules *in vivo*.

Keywords: nanocomposite polymeric capsules, fluorescent-labelled particles, drug delivery, fluorescence spectroscopy, blood microcirculation, optical measurements *in vivo* (Some figures may appear in colour only in the online journal)

1. Introduction

The conventional monitoring of administrated substance distribution in animals requires specimen preparation including the staining of the tissue to determine the localization and concentration of various analytes. Typically, invasive and destructive tests cannot be applied to record the dynamics of the distribution processes within a certain time. Therefore, methods for whole animal imaging *in vivo* have undergone rapid development [1]. Such approaches appear promising, making it possible to measure a single point of the sample or to perform the imaging of the entire animal body and reveal the related biological processes in real time. In major cases, minimally invasive intervention is required [2]. From this point of view, optical noninvasive diagnostic approaches are of particular interest because of their high sensitivity,

versatility and low cost. To obtain reliable information *in vivo*, various optical methods have been developed and successfully used in various medical applications in the past [3, 4]. Optical coherence tomography has been effectively utilized to assess the efficiency of percutaneous vaccine delivery [5, 6]. Intravital microscopy has been used for the noninvasive continuous monitoring of blood flow [7, 8] and drug transfer in the body [9]. Photoacoustic imaging has been successfully applied to visualize transport and the accumulation of substances in organs or in tumour tissue [3]. Laser-induced fluorescence techniques can also be assigned to monitoring methods inside the body utilizing microencapsulated biomarkers [10, 11]. The optical diagnostic approach also has considerable potential in preclinical and clinical trials [12].

Another vibrant area is the targeted delivery of drugs, which is able to significantly improve the effectiveness of the

treatment of various diseases, and reduce the occurrence of possible adverse side effects and disease complications. The development of such controlled-release preparations, in many cases, is associated with the design of a microscopic nanoscale system, such as capsules for loading biologically active substances and delivering them directly to the target. Thus, the encapsulation of biologically active materials for drug delivery *in vivo* is a complex task requiring significant fundamental and applied research, including the development of nanocapsules for drug transportation as well as *in vivo* delivery control technology [13, 14]. One of the recent advancements in the field is the fabrication of porous inorganic nanoparticles with high chemical and mechanical stability, as well as tunable physical and chemical properties. As transport containers, the particles can be loaded with various components. Fluorescent labelling makes it possible to optically monitor delivery efficiency [15, 16].

In the current study, fluorescence spectroscopy was used to assess the allocation of fluorescently labelled polymer nanoparticles in the blood circulatory system of healthy rats. The aim of the study was to find informative points (areas) on the rat skin for transcutaneous fluorescence measurements, and to study the dynamics of the fluorescent-labelled (rhodamine tetramethylrhodamine (TRITC)) nanocapsules injected into the circulatory system.

2. Materials and methods

The fluorescence spectroscopy system with a fibre-optical probe 'LAKK-M' (SPE 'LAZMA' Ltd, Russia) was used for the *in vivo* measurements (see figure 1). The system provides multiwavelength excitation, registers emission and processes the detected fluorescence signal. It includes fluorescence excitation in UV ($\lambda = 365$ nm, 1.5 mW), blue ($\lambda = 450$ nm, power = 3.5 mW) and green light ($\lambda = 532$ nm, power = 4.5 mW). The above-mentioned fluorescence excitation powers are provided at the tip of the fibre probe, which induces an excitation light flux in the tissue of no more than 0.16 W m⁻² for 365 nm and 0.37 W m⁻² for 450 nm. The spectrophotometer was a polychromator with a diffraction grating and a CCD (TCD1304AP, Toshiba, Tokyo, Japan) as a detector.

Polymeric capsules were fabricated using calcium carbonate (CaCO₃) particles as a sacrificial template. The CaCO₃ particles were prepared according to the standard method described by Parakhonskiy *et al* [15]. The CaCl₂ (0.33 M) and Na₂CO₃ (0.33 M) aqueous solutions, dissolved in 20 ml ethylene glycol, were mixed under vigorous stirring for 3 h, leading to the precipitation of CaCO₃ particles. Then, the CaCO₃ particles were washed with pure water to remove the unreacted species. Spherical CaCO₃ particles with an average diameter of 500 ± 100 nm were obtained. The structure of the polymeric capsule shells included biodegradable polyelectrolyte dextran sulfate (DS, MW > 70 000) and poly-L-arginine hydrochloride (PARG, MW > 70 000). A combination of PARG and DS is mostly used for the preparation of bio-capsules via the layer-by-layer method [11]. The process of layer-by-layer polymer film assembly is based on the interaction and self-organization of complementary macromolecular pairs with the formation of a water-insoluble complex on the template surface. The process begins with the adsorption of the polycation (PARG) from the aqueous solution onto the negatively charged surface of the template. At the next step, the polyanion (DS) is adsorbed onto the positively charged surface of the template, and again the sign of the surface charge of the template becomes negative. A step-by-step repetition of the described procedure leads to the formation of a water-insoluble polyanion/polycation complex on the template surface (see figure 2(a)). Further, the CaCO₃ core is removed by ethylenediaminetetraacetic acid disodium salt. The capsules were labelled with fluorescent dye rhodamine TRITC (see figure 2(b)). TRITC is a bright red fluorescent dye with excitation ideally suited to the 532 nm laser line. Using this wavelength, we can observe the whole epidermis as well as a papillary layer of the dermis, which allows the presence of the nanocapsules in the microcirculatory system of the skin to be validated. Characterization of the obtained microcapsules was carried out using confocal laser scanning microscopy (CLSM) and scanning electron microscopy (SEM) (see figure 2).

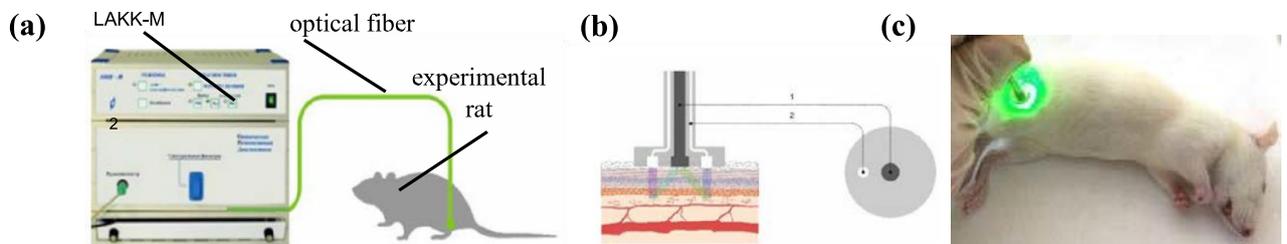


Figure 1. Exterior view of the experimental setup: (a) the multifunctional laser diagnostic complex LAKK-M control unit with laser and optical fibre; (b) the design of the fiber diagnostic probe used in the study ((1) is the collection fiber, (2) is a laser of 532 nm); (c) the laboratory rat used in the experiments.

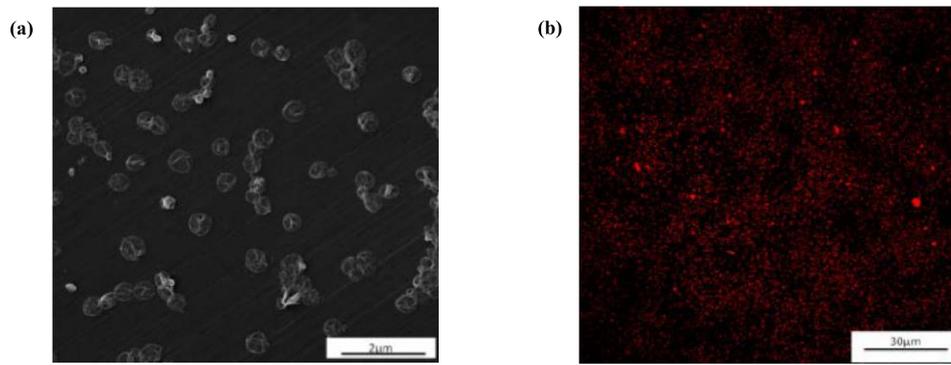


Figure 2. Capsule morphology analysis. SEM (a), and the CLSM (b) of the polyelectrolyte nanocomposite capsules. (a) The SEM measurements demonstrated the integrity of the nanofunctionalized shells and hollow inner cavity. (b) A CLSM scan at the emission bandwidth of the rhodamine TRITC dye.

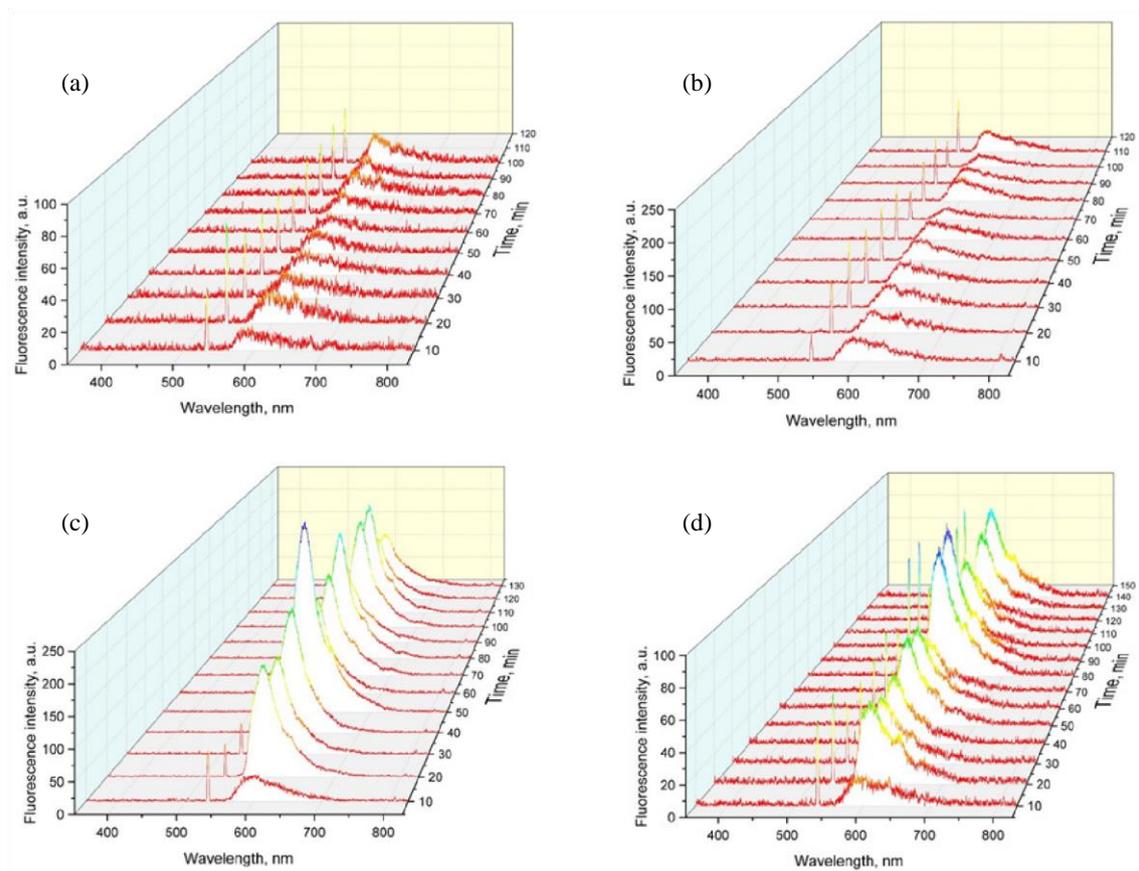


Figure 3. The averaged fluorescence spectra distribution of the leg ((a)—control rat group, (c)—capsule rat group) and tail ((b)—control rat group, (d)—capsule rat group).

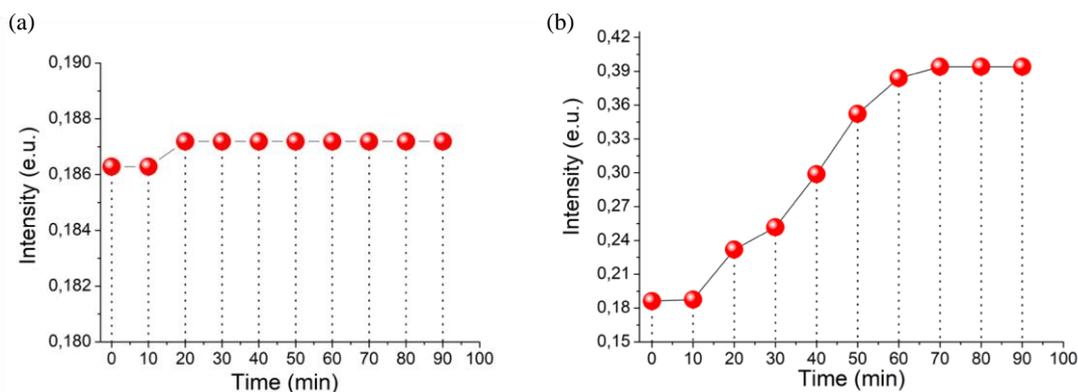


Figure 4. The dynamics of the intensity of normalized fluorescence in the control group (a) and in the group that received fluorescent-labelled (rhodamine TRITC) nanocapsules (b).

3. Results and discussion

Experimental studies were carried out on groups of clinically healthy Wistar rats. The animals were held in quarantine for two weeks in the vivarium of the Centre of Preclinical Research, JSC ‘Retinoids’, with temperature, humidity, bacterial contamination and day–night cycle conditions according to good laboratory practice principles. Every day during the quarantine the animals were examined by a veterinarian, after that they were randomised into two groups according to their weight medians. During the experiment, the rats were anaesthetised with Zoletil 100 (Virbac, France) in standard doses. The model animals were divided into two groups, which received the same food. In the study, twelve 100–120 g Wistar rats were divided into two groups: one was treated with rhodamine-loaded capsules, injected directly into the bloodstream ($n = 6$), and the second was the control ($n = 6$). Before administration of the drug, background fluorescence was measured at a 532 nm excitation wavelength and due to the better repeatability, the measurement points on the rats’ thighs were selected. The treated group of rats received injections of rhodamine capsules into the tail vein. The concentration of the resulting rhodamine in the group was 5 mg kg^{-1} of the animal weight. The fluorescence spectra were recorded from the thighs of anaesthetised rats for 90 min at 10 min intervals. A preliminary series of measurements of the repeatability of the skin fluorescence intensity was conducted in the control group. Before each measurement the skin was depilated and cleaned with 96% ethanol solution. After the experiment, the animals were euthanized in the CO_2 chamber. The experimental studies complied with EU Directive 2010/63/ EU, which defines the human attitude towards animals and refers to the principles of the three Rs (replacement, reduction and refinement). All studies were approved by the Ethical Committee of Orel State University.

The obtained fluorescence spectra show a statistically significant increase in the fluorescence intensity in the group of rats that received nanocapsules with rhodamine. In this group, a significant increase (from 42 ± 5 to 100 ± 7 a.u., two-fold the baseline level) at the wavelength of the peak of the rhodamine TRITC fluorescence intensity (about 576 nm) was registered (figure 3)

$$k_f = \frac{I_{\max}}{I_{bs} + I_{\max}} \quad (1)$$

where k_f is the normalised fluorescence intensity, I_{\max} represents the registered fluorescence intensity at 590 nm, and I_{bs} represents the maximum intensity of the backscattered laser radiation from the tissue (532 nm). The normalised procedure is necessary to compensate the variable absorption in skin and get more reliable measurement results (figure 4).

4. Conclusion

In this study, we used fluorescence spectroscopy to evaluate the penetration efficiency of nanocapsules from the circulatory system into adjacent tissues. Since porous containers have the potential to accumulate a significant amount of fluorescent dye, one of the methods for evaluating the effectiveness of transport involves measuring the fluorescence intensity on the surface of the body. The obtained fluorescence spectra show a statistically significant increase in fluorescence intensity in a group of rats that received nanocapsules with rhodamine. In this group, a significant increase (two-fold the baseline level) at the peak fluorescence intensity of the used dye ($\lambda = 590$ nm) from 42 ± 5 to 100 ± 7 a.u. was registered. The results show that fluorescence spectroscopy can be used to transcutaneously measure the concentration dynamics of labelled particles *in vivo*. The approach can increase the statistical significance and reliability of preclinical trials and reduce the required number of animals providing valuable information about pharmacodynamics and the optimal dosage of the drug. The results can be used in the field of preclinical drug research to control and ensure possible drug-in-place delivery as well as in the process of high-throughput screening during trials. Future studies will be focused on the implementation of targeted delivery—the creation of directional transport systems for medicines delivered to a particular type of tissue.

Acknowledgments

This work was supported by the Russian Foundation on Innovations U.M.N.I.K., the 2017 SPIE Optics and Photonics Education Scholarship, the CIMO Fellowship (TM-15-9729, YT), the EDUFI Fellowship (TM-17-10389, YT), the MEPHI Academic Excellence Project (contract no. 02.a03.21.0005, IM), the Tomsk State University Competitiveness Improvement Programme (IM), and the Academy of Finland (grant no. 311698, IM, grant 290596, AP). EZ kindly acknowledges the funding from the European Union's Horizon 2020 Research and Innovation Program under the Marie Skłodowska-Curie grant agreement no. 703145. AD and ES kindly acknowledges the funding by the Russian Science Foundation under project №18-15-00201.

References

- [1] Baker M 2010 Whole animal imaging: the whole picture *Nature* **463** 977
- [2] Honimann A and Nadler A 2018 The next frontier: quantitative biochemistry in living cells *J. Biochem.* **57** 47
- [3] Bremer C, Ntziachristos V and Weissleder R 2003 Optical-based molecular imaging: contrast agents and potential medical applications *Eur. Radiol.* **13** 231
- [4] Hillman E M C 2007 Optical brain imaging *in vivo*: techniques and applications from animal to man *J. Biomed. Opt.* **12** 051402
- [5] Kamali T, Doronin A, Rattanapak T, Hook S and Meglinski I 2012 Assessment of transcutaneous vaccine delivery by optical coherence tomography *Laser Phys. Lett.* **9** 607 [6] Rattanapak T, Birchall J, Young K, Ishii M, Meglinski I, Rades T and Hook S 2013 Transcutaneous immunization using micro-needles and cubosomes: mechanistic investigation using optical coherence tomography and two-photon microscopy *J. Control. Release* **172** 894
- [7] Kalchenko V, Kuznetsov Y, Meglinski I and Harmelin A 2012 Label free *in vivo* laser speckle imaging of blood and lymph vessels *J. Biomed. Opt.* **17** 050502
- [8] Kalchenko V, Ziv K, Addadi Y, Madar N, Meglinski I, Neeman M and Harmelin A 2010 Combined application of dynamic light scattering imaging and fluorescence intravital microscopy in vascular biology *Laser Phys. Lett.* **7** 60
- [9] Licha K and Olbrich C 2005 Optical imaging in drug discovery and diagnostic applications *J. Adv. Drug Deliv. Rev.* **57** 1087
- [10] Gurkov A, Sadovoy A, Shchapova E, Teh C, Meglinski I and Timofeyev M 2017 Micro-encapsulated fluorescent pH probe as implantable sensor for monitoring the physiological state of fish embryos *PLoS One* **12** e0186548
- [11] Borvinskaya E, Gurkov A, Shchapova E, Sadovoy S, Baduev B, Meglinski I and Timofeyev M 2017 Parallel *in vivo* monitoring of pH in gill capillaries and muscles of fishes using microencapsulated biomarkers *Biol. Open* **6** 673
- [12] Stelmashchuk O, Zhrebtsov E, Zhrebtsova A, Kuznetsova E, Vinokurov A, Dunaev A, Mamoshin A, Snimshchikova I, Borsukov A, Bykov A and Meglinski I 2017 Noninvasive control of the transport function of fluorescent coloured liposomal nanoparticles *Laser Phys. Lett.* **14** 65603
- [13] Gurkov A, Shchapova E, Bedulina D, Baduev B, Borvinskaya E, Meglinski I and Timofeyev M 2016 Remote *in vivo* stress assessment of aquatic animals with microencapsulated biomarkers for environmental monitoring *Sci. Rep.* **6** 36427
- [14] Sadovoy A, Teh C, Escobar M V, Corzh V and Meglinski I 2012 Micro-encapsulated bio-markers for assessment of stress conditions in aquatic organisms *in vivo* *Laser Phys. Lett.* **9** 542
- [15] Parakhonskiy B, Foss C, Carletti E, Fedel M, Haase A, Motta A, Migliaresi C and Antolini R 2013 Tailored intracellular delivery via a crystal phase transition in 400 nm vaterite particles *J. Biomater. Sci.* **1** 1273
- [16] De Geest B G, Sukhorukov G B and Möhwald H 2009 The pros and cons of polyelectrolyte capsules in drug delivery *J. Exp. Opin. Drug Deliv.* **6** 613