High sensitivity biosensor based on dual-peak LPG sensitised by light cladding etching

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ABSTRACT

We demonstrate a high sensitivity biosensor by fine tailoring mode dispersion and sensitivity of dual-peak LPGs using light-cladding-etching method. The etched device has been used to detect concentration of Hemoglobin protein in sugar solution, showing a sensitivity as high as 20nm/1%.

Keywords: Long-period grating, optical fibre sensors, chemical etching, biosensor

1. INTRODUCTION

Long-period fibre gratings (LPGs), as core to cladding mode coupling devices, have been used as band-rejection filters [1], EDFA gain flatteners [2] and optical sensors [3-6]. In comparison with fibre Bragg gratings, LPGs are much more sensitive to the variation of fibre properties and surrounding medium refractive index (SRI). To date, the majority reported work on LPGs employ typical structures with periods of $300-500\mu$ m, generating phase match resonances distributed in the range 1200-1600nm. The response of such LPGs can be modified by reducing cladding size via chemical etching [7-9]. It has also been revealed that there exists a set of dispersion turning points in LPG structures, resulting in, a set of conjugate cladding modes [5] which have been experimentally observed as dual-peak LPGs [10, 11]. The dual-peak feature is visible for LPGs with relative short period $\leq 150\mu$ m in the extended wavelength range from 900nm to 1700nm [6]. In close proximity to the dispersion turning point, the dual peaks are ultrasensitive to not just external perturbations but also fibre properties. This provides an effective fine-tuning mechanism to tailor the mode dispersion and sensitivity characteristics of dual-peak LPGs for applications.

In this paper, we report an investigation of spectral responses of dual-peak LPGs with reduced claddings realised by chemical etching using hydrofluoric (HF) acid. We experimentally monitored the evolution characteristics of dual resonant peaks, observing rapid transition of the dual-peak features from high order modes to lower ones. A light cladding etching (1% HF concentration) was then performed to finely tailor the sensitivity of the dual-peak LPG. This etched device was used to measure Hemoglobin protein concentrations in sugar solutions, showing a detection sensitivity as high as 20nm/ 1%.

2. EXPERIMENT

2.1. Spectral evolution of dual-peak LPGs with cladding etching

To produce dual-peak response, a set of LPGs with relatively small periods (140-160 μ m chosen using ref. 6) were UV-inscribed in hydrogen-loaded standard single mode fibre employing the point-by-point fabrication method and a CW frequency-doubled Ar laser. All the gratings were annealed at 80°C for 48hr to stabilise their optical property. Prior the etching, the spectra of these gratings were measured using a broadband light source and an optical spectrum analyser. Most of these LPGs showed one pair of conjugate resonances companied with a few lower order cladding modes on shorter wavelength side in range 900-1700nm

In order to effectively control the LPG etching process, we first investigated the etching rate using HF acid of 13% concentration and non grating-containing fibre samples. Fifteen fibre samples were immersed in the HF solution and were taken out in turn in every 5min. The samples with different etched claddings were then examined and measured

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using a microscope with high magnification. Fig. 1b plots the cladding radius against etching time, showing an etching rate of ~0.21 μ m/min. In following, a 20mm long dual-peak LPG with a period of 159 μ m was selected for etching experiment. As the first trace shown in Fig. 1a, this grating has four cladding modes present in the wavelength range from 900nm to 1700nm and two of which are a pair of conjugate modes located at 1214.9 nm and 1634.4 nm. Fro m our simulation, we identified them as LP_{010} , LP_{011} , and LP_{012} and LP'_{012} . When this grating was immersed in the HF acid, we monitored the spectrum *in-situ* and saw clearly a transition of generation, coalescence and annihilation of the dual-peak feature from higher order modes to lower ones. Fig. 1a shows the spectral evolution of this grating for the etching period of 67minutes. From the figure a repeating transition pattern is apparent with reducing cladding size : firstly, the dual peaks (LP_{012} and LP'_{012}) were moving towards each other, coalesced and eventually annihilated and a new pair of conjugate modes (LP_{011} and LP'_{011}) was generated companied by the red-shift of LP_{010} ; then this transition was repeated leading to the appearance of paired LP'_{010} and LP'_{010} , and LP'_{010} , modes.

Fig. 1c plots the experimentally measured wavelength shifts of the four modes versus the actual cladding size of the fibre. The dual-peak feature is also evident from Fig. 1c as LP_{010} , LP_{011} and LP_{012} mode curves are all parabolical. The coalescing points of the m=12, 11, 10 modes occurred at 1387.1 nm, 1385.7 nm and 1389.1 nm, corresponding to cladding radii of 61.8μ m, 55.9μ m and 48.5μ m, respectively. It is also noticed that the movements of the dual peaks are not linear and symmetric: the loss peak with longer wavelength moves faster than its counterpart. For example, the shift rates of each dual resonant peaks of m=11 mode are +88.7 nm/ μ m and -156.3 nm/ μ m when the cladding reduced from 57.1 μ m to 56.6 μ m, increasing to +240.5 nm/ μ m and -292.3 nm/ μ m for further cladding reduction from 56.6 μ m to 55.9 μ m. This nonlinear behaviour shows that the magnitude change of waveguide dispersion for each mode increases rapidly for wavelengths near the dispersion turning point. The simulation results, shown by lines in Fig.1c, agree quite well with experiment, especially for LP_{011} and LP_{012} .



Fig.1 (a) The spectral evolution of a dual-peak LPG of 159- m period during 67min etchingprocess; (b) The cladding radius against etching time; (c). The simulation (line) and experimental (symbol) results of resonance wavelength shift against cladding radius.

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2.2. Light cladding etching and SRI sensitivity characterisation

From above experiment we can see that the mode dispersion of dual-peak LPG is ultrasensitive to the cladding size. When the peaks are close to the dispersion turning point, ~1 μ m reduction of the cladding will result in ~ 250nm shift of the resonance. In order to finely control the mode dispersion and sensitivity of dual-peak LPGs, we performed a light etching experiment using HF acid of only 1% concentration. In this experiment, a 20mm-long LPG with 147 μ m period was subjected to etching for 96.5minutes, removing cladding thickness only by 0.9 μ m (from 62.5 μ m to 61.4 μ m, measured by the microscope). During the etching process, we also monitored the dual peak evolution *in-situ* and Fig. 2a plots the shifts of the dual peaks. The dual peaks were originally at M and M⁷ spaced by 493.6nm and finally moved to N and N⁷ separated by only 98.1nm. The sensitivity of this device was significantly enhanced by the light etching as the two peaks were in a much more close proximity to the dispersion tuning point.

The SRI sensitivity of the lightly etched dual-peak LPG was then investigated comparatively with an unetched device of the same grating parameters. The two gratings were immersed in a set of gels with refractive index ranging from 1 to 1.44 and the separation of the dual peaks was measured for each SRI value, as plotted in Fig. 2b. Clearly, the separation increases nonlinearly with increasing SRI, however, that is far larger for the lightly-etched device than for the non-etched one. For SRI varying from 1 to 1.44, the total separation between N and N^{\prime} is 373.9nm, whereas that between M and M^{\prime} is 185.4nm, only half of the former. This experiment clearly demonstrates that with appropriate etching, the dispersion property of LPG can be finely tailored to bring the dual peaks close to the dispersion turning point, realising ultrahigh SRI sensitivity devices.



Fig.2 (a) Dual peak wavelengths against etching time, showing the movement towards the dispersion tuning point; (b) SRI induced spectral separation of the dual peaks for etched (N, N) and unetched (M, M) gratings (note: the curves have been offset).

3. APPICATION

The lightly-etching dual-peak LPG was used to measure the concentration of the Hemoglobin in sugar solution. Firstly, we prepared a set of Hemoglobin solutions with concentrations from 0.0% to 1.0% (step 0.2%) by adding Hemoglobin into water. Then 5ml each of these solutions was drawn and added into six beakers, each beaker had 30g of 60% aqueous sugar solution. We then submerged the lightly-etched dual-peak LPG to these solutions in turn and measured the shifts of N-peak.

Fig. 3a shows the spectra of the N-peak under different solutions and Fig. 3b plots its central wavelength shift against Hemoglobin concentration. We can see when the Hemoglobin concentration changes from 0.0% to 1.0%, the peak red-shifts by 19.8nm Defining the concentration sensitivity as the shift induced by 1% Hemoglobin, we have a device sensitivity of ~20nm/1%. Thus, using a standard interrogation system with an optical resolution of 0.1nm, this finely tailored device could detect the Hemoglobin concentration change as small as 0.005%; a remarkably high detection sensitivity.

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Fig. 3 (a) Spectral evolution of N-peak of the lightly-etched dual-peak LPG with different Hemoglobin concentrations in sugar solutions; (b) N-peak shift against Hemoglobin concentration.

4. CONCLUSIONS

We have studied the mode dispersion and sensitivity characteristics of tailored dual-peak LPGs by cladding etching using high- and low-concentration HF acids. With decreasing cladding size, a transition of generation, coalescence and annihilation of dual-peak resonances from higher order modes to lower ones are revealed. The results clearly show that the mode dispersion of the dual-peak LPG is ultrasensitive to the cladding size and thus light-cladding-etching can effectively enhance or finely tailor the sensitivity of the devices. As an implementation of an optical biosensor, we have used the lightly-etched dual-peak LPG to measure Hemoglobin concentrations in sugar buffer solution, demonstrating a concentration sensitivity of ~20nm/1%. This value indicates that this device has a potential capability to detect protein concentration change as small as 0.005%, which should be enormously attractive for biochemical, medical and environmental sensing applications.

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